

Image Processing tutorials with python

Yann Gavet & Johan Debayle

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Image Processing tutorials with python

Yann Gavet & Johan Debayle

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Table of Contents

First part

Enhancement and Restoration

1 Introduction to image processing 11
2 Image Enhancement 23
3 2D Fourier Transform 31
4 Introduction to wavelets 37
5 Image restoration: denoising 49
6 Image Restoration: deconvolution 59
7 Shape From Focus 71
8 Logarithmic Image Processing (LIP) 79
9 Color LIP 85
10 GANIP 93
11 Image Filtering using PDEs 103
12 Multiscale Analysis 111
13 Introduction to tomographic reconstruction 119

Second part

Mathematical Morphology

14 Binary Mathematical Morphology 127
15 Morphological Geodesic Filtering 135
16 Morphological Attribute Filtering 141
17 Morphological skeletonization 145
18 Granulometry 151

Third part

Registration and Segmentation

19 Histogram-based image segmentation 159
20 Segmentation by region growing 167
21 Hough transform and line detection 173
22 Active contours 179
23 Watershed 185
24 Segmentation of follicles 191
25 Image Registration 195

Fourth part

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Stochastic Analysis

26 Stochastic Geometry / Spatial Processes 207
27 Boolean Models 219
28 Geometry of Gaussian Random Fields 225
29 Stereology and Bertrand's paradox 231
30 Convex Hull 243
31 Voronoï Diagrams and Delaunay Triangulation 249

Fifth part

Image Characterization and Pattern Analysis

32 Integral Geometry 257
33 Topological Description 263
34 Image Characterization 267
35 Shape Diagrams 273
36 Freeman Chain Code 279
37 Machine Learning 287
38 Harris corner detector 293
39 Local Binary Patterns 297

Sixth part

Exams

40 Practical exam 2016 305
41 Theoretical exam 2016 307
42 Theoretical exam 2017 309

Index 311
Bibliography 313

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Liminar considerations

This book is presented as a collection of tutorials. Each chapter presents different objectives, usually with practical applications, in order to develop the image processing and analysis skills by its own. For each tutorial, you will first find in the statement different questions that will guide you to the complete results. Our suggestion is to start by the first tutorials, that acts as a round-up stage. Then, choose the topic that interests and motivates you, and start to work on your code.

The statements does not always contain the necessary theoretical background that you need to answer to the questions. Find resources on the net. Wikipedia is usually a very good start. Go to the university library!

The correction gives you a proposition of solution: it is not unique and it might not be perfect (or it might unfortunately contain errors). This correction is also available in a dedicated website (links will be provided along with the tutorials), we suggest you have a look at it only when you encounter blocking problems or fastidious lines of code to program. Moreover, you can evaluate the processing time of your version of the code and compare it to our proposed version, which usually uses fast and optimal functions, except for readibility purposes.

With Python, you can use the following code:

```python
import time

time_start = time.clock()
# run your code
time_elapsed = (time.clock() -time_start)
```

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If you manage to code a drastically faster method, if you notice errors or mistakes, if you want to add precisions, remember that this book as well as the code is published under a FREE CC-BY license (as in FREE speech). Contact us and we will be really happy to introduce modifications and insert you in the credits, or more...

The book is available in a high quality printed format, obviously not for free, but the pdf format is free (as in FREE beer). This is due to the fact that we (Johan Debayle and Yann Gavet) are employed by the French government, and we are paid to teach and disseminate informations to students. Our work is thus belongs to the society, and it seems a normal process to give the results back to the society. Feel free to use, modify and distribute these tutorials as you wish. Just remember to keep the appropriate credits (our names and MINES Saint-Etienne). If you want to express your gratitude, send us a postcard at:

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```

You can also buy the printed version of the book, which will make our editor really happy.

Images

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Softwares

This book is available for two programming languages, MATLAB® and Python. MATLAB® is a proprietary software dedicated to scientific computing. Functions are grouped into so-called toolboxes. The documentation and the compatibility of the functions are very good, but the price is a consequence of this. Python is built upon open-source and Free softwares. Scientific modules are numerous, but other general purposes functions can also be found. Documentation and code may be of inequal qualities, but major scientific modules (numpy, scipy, opencv...) are really well presented and optimized.

Portions of code will be highlighted by the use of special boxes, like:

```python
# this is python code
```

Time to spend on a tutorial

The tutorials are almost independent. To evaluate the difficulty of the tutorial, stars are present at the header of each one. Depending on your knowledge, you will have to spend between 2 hours and 10 hours per tutorial.

- One star tutorial should be a relatively easy tutorial,
- two stars tutorials introduce some difficulties, either in programming or in the theoretical concepts,
- three stars tutorials are difficult both in theory and in programming.

They are divided into 6 parts, namely:

- Enhancement and Restoration: dedicated to image processing methods employed to eliminate noise and improve vision of data.
- Mathematical Morphology: introduction to basic operations of mathematical morphology.
- Registration and Segmentation: methods to segment, i.e. detect objects in images.
- Stochastic Analysis: method based on random processes.
- Characterization and Pattern Analysis: measures performed on objects in order to perform analysis and recognition.
- Exams: uncorrected problems and questions.

Enjoy!

You will find online corrections on the editor website and at page: http://www.iptutorials.science. You will also find qrcodes for each correction that points to code and images.

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First part

Enhancement and Restoration

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1 Introduction to image processing

In this tutorial, you will discover the basic functions in order to load, manipulate and display images. The main informations of the images will be retrieved, like size, number of channels, storage class, etc. Afterwards, you will be able to perform your first classic filters.

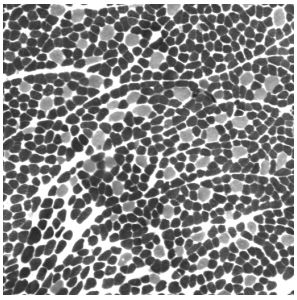
The different processes will be realized on the following images:

Figure 1.1 Image examples.

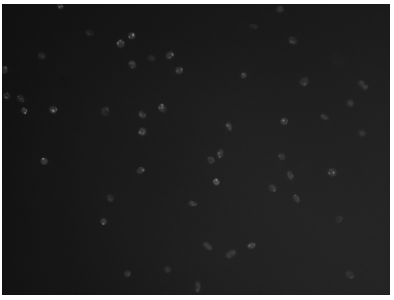
(a) Retinal vessels.



(b) Muscle cells.



(c) Cornea cells (BIIGC, Univ. Jean Monnet, Saint-Etienne, France).



1.1 First manipulations



Image loading can be made by the use of the python function `imageio.imread`. The visualization of the image in the screen is realized by using the module `matplotlib.pyplot`.

>>>?

- Load and visualize the first image as below. Notice the differences.
- Look at the data structure of the image I such as its size, type....
- Visualize the green component of the image. Is it different from the red one? What is the most contrasted color component? Why?
- Enumerate some digital image file formats. What are their main differences? Try to write images with the JPEG file format with different compression ratios (0, 50 and 100), as while as the lossless compression, and compare.

1.2 Color quantization

Color quantization is a process that reduces the number of distinct colors used in an image, usually with the intention that the resulting image should be as visually similar as possible to the original image. In principle, a color image is usually quantized with 8 bits (i.e. 256 gray levels) for each color component.

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>>>?

- By using the gray level image 'muscle', reduce the number of gray levels to 128, 64, 32, and visualize the different resulting images.
- Compute the different image histograms and compare.

1.3 Image histogram

An image histogram represents the gray level distribution in a digital image. The histogram corresponds to the number of pixels for each gray level.

The python function has the following prototype:

```python
def histogram(I):
```

>>>?

Compute and visualize the histogram of the image 'muscle.jpg'.

1.4 Linear mapping of the image intensities

The gray level range of the image 'cellules_cornee.jpg' can be enhanced by a linear mapping such that the minimum (resp. maximum) gray level value of the resulting image is 0 (resp. 255). Mathematically, it consists in finding a function $f(x) = ax + b$ such that $f(min) = 0$ and $f(max) = 255$.

>>>?

- Load the image and find its extremal gray level values.
- Adjust the intensities by a linear mapping into $[0, 255]$.
- Visualize the resulting image and its histogram.

1.5 Aliasing effect

>>>?

- Create an image (as right) that contains rings as sinusoids. The function takes two input parameters: the sampling frequency and the signal frequency.
- Look at the influence of the two varying frequencies. What do you observe? Explain the phenomenon from a theoretical point of view.

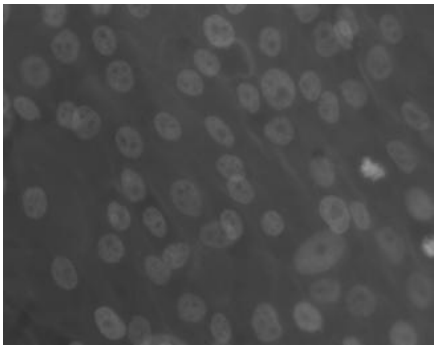


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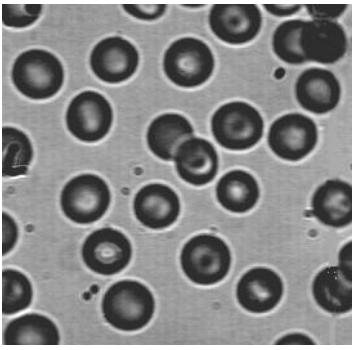
1.6 Low-pass filtering

The different processes will be realized on the following images:

(a) osteoblast cells



(b) blood cells



Low-pass filtering aims to smooth the fast intensity variations of the image to be processed.

>>>?

Test the low-pass filters 'mean', 'median', 'min', 'max' and 'gaussian' on the noisy image 'blood cells'.



The module `scipy.ndimage.filters` contains a lot of classical filters.

>>>?

Which filter is suitable for the restoration of this image?

1.7 High-pass filtering

High-pass filtering aims to smooth the low intensity variations of the image to be processed.

>>>?

- Test the high-pass filters HP on the two initial images in the following way: $HP(f) = f - LP(f)$ where LP is a low-pass filtering (see the previous exercise).
- Test the Laplacian (high-pass) filter on the two initial images with the following convolution mask:

$$\begin{bmatrix} -1 & -1 & -1 \\ -1 & +8 & -1 \\ -1 & -1 & -1 \end{bmatrix}$$

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1.8 Derivative filters

Derivative filtering aims to detect the edges (contours) of the image to be processed.

>>>?

- Test the Prewitt and Sobel derivative filters (corresponding to first order derivatives) on the image 'blood cells' with the use of the following convolution masks:

$$\begin{bmatrix} -1 & 0 & +1 \\ -1 & 0 & +1 \\ -1 & 0 & +1 \end{bmatrix} \begin{bmatrix} -1 & -1 & -1 \\ 0 & 0 & 0 \\ +1 & +1 & +1 \end{bmatrix}$$

$$\begin{bmatrix} -1 & 0 & +1 \\ -2 & 0 & +2 \\ -1 & 0 & +1 \end{bmatrix} \begin{bmatrix} -1 & -2 & -1 \\ 0 & 0 & 0 \\ +1 & +2 & +1 \end{bmatrix}$$

- Look at the results for the different gradient directions.
- Define an operator taking into account the horizontal and vertical directions.

Remark : the edges could be also detected with the zero-cressings of the Laplacian filtering (corresponding to second order derivatives).

1.9 Enhancement filtering

Enhancement filtering aims to enhance the contrast or accentuate some specific image characteristics.

>>>?

- Test the enhancement filter E on the image 'osteoblast cells' defined as: $E(f) = f + HP(f)$ where HP is a Laplacian filter (see tutorial 2.).
- Parameterize the previous filter as: $E(f) = \alpha f + HP(f)$, where $\alpha \in \mathbb{R}$.

1.10 Open question

Find an image filter for enhancing the gray level range of the image 'osteoblast cells'.

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1.11. Python correction

```python
# display images
import matplotlib.pyplot as plt
# ndimage defines a few filters
from scipy import misc, ndimage
# numeric calculation
import numpy as np
# measure time
import time
# read and save images
import imageio
```

1.11.1 First manipulations

Open, write images

The following file loads the ascent image and display it. The `print` function is optional.

```python
# load file ascent
ascent = misc.ascent()
# load file cerveau.jpg
brain = imageio.imread('cerveau.jpg')
print(type(brain))
print(brain.shape, brain.dtype)
# save file
imageio.imwrite('test.png', brain)
```

Display images

You can modify to previous example to add the following lines:

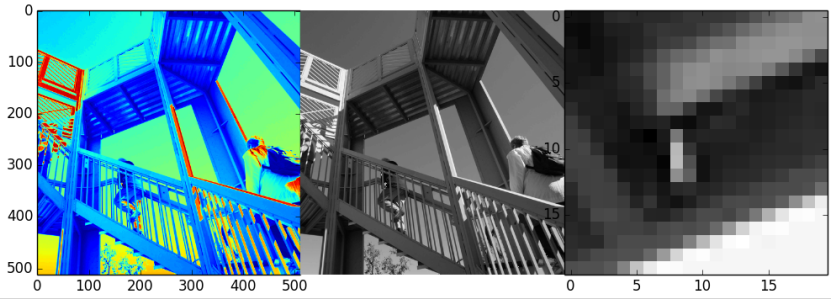
```python
plt.imshow(ascent)
plt.show()
```

Notice that you have to close the image window to write commands again. Also, the colormap is not the good one by default (see Fig. 1.2).

```python
plt.figure(figsize=(10, 3.6))
# first subplot
plt.subplot(131)
plt.imshow(ascent)
# second subplot
plt.subplot(132)
plt.imshow(ascent, cmap=plt.cm.gray)
plt.axis('off')
# third subplot (zoom)
plt.subplot(133)
plt.imshow(ascent[200:220, 200:220], cmap=plt.cm.gray, interpolation='nearest')
plt.subplots_adjust(wspace=0, hspace=0.,
                top=0.99, bottom=0.01,
                left=0.05, right=0.99)
plt.show()
```

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Figure 1.2 Displaying images with an adapted colormap.



Color channels

A color image is constituted of (generally) three channels. This representation follows the human visual perception principles: in the human retina, the sensitive cells (the cones) react to specific wavelength that correspond to red, green and blue. The sensors technology adopted the *same* characteristics and a so-called Bayer filter has 2 green filters for 1 red and 1 blue. Consequently, the green channel presents a better resolution than the other channels.

Figure 1.3 The green channel presents the best contrasts in the case of retina images.

(a) Color image. **(b)** Red channel. **(c)** Green channel **(d)** Blue channel.



Image Resizing

The number of pixels is reduced by subsampling the image. Notice that there is no anti-aliasing filter applied to the image before reducing its size. The result is presented in Fig.1.4 with images of the same size, and in Fig.1.5 with images at the same resolution.

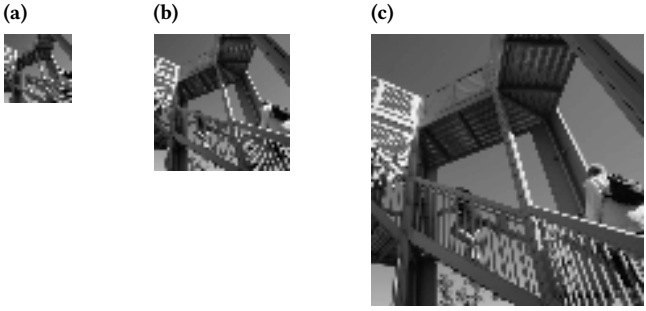
Figure 1.4 Reduction of the scale of the image on each axis, showing a so-called *pixellisation* effect. Represented at the same size, the density of pixels is thus reduced.

(a) Scale divided by 20. **(b)** Scale divided by 10. **(c)** Scale divided by 5.



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Figure 1.5 At a constant resolution, images with different definitions are represented with different sizes.



Color quantization

The following code uses the properties of integer operations to round values to the nearest integer. Illustration is presented Fig. 1.6.

```
q4 = ascent // 4*4;
q16= ascent //16*16;
q32= ascent //32*32;
```

Figure 1.6 Reduction of the number of gray levels (quantization).

(a) q4. **(b)** q16. **(c)** q32.



JPEG file format

In order to test the effect of jpeg compression, one can use the parameter `quality`. For the lowest quality, the loss of informations is really important (see Fig.1.7).

```
# test jpeg quality
imageio.imwrite("a_25.python.jpeg", ascent, quality=25);
imageio.imwrite("a_100.python.jpeg", ascent, quality=100);
imageio.imwrite("a_50.python.jpeg", ascent, quality=50);
imageio.imwrite("a_75.python.jpeg", ascent, quality=75);
imageio.imwrite("a_1.python.jpeg", ascent, quality=1);
```

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Figure 1.7 Different quality used to compress jpeg files.

(a) Quality 1. **(b)** Quality 25. **(c)** Quality 75.

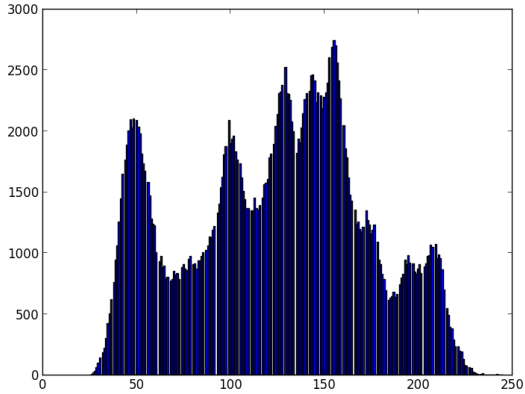


1.11.2 Histogram

To plot the histogram of an image, you can use the hist function (see result in Fig. 1.8).

```
plt.hist(ascent.flatten(), 256)
plt.show()
```

Figure 1.8 Histogram of ascent image.



You can also write your own code. The execution time is higher for these two functions than for the previous one.

```
# Histogram function with 2D image
def compute_histogram(image):
    tab = np.zeros((256, ), dtype='I')
    X, Y = image.shape
    for i in range(X):
        for j in range(Y):
            tab[image[i,j]]+=1

    return tab
```

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```python
# Histogram function with flatten image (vector)
def compute_histogram2(image):
    im = image.flatten()
    tab = np.zeros((256, ), dtype='I')
    for i in im:
        tab[i]+=1
    return tab
```

The following code presents a comparison of the different method for histogram computation.

```python
# load ascent image and compute histograms
ascent = misc.ascent()
t0 = time.clock()
h = compute_histogram(ascent)
t1 = time.clock()
h2=compute_histogram2(ascent)
t2 = time.clock()
# .... plots
print "execution time 2D:%g" %(t1-t0)
plt.subplot(131)
plt.plot(h)
plt.title('2D function')

print "execution time 1D:%g" %(t2-t1)
plt.subplot(132)
plt.plot(h2)
plt.title('1D function')
# last plot: with matplotlib function
plt.subplot(133)
t3 = time.clock()
plt.hist(ascent.flatten(), 256)
t4 = time.clock()
print "execution time matplotlib:%g" %(t4-t3)
# display
plt.show()
```

The console outputs the following computation durations:

```
execution time 2D: 1.40284 s
execution time 1D: 1.27649 s
execution time matplotlib: 0.261095 s
```

1.11.3 Linear mapping of the image intensities

The linear mapping is a simple method that stretches linearly the histogram. If displayed with `matplotlib`, the images is linearly stretched, thus the modification cannot be observed.

```python
def image_stretch(image):
   # return image with new maximum and minimum at 255 and 0
   minimum = image.min();
   maximum = image.max();
   a = 255/(maximum-minimum);
   b = -255*minimum/(maximum-minimum);
   return a*image+b;
```

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1.11.4 Aliasing effect

```python
# aliasing effect (Moire)
def circle(fs, f):
    # Generates an image with aliasing effect
    # fs: sample frequency
    # f : signal frequency
    t = np.arange(0,1,1./fs);
    ti,tj = np.meshgrid(t,t);
    C = np.sin(2*np.pi*f*np.sqrt(ti**2+tj**2));
    return C
```

The image of Fig. 1.9 is generated with the following code.

```python
C = circle(300,50);
plt.imshow(C, cmap=plt.cm.gray);
plt.show()
imageio.imwrite('moire.png', C);
```

Figure 1.9 Moiré effect, generated with $f_s = 300$ and $f = 50$.



1.11.5 Low-pass filtering

The module `scipy.ndimage.filters` contains the usual filter functions.

The mean filter is illustrated in Fig. 1.10.

```python
# mean on a 3x3 neighborhood
m3 = ndimage.filters.uniform_filter(ascent)
m25= ndimage.filters.uniform_filter(ascent, 25)

plt.subplot(121)
```

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```
plt.imshow(m3, cmap=plt.cm.gray)
plt.axis('off')
plt.title('3x3 mean filter')

plt.subplot(122)
plt.imshow(m25, cmap=plt.cm.gray)
plt.axis('off')
plt.title('25x25 mean filter')

plt.show()
```

Figure 1.10 Mean filters.

(a) Neighborhood of size 3x3.



(b) Neighborhood of size 25x25.



Gaussian filter

The gaussian filter is presented in Fig. 1.11.

```
# ascent image
ascent = misc.ascent()

# Gaussian filter
gaussian = ndimage.filters.gaussian_filter(ascent, 5)
```

Figure 1.11 Gaussian filter of size 5.



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1.11.6 Derivative filters

Derivative filters (Prewitt, Sobel...) use a finite derivation approximation. They are very sensitive to noise (as every system using a derivation). The gradient is defined as a vector, and a norm should be used to display a resulting image. Notice that with these filters, the connexity of the contours is not preserved. Illustration is proposed in Fig. 1.12.

```python
# ascent image
ascent = misc.ascent()
ascent.astype('int32');

# Prewitt filter
prewitt0 = ndimage.filters.prewitt(ascent, axis=0)
prewitt1 = ndimage.filters.prewitt(ascent, axis=1)

# Sobel filter
dy = ndimage.filters.sobel(ascent, axis=0) # vertical
dx = ndimage.filters.sobel(ascent, axis=1) # horizontal
mag = np.hypot(dx, dy) # magnitude
sobel = mag * 255.0 / mag.max() # normalize (Q&D)

# display results
plt.subplot(131)
plt.imshow(prewitt0, cmap=plt.cm.gray)
plt.axis('off')
plt.title('Prewitt filter axis 0')

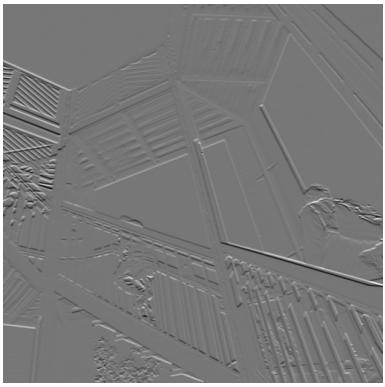
plt.subplot(132)
plt.imshow(prewitt1, cmap=plt.cm.gray)
plt.axis('off')
plt.title('Prewitt filter axis 1')

plt.subplot(133)
plt.imshow(sobel, cmap=plt.cm.gray)
plt.axis('off')
plt.title('Sobel filter')

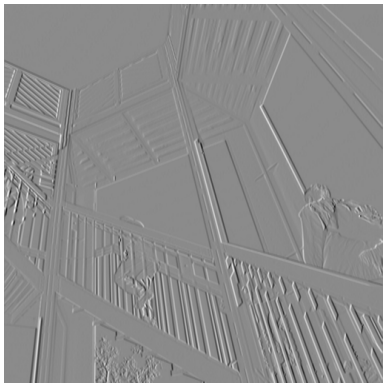
plt.show()
```

Figure 1.12 Prewitt filter.

(a) Prewitt filter for axis x.



(b) Prewitt filter for axis y.



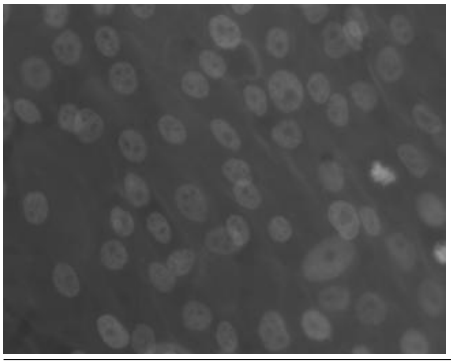
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2 Image Enhancement

The objective of this tutorial is to implement some image enhancement methods, based on intensity transformations or histogram modifications. It will make use of statistical notions like probability density functions or cumulative distribution functions.

Figure 2.1 The different processes of this tutorial will be applied on these images.

(a) Osteoblasts.



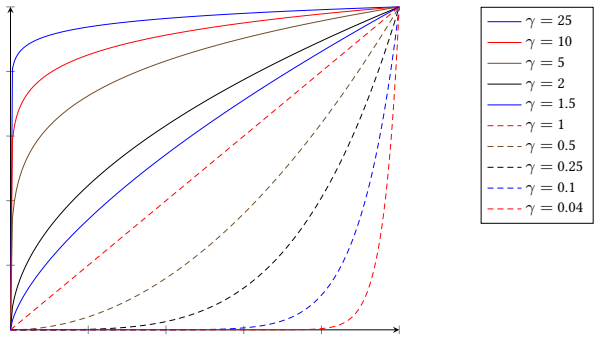
(b) Phobos (ESA/DLR/FU Berlin, CC-By-SA).



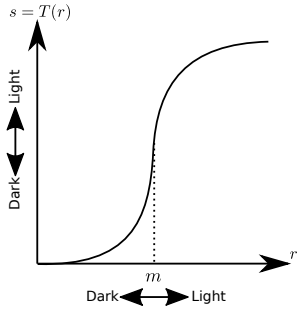
2.1 Intensity transformations (LUT)

Two transformations will be studied: the γ correction and the contrast stretching. They enable the intensity dynamics of the gray tone image to be changed. These two operators are based on the following Look Up Tables (LUT):

(c) γ correction LUT.



(d) Contrast stretching LUT.



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>>>?

1. Test the transformation 'γ correction' on the image 'osteoblast'.
2. Implement the operator 'contrast stretching' with the following LUT (also called cumulative distribution function cdf), with m being the mean gray value of the image, and r being a given gray value:

$$s = T(r) = \frac{1}{1 + (m/r)^E}$$

3. Test this transformation with different values of E on the image 'osteoblast'.



The module `skimage.exposure` contains different methods for contrast enhancement, among them `adjust_gamma`.

2.2 Histogram equalization

The objective is to transform the image so that its histogram would be constant (and its cumulative distribution function would be linear). The notations are:

- I is the image of n pixels, with intensities between 0 and L.
- h is the histogram, defined by:

$$h_I(k) = p(x = k) = \frac{n_k}{n}, \quad 0 \leq k < L$$

The following transformation $T(I)$ is called histogram equalization.

$$T(x_k) = (L-1) \sum_{j=0}^{k} p(x_j)$$

where

$$\mathrm{cdf}_I(k) = \sum_{j=0}^{k} p(x_j)$$

is the cumulative distribution function (cumulative histogram).

>>>?

1. Compute and visualize the histogram of the image 'osteoblast'.
2. Test this histogram equalization transformation on the image 'osteoblast' (with builtin functions) and visualize the resulting histogram.
3. Code your own function.
4. The corresponding LUT to this transformation is the cumulative sum of the normalized histogram. Evaluate and visualize this intensity transformation.



See the `numpy.histogram` and `skimage.exposure` functions.

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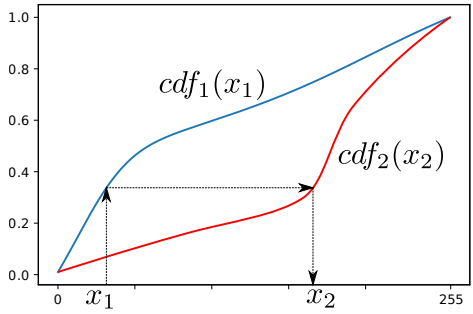
2.3 Histogram matching

The objective is to enhance the original image by matching its histogram with a modeled one. The principle is to transform the gray value x_1 of first image into x_2: $T(x_1) = x_2$ (see Fig.2.2). Based on the fact that $\mathrm{cdf}_1(x_1) = \mathrm{cdf}_2(x_2)$, the formula to find x_2 is:

$$x_2 = \mathrm{cdf}_2^{-1}\left(\mathrm{cdf}_1(x_1)\right).$$

As x_1 and x_2 are discrete values, this requires an interpolation.

Figure 2.2 Histogram matching principle.



>>>?

1. Visualize the histogram of the image 'phobos'.
2. Make the histogram equalization and visualize the resulting image.
3. Construct a bi-modal histogram (for example) and code your own function for histogram matching.



See `numpy.interp` for interpolation and LUT application.

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2.4. Python correction

```python
from scipy import misc
import matplotlib.pyplot as plt
from skimage import exposure
import numpy as np
import sys
```

2.4.1 Intensity transformations

γ correction

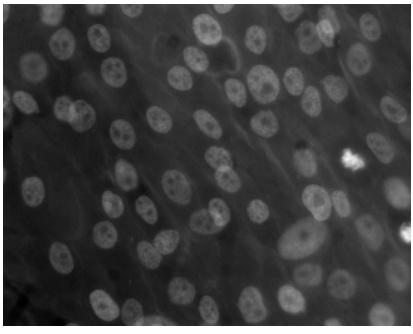
The function `skimage.exposure.adjust_gamma` is used in order to adjust the gamma of the image. It is before normalized (values are float between 0 and 1). The results are illustrated in Fig.2.3.

```python
I=imageio.imread("osteoblaste.png")
I = I / np.max(I);

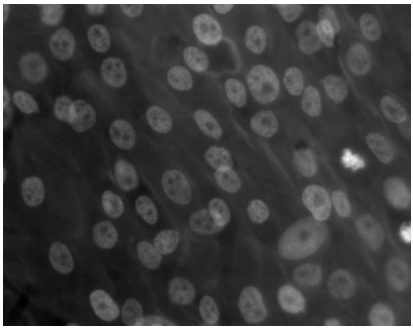
gamma=2;
I2= exposure.adjust_gamma(I, gamma);
plt.imshow(I2);
plt.show();
```

Figure 2.3 Gamma transforms.

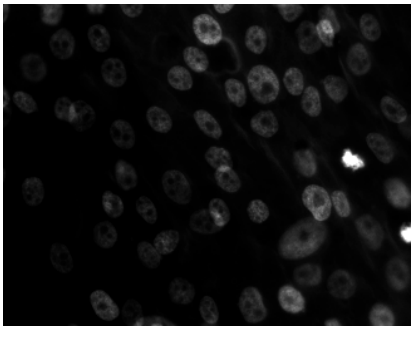
(a) Original image.



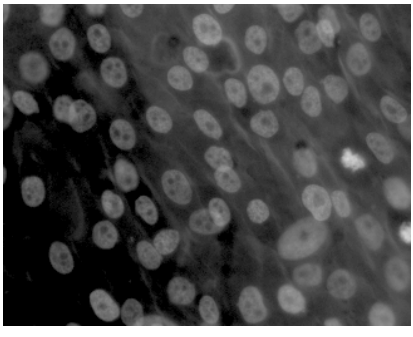
(b) $\gamma = 1$.



(c) $\gamma = 2$.



(d) $\gamma = 0.5$.



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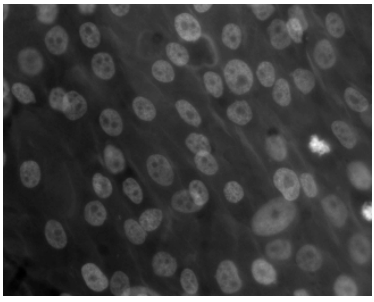
Contrast stretching

The LUT look-up-table is simply a function applied to the original image. In order to avoid division by zero, the smallest float value is introduced. Fig.2.4 illustrates the results.

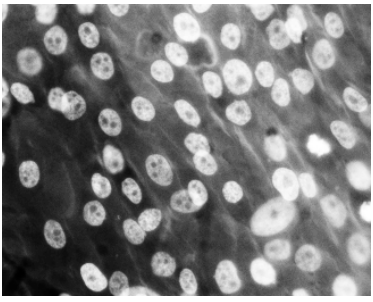
```python
def contrast_stretching(I, E):
    epsilon = sys.float_info.epsilon;
    m = np.mean(I);
    I = I.astype("float");
    Ar = 1. / (1.+(m/(I+epsilon))**E);
    return Ar;
```

Figure 2.4 Constrast stretching.

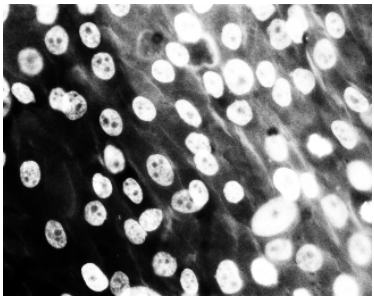
(a) Original image.



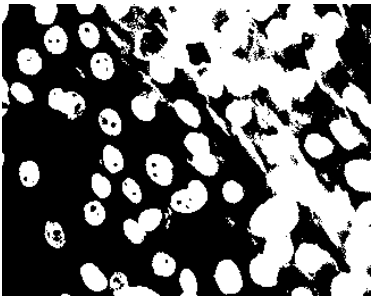
(b) $E = 10$.



(c) $E = 20$.



(d) $E = 1000$.



2.4.2 Histogram equalization

The histogram is displayed with the following function:

```python
def displaySaveHisto(I, filename=None):
    """
    Display and save pdf (if filename provided) of histogram of image I
    If values are between 0 and 1, they are multiplied by 255
    """
    if np.max(I)<=1:
        I = 255 * I;
    hist,bins = np.histogram(I.flatten(), 256, range=(0,255))
    fig = plt.figure()
    plt.bar(bins[:-1], hist, width=1);
    plt.show();
    if filename!=None:
        fig.savefig(filename, bbox_inches='tight')
```

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The histogram equalization is done via the `skimage.exposure.equalize_hist` function. The results are illustrated in Fig.2.5.

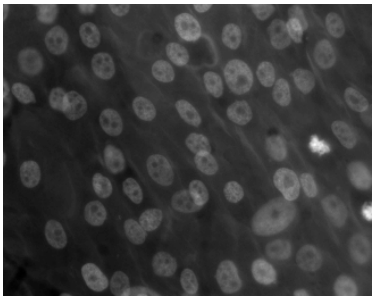
```
# histogram equalization
I2 = exposure.equalize_hist(I);
plt.imshow(I2);
plt.show()
```

The look-up-table (LUT) or cumulative distribution function (cdf) is computed and used in the next function:

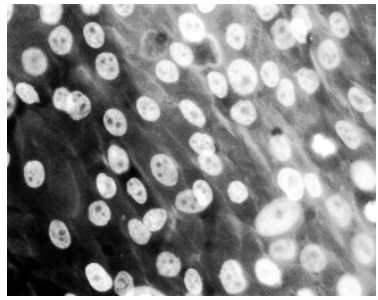
```
def histeq(I):
    """
    histogram equalization, version with look-up-table
    I: original image, with values in 8 bits integer
    """
    hist,bins=np.histogram(I.flatten(), 256, range=(0,255))
    cdf = hist.cumsum();
    cdf = (cdf / cdf[-1]);
    return cdf[I];
```

Figure 2.5 Histogram equalization.

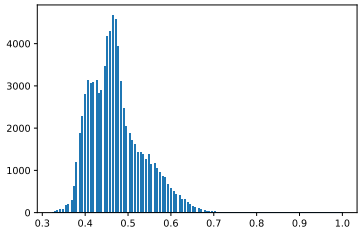
(a) Original image.



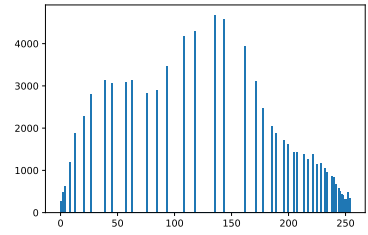
(b) Histogram equalization.



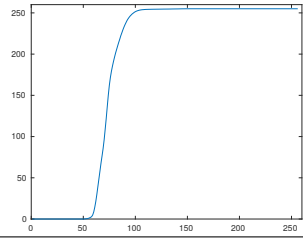
(c) Histogram of original image.



(d) Histogram after equalization.



(e) LUT (cumulative distribution function).



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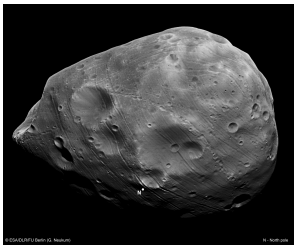
2.4.3 Histogram matching

This method is only an approximate method. It requires an interpolation of the cumulative distribution functions in order to find the transformation. Results are shown in Fig.2.6

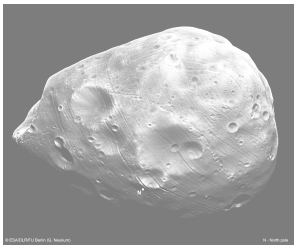
```python
def hist_matching(I, cdf_dest):
    """
    Histogram matching of image I, with cumulative histogram cdf_dest
    This should be normalized, between 0 and 1.
    This version uses interpolation
    """
    imhist,bins = np.histogram(I.flatten(), len(cdf_dest), density=True)
    cdf = imhist.cumsum() #cumulative distribution function
    cdf = (cdf / cdf[-1]) #normalize between 0 and 1
    # first: histogram equalization
    im2 = np.interp(I.flatten(), bins[:-1], cdf)
    # 2nd: reverse function
    im3 = np.interp(im2, cdf_dest, bins[:-1])
    # reshape into image
    imres = im3.reshape(I.shape)
    return imres;
```

Figure 2.6 Histogram matching.

(a) Original image.



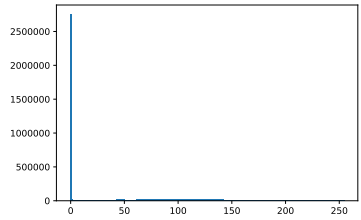
(b) Histogram equalization.



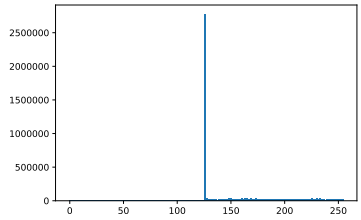
(c) Histogram matching.



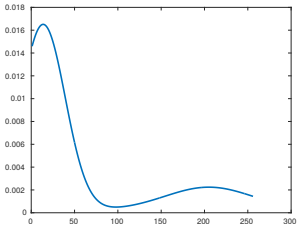
(d) Histogram of original image.



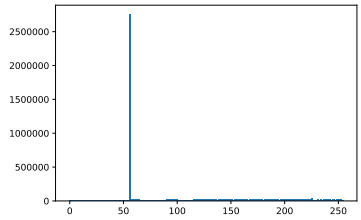
(e) Histogram after equalization.



(f) Target histogram (cumulative distribution function).



(g) Histogram after histogram matching.



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3 2D Fourier Transform

The main objective of this tutorial is to study image filters applied in the frequencial or spatial domain with the Fourier transform.

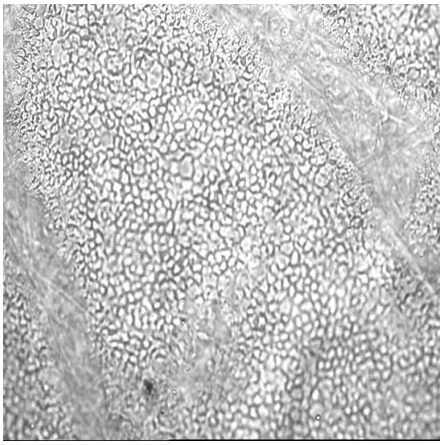


Use module `np.fft` for Fourier Transform functions (function `fft2`), `phase` and `abs` for phase and amplitude.

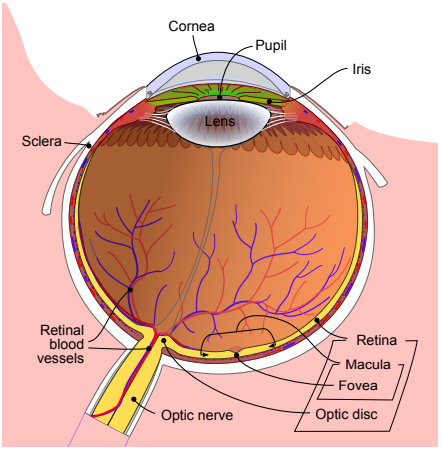
The image to be used comes from a human cornea endothelium observed ex vivo by optical microscopy.

Figure 3.1 Image of human cornea endothelium observed by optical microscopy. The ophthalmologists would like to know the cell density, without manually counting all the cells.

(a) Human corneal endothelium, extracted from a donor and observed here before grafting.



(b) Human eye (from Wikipedia, authors: Rhcastilhos and Jmarchn, CC-By-SA).



3.1 Fourier transform

>>>?

1. Load an image and visualise it.
2. Compute the Fourier Transform by the fft algorithm.
3. Visualise the images of the phase and amplitude of the Fourier Transform.

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3.2 Inverse Fourier transform

In this exercise, it can be interesting to consider different images, like a Lena picture for example.

>>>?

1. Apply the inverse Fourier transform on the Fourier transform to find the original image.
2. Now, apply the inverse Fourier transform on the phase information only (without using the frequency informations).
3. In a same spirit, apply the inverse Fourier transform on the frequency informations only (without the phase).

3.3 Low-pass and high-pass filtering

>>>?

1. Modify the Fourier transform of the image to
   - keep only low frequencies,
   - keep only high frequencies.
2. Apply the inverse Fourier transform on both and comment.

3.4 Application: evaluation of cellular density

The ophthalmologists would like to evaluate the cell density of the cornea endothelium observed in Fig. 3.1.

>>>?

1. Compute the Fourier transform of the image. If one considers that the cells constitute a repeated pattern on the whole image, locate the repetition frequency on the amplitude image.
2. Can this frequency be linked to the cell density ?

The answer to this last question is obviously yes. Here follows a simple method to evaluate the cell density (or the mean cell radius), if these cells a considered as circular [37].

>>>?

1. The amplitude information is very noisy. First of all, a gaussian filter should be applied (see functions `fspecial` and `imfilter`).
2. Find a simple way to evaluate the mean radius of the cells.

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3.5. Python correction

```python
import numpy as np
from scipy import misc, ndimage #read/write images
import matplotlib.pyplot as plt # plots
```

3.5.1 Introduction and utilities

To display a spectrum, the following function can be useful:

```python
# Displays spectrum and phase in an image (grayscale)
def viewSpectrumPhase(amplitude, phase):
    plt.figure()
    plt.subplot(1,2,1)
    plt.imshow(np.log(1+amplitude), plt.cm.gray);

    plt.subplot(1,2,2)
    mmax = np.max(phase);
    mmin = np.min(phase);
    if (mmax == mmin):
        B=0;
    else:
        B = 255*(phase-mmin)/(mmax-mmin);

    plt.imshow(B, cmap=plt.cm.gray);
```

3.5.2 Fourier transform

Results (amplitude and phase) are represented in Fig. 3.4.

```python
cornea = imageio.imread('cornee.png')
print type(cornea)
print cornea.shape, cornea.dtype

plt.subplot(131)
plt.imshow(cornea, cmap=plt.cm.gray)
```

```python
## Fourier transform
# result is complex
# fftshift is used by convention the get frequency 0 at center of image
spectre = np.fft.fftshift(np.fft.fft2(cornea));

A = abs(spectre);
G = np.angle(spectre);

viewSpectrumPhase(A, G);
```

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3.5.3 Inverse Fourier Transform

```
## inverse Fourier transform
cornee2 = np.real(np.fft.ifft2(np.fft.fftshift(spectre)));
plt.figure()
plt.imshow(cornee2, cmap=plt.cm.gray);
plt.title('inverse FT');
```

The Fourier transform, although very powerful, is really difficult to interpret in 2D. The main information is not contained in the amplitude, but in the phase. The following reconstructions will illustrate it (see Fig.3.2).

```
## inverse Fourier transform, without the phase
cornee_amplitude= np.real(np.fft.ifft2(np.fft.fftshift(A)));
plt.figure();
plt.imshow(cornee_amplitude, cmap=plt.cm.gray);
plt.title('inverse FT on amplitude');
```

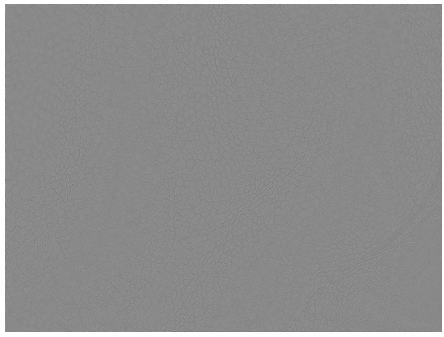
```
## inverse Fourier transform on phase only
complex_phase = np.exp(1j*G);
cornee_phase=np.real(np.fft.ifft2(np.fft.fftshift(complex_phase)));
plt.figure()
plt.imshow(cornee_phase, cmap=plt.cm.gray);
plt.title('inverse FT on phase');
```

Figure 3.2 Reconstruction of partial informations (phase or amplitude only).

(a) Reconstruction with amplitude only.



(b) Reconstruction with phase only.



3.5.4 Low-pass and high-pass filtering

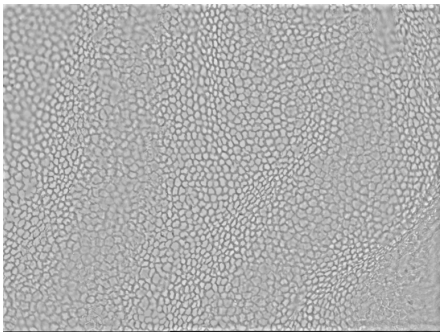
The results are illustrated in Fig. 3.3. Two functions are defined.

A low pass-filter consists in the suppression of values for frequencies lower than a cut-off frequency.

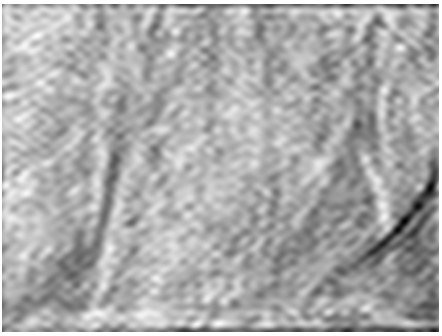
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Figure 3.3 Fourier basic filtering of cornea image.

(a) High Pass filter.



(b) Low Pass filter.



```python
def LowPassFilter(spectrum, cut):
    """Low pass filter of the FFT (spectrum)
    The shape of this filter is a square. fftshift has been applied so that
    frequency 0 lays at center of spectrum image
    @param spectrum: FFT2 transform
    @param cut : cut value of filter (no physical unit, only number of pixels)
    """
    X,Y = spectrum.shape;
    mask = np.zeros((X,Y), "int");
    mx = X/2; my = Y/2;
    mask[mx-cut:mx+cut, my-cut:my+cut] = 1;
    f = spectrum * mask;
    plt.figure
    plt.imshow(abs(f)); plt.title('Low pass filter')
    return f;
```

A high pass filter is exactly the opposite: suppression of the values under the cut-off frequency.

```python
def HighPassFilter(spectrum, cut):
    """High pass filter of the FFT (spectrum)
    The shape of this filter is a square. fftshift has been applied so that
    frequency 0 lays at center of spectrum image
    @param spectrum: FFT2 transform
    @param cut : cut value of filter (no physical unit, only number of pixels)
    """
    X,Y = spectrum.shape;
    mask = np.ones((X,Y), "int");
    mx = X/2; my = Y/2;
    mask[mx-cut:mx+cut, my-cut:my+cut] = 0;
    f = spectrum * mask;
    plt.figure
    plt.imshow(abs(f)); plt.title('High pass filter')
    return f;
```

In the following application, the image is loaded and the effects of a low-pass and high-pass filters are illustrated.

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```python
# FT of original image
cornea = imageio.imread('cornee.png')
spectre = np.fft.fftshift(np.fft.fft2(cornea));
# low pass filter
L = LowPassFilter(spectre, 30)
viewSpectrumPhase(abs(L), np.angle(L))
corneaLP = np.real(np.fft.ifft2(np.fft.fftshift(L)))
# high pass filter
H = HighPassFilter(spectre, 30)
viewSpectrumPhase(abs(H), np.angle(H))
corneaHP = np.real(np.fft.ifft2(np.fft.fftshift(H)))
# display results and filters
plt.figure();
plt.subplot(1,2,1)
plt.imshow(corneaLP, plt.cm.gray);plt.title('reconstruction after LP filtering')
plt.subplot(1,2,2)
plt.imshow(corneaHP, plt.cm.gray);plt.title('reconstruction after HP filtering')
```

3.5.5 Application: evaluation of cellular density

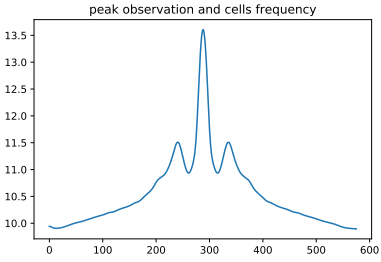
The cells can be considered as a pattern, and its frequency repetition can found in the Fourier transform. More precisions on this application can be found in [33, 14, 34, 37] on the relation between the real cellular density and the image pixels.

```python
cornea = imageio.imread('cornee.tif')
# Fourier Transform
spectre = np.fft.fftshift(np.fft.fft2(cornea));
amplitude = abs(spectre);
# Filter amplitude
Blurred = ndimage.filters.gaussian_filter(amplitude, 5);
plt.figure
plt.subplot(1,2,1);
plt.imshow(np.log(1+Blurred), plt.cm.gray);
plt.title('filtered amplitude')
# Observe frequency peaks
plt.subplot(1,2,2);
plt.plot(np.log(1+Blurred[:,Y/2]));
plt.title('peak observation and cells frequency')
```

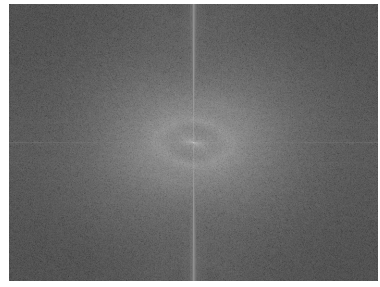
The results are illustrated in Fig. 3.4.

Figure 3.4 The two peaks represent the frequency of repetition of the cellular pattern, i.e. it can be used to compute the cellular density.

(a) Amplitude of Fourier Transform.



(b) Filtering of amplitude.



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4 Introduction to wavelets

This tutorial introduces practically the basic wavelet decomposition and reconstruction algorithms. The objectives are to code some basic programs that will decompose and reconstruct 1D and 2D signals.

4.1 Introduction

Wavelets are based on a mother wavelet Ψ (s is a scale parameter, τ is the time translation factor $(s,\tau) \in \mathbb{R}_+^* \times \mathbb{R}$):

$$\forall t \in \mathbb{R}, \psi_{s,\tau}(t) = \frac{1}{\sqrt{s}}\Psi\left(\frac{t-\tau}{s}\right)$$

The continuous wavelet transform is written as follows, where ψ^* means the complex conjugate of ψ and $< ., . >$ is the complex scalar product (Hermitian form):

$$g(s,\tau) = \int_{-\infty}^{\infty} f(t)\psi_{s,\tau}^*(t)\mathrm{d}s\mathrm{d}\tau = < f, \psi_{s,\tau} >$$

The reconstruction is defined by:

$$f(t) = \frac{1}{C}\int_{-\infty}^{\infty}\int_{-\infty}^{\infty}\frac{1}{|s|^2}g(s,\tau)\psi_{s,\tau}(t)\mathrm{d}s\ \mathrm{d}\tau$$

with

$$C = \int_{-\infty}^{\infty}\frac{|\hat{\Psi}(\omega)|^2}{|\omega|}\mathrm{d}\omega$$

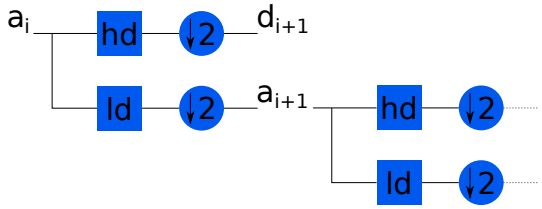
and $\hat{\Psi}$ is the Fourier Transform of Ψ.

The discrete wavelet transform corresponds to a sampling of the scales. To compute the different scales, one has to introduce a "father" wavelet, that similarly defines a family of functions orthogonal to the family $\psi_{s,\tau}$.

4.2 Fast discrete wavelet decomposition / reconstruction

A simple algorithm (cascade algorithm, from Mallat) is defined as two convolutions (by a lowpass ld filter for the projection on the ψ family, and a high pass hd filter for the orthogonal projection) followed by a subsampling (see Fig. 4.1).

Figure 4.1 Algorithm for wavelet decomposition. First, a convolution is performed (square node), then, a subsampling. a_i stands for decomposition at scale i, d_i stands for detail at scale i.



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4.2.1 Simple 1D example

Let's consider the signal $[4; 8; 2; 3; 5; 18; 19; 20]$. We will use the Haar wavelets defined by $ld = [1; 1]$ and $hd = [-1; 1]$. Basically, these filters perform a mean and a difference (see Table 4.1). The result of the decomposition in 3 scales with these wavelets is the concatenation of the details and the final approximation

$$C = \{[-4; -1; -13; -1]; [7; -16]; [-45]; [79]\}$$

Table 4.1 Illustration of Haar decomposition in a simple signal.

Scale i	Approximation a_i	Details d_i
0 (original signal)	$[4; 8; 2; 3; 5; 18; 19; 20]$	
1	$[12; 5; 23; 39]$	$[-4; -1; -13; -1]$
2	$[17; 62]$	$[7; -16]$
3	$[79]$	$[-45]$

>>>?

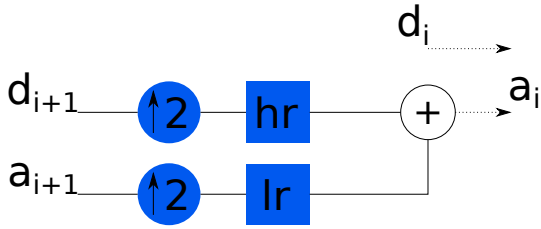
In the case of these Haar wavelets, code a function that performs the decomposition for a given number of scales. The prototype of this function will be:

```python
def simpleWaveDec(signal, nb_scales):
    """
    wavelet decomposition of <signal> into <nb_scales> scales
    This function uses Haar wavelets for demonstration purposes.
    """
```

4.2.2 Reconstruction

To reconstruct the original signal (see Fig. 4.2), we need the definition of two reconstruction filters, hr and lr. For the sake of simplicity, we use $lr = ld/2$ and $hr = -hd/2$. These filter will perform an exact reconstruction of our original signal.

Figure 4.2 Reconstruction algorithm. The oversampling is done by inserting zeros.



Using this algorithm, you can now go on to the next exercise.

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>>>?

Code a function that performs the reconstruction of the signal. The prototype of this function will be, with the previous definition of C:

```python
def simpleWaveRec(C):
    """
    wavelet simple reconstruction function of a 1D signal
    C: Wavelet coefficients
    """
```

4.3 2D wavelet decomposition

Let A be the matrix of an image. We consider that A is of size $2^n \times 2^n$, $n \in \mathbb{N}$. We consider, as for the 1D transform, the filters ld and hd.

The wavelet decomposition is as follows:

- Apply ld and hd on rows of A. Results are denoted $ld_r A$ and $hd_r A$, of size $2^n \times 2^{n-1}$, with r standing for row.
- Then, apply ld and hd again, to get the four new matrices: $ld_c ld_r A$, $ld_c hd_r A$, $hd_c ld_r A$ and $hd_c hd_r A$, of sizes $2^{n-1} \times 2^{n-1}$, with c standing for column. The matrix $ld_c ld_r A$ is the approximation, and the other matrices are the details.

>>>?

- Code a function to perform the wavelet decomposition and for a given number of scales (lower than n). Test it on images of size $2^n \times 2^n$.
- Code the reconstruction function.

4.4 Built-in functions

Let us explore some built-in functions.

4.4.1 Continuous wavelet decomposition

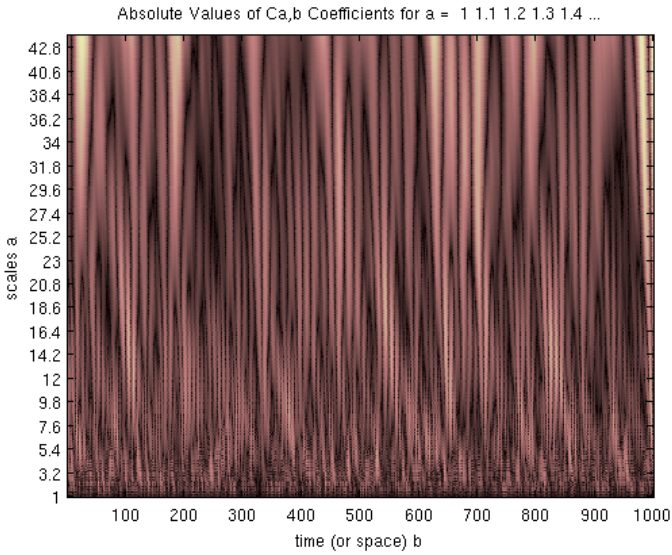
One has to make the difference between the continuous wavelet transform and the discrete transform.

Informations

In `scipy.signal` you can find function to perform wavelets decomposition, and among them `cwt` for the continuous wavelet transform. There is also the module `pywt` that may be more developped (see also `cwt`).

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Figure 4.3 Continuous wavelet transform.



4.4.2 Discrete decomposition

>>>?

1. Generate the signal $\sin(2\pi * f_1 * t) + \sin(2\pi * f_2 * t)$, with $f_1 = 3$Hz and $f_2 = 50$Hz.
2. Apply the wavelet transformation for a given wavelet (like 'db4').
3. Display the 5th approximation of the wavelet decomposition.
4. Display the 4th detail coefficients of the wavelet decomposition.



Look at `pywt.downcoef` for the decomposition at a given level and `pywt.wavedec` for the entire decomposition.

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4.5. Python correction



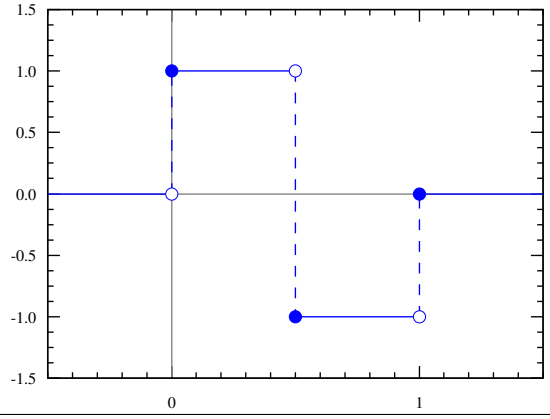


```
import numpy as np
from scipy import misc
import matplotlib.pyplot as plt
```

4.5.1 1D signals

Two functions are required: a function (`simpleWaveDec`) that loops over the different scales and calls the second function (`waveSingleDec`) that performs the single step wavelet decomposition. Notice that the Haar wavelet is defined here with integer values (see Fig.4.4), so that the mental computation can be done easily.

Figure 4.4 Haar wavelets. From wikipedia, author Omegatron.



Simple 1D decomposition



```
def simpleWaveDec(signal, nb_scales):
    """
    wavelet decomposition of <signal> into <nb_scales> scales
    This function uses Haar wavelets for demonstration purposes.
    """
    # Haar Wavelets filters for decomposition and reconstruction
    ld = [1, 1];
    hd = [-1, 1];

    # transformation
    C=[];
    A = signal; # approximation
    for i in range(nb_scales):
        A, D = waveSingleDec(A, ld, hd);
        #get the coefficients
        C.append(D);

    C.append(A);
    return C;
```

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```python
def waveSingleDec(signal, ld, hd):
    """
    1D wavelet decomposition into
    A: approximation vector
    D: detail vector
    ld: low pass filter
    hd: high pass filter
    """
    # convolution
    A = np.convolve(signal, ld, 'same');
    D = np.convolve(signal, hd, 'same');
    # subsampling
    A = A[1::2];
    D = D[1::2];
    return A, D;
```

Simple 1D reconstruction

The reconstruction starts from the highest scale and computes the approximation signal with the given details.

```python
def simpleWaveRec(C):
    """
    wavelet simple reconstruction function of a 1D signal
    C: Wavelet coefficients
    The Haar wavelet is used
    """
    ld = np.array([1, 1]);
    hd = np.array([-1, 1]);
    lr = ld/2;
    hr = -hd/2;

    A = C[-1];
    for scale in reversed(C[:-2]):
       A = waveSingleRec(A, scale, lr, hr);
    return A;
```

```python
def waveSingleRec(a, d, lr, hr):
    """
    1D wavelet reconstruction at one scale
    a: vector of approximation
    d: vector of details
    lr: low pass filter defined by wavelet
    hr: high pass filter defined by wavelet
    This is Mallat algorithm.
    NB: to avoid side effects, the convolution function does not use the
    'same' option
    """
    approx = np.zeros((len(a)*2,));
    approx[::2] = a;
    approx = np.convolve(approx, lr);

    detail = np.zeros((len(a)*2,));
    detail[::2] = d;
    detail = np.convolve(detail, hr);
    # sum up approximation and details to reconstruct signal at lower scale
    approx = approx + detail;
```

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```
    #get rid of last value
    approx = np.delete(approx, -1)
    return approx
```

Results

This is the result for the decomposition of the vector with 3 scales.

```
s = [4, 8, 2, 3, 5, 18, 19, 20];
print(s)
C = simpleWaveDec(s, 3);
print(C)
srec = simpleWaveRec(C);
print(srec);
```

```
[4, 8, 2, 3, 5, 18, 19, 20]
[array([ -4, -1, -13, -1]), array([ 7, -16]), array([-45]), array([79])]
```

4.5.2 2D signals

Decomposition

The `simpleImageDec` function is the main interface. It takes the image as first parameter, and the number of scales of decomposition. It makes a call to `decWave2D` for the decomposition at one given scale. The latter uses the previous 1D decomposition method.

```
def decWave2D(image, ld, hd):
    """
    % wavelet decomposition of a 2D image into four new images.
    % The image is supposed to be square, the size of it is a power of 2 in the
    % x and y dimensions.
    """

    # Decomposition on rows
    sx, sy = image.shape;

    LrA = np.zeros((sx, int(sy/2)));
    HrA = np.zeros((sx, int(sy/2)));

    for i in range(sx):
        A, D= waveSingleDec(image[i,:], ld, hd);
        LrA[i,:]= A;
        HrA[i,:]= D;

    # Decomposition on cols
    LcLrA = np.zeros((int(sx/2), int(sy/2)));
    HcLrA = np.zeros((int(sx/2), int(sy/2)));
    LcHrA = np.zeros((int(sx/2), int(sy/2)));
    HcHrA = np.zeros((int(sx/2), int(sy/2)));
    for j in range(int(sy/2)):
        A, D= waveSingleDec(LrA[:,j], ld, hd);
        LcLrA[:,j] = A;
        HcLrA[:,j] = D;

        A, D= waveSingleDec(HrA[:,j], ld, hd);
        LcHrA[:,j] = A;
        HcHrA[:,j] = D;

    return LcLrA, HcLrA, LcHrA, HcHrA
```

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```python
def simpleImageDec(image, nb_scales):
    """
    wavelet decomposition of <image> into <nb_scales> scales
    This function uses Haar wavelets for demonstration purposes.
    """

    #Haar Wavelets filters for decomposition and reconstruction
    ld = [1,1];
    hd = [-1, 1];

    #transformation
    C=[];
    A = image; # first approximation

    coeffs = [];
    for i in range(nb_scales):
        [A, HcLrA, LcHrA, HcHrA] = decWave2D(A, ld, hd);
        coeffs.append( HcLrA);
        coeffs.append(LcHrA);
        coeffs.append(HcHrA);
        #set the coefficients
        C.append(coeffs.copy());
        coeffs.clear();
    C.append(A);
    return C;
```

2D reconstruction

The `simpleImageRec` function performs the reconstruction of a multiscale wavelet decomposition. The `recWave2D` performs the reconstruction of one scale.

```python
def recWave2D(LcLrA, HcLrA, LcHrA, HcHrA, lr, hr):
    """
    Reconstruction of an image from lr and hr filters and from the wavelet
        ↪ decomposition.
    A: resulting (reconstructed) image

    NB: This algorithm supposes that the number of pixels in x and y dimensions
        ↪ is a power of 2.
    """

    sx, sy = LcLrA.shape;

    # Allocate temporary matrices
    LrA = np.zeros((sx*2, sy));
    HrA = np.zeros((sx*2, sy));
    A  = np.zeros((sx*2, sy*2));

    #Reconstruct from cols
    for j in range(sy):
        LrA[:,j] = waveSingleRec(LcLrA[:,j], HcLrA[:,j], lr, hr);
        HrA[:,j] = waveSingleRec(LcHrA[:,j], HcHrA[:,j], lr, hr);

    # Reconstruct from rows
    for i in range(sx*2):
        A[i,:] = waveSingleRec(LrA[i,:], HrA[i,:], lr, hr);

    return A;
```

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```python
def simpleImageRec(C):
    """
    wavelet reconstruction of an image described by the wavelet coefficients C
    """
    #The Haar wavelet is used
    ld = np.array([1, 1]);
    hd = np.array([-1, 1]);
    lr = ld/2;
    hr = -hd/2;
    A = C[-1];
    for scale in reversed(C[:-1]):
        A = recWave2D(A, scale[0], scale[1], scale[2], lr, hr);

    return A;
```

Results

The illustration Fig. 4.5 is obtained by the following code. The useful functions are presented below.

```
I = imageio.imread('lena256.png');
C = simpleImageDec(I, 3);
Irec = simpleImageRec(C);
plt.imshow(Irec);
plt.show()
```

The image is recursively split into 4 areas, where the left upper corner is the approximation, and the three others are the details. As the details can have negative values, the intensities are adjusted in order to display the image correctly.

```python
def displayImageDec( C ):
    """
    Construct a single image from a wavelet decomposition
    C: the decomposition
    """
    n, m = C[0][0].shape;
    A = np.zeros((2*n, 2*m));
    prev = C[-1];
    for s, scales in reversedEnumerate(C[:-1]):

        ns = n / 2**(s-1);
        ms = m / 2**(s-1);
        T = imdec2im(prev, scales);
        A[0:int(ns), 0:int(ms)] = T;
        prev = A[0:int(ns), 0:int(ms)];
    return prev
```

These two functions `adjust` and `reversedEnumerate` are used to simplify the notations. The first one performs a linear stretching of the image intensities, and the second one allows an enumeration of a list in a reverse order.

```python
def adjust(I):
    """
    simple image intensity stretching
    return I
    """
```

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```
    I = I -np.min(I);
    I = I / np.max(I);
    return I;

def reversedEnumerate(l):
    """
    Utility function to perform reverse enumerate of a list
    returns zip
    """
    return zip(range(len(l)-1, -1, -1), l[::-1]);
```



```
def imdec2im(LcLrA, lvlC):
    """
    constructs a single image from:
    LcLrA: the approximation image
    lvlC: the wavelet decomposition at one level

    for display purposes
    """

    HcLrA=lvlC[0];
    LcHrA=lvlC[1];
    HcHrA=lvlC[2];
    n, m = HcLrA.shape;

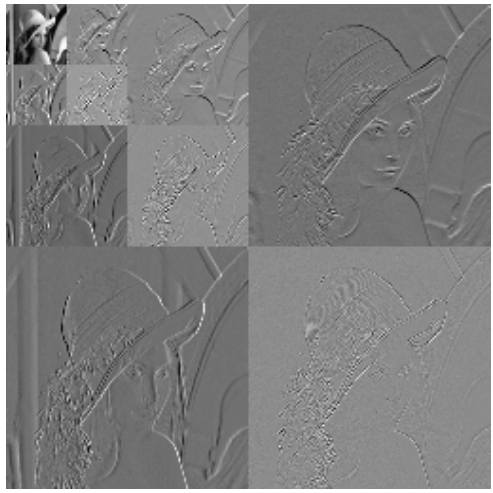
    A = np.zeros((2*n, 2*m));

    # Approximation image can be with high values when using Haar coefficients
    A[0:n, 0:m] =adjust(LcLrA);

    # details are low, and can be negative
    A[0:n, m:2*m] = adjust(HcLrA);
    A[n:2*n, 0:m] = adjust(LcHrA,);
    A[n:2*n, m:2*m] = adjust(HcHrA);

    return A;
```

Figure 4.5 (Haar) Wavelet decomposition of the Lena image.



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4.5.3 Built-in functions

An interesting module is `pywt`. This is illustrated by the following example. This gives the same results as previously, with the multiplication by $1/\sqrt{2}$.

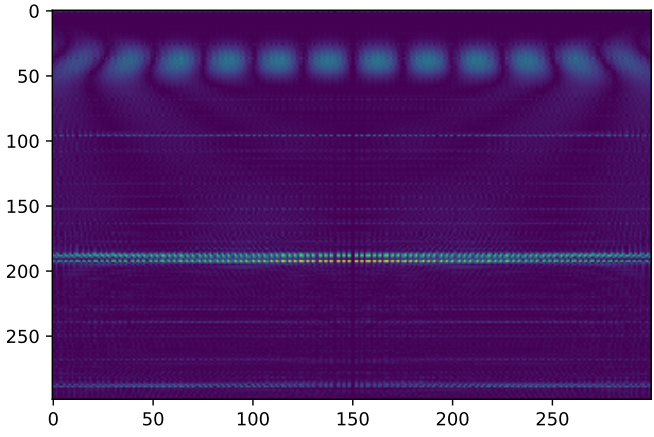
```python
import pywt
cA, cD = pywt.dwt(s, 'haar');
print(cA, cD);
```

```
[ 8.48528137 3.53553391 16.26345597 27.57716447]
[-2.82842712 -0.70710678 -9.19238816 -0.70710678]
```

The continuous wavelet transform is applied in the following code and the result is displayed in Fig.4.6.

```python
t = np.linspace(-1, 1, 1000, endpoint=False)
f1 = 3;
f2 = 50;
sig = np.sin(2 * np.pi * f1 * t) + np.sin(2*np.pi * f2 * t);
widths = np.arange(1, 129)
coef, freqs=pywt.cwt(sig,widths,'morl')
fig = plt.figure();
plt.imshow(coef, extent=[-1, 1, 1, 31], cmap='PRGn', aspect='auto',
           vmax=abs(coef).max(), vmin=-abs(coef).max())
plt.show()
fig.savefig('cwt.python.pdf', bbox_inches='tight')
```

Figure 4.6 Continuous wavelet decomposition of the sum of sinusoids.



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** 5 Image restoration: denoising

This tutorial aims to study some random noises and to test different image restoration methods (image denoising).

The different processes will be applied on the following MR image.

Figure 5.1 Leg.



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5.1 Generation of random noises

Some random noises are defined with the given functions (corresponding to specific distributions):

- uniform noise: $R = a + (b - a) * U(0, 1)$.
- Gaussian noise: $R = a + b * N(0, 1)$.
- Salt and pepper noise: $R : \begin{cases} 0 \leq U(0,1) \leq a & \mapsto & 0 \\ a < U(0,1) \leq b & \mapsto & 0.5 \\ b < U(0,1) \leq 1 & \mapsto & 1 \end{cases}$
- Exponential noise : $R = -\frac{1}{a} * \ln(1 - U(0, 1))$

>>>?

Generate sample images with the four kinds of random noise and visualize their histograms with the built-in functions. Pay attention to the intensity range of the resulting images when calculating the histograms

5.2 Noise estimation

The objective is to evaluate the characteristics of the noise in a damaged/noisy image (in a synthetic manner in this tutorial).

>>>?

1. Visualize the histogram of a Region Of Interest (ROI) of the image of Fig.5.1. The ROI should be extracted from a uniform (intensity) region.
2. Add an exponential noise to the original image and visualize the histogram of the selected ROI.
3. Add a Gaussian noise to the original image and visualize the histogram of the selected ROI.

5.3 Image restoration by spatial filtering

>>>?

1. Add a salt-and-pepper noise to the image of Fig.5.1.
2. Test the 'min', 'max', 'mean' and 'median' image filters.



See the module `scipy.ndimage`

The median filter is efficient in the case of salt-and-pepper noise. However, it replaces every pixel value (first problem) by the median value determined at a given scale (second problem). In order to avoid these two problems, Gonzalez and Woods proposed an algorithm [11].

Algorithm 1: Adaptive median filter [11]. The main function takes two arguments: the image I to be filtered and the maximal size of neighborhood S_{max}. For each pixel (i, j), the good scale is the scale where the median value is different from the min and the max (median value is thus not an impulse noise). Then, if the pixel value is an impulse noise or the maximal scale has been reached, it must be filtered. Otherwise, it is kept untouched. Min, Max and Med functions compute the minimum, maximum and the median value in a neighborhood of size S centered at a pixel (i, j) in image I.

Data: Input (noisy) image I
Data: Maximal scale S_{max}
Result: Filtered image F

Main Function `amf`(I, S_{max})**:**
  forall *pixels* (i, j) **do**
    $S \leftarrow 1$
    while `isMedImpulseNoise`(I, i, j, S) *AND* $S \leq S_{max}$ **do**
      $S \leftarrow S + 1$
      $med \leftarrow$ `Med`(I, i, j, S)
    end
    if $I(i, j) =$`Min`(I, i, j, S) `OR` $I(i, j) =$`Max`(I, i, j, S) `OR` $S = S_{max}$ **then**
      $F(i, j) \leftarrow$ `Med`(I, i, j, S)
    else
      $F(i, j) \leftarrow I(i, j)$
    end
  end

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Algorithm 1: End.

Function `isMedImpulseNoise`(I, i, j, S)**:**
    $med \leftarrow$ `Med`(I, i, j, S)
    if *med*=`Max`(I, i, j, S) `OR` *med*=`Min`(I, i, j, S) **then**
        return True
    else
        return False
    end

>>>?

Implement the adaptive median filter from the following algorithm (Alg.1) based on two steps (the operator acts on an operational window of size $k \times k$ where different statistics are calculated: median, min or max).

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5.4. Python correction

```python
import matplotlib.pyplot as plt
import numpy as np
from scipy import ndimage
from scipy import misc
```

5.4.1 Generation of random noises

In order to convert stretch the images into the range [0;1], the following function can be used:

```python
def hist_stretch(I):
    # histogram stretching
    # returns values of I linearly stretched to range [0;1]
    I = I -np.min(I);
    I = I / np.max(I);
    return I;
```

Random noise illustrations are proposed in Figs.5.2 and 5.3, and a size $S = 32$ is used to generate the noisy images.

Uniform noise

The python `rand` function generates values between 0 and 1 with uniform distribution.

```python
S=32
a=0; b=255;
R1 = a + (b-a) * np.random.rand(S, S);
```

Gaussian noise

The python `randn` function generates values with normal centered distribution.

```python
a=0; b=1;
R2 = a + (b-a)*np.random.randn(S, S);
```

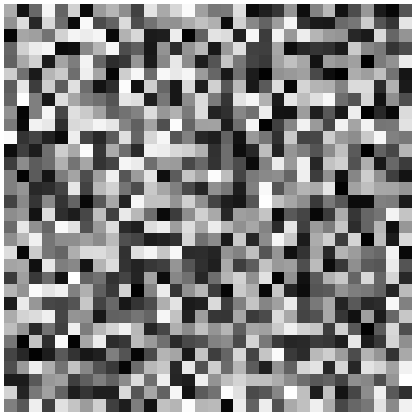
Salt and pepper noise

```python
a = 0.05; b = 0.1;
R3 = 0.5 * np.ones((S,S));
X = np.random.rand(S,S);
R3[X<=a] = 0;
R3[(X>a) & (X <= b)] = 1;
R3 = hist_stretch(R3);
```

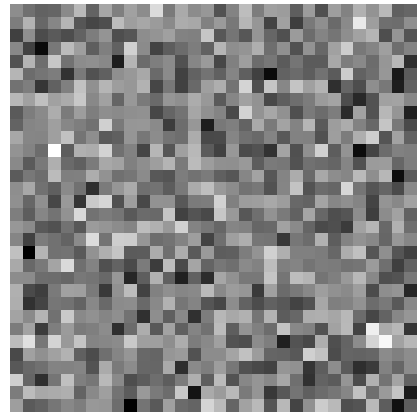
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Figure 5.2 Resulting noise images.

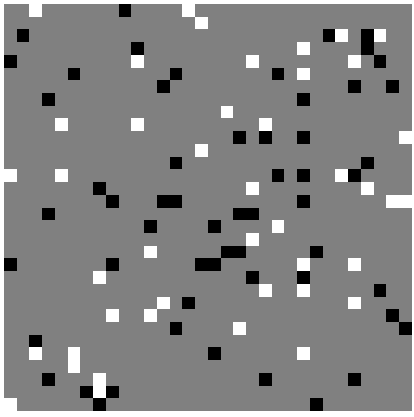
(a) Uniform noise.



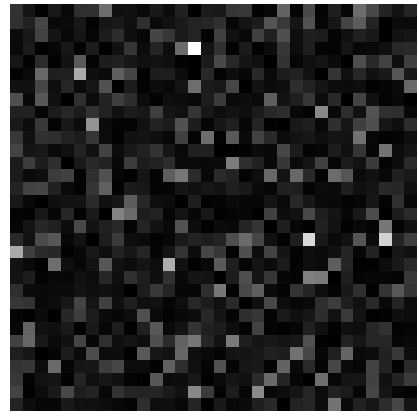
(b) Gaussian noise.



(c) Salt and pepper noise.



(d) Exponential noise.



Exponential noise

```
a=1;
R4 = -1/a * np.log(1-np.random.rand(32, 32));
R4 = hist_stretch(R4);
```

5.4.2 Noise estimation

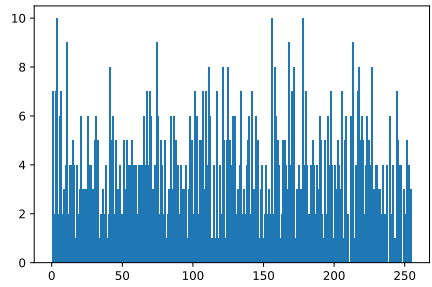
In order to estimate the noise, a ROI of visually constant gray level is chosen, and its histogram is displayed. This is simulated by the following code, the result is displayed in Fig.5.4:

```
# noise estimation
fig = plt.figure()
A = imageio.imread('jambe.png');
roi = A[160:200, 200:240];
plt.hist(roi.flatten(),255);
fig.savefig("histo_roi_leg.pdf", bbox_inches='tight');
```

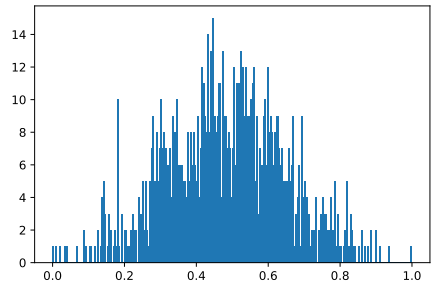
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Figure 5.3 Histograms of the noise images generated with 32×32 pixels.

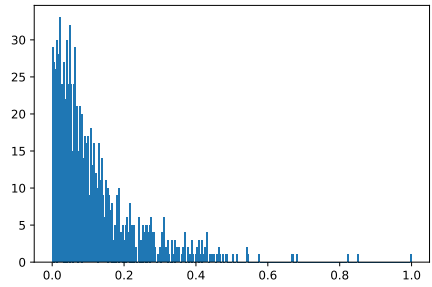
(a) Uniform noise.



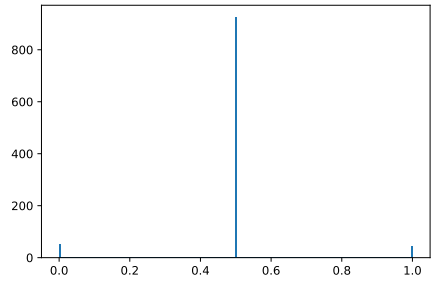
(b) Gaussian noise.



(c) Exponential noise.



(d) Salt and pepper noise.



Then, some noise is added to the image, and the histogram of the ROI is displayed. The results are observed in Figs.5.5 and 5.6.

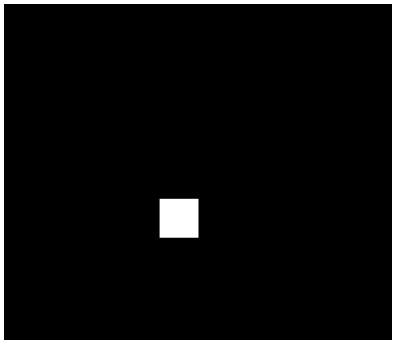
```python
# add exponential noise to image
nx, ny = A.shape;
expnoise = -1/.5 * np.log(1-np.random.rand(nx, ny));
expnoise = expnoise / np.max(expnoise);
B = A + 255*expnoise;
B = hist_stretch(B);
fig = plt.figure()
plt.imshow(B, cmap='gray');
imageio.imwrite("leg_exponential.png", B);
#plt.show()
```

```python
# add gaussian noise to image
nx, ny = A.shape;
gaussnoise = 50*np.random.rand(nx, ny);
B = A + gaussnoise;
B = hist_stretch(B);
fig = plt.figure()
plt.imshow(B, cmap='gray');
imageio.imwrite("leg_gaussian.png", B);
```

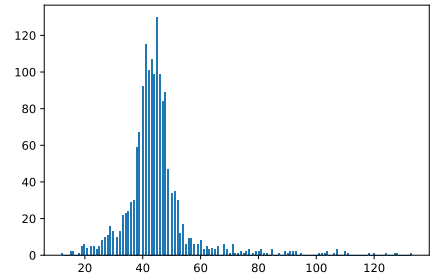
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Figure 5.4 Histogram of the Region of Interest.

(a) ROI.



(b) Histogram.



In the case of exponential and Gaussian noise added to the image, The histograms are displayed in Figs.5.5 and 5.6.

Figure 5.5 Exponential noise.

(a) Addition of exponential noise to the original image of the leg.



(b) Histogram of the ROI.

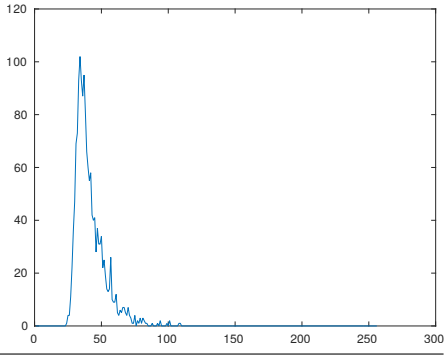
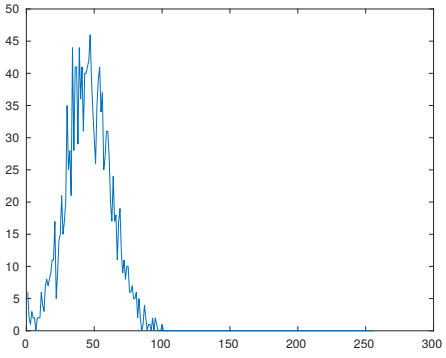


Figure 5.6 Gaussian noise.

(a) Addition of Gaussian noise to the original image of the leg.



(b) Histogram of the ROI.



5.4.3 Image restoration by spatial filtering

The following code is used to filter the images. The results are displayed in Fig.5.7. Salt and Pepper noise is added to the image.

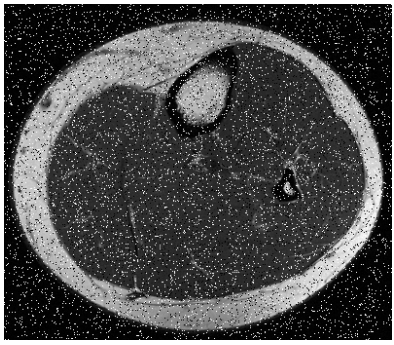
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Figure 5.7 Different filters applied to the noisy image. The median filter is particularly adapted in the case of salt and pepper noise (impulse noise), but still destroy the structures observed in the images.

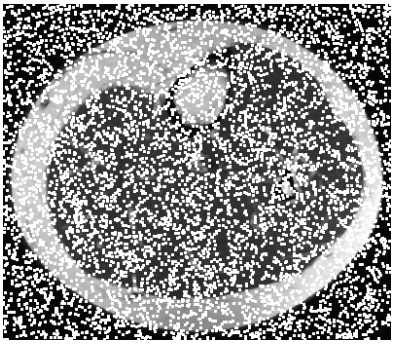
(a) Original image.



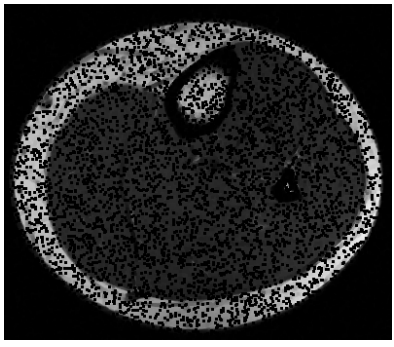
(b) Noisy image (salt and pepper).



(c) Maximum filter.



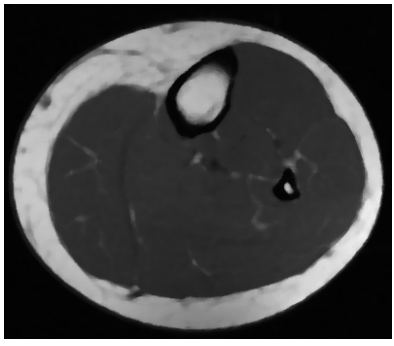
(d) Minimum filter.



(e) Mean filter.



(f) Median filter.



```
a = 0.05; b = 0.05;
spnoise = 0.5 * np.ones((nx,ny));
X = np.random.rand(nx,ny);
B = A.copy();
B[X<=a] = 0;
B[(X>a) & (X <= (a+b))] = 255;
fig = plt.figure()
plt.imshow(B, cmap='gray');
imageio.imwrite("leg_sp.png", B);
#plt.show()
```

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Then, different filters are illustrated. Notice that the contours informations are somehow damaged. The median filter corresponds to the best filter in this case.

```
### filtering by convolution
#average filtering
B1 = ndimage.uniform_filter(B,5);
imageio.imwrite("leg_uniform.png", B1);
B2 = ndimage.minimum_filter(B,3);
imageio.imwrite("leg_minimum.png", B2);
B3 = ndimage.maximum_filter(B,3);
imageio.imwrite("leg_maximum.png", B3);
B4 = ndimage.median_filter(B, 7);
imageio.imwrite("leg_median.png", B4);
B5 = amf(B, 7);
plt.imshow(B5, cmap='gray');
imageio.imwrite("leg_amf.png", B5);
```

What can be noticed is that min and max filters are unable to restore the image (opening and closing filters, from the mathematical morphology, could be a solution to explore). The mean filter is a better solution, but an average value is highly modified by an impulse noise. The median filter is the optimal solution is order to suppress the noise, but fine details are lost. An interesting solution is to apply an adaptive median filter.

Adaptive median filter

The following code is a simple implementation of the algorithm previously presented. It has not been optimized in order to have a simple presentation. A more sophisticated version can be found in [11]. The results are illustrated in Fig.5.8 for $S_{max} = 7$.

```
def amf(I, Smax):
    """
    Adaptive median filter
    I: grayscale image
    Smax: maximal size of neighborhood. Limits the effect of median filter
    """
    f = np.copy(I);
    nx, ny = I.shape;
    sizes = np.arange(1, Smax, 2);
    zmin = np.zeros((nx, ny, len(sizes)));
    zmax = np.zeros((nx, ny, len(sizes)));
    zmed = np.zeros((nx, ny, len(sizes)));
    for k,s in enumerate(sizes):
        zmin[:,:,k] = ndimage.minimum_filter(I, s);
        zmax[:,:,k] = ndimage.maximum_filter(I, s);
        zmed[:,:,k] = ndimage.median_filter (I, s);
    isMedImpulse = np.logical_or(zmin==zmed,zmax==zmed);

    for i in range(nx):
        for j in range(ny):
            k = 0;
            while k<len(sizes)-1 and isMedImpulse[i,j,k] :
                k+=1;

            if I[i,j] == zmin[i,j,k] or I[i,j]==zmax[i,j,k] or k==len(sizes):
                f[i,j] = zmed[i,j,k];
    return f;
```

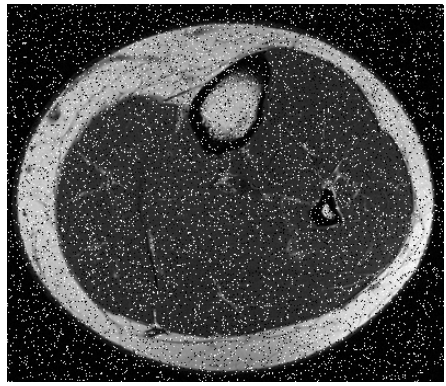
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Figure 5.8 Illustration of the adaptive median filter.

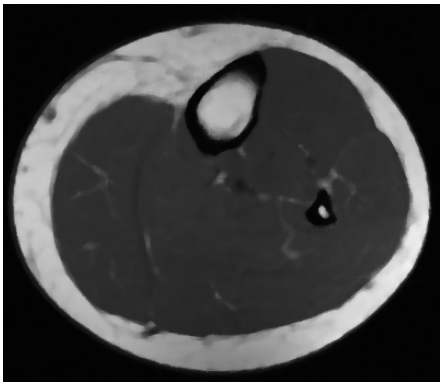
(a) Original image.



(b) Noisy image (salt and pepper).



(c) Median filter of size 7×7.



(d) Adaptive median filter, $S_{max} = 7$.



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6 Image Restoration: deconvolution

This tutorial aims to study and test different image restoration methods for blurred and noisy images. Altough the different software tools contain functions for each filter the objective is to exhaustively code these methods to fully understand their principles. The reader can refer to [36] for more informations on the algorithms. Some of the images are based on observations made with the NASA/ESA Hubble Space Telescope, and obtained from the Hubble Legacy Archive, which is a collaboration between the Space Telescope Science Institute (STScI/NASA), the Space Telescope European Coordinating Facility (ST-ECF/ESA) and the Canadian Astronomy Data Centre (CADC/NRC/CSA). You may access to these resources at https://hla.stsci.edu/

The different processes will be applied on the following images.

6.1 Damage modeling

A damage process can be modeled by both a damage function D and an additive noise n, acting on an input image f for producing the damaged image g.

$$g = D(f) + n \tag{6.1}$$

Knowing g, the objective of restoration is to get an estimate $\hat{f}$ (the restored image) of the original image f. If D is a linear process, spatially invariant, then the equation can be simplified as:

$$g = h * f + n \tag{6.2}$$

where h is the spatial representation of the damage function (called the Point Spread Function - PSF), and $*$ denotes the convolution operation. In general, the more knowledge you have about the function H and the noise n, the closer $\hat{f}$ is to f.

This equation can be written in the frequency domain:

$$G = H.F + N \tag{6.3}$$

where the letters in uppercase are the Fourier transforms of the corresponding terms in the eq. 6.2.

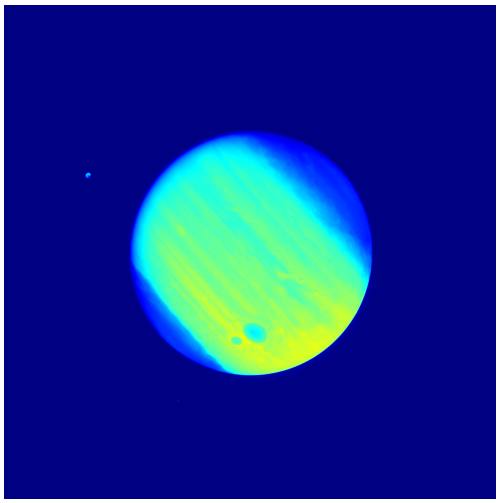
>>>?

- Generate the 'chessboard' image.
- Generate a PSF corresponding to a blur (motion or isotropic).
- Create a damaged image (a circular option is used, because the FFT implies that functions are periodical) and add a Gaussian noise.
- Visualize the different images.

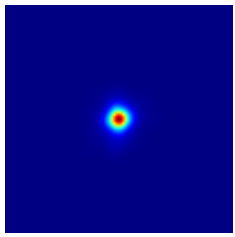
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Figure 6.1 Images that can be used for testing the different restoration algorithms. Intensity levels are represented in false colors.

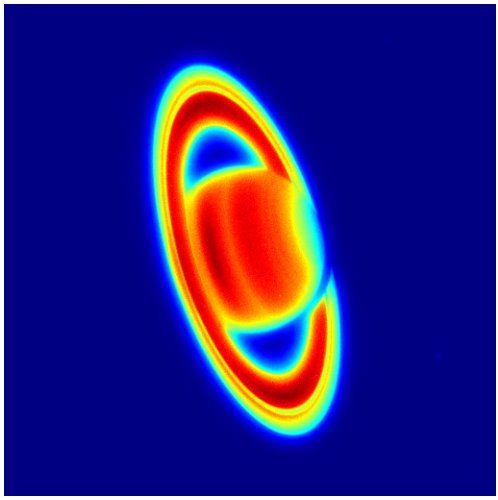
(a) Jupiter, from Hubble Space Telescope, ads/Sa.HST#ic3g01qlq.



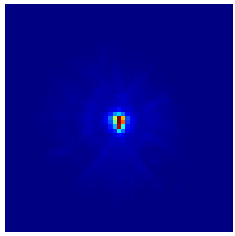
(b) PSF for Jupiter image



(c) Saturn, HST.



(d) PSF for Saturn image



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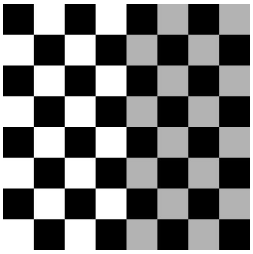
6.2 Simple case: no noise

The objective is now to restore the damaged image.

For the first steps, no noise will be added. The degradation functions is $g = h * f$. Knowing H (Fourier Transform of the psf h) and ignoring the noise in the damage model, a simple estimate of the initial image can be done by the inverse filtering:

$$f = FT^{-1}\left(\frac{G}{H}\right) \tag{6.4}$$

Figure 6.2 Chessboard image.



where FT^{-1} denotes the inverse Fourier transform.

>>>?

- Try the inverse filter in the Fourier space. Why is this filter not working?
- Try to prevent division by 0, with $f = FT^{-1}\left(\frac{G}{H+\alpha}\right)$, α being a small constant value (e.g. $\alpha = 0.1$).

6.3 Wiener filter

The Wiener filter is an optimal filter that minimizes the following error:

$$e^2 = E\{(f - \hat{f})^2\}$$

where E denotes the expected (mean) value, f is the original image and $\hat{f}$ is the restored image.

The solution to this expression, within the frequency domain, is given by:

$$\hat{F} = \underbrace{\left(\frac{1}{H}\frac{|H|^2}{|H|^2 + R}\right)}_{H_w} G$$

The value of R can be arbitrarily fixed. Another way is to define $R = S_n/S_f$, where S_n and S_f denote the power spectrum of the noise n and the original image f, i.e. $|N|^2$ and $|F|^2$ (matrices), respectively. This ratio can be defined globally (as the constant) or locally (i.e. it is computed for each pixel). If the ratio S_n/S_f (function) is non null, it can be passed to the Wiener filtering process.

6.3.1 Simple case: no noise

In the noiseless case, the Wiener filter reduces to the inverse filter:

$$H_w = \begin{cases} \dfrac{1}{H(u,v)} & \text{if } |H(u,v)| \neq 0 \\ 0 & \text{otherwise} \end{cases}$$

>>>?

Try a Wiener filter for the noiseless case.

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6.3.2 Noisy images

Generally, the ratio S_n/S_f used in the Wiener filter is replaced by a constant value equal to the ratio of the mean power spectrum:

$$R = \frac{\frac{1}{PQ} \cdot \sum_u \sum_v S_n(u,v)}{\frac{1}{PQ} \cdot \sum_u \sum_v S_f(u,v)} \tag{6.5}$$

where PQ denotes the matrix size (the number of elements).

>>>?

1. Calculate the constant ratio R and code the Wiener filter .
2. Test the different algorithms on the image 'brain' damaged by a blur and an additive noise.

6.4 Iterative filters for noisy images

6.4.1 Van Cittert iterative filter

The VanCittert iterative filter is based on the following iterative relation :

$$f_{k+1} = f_k + \beta(g - h * f_k)$$

with $f_0 = g$, the damaged image.

>>>?

Code and test on different cases a function that performs the VanCittert restoration filter.

It should have the following prototype:

```
function [ fr ] = vca( g, psf, n_iter)
% Van Cittert iteration algorithm for deconvolution
%
% g: degraded image
% psf: point spread function
% n_iter: number of iterations
```

```
def vca(g, psf, n_iter, beta=.01):
    """
    Van Cittert iterative filter
    g: noisy image
    psf: point spread function
    n_iter: number of iterations
    beta: Jansson parameter
    """
```

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6.4.2 Lucy-Richardson filtering

We are now going to use the nonlinear restoration filtering of Lucy-Richardson that is based on a maximum likelihood formulation in which the image is modeled by Poisson statistics. This optimization leads to the solution if the following iterative equation converges:

$$f_{k+1}(x,y) = f_k(x,y) \cdot \left(h(-x,-y) * \frac{g(x,y)}{h(x,y) * f_k(x,y)} \right) \tag{6.6}$$

>>>?

Code and test your own function for the Lucy-Richardson filtering process. It should have the same prototype as the VanCittert function. Remember that $\cdot$ is the classical multiplication (point to point) and that $*$ is the convolution operation. You then have the choice to make a direct call to the convolution function, or to perform this operation in the Fourier space.

6.5 Blind deconvolution: restoration with no a priori

If the PSF is unknown, one of the main difficulties in image restoration is to get an accurate estimate of this PSF in order to use it in the deconvolution algorithms. These methods are called blind deconvolution methods. Generally, the PSF is estimated in an iterative way from an initial PSF.

>>>?

1. Generate a damaged image of 'chessboard' with a Gaussian blur and an additive Gaussian noise.
2. Restore from a blind deconvolution the damaged image and compare the results with the previous ones.

Informations

Use the function `skimage.restoration.unsupervised_wiener` for example.

6.6 Astronomy images

A classical file format used in astronomy is the FITS format.

With python, fits images can be manipulated with the `astropy` module. You can use the following code to display an image.

```
hdu_list = fits.open('ic3g01qlq_drz.fits');
image = hdu_list[1].data;
image = np.nan_to_num(image);
plt.imshow(image, cmap='gray')
plt.show()
```

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6.7. Python correction

```python
from astropy.io import fits
import matplotlib.pyplot as plt
import numpy as np
from scipy.misc import imresize
from scipy import signal
import progressbar
```

6.7.1 Damage modeling

There is no built-in function to generate the checkerboard image. A simple code can be used.

```python
def checkerboard():
    arr = np.zeros((8,8),dtype=int)
    arr[::2,::2] = 1
    arr[1::2,1::2] = 1
    out = imresize(arr,8*np.array(arr.shape),interp='nearest')/255;
    return out;
```

The psf can be generated as a Gaussian psf, or a motion psf. In this tutorial, the motion psf is loaded from a file that comes from the MATLAB® function `fspecial`.

```python
C = checkerboard();
psf = np.load('psf_motion.npy');
```

In order to add Gaussian noise, the following function is used:

```python
def addGaussianNoise(I, sigma=1000):
    """Adds Gaussian noise to an image
    I: original image
    sigma: signal/noise ratio
    """
    I2 = I.copy();
    m=np.min(I);
    M=np.max(I);
    N = (M-m)/sigma*np.random.randn(I.shape[0], I.shape[1]);
    I2 = I2 + N;
    I2[I2>M] = M;
    I2[I2<m]=m;
    return I2, I-I2;
```

The image is blurred and noise is then added.

```python
Cb = signal.convolve2d(C, psf, boundary='wrap', mode='same');
Cbn, noise = addGaussianNoise(Cb);
plt.imshow(Cbn, cmap='gray')
plt.title('Motion blur + Gaussian noise on checkerboard')
plt.show();
```

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Optical Transfer Function: OTF

The OTF is the centered Fourier Transform of the PSF (Point Spread Function). The following function is used to get the OTF from the PSF:

```python
def psf2otf(psf, s):
    """
    Get OTF (Optical Transfer Function) from PSF (Point Spread Function)
    OTF is basically the Fourier Transform of the PSF, centered
    psf: PSF
    s: shape of the result, zero-padding is used to center is Fourier Transform
    """
    sh = psf.shape;
    sh = np.array(sh);
    s = np.array(s);
    pad = s -sh;
    h = np.pad(psf, ((0,pad[0]), (0, pad[1])), mode='constant');
    shift = (int(pad[0]/2+1), int(pad[1]/2+1));
    h_centered = np.roll(h, tuple(shift), axis=(0,1));
    h_centered = np.fft.fftshift(h_centered);
    H = np.fft.fft2(h_centered, s);
    H = np.real(H);
    return H;
```

6.7.2 Simple case: no noise

For the direct reconstruction, just ensure that there is no division by 0. The different results are illustrated in Fig.6.3.

```python
H = psf2otf(psf, C.shape);
G = np.fft.fft2(Cb);
alpha = 0.001;
F = G / (H+alpha);
fr = np.real(np.fft.ifft2(F));
plt.imshow(fr);
plt.title('Noiseless (only motion blur) direct reconstruction')
plt.imsave("cb_reconstruction.png", fr, cmap='gray');
plt.show()
```

In the presence of noise, the reconstructed image is not perfect.

```python
H = psf2otf(psf, C.shape);
G = np.fft.fft2(Cbn);
alpha = 0.001;
F = G / (H+alpha);
fr = np.real(np.fft.ifft2(F));
```

The automatic evaluation of the noise parameter is done in the Wiener filter by:

```python
SpecPuissNoise=np.abs(np.fft.fft2(noise))**2;
PuissMoyNoise=np.mean(SpecPuissNoise);
SpecPuissImageOrig=np.abs(np.fft.fft2(C))**2;
PuissMoyImageOrig=np.mean(SpecPuissImageOrig);
ratio=PuissMoyNoise/PuissMoyImageOrig;
Hw = np.conjugate(H)/(np.abs(H)**2+ratio);
fr = np.fft.ifft2( Hw * np.fft.fft2(Cbn));
```

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6.7.3 Iterative filters

Van-Cittert iterative filter

The parameter (Jansson parameter) controls the precision of convergence, but a small value requires a high number of iterations (and thus a high computation time).



```
def vca(g, psf, n_iter, beta=.01):
    """
    Van Cittert iterative filter
    g: noisy image
    psf: point spread function
    n_iter: number of iterations
    beta: Jansson parameter
    """
    H = psf2otf(psf, g.shape);

    # init iterations
    fr = g.copy();
    bar = progressbar.ProgressBar();
    for iter in bar(range(n_iter)):
        estimation = np.real(np.fft.ifft2(H * np.fft.fft2(fr)));
        fr= fr + beta* ( g -estimation);

    return fr;
```

Richardson-Lucy iterative filter

This algorithm is probably the most famous one in the domain. Remember that the symmetry in the space domain becomes the complex conjugate in the spectral domaine (after Fourier transform).



```
def rla(g, psf, n_iter):
    """
    Richardson Lucy algorithm
    g: noisy image
    psf: point spread function
    n_iter: number of iterations
    """
    H = psf2otf(psf, g.shape);
    # init iterations
    fr = g.copy();

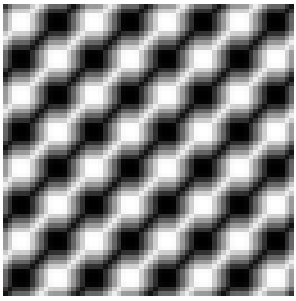
    bar = progressbar.ProgressBar()
    for iter in bar(range(n_iter)):
        estimation = np.fft.ifft2(H * np.fft.fft2(fr));
        M = np.real(np.fft.ifft2(np.conjugate(H) * np.fft.fft2(g / estimation)));
        fr= fr * M;
        fr[fr<0] = 0;

    return fr;
```

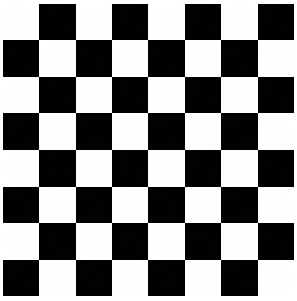
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Figure 6.3 Different deconvolution methods applied on the synthetic image 'checkerboard'.

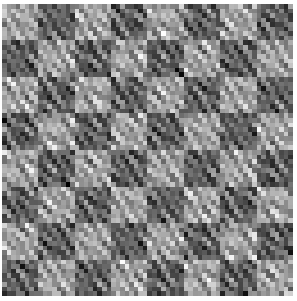
(a) Damaged checkerboard image, with motion blur and Gaussian noise.



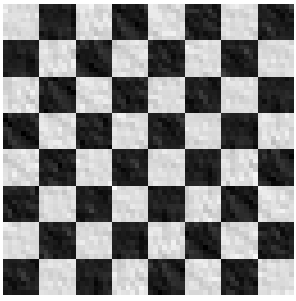
(b) Reconstruction of the checkerboard without noise.



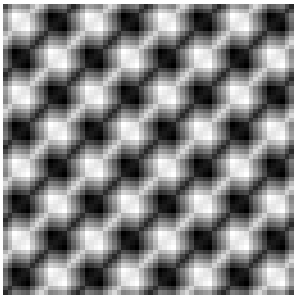
(c) Reconstruction of the checkerboard with noise.



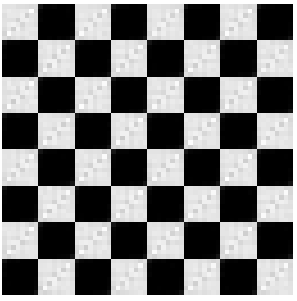
(d) Wiener deconvolution.



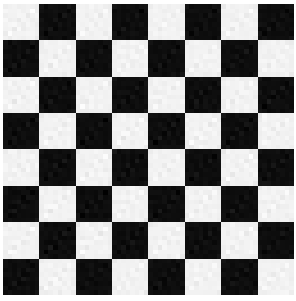
(e) Van-Cittert iterative deconvolution with 100 iterations, and Jansson parameter at 0.01.



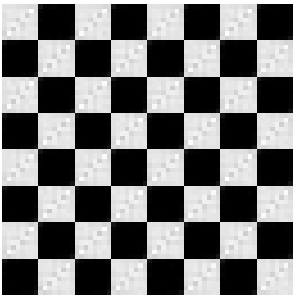
(f) Richardon-Lucy iterative deconvolution with 1000 iterations.



(g) Landweber iterative deconvolution with 1000 iterations and Jansson parameter at 1.



(h) Poisson Maximum A Posteriori iterative deconvolution with 1000 iterations.



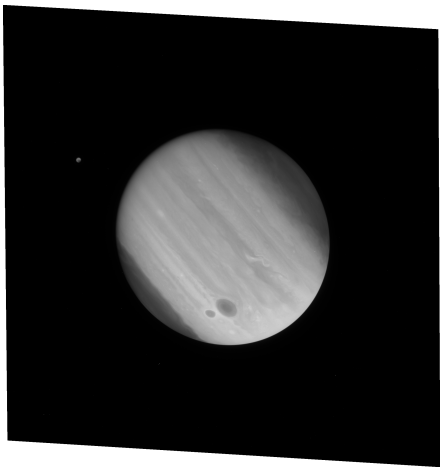
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6.7.4 Astronomy images

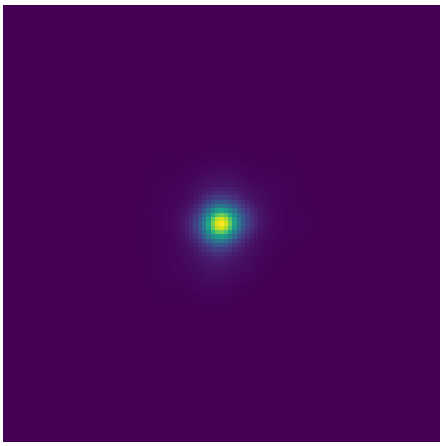
These real images come from the Hubble Space Telescope (HST, see credits), shown in Fig.6.4. The results for the Richardson-Lucy, Van-Cittert and Landweber algorithms are shown in Fig.6.5. The direct deconvolution does not give a correct result.

Figure 6.4 Original images and PSF, from the HST.

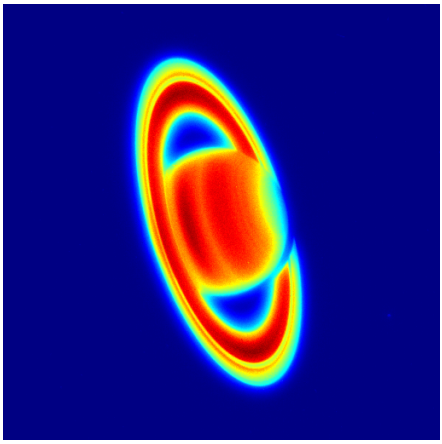
(a) Jupiter.



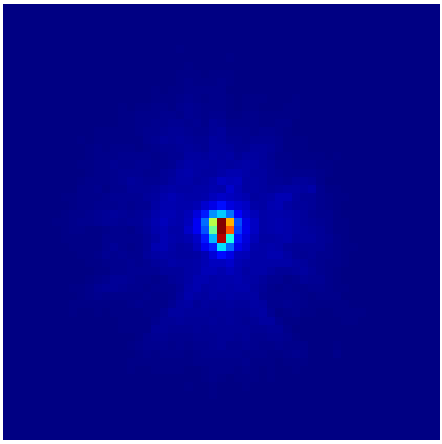
(b) PSF for the observation of Jupiter.



(c) Saturn.



(d) PSF for the observation of Saturn.



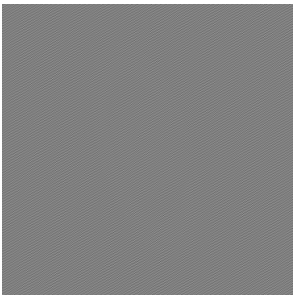
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Figure 6.5 Different deconvolution methods applied for the astronomy images.

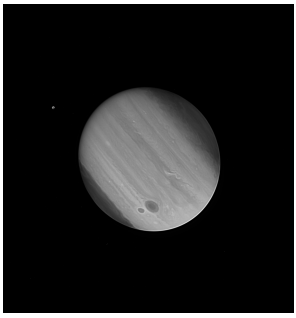
(a) Direct deconvolution.



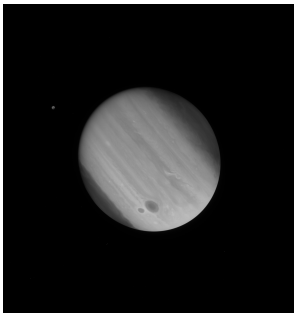
(b) Direct deconvolution.



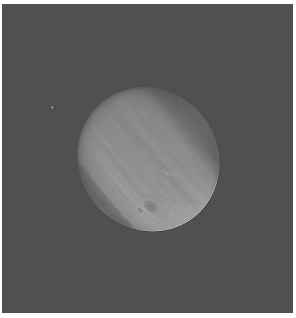
(c) Richardon-Lucy iterative deconvolution with 10 iterations.



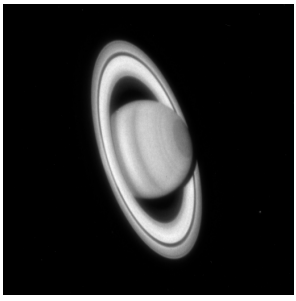
(d) Van-Cittert iterative deconvolution with 10 iterations.



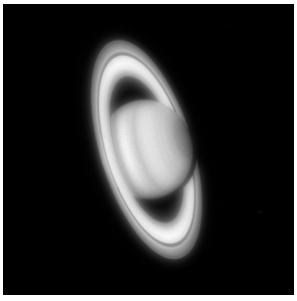
(e) Landweber iterative deconvolution with 200 iterations and Jansson parameter at 1.



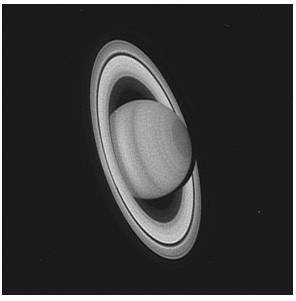
(f) Richardon-Lucy iterative deconvolution with 10 iterations.



(g) Van-Cittert iterative deconvolution with 10 iterations.



(h) Landweber iterative deconvolution with 200 iterations and Jansson parameter at 1.



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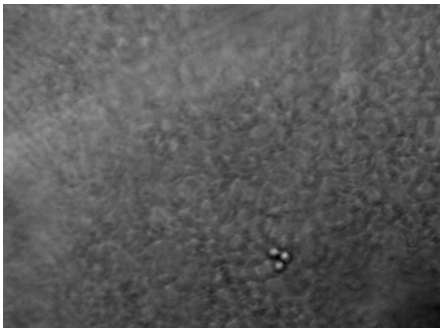
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7 Shape From Focus

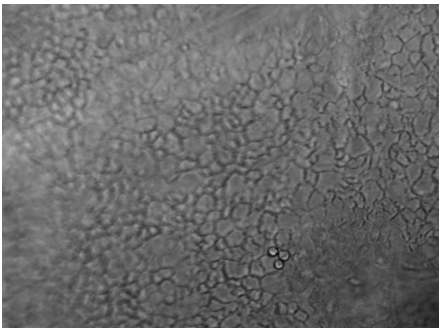
This tutorial introduces the basic shape from focus concepts. The objective is to reconstruct a focused image from a serie (generally a stack) of images with inhomogene focus (see Fig. 7.1).

Figure 7.1 Different images of the stack, from a corneal endothelium in optical microscopy (with 3D microscope).

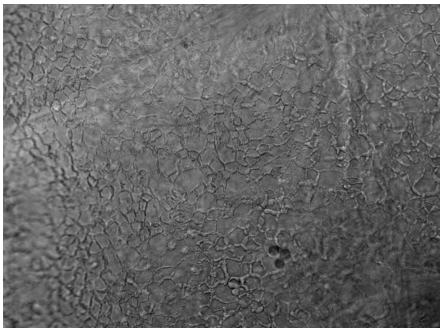
(a) Layer 1



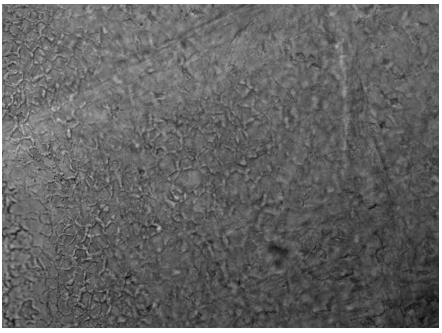
(b) Layer 9



(c) Layer 18



(d) Layer 24



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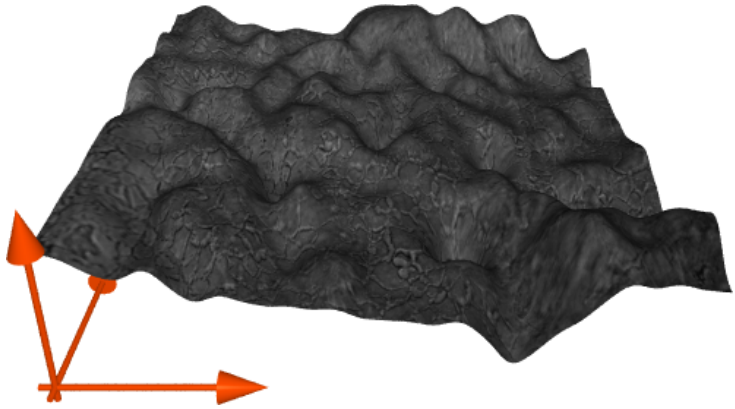
7.1 Introduction to classical methods

An optic system has a limited depth of field. When observing non plane surfaces with a microscope, some parts of the observation may be blurred as well as some others may be correctly focused.

To overcome this problem and reconstruct an all-focused image as well as a surface (see Fig. 7.2), an algorithm will look at every pixel of the images in the stack and select the most focused one, by the way of a focus measure. This tutorial proposes to test some classical focus measures. You can have a look at [7] and [8] to see real applications.

Practically, TIF files can handle stacks of images. Here is a way to open such a file:

Figure 7.2 Reconstruction of the surface and the texture.



```python
from skimage import io

I = io.imread('volume.tif');
I = I.astype('float');
```

```matlab
% load a stack of images in file
info = imfinfo(stackfile);
num_images = numel(info);
% store the images into stack
stack=zeros(info(1).Height, info(1).Width, num_images);
for k = 1:num_images
   stack(:,:,k)=imread(stackfile, k);
   % you can now do something with each image
end
```

In the following, each of the proposed methods will compute a focus measure layer by layer, and will maximize this measure over the stack to find the most focused layer.

7.1.1 Sum of Modified Laplacian

One of the first methods had been proposed by [25]. It is based on the second derivatives, specifically the Laplacian operator:

$$\triangle^2 I = \frac{\partial^2 I}{\partial x^2} + \frac{\partial^2 I}{\partial y^2}$$

The problem with this operator is that the second derivatives in the x and y dimensions can have opposite signs. One way to overcome this problem is to introduce the modified Laplacian as follows:

$$\triangle^2_M I = \left|\frac{\partial^2 I}{\partial x^2}\right| + \left|\frac{\partial^2 I}{\partial y^2}\right|$$

The discrete approximation of the modified Laplacian is computed as:

$$ML(x,y) = |2I(x,y) - I(x-1,y) - I(x+1,y)| + |2I(x,y) - I(x,y-1) - I(x,y+1)| \quad (7.1)$$

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Then, the focus measure based on the modified Laplacian is:

$$F_{ML} = \sum_{(x,y)\in\omega} ML(x,y)$$

7.1.2 Variance

The measure of focus based on the variance is today the mainly used method [15, 41]. It is based on the computation of the variance in a window ω, with $N = \#\omega$ being the size of the window:

$$F_v = \sum_{\omega} \left(I - \underbrace{\frac{1}{\#\omega}\sum_{\omega} I}_{\text{Mean of I}} \right)^2$$

7.1.3 Tenengrad

In [21], we can find the definition of the tenengrad [42]. Let $S(x,y)$ be the norm of the Sobel gradient of image I.

$$F_t(I) = \sum_{\omega} S^2$$

Notice that the original definition requires a threshold value that requires heuristic choices, which is out of the topic of this tutorial.

7.1.4 Variance of Tenengrad

We define the variance of Tenengrad measure of focus by:

$$F_{vt}(I) = F_v(S)$$

.

7.2 Texture and surface reconstruction

>>>?

A set of images (Vickers indentation test [7], and a human corneal endothelium [8]) are proposed. For all the detailed methods:

- reconstruct the surface and the texture of the image (an image focused on its all field of view).

7.2.1 Open question

>>>?

Several methods have been implemented in order to perform the 3D surface/texture reconstruction. Propose a numerical measure that could compare the results and measure the effciciency of these methods? What is the best method?

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7.3. Python correction

```python
import numpy as np
import matplotlib.pyplot as plt
from mpl_toolkits.mplot3d import Axes3D
from skimage import io
from scipy import ndimage
from matplotlib import cm
```

7.3.1 Main function

This code is used as the main function to perform shape-from-focus reconstruction.

```python
volumes = ['cornee', 'vickers'];
for v in volumes:
    I = io.imread('volume_'+v+'.tif');
    I = I.astype('float');
    F = np.zeros(I.shape)
    N = 11;

    myfunctions = [variance, tenengrad, sml];
    for f in myfunctions:
        for i,im in enumerate(I):
            F[i] = f(im, N);

        # Evaluates altitudes and textures
        Z = np.argmax(F, axis=0);
        Z = ndimage.minimum_filter(Z, size=5);
        T = extractTexture(I, Z);
```

The extraction of the texture from the altitudes (indexes) in the stack of images is performed by the following function:

```python
def extractTexture(I, Z):
    """
    Extract texture from stack of images I, where Z is the index (altitude)
    I: stack of images, of shape (n, X, Y)
    Z: index of SFF maximum (of shape (X,Y)), values are between 0 and n-1
    returns basically I[Z(i,j], i, j)] for all (i,j)
    """
    m,n = I.shape[1:]
    ii,jj = np.ogrid[:m,:n]
    T = I[Z, ii, jj];
    return T;
```

7.3.2 Sum of Modified Laplacian

Results are illustrated in Fig.7.3.

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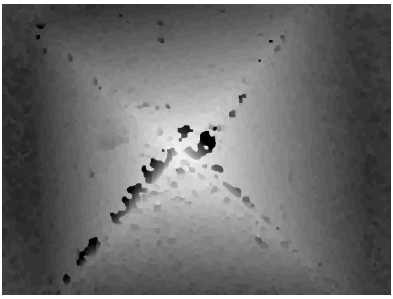
```python
def sml(I, N):
    """
    SFF measure, SUM of modified Laplacian
    I: image
    N: neiborhood size
    returns: SFF measure for each pixel
    """
    h=np.array([[-1, 2, -1]]);
    ML=np.abs(ndimage.convolve(I,h))+np.abs(ndimage.convolve(I,np.transpose(h)));
    S=ndimage.uniform_filter(ML, N);
    return S;
```

Figure 7.3 Texture and altitude reconstruction with the SML method.

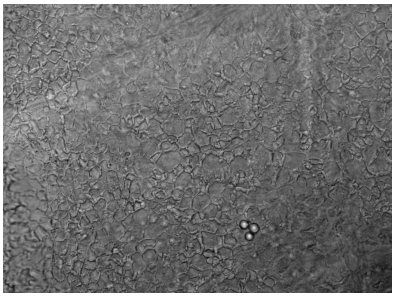
(a) Texture.



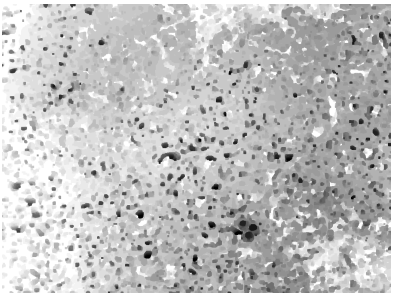
(b) Altitudes.



(c) Texture.



(d) Altitudes.



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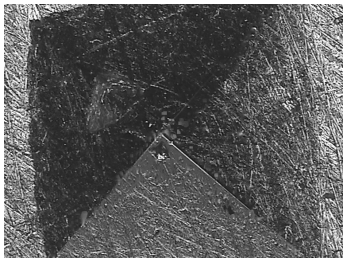
7.3.3 Variance

The focus measure based on the variance i a really simple method that works in most cases, see Fig.7.4.

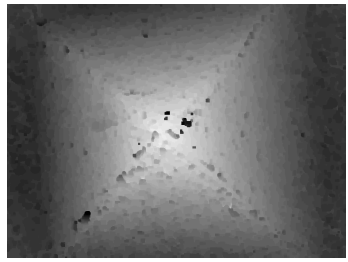
```python
def variance(I, N):
    """
    SFF measure
    I: image
    N: neighborhood size
    returns: SFF measure for each pixel, results is the same shape as I
    """
    M = ndimage.uniform_filter(I, N);
    D2 = (I -M) ** 2;
    V = ndimage.uniform_filter(D2, N);
    return V;
```

Figure 7.4 Texture and altitude reconstruction with the variance method.

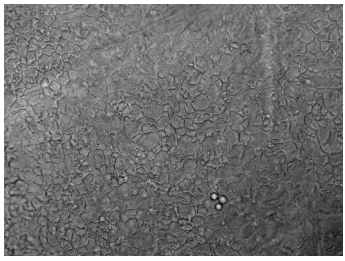
(a) Texture.



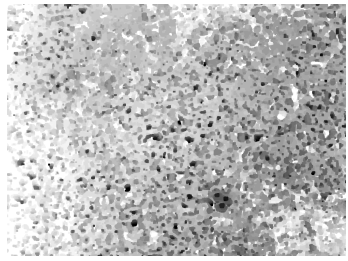
(b) Altitudes.



(c) Texture.



(d) Altitudes.



7.3.4 Tenengrad

The tenengrad method is base on a Sobel filter, see Fig.7.5.

```python
def tenengrad(I, N):
    """
    SFF measure, Tenengrad method
    I: image
    N: neighborhood size
    returns: SFF measure for each pixel, results is the same shape as I
    """
    Sx = ndimage.sobel(I, axis=0);
    Sy = ndimage.sobel(I, axis=1);
    S = np.hypot(Sx, Sy);
    T = ndimage.uniform_filter(S, N);
    return T;
```

7.3.5 Variance of Tenengrad

The variance of Tenengrad is an improvement of the Tenengrad method, see Fig.7.6.

```python
def varianceTenengrad(I, N):
    """
    SFF measure, variance of Tenengrad
    I: image
    N: neiborhood size
    returns: SFF measure for each pixel
    """
    Sx = ndimage.sobel(I, axis=0);
    Sy = ndimage.sobel(I, axis=1);
    S = np.hypot(Sx, Sy);
    vt = variance(S, N);
    return vt;
```

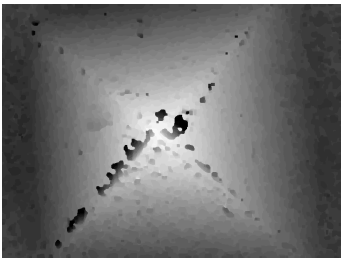
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Figure 7.5 Texture and altitude reconstruction with the SML method.

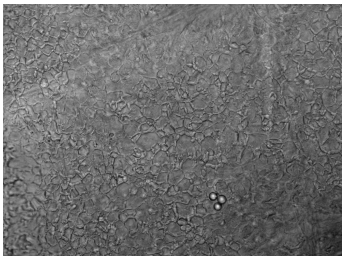
(a) Texture.



(b) Altitudes.



(c) Texture.



(d) Altitudes.

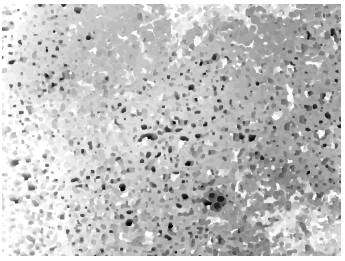
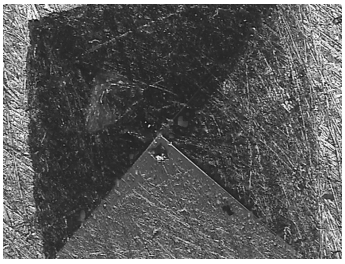
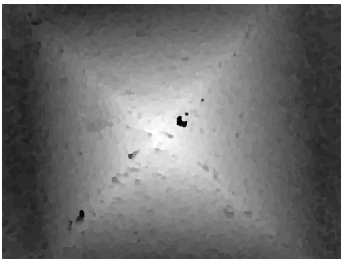


Figure 7.6 Texture and altitude reconstruction with the variance of Tenengrad method.

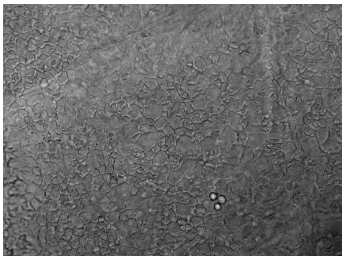
(a) Texture.



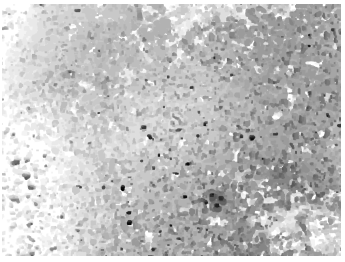
(b) Altitudes.



(c) Texture.



(d) Altitudes.



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8 Logarithmic Image Processing (LIP)

This tutorial aims to study the LIP model, which is a vector space of gray-level images, consistent with the physical laws of Weber and Fechner as well with the visual perception laws. More particularly, the LIP dynamic expansion, used for image enhancement, will be implemented as well as the Sobel LIP filter for edge detection.

The different processes will be applied on a mammographic image.

Figure 8.1 Breast



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8.1 Introduction

The LIP model (Logarithmic Image processing) has been introduced in the mid 1980s. It defines a mathematical framework for image processing in a bounded interval. It is mathematically rigorous and physically justified. For more informations, refer to [28, 16, 29].

An image is represented by its gray-tone function f, defined on a spatial domain $D \subset \mathbb{R}^2$, and with values into $[0, M[$, where $M > 0$. For all gray-tone functions S defined on D, a vector space is defined by the operations of addition $\mathbin{\triangleq}$ and multiplication $\mathbin{\triangleq}$, and by extension with the operations of subtraction $\mathbin{\triangleq}$ and negation:

$$\forall f, g \in S,\ f \mathbin{\triangleq} g = f + g - \frac{fg}{M} \tag{8.1}$$

$$\forall f \in S, \forall \lambda \in \mathbb{R},\ \lambda \mathbin{\triangleq} f = M - M\Big(1 - \frac{f}{M}\Big)^{\lambda} \tag{8.2}$$

$$\forall f \in S,\ \ \mathbin{\triangleq} f = \frac{-Mf}{M - f} \tag{8.3}$$

$$\forall f, g \in S,\ f \mathbin{\triangleq} g = M\frac{f - g}{M - g} \tag{8.4}$$

The vector space S of gray-tone functions is algebrically and topologically isomorph to the classical vector space, defined by the isomorphism φ:

$$\forall f \in S,\ \varphi(f) = -M\ln\Big(1 - \frac{f}{M}\Big) \tag{8.5}$$

The inverse isomorphism φ^{-1} is then defined by:

$$f = \varphi^{-1}(\varphi(f)) = M\Big(1 - \exp\Big(-\frac{\varphi(f)}{M}\Big)\Big) \tag{8.6}$$

This fundamental isomorphism allows the definition of the following operations on gray-tone functions:

- Dot product: $\forall f, g \in S, < f, g >_{\triangle} = \int \varphi(f)\varphi(g)$
- Euclidean norm: $\forall f \in S,\ \|f\|_{\triangle} = |\varphi(f)|_{\mathbb{R}}$, with $|\cdot|_{\mathbb{R}}$ is the classical absolute value.

8.2 Elementary LIP operations

Classically, gray-tones are coded with 8 bits, and thus one can choose $M = 256$. Be careful that there might exist sampling issues, and it might be required to considere images in the LIP space with a double precision.

>>>?

1. Implement the elementary LIP operations $\triangleq$, $\triangleq$ and $\triangleq$.
2. Test these operators on the image 'breast'.

8.3 LIP dynamic expansion

The LIP model enables to define an image transformation that expanses, in an optimal way, the overall dynamic range (gray-tones) while preserving a physical or visual sense. Let a graytone function denoted f be defined on the spatial support $D \subset \mathbb{R}^2$. Its upper and lower bounds are denoted $f_u = \sup_{x \in D} f(x)$ and $f_l = \inf_{x \in D} f(x)$, with $0 < f_l < f_u < M_0$.

The dynamic range of f on D is defined by $R(f) = f_u - f_l$. The LIP scalar multiplication of f by a real number $\lambda > 0$ yields to the following dynamic :

$$R(\lambda \triangleq f) = \lambda \triangleq f_u - \lambda \triangleq f_l \tag{8.7}$$

It has been shown [17] that there exists an optimal value $\lambda_0(f)$ that maximizes the dynamic range, i.e.:

$$R(\lambda_0(f) \triangleq f) = \max_{\lambda > 0} R(\lambda \triangleq f). \tag{8.8}$$

>>>?

1. Determine the explicit (analytic) expression of the parameter $\lambda_0(f)$.
2. Calculate the value of the parameter $\lambda_0(f)$ for the image 'breast'.
3. Enhance the image and compare the result with the histogram equalization.



In python, one can use the scikit-image module, and the `skimage.exposure.equalize_hist` function.

8.4 LIP edge detection

>>>?

1. Implement the Sobel filter within the LIP framework.
2. Compare the results with the classical Sobel filter.

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8.5. Python correction



8.5.1 Elementary operations

The most important function to code is the graytone transformation function. It considers M as the maximum value (the absolute white). This code means that the absolute white cannot be reached, and thus $f \in [0; M[$. After discretizing the gray values, $F \in [0; M-1]$.



```
"""
file LIP.py
LIP simple module
USAGE: import LIP

"""
import numpy as np

def graytone(F, M):
    # graytone function transform
    # M: maximal value
    # F: image function
    f = M-np.finfo(float).eps-F;
    return f;
```



```
def phi(f, M):
    # LIP isomorphism
    # f: graytone function
    # M: maximal value
    l = -M * np.log(-f/M+1);
    return l
```



```
def invphi(l, M):
    # inverse isomorphism
    f = M*(1-np.exp(-l/M));
    return f
```



```
def plusLIP(a, b, M):
    # LIP addition
    z = a+b-(a*b)/M;
    return z;
```



```
def timesLIP(alpha, x, M):
    # LIP multiplication by a real
    z = M-M*(np.ones(x.shape)-x/M)**alpha;
    return z;
```

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8.5.2 LIP dynamic expansion

The optimal value for dynamic expansion is given by λ_0:

$$\lambda_0(f) = \arg\max_{\lambda} \{\max(\lambda \vartriangleleft f) - \min(\lambda \vartriangleleft f)\}$$

Let $A(\lambda) = \max(\lambda \vartriangleleft f) - \min(\lambda \vartriangleleft f) = \lambda \vartriangleleft \max(f) - \lambda \vartriangleleft \min(f)$ and $B = \ln(1 - \min(f)/M)$ et $C = \ln(1 - \max(f)/M)$.

$$\begin{aligned}
A'(\lambda) = 0 &\Leftarrow [(M - M\exp(\lambda C)) - (M - M\exp(\lambda B))]' = 0 \\
&\Leftarrow [\exp(\lambda B) - \exp(\lambda C)]' = 0 \\
&\Leftarrow B\exp(\lambda B) - C\exp(\lambda C) = 0 \\
&\Leftarrow \ln(B) + \lambda B = \ln(C) - \lambda C \\
&\Leftarrow \lambda = \frac{\ln(C) - \ln(B)}{B - C} \\
&\Leftarrow \lambda = \frac{\ln(C/B)}{B - C}
\end{aligned}$$

Thus, yielding to:

$$\lambda_0(f) = \frac{\ln\left(\dfrac{\ln(1 - \max(f)/M)}{\ln(1 - \min(f)/M)}\right)}{\ln\left(\dfrac{M - \min(f)}{M - \max(f)}\right)}$$

This is coded in python by:

```python
def computeLambda(f, M):
    # compute optimal value for dynamic expansion
    B = np.log(1-f.min()/M);
    C = np.log(1-f.max()/M);
    l = np.log(C/B)/(B-C);
    return l;
```

8.5.3 Complete code

This code uses a transform called histogram equalization. This version proposes our own code for the histogram equalization (see also 2.

```python
import LIP
import numpy as np
from scipy import misc
import matplotlib.pyplot as plt
import skimage
""" Histogram equalization
"""
def histeq(im,nbr_bins=256):
   #get image histogram
   imhist,bins = np.histogram(im.flatten(),nbr_bins,normed=True)
   cdf = imhist.cumsum() #cumulative distribution function
   cdf = 255 * cdf / cdf[-1] #normalize
   #use linear interpolation of cdf to find new pixel values
   im2 = np.interp(im.flatten(),bins[:-1],cdf)

   return im2.reshape(im.shape), cdf
```

It is compared to the LIP dynamic enhancement. The results are illustrated in Fig. 8.2.

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```python
M = 256.

# reads original image
B = imageio.imread("breast.jpg");

# conversion to gray-tones (see LIP definition)
tone = LIP.graytone(B, M);
D = LIP.graytone(LIP.timesLIP(.5, tone, M), M);

# compute optimal enhancement value
l = LIP.computeLambda(tone, M);
print "lambda: %f" % l
# apply enhancement and get back into classical space
E = LIP.graytone(LIP.timesLIP(l, tone, M), M);

# histo equalization, for comparison purposes
heq,cdf = histeq(B);

# display results
plt.figure();
plt.subplot(1,3,1); plt.imshow(E/M, cmap=plt.cm.gray, vmin=0, vmax=1); plt.title
    ↪ ('dynamic expansion');
plt.subplot(1,3,2); plt.imshow(B/M, cmap=plt.cm.gray, vmin=0, vmax=1); plt.title
    ↪ ('original image');
plt.subplot(1,3,3); plt.imshow(heq/M, cmap=plt.cm.gray, vmin=0, vmax=1); plt.
    ↪ title('after histo equalization');
```

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8.5.4 Edge detection

When applying an operator in the LIP framework, it is better to apply first the isomorphisme, then the operator, and then get back into the classical space. This is applied for example for an edge detection operator.

The method applied here is the Sobel gradient. The results are presented in Fig. 8.3.

```python
# contours detection
# Sobel detection
def Sobel(I):
    sobx=cv2.Sobel(I, -1, 1, 0);
    soby=cv2.Sobel(I, -1, 0, 1);
    sob = np.sqrt(sobx**2 + soby**2);
    return sob;

# go into LIP space
tonelip = LIP.phi(tone, M);

# apply Sobel filter
sobellip = LIP.graytone(LIP.invphi(Sobel(tonelip), M), M);
imageio.imwrite("sobellip.png", sobellip);
plt.figure();
plt.subplot(1,2,1);plt.imshow(sobellip, cmap=plt.cm.gray);
plt.title('LIP Sobel edge detection')

# apply Sobel filter in the classic space
sobel = 255-Sobel(B);
plt.subplot(1,2,2); plt.imshow(sobel, cmap=plt.cm.gray);
plt.title('Sobel edge detection')
imageio.imwrite("sobel.png", sobel);
```

Figure 8.2 Comparison of the LIP enhancement with the classical histogram equalization method.

(a) Original image



(b) LIP enhancement.



(c) Histogram equalization.

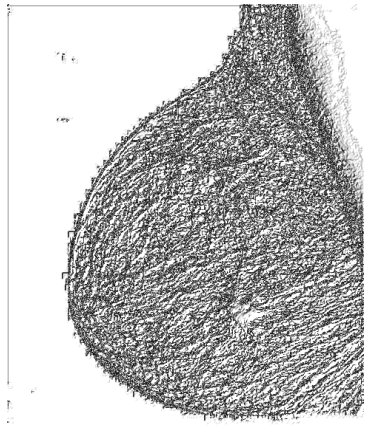


Figure 8.3 Sobel edge detection

(a) LIP Sobel edge detection.



(b) Classic Sobel edge detection.



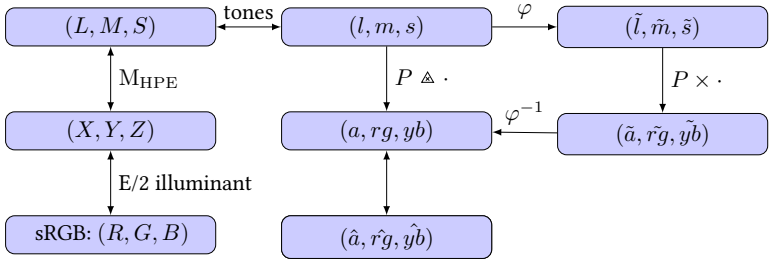
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9 Color Logarithmic Image Processing (CoLIP)

The objective of this tutorial is to have an overview of the Color Logarithmic Image Processing (CoLIP) framework [12, 13, 9, 10]. The CoLIP is a mathematical framework for the representation and processing of color images. It is psychophysically well justified since it is consistent with several human visual perception laws and characteristics. It allows to consider color images as vectors in an abstract linear space, contrary to the classical color spaces (e.g., RGB and $L^*a^*b^*$). The purpose of this tutorial is to present the mathematical fundamentals of the CoLIP by manipulating the color matching functions and the chromaticity diagram.

9.1 Definitions

This diagram summarizes the transitions between the classical RGB space and the CoLIP space. The transfer matrices are presented in the following.



9.1.1 RGB to XYZ

Here, we choose to keep the conventions of the CIE 1931, i.e. a 2° 1931 observer, with the equal energy illuminant E and the sRGB space. Depending on the illuminant, there exist many conversion matrices.

Use the module `skimage.color`.

9.1.2 XYZ to LMS

The matrix M_{HPE} (Hunt, Pointer, Estevez) is defined by:

$$\begin{pmatrix} L \\ M \\ S \end{pmatrix} = \mathrm{M_{HPE}} \times \begin{pmatrix} X \\ Y \\ Z \end{pmatrix}, \tag{9.1}$$

with

$$\mathrm{M_{HPE}} = \begin{pmatrix} 0.38971 & 0.68898 & -0.07868 \\ -0.22981 & 1.18340 & 0.04641 \\ 0.00000 & 0.00000 & 1.00000 \end{pmatrix}. \tag{9.2}$$

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9.1.3 LMS to lms

$$\forall c \in \{l, m, s\}, C \in \{L, M, S\}, c = M_0 \left(1 - \frac{C}{C_0}\right), \tag{9.3}$$

with C_0 is the maximal transmitted intensity value. M_0 is arbitrarily chosen at normalized value 100. Notice that $C \in]0; C_0]$ and $c \in [0; M_0[$.

9.1.4 CoLIP homeomorphisme

$$\forall f \in S,\ \varphi(f) = -M_0 \ln\left(1 - \frac{f}{M_0}\right).$$

The logarithmic response of the cones, as in the LIP theory, is modeled through the isomorphism φ:

$$\text{for } c \in \{l, m, s\},\ \tilde{c} = \varphi(c) = -M_0 \ln\left(1 - \frac{c}{M_0}\right), \tag{9.4}$$

where $(\tilde{l}, \tilde{m}, \tilde{s})$ are called the logarithmic chromatic tones.

9.1.5 Opponent process

$$\begin{pmatrix} \tilde{a} \\ \tilde{rg} \\ \tilde{yb} \end{pmatrix} = P \times \begin{pmatrix} \tilde{l} \\ \tilde{m} \\ \tilde{s} \end{pmatrix}, \tag{9.5}$$

with

$$P = \begin{pmatrix} 40/61 & 20/61 & 1/61 \\ 1 & -12/11 & 1/11 \\ 1/9 & 1/9 & -2/9 \end{pmatrix}. \tag{9.6}$$

9.1.6 Bounded vector space

Three channels $\hat{f} = (\hat{a}, \hat{rg}, \hat{yb})$ are defined by:

$$\hat{a} = a \tag{9.7}$$

$$\hat{rg} = \begin{cases} rg & \text{if } rg \geq 0 \\ -\triangleq rg & \text{if } rg < 0 \end{cases} \tag{9.8}$$

$$\hat{yb} = \begin{cases} yb & \text{if } yb \geq 0 \\ -\triangleq yb & \text{if } yb < 0 \end{cases} \tag{9.9}$$

9.2 Applications

9.2.1 CMF

>>>?

Represent the classical chromaticity by using the color matching functions.



The color matching functions in the different spaces, as well as the wavelength and the purple line, are provided in the matrix `'cmf.npz'`. Load it with `numpy.load`.

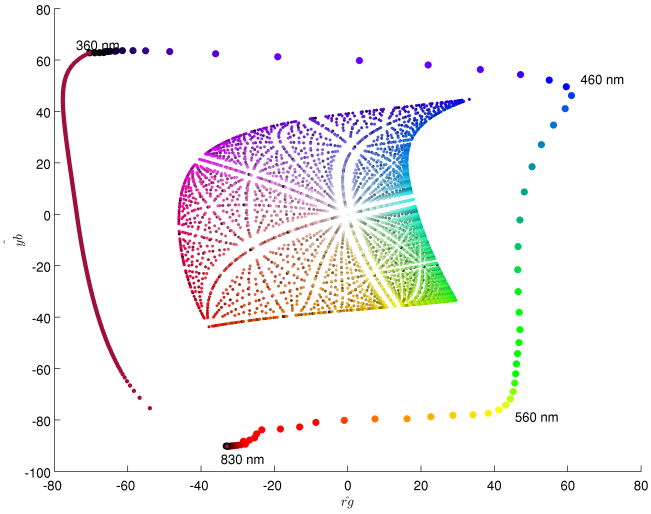
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9.2.2 CoLIP chromaticity diagram

>>>?

Represent the chromaticity diagram in the plane $(\hat{rg}, \hat{yb})$ as well as the Maxwell triangle of the RGB colors, as in Fig.9.1.

Figure 9.1 Chromaticity diagram in the plane $(\hat{rg}, \hat{yb})$.



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9.3. Python correction

```python
import numpy as np
import matplotlib.pyplot as plt
import skimage.color as color
```

First of all, the maximal value M_0 is arbitrarily fixed at 100.

```python
def getColipM0():
    # return M0 value
    return 100;
```

9.3.1 LMS tones

This is the difficult part of LIP and CoLIP. Be careful with the use of the function `eps` that returns the precision at a given double value.

```python
def lmstone(LMS):
    M0= getColipM0();
    return (M0-np.finfo(float).eps)*(1-LMS/M0);
```

9.3.2 Isomorphism

The isomorphism is the conversion into/back from the logarithmic space.

```python
def phi(f, M):
    # LIP isomorphism
    # f: graytone function
    # M: maximal value
    l = -M * np.log(-f/M+1);
    return l
```

```python
def invphi(l, M):
    # inverse isomorphism
    f = M*(1-np.exp(-l/M));
    return f
```

9.3.3 XYZ to LMS

This conversion uses the HPE matrix (Hunt, Pointer, Estevez).

```python
def XYZ2LMS(XYZ):
    """
    conversion function
    XYZ: data in XYZ space
    """
```

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```
    U=np.array([[0.38971, 0.68898, -0.07869],
      [-0.22981,1.18340, 0.04641],
      [0,     0,      1     ]]);
    m, n = XYZ[:,:,0].shape;
    print(m,n)
    XYZ = XYZ.reshape((m*n, 3)).transpose();
    print(XYZ.shape)
    LMS = np.matmul(U, XYZ);

    return LMS.transpose().reshape((m, n, 3));
```

9.3.4 Conversions into Colip space

The conversion into $(\hat{a}, \hat{rg}, \hat{yb})$ goes first into $(\tilde{a}, \tilde{rg}, \tilde{yb})$. It consists on a conversion matrix followed by the absolute value and the operation to get symmetric channels in the colip space.

```
def LMS2ARGYBhat(LMS):
    ARGYBtilde = LMS2ARGYBtilde(LMS);
    return ARGYBtilde2ARGYBhat(ARGYBtilde);
```

```
def LMS2ARGYBtilde(LMS):
    """
    conversion function
    LMS: data in LMS space
    """
    M0 = getColipM0();
    m, n, p = LMS.shape;
    LMStone = lmstone(LMS);
    LMStilde= phi(LMStone, M0);
    P = [[40/61,20/61,1/61], [1,-12/11,1/11], [1/9,1/9,-2/9 ]];

    LMStilde = LMStilde.reshape((m*n, 3)).transpose();
    ARGYBtilde = np.matmul(P, LMStilde).transpose();
    return ARGYBtilde.reshape((m, n, 3));
```

```
def ARGYBtilde2ARGYBhat(ARGYBtilde):
    """
    conversion into ARGYB tilde space
    ARGYBtilde: data in ARGYB tilde space

    """
    M0 = getColipM0();

    ARGYBhat = np.zeros(ARGYBtilde.shape);
    ARGYBhat[:,:,0] = invphi(ARGYBtilde[:,:,0], M0);

    for c in (1,2):
       tmp = np.abs(ARGYBtilde[:,:,c]);

       ARGYBhat[:,:,c] = np.sign(ARGYBtilde[:,:,c]) * invphi(tmp, M0);

    return ARGYBhat;
```

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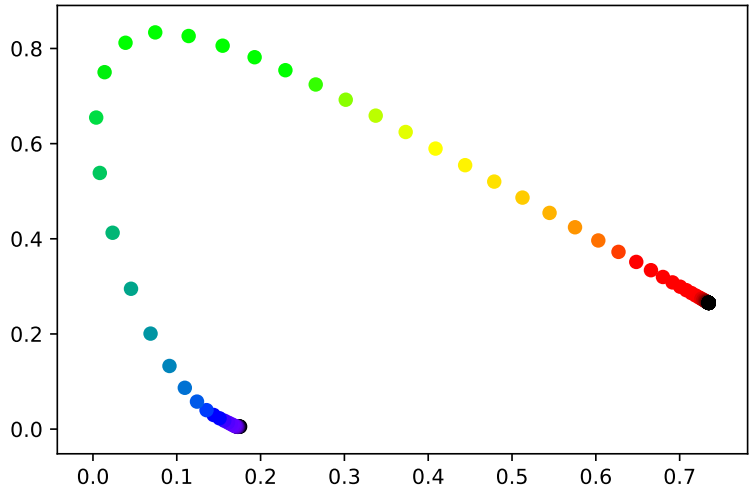
9.3.5 CMF

The color matching functions are provided for convenience. There exist many resources on the internet where they can be found. The classical diagram in the xy space (the horseshoe) is shown in Fig.9.2.

```
with np.load('cmf.npz') as data:
    cmap = data['cmap'];
    pourpresLMS = data['pourpresLMS'];
    SpecXYZ = data['SpecXYZ'];
    SpecLMS = data['SpecLMS'];
    SpecRGB = data['SpecRGB'];
    l = data['l'];

# display classical CMF in xy
xn = SpecXYZ[:,:,0]/np.sum(SpecXYZ, axis=2);
yn = SpecXYZ[:,:,1]/np.sum(SpecXYZ, axis=2);
zn = 1-xn-yn;
plt.scatter(xn, yn, c=cmap);
```

Figure 9.2 Color matching functions in the xy space.



To display the CMF and the cube of all RGB colors in the $(\hat{rg}, \hat{yb})$ space, the following code is used: The result is shown in Fig.9.3.

```
#Color matching functions in colip space
ARGYB_hat = LMS2ARGYBhat(SpecLMS);
plt.figure();
plt.scatter(ARGYB_hat[:,0,1], ARGYB_hat[:,0,2], c = cmap);
# purple line
purple_ARGYB_hat = LMS2ARGYBhat(pourpresLMS);
plt.scatter(purple_ARGYB_hat[:,0,1], purple_ARGYB_hat[:,0,2], c='black');
```

The RGB cube is first generated and then converted into the colip space.

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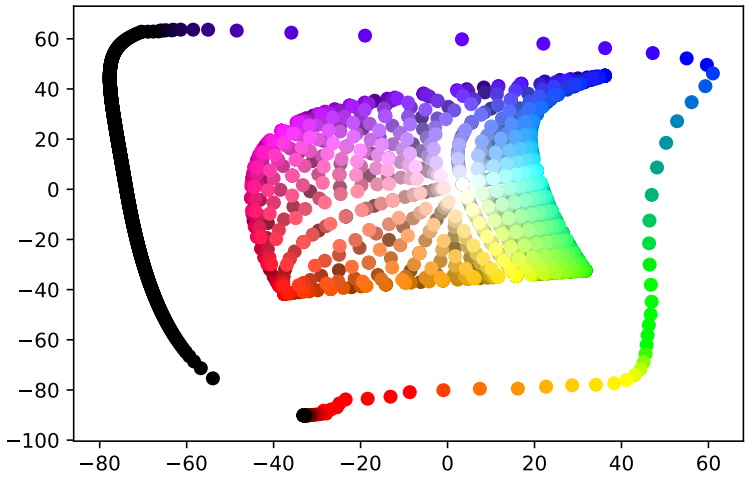
```python
# number of color in each direction
N=10;
cols = np.linspace(0, 255, num=N);
R, G, B = np.meshgrid(cols, cols, cols);

# reshape the cube for manipulation
R = R.reshape((R.size, 1));
G = G.reshape((G.size, 1));
B = B.reshape((B.size, 1));
NN = R.size;
colRGB = np.concatenate((R, G, B), axis=1);
cubeRGB = colRGB.reshape((NN, 1, 3));
colRGB = colRGB / 255;

# conversions
cubeXYZ = color.rgb2xyz(cubeRGB);
cubeLMS = XYZ2LMS(cubeXYZ);
cubeARGYBhat = LMS2ARGYBhat(cubeLMS);
plt.scatter(cubeARGYBhat[:,0,1], cubeARGYBhat[:,0,2], c=colRGB);
```

The color matching functions in the colip space are represented in Fig.9.3. A lot could be said about this diagram. For examples, one can notice the approximations in the high (red) wavelengths: this comes from the numerical approximations and the lack of data of the original CMFs. Moreover, the purple line (represented here in black) is not a line in this diagram. This raises the question of the choice of this line in (xy), which was made only by simplicity.

Figure 9.3 Color matching functions in the $(\hat{rg}, \hat{yb})$ space.



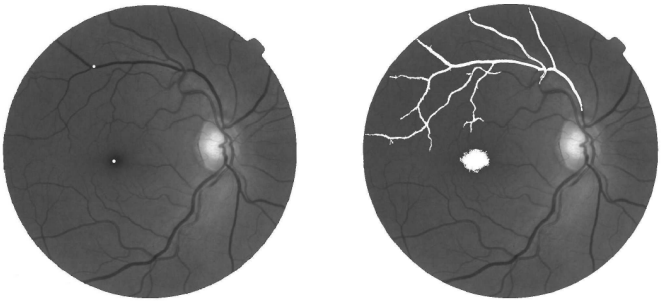
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10 GANIP

This tutorial aims to test the elementary operators of the GANIP framework.
The General Adaptive Neighborhood Image Processing (GANIP) is a mathematical framework for adaptive processing and analysis of gray-tone and color images. An intensity image is represented with a set of local neighborhoods defined for each pixel of the image to be studied. Those so-called General Adaptive Neighborhoods (GANs) are simultaneously adaptive with the spatial structures, the analyzing scales and the physical settings of the image to be addressed and/or the human visual system.

The following figure illustrates the GANs of two points on an image of retinal vessels.



The GANs are then used as adaptive operational windows for local image transformations (morphological filters, rank/order filters...) and for local image analysis (local descriptors, distance maps...).
The different processes will be applied on the following gray-tone images:

10.1 GAN

Let f be a gray-tone image. The GAN of a point x using the luminance criterion and the homogeneity tolerance m within the CLIP framework is defined as:

$$V_m^f(x) = C_{\{y;|f(y)-f(x)|\leq m\}}(x) \tag{10.1}$$

where $C_X(x)$ denotes the connected component of X holding x.

>>>?

1. Load the image 'lena' and compute the GAN of a selected point in the image.
2. Look at the influence of the homogeneity tolerance.
3. Compute the GAN of different points and comment.

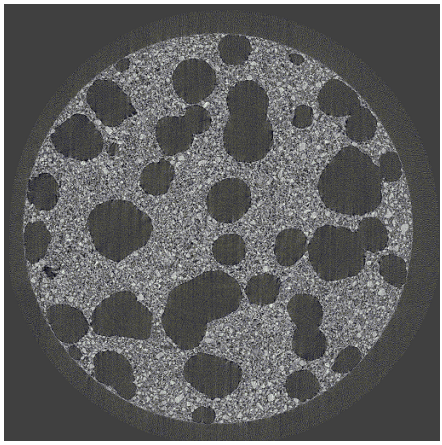
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Figure 10.1 Two example images for testing the GAN framework.

(a) lena



(b) cement paste (2-D section / X-ray tomography)



10.2 GAN Choquet filtering

The Choquet filters generalize the rank-order filters. In this exercise, we are going to implement some GAN Choquet filters such as the GAN mean operator. For each point x of the image, the mean value of all the intensities of the points inside the GAN of x is computed. So, a first algorithm consists in making a loop on the image points for computing the different GAN and the mean intensity values, but it is time consuming. Nevertheless, by using some properties of the GAN (particularly the one giving that iso-valued points can have exactly the same GAN), it is possible to create a second algorithm by making a loop on the gray-tone range:

Data: original (8-bit) image f, homogeneity tolerance m
Result: GAN mean filtered image g
for $s = 0$ **to** 255 **do**
  $seed =$ points x with intensity $f(x) = s$;
  $thresh =$ points y with intensity satisfying $s - m \leq f(y) \leq s + m$;
  $threshGAN =$ connected components of $thresh$ holding $seed$;
  foreach *label of* $threshGAN$ **do**
    $currentLabel =$ current connected component of $threshGAN$;
    $meanValue =$ intensity mean value of the image points inside $currentLabel$;
    set $g(x) = meanValue$ to the points x of $seed$ belonging to $currentLabel$;
  end
end

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>>>?

1. Implement the proposed algorithm.
2. Test this operator on the 'lena' image with different homogeneity tolerances.
3. Compare the result with a classical mean filtering.



See `scipy.ndimage.filters`.

10.3 GAN morphological filtering

As previously explained, it is also possible to compute the GAN dilation and GAN erosion by making a loop on the gray-tone range. The algorithm for the GAN dilation is:

Algorithm 2: GAN dilation

Data: original (8-bit) image f, homogeneity tolerance m
Result: GAN dilated image g
set $g(x) = 0$ for all points x;
for $s = 0$ **to** 255 **do**
  $seed =$ points x with intensity $f(x) = s$;
  $thresh =$ points y with intensity satisfying $s - m \leq f(y) \leq s + m$;
  $threshGAN =$ connected components of $thresh$ holding $seed$;
  foreach *label of* $threshGAN$ **do**
    $currentLabel =$ current connected component of $threshGAN$;
    $maxValue =$ intensity maximum value of the image points inside $currentLabel$;
    set $g(x) = max(g(x), maxValue)$ to the points x belonging to $currentLabel$;
  end
end

The algorithm for the GAN erosion is similar.

>>>?

1. Implement the GAN dilation and GAN erosion.
2. Test this operator on the 'lena' image with different homogeneity tolerances.
3. Compare the results with the classical morphological dilation and erosion..
4. Compute, test, compare and check the properties (idempotence, extensivity/anti-extensivity) of the GAN opening and GAN closing.



Compare with the functions `dilation` and `erosion` from `skimage.morphology`.

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10.4. Python correction

```python
import numpy as np
import skimage.morphology
import skimage.io
import skimage.measure
import matplotlib.pyplot as plt
import scipy.ndimage.filters
```

10.4.1 GAN

In order to show the General Adaptive Neighborhood (GAN) of one image point, the following function is implemented. Note that the function is given within the Classical Linear Image Processing (CLIP) framework, i.e. with the usual addition, subtraction and scalar multiplication. But the function could be generalized to other models such as the Logarithmic Image Processing (LIP).

```python
def GAN(A, p, m):
    """
    GAN construction
    A: grayscale image
    p: point
    m: tolerance
    """
    RES = np.zeros(A.shape);
    RES[p[0], p[1]] = 1;
    s = A[p[0], p[1]];
    thresh = np.logical_and(A>= s-m, A<=s+m);
    SE = np.ones((3,3));
    RES = skimage.morphology.reconstruction(RES, thresh, selem=SE);
    return RES;
```

In this way, we can visualize the GAN of any point of the 'Lena' image:

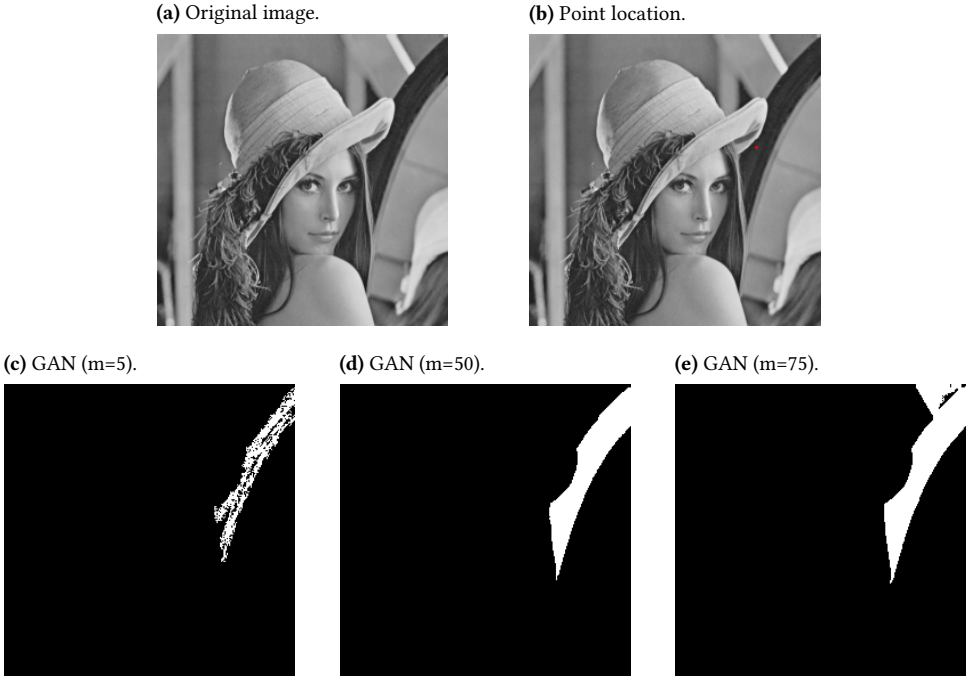
```python
I = skimage.io.imread('lena.png');
p=[100,200];
for m in 5,50,75:
    RES = GAN(I, p, m);
    plt.imshow(RES, cmap='gray');
    plt.show()
```

10.4.2 GAN Choquet filtering

In order to compute the GAN mean filtering, the basic idea is to make a loop on the image points, compute the GAN of the current point and then calculate the mean intensity of the points within the GAN. But this is time computing in the sense that two points with the same intensity can have exactly the same GAN (when one point is included in the GAN of the second point with same intensity). Therefore, a more effective way is to make a loop on the gray levels of the image. The GAN mean filtering is then implemented as:

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Figure 10.2 GAN of a specific point of the 'Lena' image using different homogeneity tolerances m within the CLIP framework.




```python
def GANmean(A, m):
    """
    GAN mean filter
    Apply mean value of the adaptive neighborhood to result
    A: original image
    m: homogeneity tolerance
    return: GAN mean filter
    """
    RES = np.zeros(A.shape).astype('float');
    SE = np.ones((3,3));
    for s in np.arange(256):
        thresh = np.logical_and(A>=s-m, A<=s+m);
        seed = A==s;
        thresh = skimage.morphology.reconstruction(seed, thresh, selem=SE);
        L,n = skimage.measure.label(thresh, connectivity=2, return_num=True);
        for l in np.arange(1, n+1):
            currentLabel = L==l;
            values = A[currentLabel];
            meanValues = np.mean(values);
            result = meanValues * np.logical_and(seed,currentLabel).astype('float');
            RES = RES + result;
    return RES;
```

Looking at this function, for the first loop on the gray levels s, we detect the GANs of the pixels with gray level s. So 'thresh' contains all these connected components (GANs), where some points with identical gray levels s can have the same GAN. 'label' enables the different GANs to be labeled. For the second loop on these GANs, we extract for each GAN its gray levels which are stored in 'values'. Afterwards, we take the mean value 'meanVaue' that is stored as the resulting gray level for pixels inside the GAN with the same gray level s.

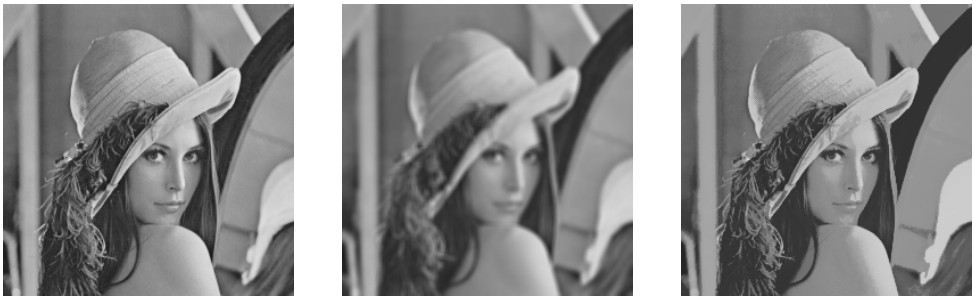
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We can compare this GAN filtering with the classical one using a fixed operational window.

```
B=scipy.ndimage.filters.uniform_filter(I, size=5);
m=30;
C = GANmean(I, m);
```

Figure 10.3 Classical ($r = 5$) vs. GAN ($m = 30$) mean filtering of the 'Lena' image.

(a) Original image. **(b)** Classical filtering ($r = 5$). **(c)** GAN filtering ($m = 30$).



You can see the blurring effect caused by the classical filtering, contrary to the adaptive GAN filtering where the transitions are much more preserved while smoothing the image.

GAN morphological filtering

The following codes enable the GAN dilation and erosion to be computed. As previously mentioned, it is based on a loop on the gray levels and not on the image points. Note that the GANs ae computed on the criterion image (it is important for satisfying the good properties of opening and closing, such as idempotence). Please notice that this function as well as the following will have the same parameters:

```
"""
A: original image
criterion: criterion image
m: tolerance
"""
```

```
def GANdilation(A, criterion, m):
    RES = np.zeros(A.shape).astype('float');
    SE = np.ones((3,3));
    for s in np.arange(256):
        thresh = np.logical_and(criterion>=s-m, criterion<=s+m);
        seed = criterion==s;
        thresh = skimage.morphology.reconstruction(seed, thresh, selem=SE);
        L,n = skimage.measure.label(thresh, connectivity=2, return_num=True);
        for l in np.arange(1, n+1):
            currentLabel = L==l;
            values = A[currentLabel];
            values.sort();
            result = currentLabel.astype('float') * values[-1];
            RES = np.maximum(RES, result);
    return RES;
```

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```python
def GANerosion(A, criterion, m):
    RES = 255 * np.ones(A.shape).astype('float');
    SE = np.ones((3,3));
    for s in np.arange(256):
        thresh = np.logical_and(criterion>=s-m, criterion<=s+m);
        seed = criterion==s;
        thresh = skimage.morphology.reconstruction(seed, thresh, selem=SE);
        L,n = skimage.measure.label(thresh, connectivity=2, return_num=True);
        for l in np.arange(1, n+1):
            currentLabel = L==l;
            values = A[currentLabel];
            values.sort();
            result = currentLabel.astype('float') * values[0] + 255*np.logical_not(
                ↪ currentLabel.astype('float'));
            RES = np.minimum(RES, result);
    return RES;
```

The following script shows the difference between classical and adaptive morphology.

```python
Cdil = GANdilation(I, m);
Cero = GANerosion(I, m);
se =skimage.morphology.disk(2);
Bdil = skimage.morphology.dilation(I, selem=se);
Bero = skimage.morphology.erosion(I, selem=se);
```

Figure 10.4 Classical ($r = 2$) vs. GAN ($m = 30$) morphological filtering of the 'Lena' image.

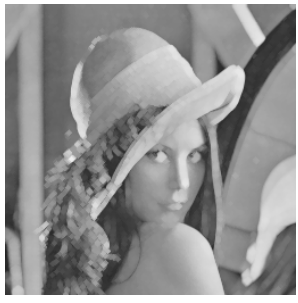
(a) Original image.



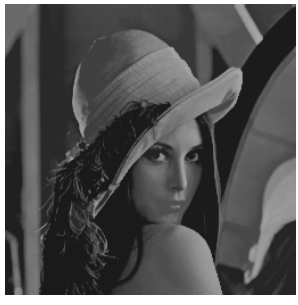
(b) Classical erosion ($r = 2$).



(c) Classical dilation ($r = 2$).



(d) GAN erosion ($m = 30$).



(e) GAN dilation ($m = 30$).



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As previously mentioned with the Choquet filtering, you can see the blurring effect caused by the classical filtering, contrary to the adaptive GAN filtering where the transitions are much more preserved while smoothing the image.

Now, we can compute the GAN opening and closing as combined operators of dilation and erosion.

```
def GANopening(A, criterion, m):
    """
    """
    temp = GANerosion(A, criterion, m);
    RES = GANdilation(temp, criterion, m);
    return RES;
```

```
def GANclosing(A, criterion, m):
    """
    """
    temp = GANdilation(A, criterion, m);
    RES = GANerosion(temp, criterion, m);
    return RES;
```

It is very important to use the same criterion h when combining these two operators of GAN dilation and erosion. It means that we compute the GANs at the beginning and therefater we use these same GANs for computing dilation and erosion. It enables the idempotence, extensivity/anti-extensivity of the GAN opening and GAN closing to be satisfied.

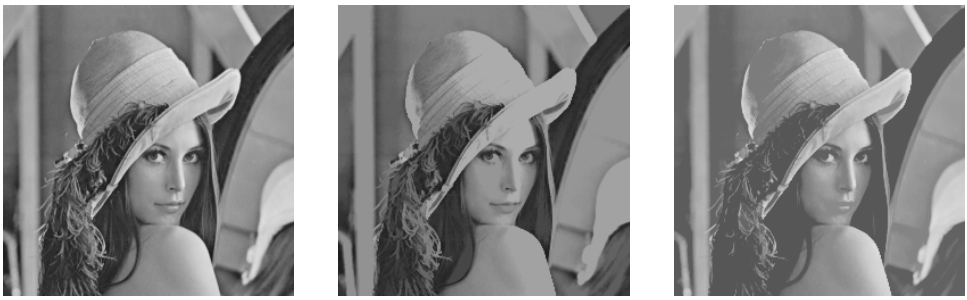
```
Copen=GANopening(I, I, m);
Cclose=GANclosing(I, I, m);

# classical open close
Bopen = skimage.morphology.opening(I, selem=se);
Bclose= skimage.morphology.closing(I, selem=se);
```

The result of such morphological filters is presented in Fig.10.5.

Figure 10.5 GAN ($m = 30$) opening and closing of the 'Lena' image.

(a) Original image. **(b)** GAN opening ($m = 30$). **(c)** GAN closing ($m = 30$).



We can check some properties of these morphological filters such as extensivity/anti-extensivity and idempotence:

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```
Copen2 = GANopening(Copen, I, m);
Cclose2= GANclosing(Cclose, I, m);
if np.max(np.abs(Copen2-Copen))==0:
   print("OK: idempotence in opening");
else:
   print("error in opening");

if np.max(np.abs(Cclose2-Cclose))==0:
   print("OK: idempotence in closing");
else:
   print("error in opening");
```

```
#%% check extensivity and anti-extensivity
if np.all(Copen<=I):
   print("OK: extensivity");
else:
   print("error in extensivity");

if np.all(Cclose>=I):
   print("OK: anti-extensivity");
else:
   print("error in anti-extensivity");
```

Result verifies these properties.

```
OK: idempotence in opening
OK: idempotence in closing
OK: extensivity
OK: anti-extensivity
```

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11 Image Filtering using PDEs

This tutorial aims to process images with the help of partial differential equations.

The different processes will be applied on the following MR image Fig. 11.1.

Figure 11.1 MRI image of a human brain.



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Notations

The different operators used here are:

$$\vec{A} = \begin{pmatrix} A_x \\ A_y \end{pmatrix} \tag{11.1}$$

$$\operatorname{div} \overrightarrow{A} = \frac{\partial A_x}{\partial x} + \frac{\partial A_y}{\partial y} \tag{11.2}$$

$$\vec{\operatorname{grad}}\, u(x,y) = \nabla u = \begin{pmatrix} \frac{\partial u}{\partial x} \\ \frac{\partial y}{\partial y} \end{pmatrix} \tag{11.3}$$

The Laplacian operator is denoted $\Delta u = \nabla^2 u = \operatorname{div} \overrightarrow{\operatorname{grad}}\, u$. A numerical approximation can be used, but is not recommanded in this tutorial.

11.1 Linear diffusion

The heat equation is defined as follows:

$$\begin{cases} \dfrac{\partial u}{\partial t}(x,y,t) &= \operatorname{div}(\nabla u(x,y,t)) \\ &= \dfrac{\partial^2 u}{\partial x^2}(x,y,t) + \dfrac{\partial^2 u}{\partial y^2}(x,y,t) \\ u(x,y,0) &= f(x,y) \end{cases} \tag{11.4}$$

If $f(x,y)$ is an image (with $(x,y) \in D \subset \mathbb{R}^2$, D is the spatial support), this defines a filtering method that is equivalent to the convolution of f by a Gaussian function [19]. This equation can be solved by a finite difference numerical method.

11.1.1 Numerical scheme

The following notations are employed. N, S, E, W stand for north, south, east and west.

$$\begin{array}{rcl} +\delta^N u & = & \frac{u(x,y+h)-u(x,y)}{h} \\ -\delta^S u & = & \frac{u(x,y-h)-u(x,y)}{h} \\ -\delta^E u & = & \frac{u(x-h,y)-u(x,y)}{h} \\ +\delta^W u & = & \frac{u(x+h,y)-u(x,y)}{h} \end{array} \tag{11.5}$$

Thus, the numerical scheme is (h has value 1):

$$\frac{u^{t+1}-u^t}{\delta t} = \frac{1}{h}\left\{\delta^N u - \delta^S u + \delta^E u - \delta^W u\right\} \tag{11.6}$$

>>>?

1. Code the numerical scheme. It should use two parameters: the number of iterations n, and the step time δt.
2. Filter the original image by varying the parameters of the discrete diffusion process.
3. Comment the filtering results. Compare the results with the Gaussian filter.

11.2 Nonlinear diffusion

Image filtering by nonlinear diffusion reduces noise in a controled way. The diffusion coefficient is locally adapted, becoming negligible as object boundaries are approached. The heat equation is replaced by the following PDE:

$$\left\{ \begin{array}{rcl} \frac{\partial u}{\partial t}(x,y,t) & = & \mathrm{div}\left(c(\|\nabla u(x,y,t)\|) \cdot \nabla u(x,y,t)\right) \\ u(x,y,0) & = & f(x,y) \end{array} \right. \tag{11.7}$$

with c the diffusion fonction satisfying the following properties:

- $c(0) = 1$,
- $\lim\limits_{s \to +\infty} sc(s) = 0$,
- $\forall s > 0, c'(s) \leq 0$.

Perona and Malik have proposed 2 diffusion coefficients [27, 5]:

- $c_1 : \exp\left(-\left(\frac{s}{\alpha}\right)^2\right)$,
- $c_2 : \frac{1}{1+\left(\frac{s}{\alpha}\right)^2}$.

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11.2.1 Numerical scheme

The numerical scheme is the following:

$$\frac{u^{t+1}-u^t}{\delta t} = \frac{1}{h^2}\{c(|\delta^N u|)\cdot\delta^N u + c(|\delta^S u|)\cdot\delta^S u + c(|\delta^E u|)\cdot\delta^E u + c(|\delta^W u|)\cdot\delta^W u\} \tag{11.8}$$

>>>?

1. Code the numerical scheme
2. Filter the original image by varying the parameters of the discrete nonlinear diffusion process.
3. Comment and compare the filtering results with the previous scheme.

11.3 Degenerate diffusion

The following degenerate PDEs have been shown to be equivalent to the morphological operators of dilation and erosion (using a disk as structuring element, see tutorial on mathematical morphology):

$$\begin{cases} \frac{\partial u}{\partial t}(x,y,t) &= +\|\nabla u(x,y,t)\| \\ u(x,y,0) &= f(x,y) \end{cases} \tag{11.9}$$

$$\begin{cases} \frac{\partial u}{\partial t}(x,y,t) &= -\|\nabla u(x,y,t)\| \\ u(x,y,0) &= f(x,y) \end{cases} \tag{11.10}$$

11.3.1 Numerical schemes

The previous numerical scheme is easy to find, but the results present large differences with the dilation and erosion operators (shocks due to discontinuities in the original image). This is why the following numerical scheme is preferred [23]:

For the erosion:

$$\frac{u^{t+1}-u^t}{\delta t} = \frac{1}{h^2}\sqrt{max^2(0,-\delta^N u) + min^2(0,-\delta^S u)\ldots + max^2(0,-\delta^W u) + min^2(0,-\delta^E u)} \tag{11.11}$$

For the dilation:

$$\frac{u^{t+1}-u^t}{\delta t} = \frac{1}{h^2}\sqrt{min^2(0,-\delta^N u) + max^2(0,-\delta^S u)\ldots + min^2(0,-\delta^W u) + max^2(0,-\delta^E u)} \tag{11.12}$$

>>>?

1. Code the numerical scheme.
2. Filter the original image while varying the parameters of the discrete degenerate diffusion process.
3. Comment the morphological filtering results and compare the numerical scheme to the approach with operational windows.

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11.4. Python correction

```python
import numpy as np
from scipy import ndimage , misc
import matplotlib.pyplot as plt
```

11.4.1 Linear diffusion

The linear diffusion filter is equivalent to the classical gaussian filter. The gradients are decomposed into the 4 directions so that the next developments (non linear diffusion filters) are made easy.

```python
def linearDiffusion(I, nbIter, dt):
    # linear diffusion # I: image # nbIter: number of iterations # dt: step time
    hW = np.array([[1, -1, 0]]);
    hE = np.array([[0,-1,1]]);
    hN = np.transpose(hW);
    hS = np.transpose(hE);
    Z = I.copy();
    for i in range(nbIter):
        gW = ndimage.convolve(Z, hW, mode='constant');
        gE = ndimage.convolve(Z, hE, mode='constant');
        gN = ndimage.convolve(Z, hN, mode='constant');
        gS = ndimage.convolve(Z, hS, mode='constant');
        Z = Z + dt*(gW+gE+gN+gS);
    return Z
```

The code to filter images is presented as follows. Results are in Fig. 11.2.

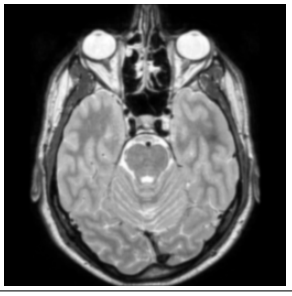
```python
I = imageio.imread("cerveau.png")/255.;
F = linearDiffusion(I, 50, .05);
F2 = linearDiffusion(I, 200, .05);
plt.subplot(1,3,1);
plt.imshow(I, cmap=plt.cm.gray);
plt.subplot(1,3,2);
plt.imshow(F, cmap=plt.cm.gray);
plt.subplot(1,3,3);
plt.imshow(F2, cmap=plt.cm.gray);
```

Figure 11.2 Linear diffusion filter. Contours are not preserved: this is equivalent to a Gaussian filter.

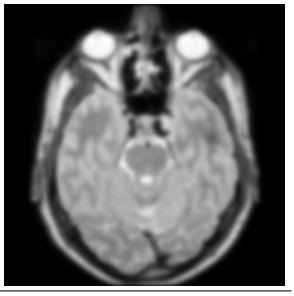
(a) Original image.



(b) Linear diffusion filter, with $\alpha = 0.1$, $dt = 0.05$ and 10 iterations.



(c) Linear diffusion filter, with $\alpha = 0.1$, $dt = 0.05$ and 50 iterations.



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11.4.2 Nonlinear diffusion

The nonlinear diffusion is an adaptation of the diffusion to the informations contained in the images. These informations are high frequency components. The following diffusion coefficient is proposed by Perona and Malik.

```python
def c(I, alpha):
    # diffusion coefficient
    # I: image
    # alpha: diffusion parameter
    return np.exp(-(I/alpha)**2);
```

The gradients are evaluated in the 4 directions, a specific coefficient is thus applied to each one.

```python
def nonlinearDiffusion(I, nbIter, alpha, dt):
    # linear diffusion
    # I: image
    # nbIter: number of iterations
    # dt: step time
    hW = np.array([[1, -1, 0]]);
    hE = np.array([[0,-1,1]]);
    hN = np.transpose(hW);
    hS = np.transpose(hE);

    Z = I.copy();

    for i in range(nbIter):
       #print "%d" % i
       gW = ndimage.convolve(Z, hW, mode='constant');
       gE = ndimage.convolve(Z, hE, mode='constant');
       gN = ndimage.convolve(Z, hN, mode='constant');
       gS = ndimage.convolve(Z, hS, mode='constant');

       Z= Z + dt*(c(np.abs(gW), alpha)*gW + c(np.abs(gE), alpha)*gE
       + c(np.abs(gN), alpha)*gN + c(np.abs(gS), alpha)*gS);

    return Z
```

The script to filter the images, for $\alpha = 0.1$, $\mathrm{d}t = 0.05$ and for 10 and 50 iterations, is the following. Results are presented in Fig. 11.3.

```python
alpha = 0.1;
dt = .05;
I = imageio.imread("cerveau.png")/255.;

F = nonlinearDiffusion(I, 10, alpha, dt);
F2= nonlinearDiffusion(I, 50, alpha, dt);
```

11.4.3 Degenerate diffusion

Erosion and dilation can theoretically be coded with this numerical scheme. However, some numerical problems appear in the first version, which are corrected in the second version.

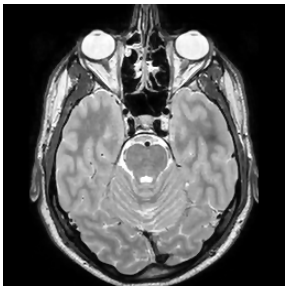
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Figure 11.3 Nonlinear diffusion filter. Contours are preserved.

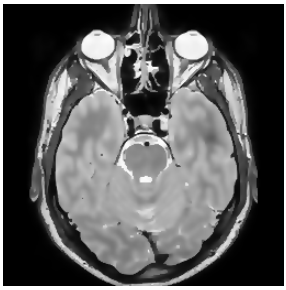
(a) Original image.



(b) Non linear diffusion filter, with $\alpha = 0.1$, $dt = 0.05$ and 10 iterations.



(c) Non linear diffusion filter, with $\alpha = 0.1$, $dt = 0.05$ and 50 iterations.



First version

This first version is the direct transcription of the numerical scheme. As observed in Fig.11.4, shocks (peaks) appear after a few iterations.

```
def degenerateDiffusion1(image, nbIter, dt):
    # degenerate diffusion
    # I: image
    # nbIter: number of iterations
    # dt: step time
    h = np.array([[-1,0,1]]);
    ht= np.transpose(h);
    Zdilation = image;
    Zerosion = image;
    for i in range(nbIter):
        gH = ndimage.convolve(Zdilation, h , mode='constant');
        gV = ndimage.convolve(Zdilation, ht, mode='constant');
        jH = ndimage.convolve(Zerosion, h , mode='constant');
        jV = ndimage.convolve(Zerosion, ht, mode='constant');
        Zdilation = Zdilation + dt*np.sqrt(gV**2 + gH**2);
        Zerosion = Zerosion + dt*np.sqrt(jV**2 + jH**2);
    return (Zdilation, Zerosion)
```

Figure 11.4 Mathematical morphology operations by diffusion.

(a) Dilation by diffusion, for $dt = 0.05$ and $nbIter = 10$.



(b) Dilation by diffusion, for $dt = 0.05$ and $nbIter = 50$.



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More sophisticated version

Another scheme, more numerically stable, can be preferred to the previous one. Results are presented in Fig. 11.5.

```python
def degenerateDiffusion2(image, nbIter, dt):
    # degenerate diffusion
    # I: original image
    # nbIter: number of iterations
    # dt: step time
    hW = np.array([[1,-1,0]]);
    hE = np.array([[0, -1, 1]]);
    hN = np.transpose(hW);
    hS = np.transpose(hE);
    Zdilation = image;
    Zerosion = image;

    for i in range(nbIter):
        gW = ndimage.convolve(Zdilation, hW, mode='constant');
        gE = ndimage.convolve(Zdilation, hE, mode='constant');
        gN = ndimage.convolve(Zdilation, hN, mode='constant');
        gS = ndimage.convolve(Zdilation, hS, mode='constant');

        jW = ndimage.convolve(Zerosion, hW, mode='constant');
        jE = ndimage.convolve(Zerosion, hE, mode='constant');
        jN = ndimage.convolve(Zerosion, hN, mode='constant');
        jS = ndimage.convolve(Zerosion, hS, mode='constant');

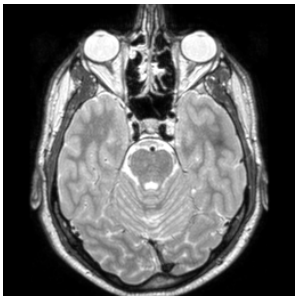
        g = np.sqrt( np.minimum(0, -gW)**2 + np.maximum(0, gE)**2 + np.minimum(0, -
            ↪ gN)**2 + np.maximum(0, gS)**2);
        j = np.sqrt( np.maximum(0, -jW)**2 + np.minimum(0, jE)**2 + np.maximum(0, -
            ↪ jN)**2 + np.minimum(0, jS)**2);

        Zdilation = Zdilation + dt * g;
        Zerosion = Zerosion -dt * j;

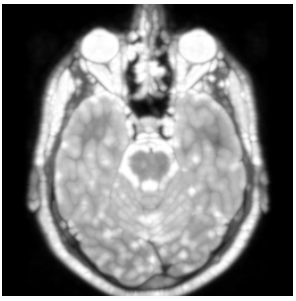
    return Zdilation, Zerosion
```

Figure 11.5 Mathematical morphology operations by diffusion, sophisticated version.

(a) Dilation by diffusion, for $dt = 0.05$ and nbIter=10.



(b) Dilation by diffusion, for $dt = 0.05$ and nbIter=50.



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12 Multiscale Analysis

This tutorial aims to study some multiscale image processing and analysis methods, based on pyramidal and scale-space representations.

The different processes will be applied on the following MR image.

Figure 12.1 Brain MR image.



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12.1 Pyramidal decomposition and reconstruction

12.1.1 Decomposition

Algorithm 3: The algorithm of the pyramidal decomposition

Data: image A_0
Result: pyramid of approximations $\{A_i\}_i$, pyramid of details$\{D_i\}_i$
for *i=1 to 3* **do**
  filtering: $F = filt(A_{i-1})$;
  subsampling: $A_i = ech(F, 0.5)$;
  details: $D_i = A_{i-1} - ech(A_i, 2)$;
end

The initial image (with the highest resolution), denoted A_0, represents the level 0 of the pyramid. To build the pyramid, we successively carry out the following steps:

1. a Gaussian filtering,
2. a subsampling,
3. a calculation of the details (residues).

>>>?

Make a pyramidal decomposition with 4 levels of the image 'brain'.

12.1.2 Reconstruction

To reconstruct the original image, we carry out the following steps at each level of the pyramid:

1. an oversampling,
2. an addition of the details.

Algorithm 4: The algorithm of the pyramidal reconstruction

Data: image A_3, pyramid of details$\{D_i\}_i$
Result: reconstructed pyramid $\{B_i\}_i$
initialization : $B_3 = A_3$;
for *i=3 to 1* **do**
1 oversampling: $R = ech(B_i, 2)$;
2 adding details: $B_{i-1} = R + D_i$
end

>>>?

1. Reconstruct the original image from the last level of the pyramid.
2. Make the same reconstruction without adding the details.
3. Calculate the resulting error between the reconstruted image and the original image.

12.2 Scale-space decomposition and multiscale filtering

We are going to decompose (without any sampling) the image with the highest resolution with a morphological operator, dilation or erosion. The resulting images will have the same size.

12.2.1 Morphological multiscale decomposition

>>>?

Build the two scale-space decompositions of the 'brain' image, with a disk of increasing radius as a structuring element

Informations

See the functions `morphology.erosion` and `morphology.dilation` from `skimage`.

12.2.2 Kramer and Bruckner multiscale decomposition

Now, we are going to use the iterative filter of Kramer and Bruckner [20] defined as:

$$MK_B^n(f) = K_B(MK_B^{n-1}(f)) \tag{12.1}$$

where B denotes a disk of a fixed radius r, and:

$$K_B(f)(x) = \begin{cases} D_B(f)(x) & \text{if } D_B(f)(x) - f \leq f - E_B(f)(x) \\ E_B(f)(x) & \text{otherwise} \end{cases} \tag{12.2}$$

where $D_B(f), E_B(f)$ represent respectively the dilation and the erosion of the image f with the structuring element B.

>>>?

Implement and test this filter on the image 'brain' for different values of n.

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12.3. Python correction

12.3.1 Pyramidal decomposition and reconstruction

Decomposition

The following function makes the decomposition of the Laplacian and Gaussian pyramids at the same time. The Laplacian pyramid can be reconstructed without any additional information. This is illustrated in Fig. 12.2.

```python
def LaplacianPyramidDecomposition(Image, levels, interp='bilinear'):
    """
    Laplacian / Gaussian Pyramid
    The last image of the laplacian pyramid allows a full reconstruction of the original image.
    Image: original image, float32
    levels: number of levels of decomposition
    interp: interpolation mode for downsizing the image

    returns: pyrL, pyrG: Laplacian and Gaussian pyramids, respectively, as a list of arrays
    """

    pyrL = [];
    pyrG = [];

    sigma = 3.;
    for l in range(levels):
        prevImage = Image.copy();
        g = ndimage.gaussian_filter(Image, sigma);
        print(g.dtype)

        Image = misc.imresize(g, .5, interp=interp, mode='F');
        primeImage= misc.imresize(Image, prevImage.shape, interp=interp, mode='F');

        pyrL.append(prevImage -primeImage);
        pyrG.append(prevImage);

    pyrL.append(Image);
    pyrG.append(Image);
    return pyrL, pyrG;
```

Informations

Notice that with the `misc.imresize` function, the float mode of the operation has to be specified.

Reconstruction

The reconstruction is straighforward and exact because of the construction of the residue. The details can be filtered (removed for example), thus giving the following result Fig. 12.3.

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Figure 12.2 Gaussian and Laplacian pyramids, for 3 levels of decomposition. The Laplacian pyramid in addition to the last level of the Gaussian pyramid is required to exactly reconstruct the original image.

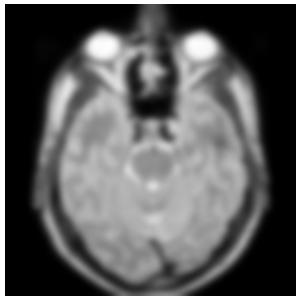
(a) Original image.



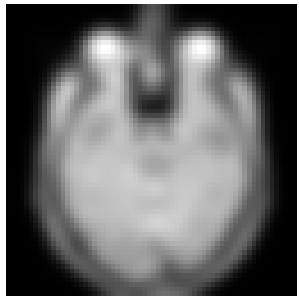
(b) Gaussian pyramid level 1.



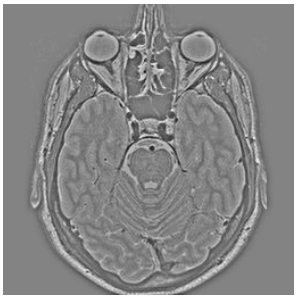
(c) Level 2.



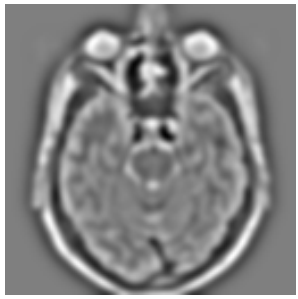
(d) Level 3.



(e) Laplacian pyramid level 1.



(f) Level 2.



(g) Level 3.



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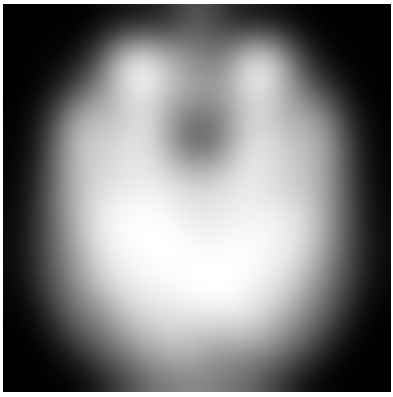
```python
def LaplacianPyramidReconstruction(pyr, interp='bilinear'):
    """
    Reconstruction of the Laplacian pyramid, starting from the last image
    pyr: pyramid of images (list of arrays)
    interp: interpolation mode, for upsizing the image
    returns: Image, reconstructed image
    """

    Image = pyr[-1];
    for i in range(len(pyr)-2, -1, -1):
        Image = pyr[i] + misc.imresize(Image, pyr[i].shape, interp=interp, mode='F'
            ↪ );

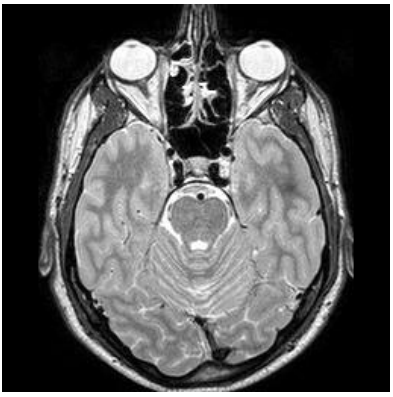
    return Image;
```

Figure 12.3 Reconstruction of the Laplacian pyramid.

(a) Reconstruction of the pyramid without any detail.



(b) Reconstruction of the pyramid with all the details.



12.3.2 Scale-space decomposition and multiscale filtering

The pyramid of erosions and dilations is illustrated in Fig.12.4.

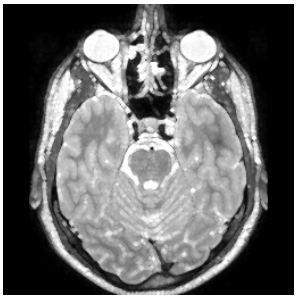
```python
def morphoMultiscale(I, levels):
    """
    Morphological multiscale decomposition
    I: original image, float32
    levels: number of levels, int

    returns: pyrD, pyrE: pyramid of Dilations/Erosions, respectively
    """
    pyrD=[];
    pyrE=[];
    for r in np.arange(1,levels):
        se = morphology.disk(r);
        pyrD.append( morphology.dilation(I, selem=se));
        pyrE.append( morphology.erosion(I, selem=se));
    return pyrD, pyrE;
```

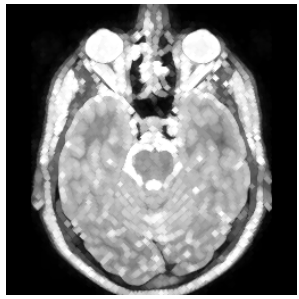
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Figure 12.4 Morphological multiscale decomposition by dilation and erosion.

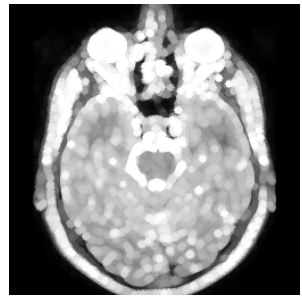
(a) Dilation scale 1.



(b) Dilation scale 2.



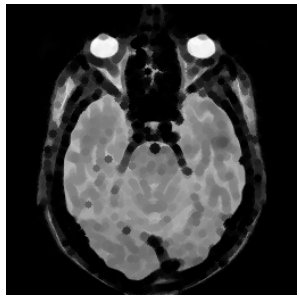
(c) Dilation scale 3.



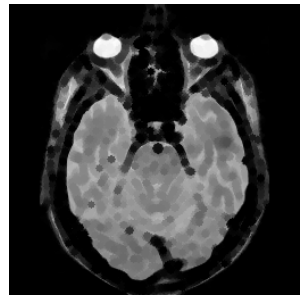
(d) Erosion scale 1.



(e) Erosion scale 2.



(f) Erosion scale 3.



12.3.3 Kramer and Bruckner multiscale decomposition

The results are illustrated in Fig.12.5.

Figure 12.5 Kramer and Bruckner multiscale decomposition, with $r = 5$.

(a) MK_B^1.



(b) MK_B^2.



(c) MK_B^3.



```python
def kb(I, r):
    """
    Elementary Kramer/Bruckner filter. Also called toggle filter.
    I: image
    r: radius of structuring element (disk), for max/min evaluation
    """
    se = morphology.disk(r);
    D=morphology.dilation(I, selem=se);
```

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```
    E=morphology.erosion(I, selem=se);
    difbool = D-I < I-E;
    k = D*difbool + E * (~difbool);
    return k;
```



```
def KBmultiscale(I, levels, r=1):
    """
    Kramer and Bruckner multiscale decomposition

    I: original image, float32
    pyrD: pyramid of Dilations
    pyrE: pyramid of Erosions

    returns: MKB: Kramer/Bruckner filters
    """
    MKB = [];
    MKB.append(I);
    for i in range(levels):
       MKB.append(kb(MKB[i-1], r));
    return MKB
```

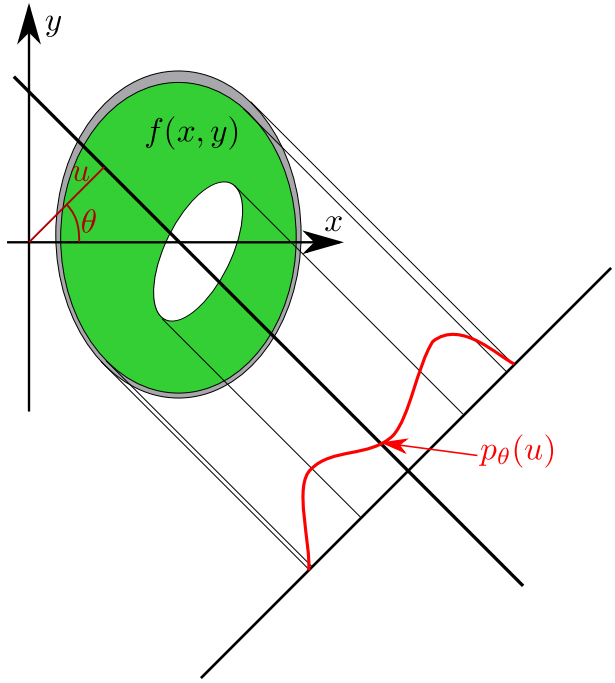
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13 Introduction to tomographic reconstruction

13.1 X ray tomography

Figure 13.1 Radon transform notations.



An X-ray beam (considered as monochromatic) going through objects is attenuated, following a logarithmic law (f is the linear attenuation, v an elementary volume, I the intensity of the beam entering the volume dv and $I + dI$ the intensity exiting the volume):

$$\log \frac{I + dI}{I} = -f dv$$

By integrating this formula on a line D (direction of the beam), yields:

$$I = I_0 \exp\left(\int_D f(x, y) dv\right)$$

where $f(x, y)$ is the attenuation at point (x, y). This principle is used in scanners, scintigraphy, PET...

13.2 Acquisition simulation

This first exercise will allow us to simulate the projections. The mathematical operator behing this is the Radon transform.

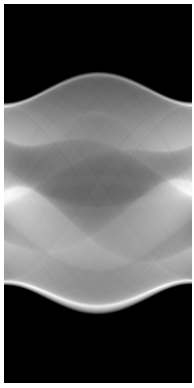
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>>>?

- Generate a "phantom" image of size 256×256. Display it. Notice that any image may be good for testing the simulation and reconstruction via backprojection.
- To simulate the attenation process, considere the sum of all gray levels of all pixels. Angles of projections will be between 0 and 180 degres with a unit step. The result is presented as a sinogram $p_\theta(u)$ (see Fig. 13.2), with u the length (in ordinates), and θ the projection angle (in abscissa).

Figure 13.2 Simulated sinogram of the phantom image.

(a) Sinogram.



(b) Phantom image.



13.3 Backprojection algorithm

A non exact reconstruction is the backprojection operator B (it is not the inverse Radon transform). It attributes the value $p_\theta(u)$ to each point of the projection line that gave this attenation, and sum up all contributions from all projections (at the different angles).

$$B[p](x, y) = \int_0^\pi p_\theta(x \cos\theta + y \sin\theta) d\theta$$

A simple (but slow) method is described to compute the backprojection. p_θ is the attenuation vector for a given angle θ.

- Use a command to replicate a matrix to obtain the contribution of each line D, like on Fig. 13.3a.
- Each contribution line D should be turned of a certain angle to be added to the overall contribution. This backprojection is really fuzzy compared to the original phantom image (see Fig. 13.3b).

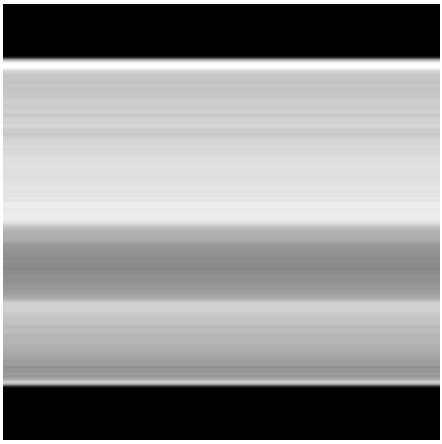
13.4 Filtered backprojection

It can be shown that backprojection is in fact the convolution of f by a filter. A solution would be to make a deconvolution in the Fourier domain. The solution used here is the filtered backprojection.

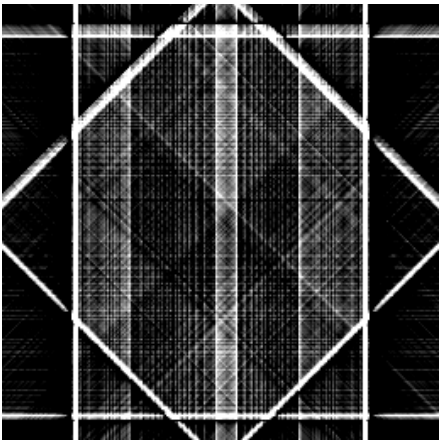
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Figure 13.3 Backprojection

(a) Contribution of a line D before rotation.



(b) Reconstruction after projection every 45 degrees (4 projections).



Numerous filters can be used. Among them, the Ram-Lak filter RL is approximated by :

$$\begin{aligned} k \in [-B;B] \subset \mathbb{N}, RL(k) &= \frac{\pi}{4} \text{ if } k = 0 \\ &= 0 \text{ if } |k| \text{ is even} \\ &= \frac{-1}{\pi k^2} \text{ if } |k| \text{ is odd} \end{aligned}$$

>>>?

- Write a function that generates this filter (see prototype). The parameter $width$ is the number of points of the resulting vector.
- Modify the backprojection algorithm to filter (by convolution of the projection vector) each contribution line before the summation. Observe the improved result.

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13.5. Python correction

```python
import numpy as np
import matplotlib.pyplot as plt

from skimage.io import imread
from skimage.transform import radon, rescale, rotate
from scipy.signal import convolve
import skimage.io
```

13.5.1 Acquisition simulation

The phantom image is first loaded and displayed.

```python
# Read image
image = imread("phantom.png", as_gray=True)
image = image[:,:,0];
plt.imshow(image, cmap='gray');
```

The simulation of the projection is simply an addition of all gray-levels of the pixels, after rotating the image in order to simulate the rotation of the object (or of the sensor). See Fig.13.3a

```python
def simuProjection(I, theta):
    """
    simulation of the generation of a sinogram
    I : original image (phantom for example)
    theta: angles of projection
    """
    N = I.shape[1];
    M = len(theta);
    S = np.zeros((N,M));
    for i,ang in enumerate(theta):
        image1 = rotate(I, ang);
        S[:,i] = np.sum(image1, axis=1);

    return S;
```

13.5.2 Backprojection algorithm

The backprojection algorithm will sum-up all the contributions of each projection.

```python
def backprojection(P, theta, filtre):
    """
    Backprojection of
    P: image
    theta: list of projection angles
    filtre: bool, True if filtered
    """
```

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```
    N = P.shape[0];
    R = np.zeros((N,N));

    # in case of filtered back-projection
    if filtre:
       h = RamLak(31);

    # loops over all angles
    for i,ang in enumerate(theta):
       proj = P[:,i];

       # filtered back-projection
       if filtre:
          proj = convolve(proj, h, mode='same');

       proj2 = np.matlib.repmat(proj, N, 1);
       proj2 = rotate(proj2, ang);
       R = R + proj2;
    return R.transpose();
```

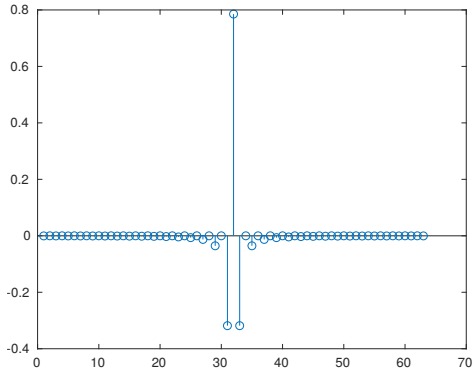
The results is better in the case of a filtered backprojection. The RamLak function is provided and illustrated in Fig.13.4.

```
def RamLak(width):
    """
    Ramlak filter of size width
    width must be odd
    """
    ramlak = np.zeros((2*width+1,));
    for indice, val in enumerate(np.arange(-width, width+1)):
      val = np.abs(val);

      if val==0: # center
         ramlak[indice]=np.pi/4;
      else:
        if val%2==1: # even indices
           ramlak[indice]=-1/(np.pi*val**2);
        else: # odd indices
           ramlak[indice]=0;

    return ramlak;
```

Figure 13.4 RamLak function.



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The reconstruction of the original image is obtained by the following code:

```
# Performs unfiltered backprojection
ubp = backprojection(P, theta, False);
plt.figure();
plt.imshow(ubp, cmap='gray');
plt.show()

# Performs filtered backprojection
fbp = backprojection(P, theta, True);
plt.figure();
plt.imshow(fbp, cmap='gray');
plt.show()
```

Figure 13.5 Reconstruction by backprojection.

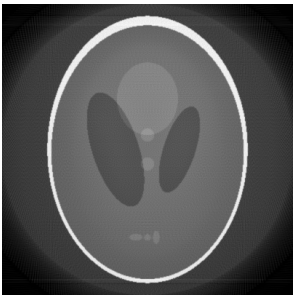
(a) Original phantom image.



(b) Unfiltered backprojection.



(c) Filtered backprojection.



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Second part

Mathematical Morphology

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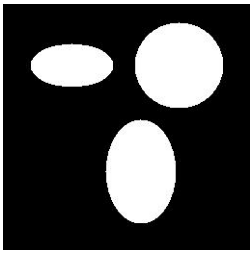
14 Binary Mathematical Morphology

The objective of this tutorial is to process binary images with the elementary operators of mathematical morphology. More particularly, different image transformations, based on the morphological reconstruction, will be studied (closing holes, removing small objects…).

The different transformations will be applied on the following images Fig. 14.1:

Figure 14.1 Images to use for this tutorial.

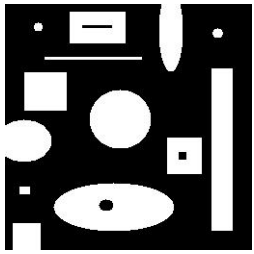
(a) I_1.



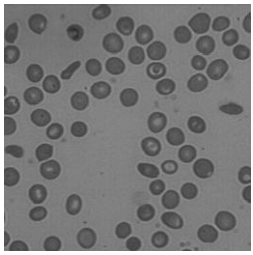
(b) M.



(c) I_2.



(d) Cells.



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14.1 Introduction to mathematical morphology

Mathematical morphology started in the 1960s with Serra and Matheron [38]. It is based on Minkowski addition of sets. The main operators are erosion and dilation, and by composition, opening and closing. More informations can be found in [40].

The erosion of a binary set A by the structuring element B is defined by:

$$\varepsilon_B(A) = A \ominus B = \{z \in A | B_z \subseteq A\} \tag{14.1}$$

where, $B_z = \{b + z | b \in B\}$.

The dilation can by obtained by:

$$\delta_B(A) = A \oplus B = \{z \in A | (B^s)_z \cap A \neq \varnothing\} \tag{14.2}$$

where $B^s = \{x \in E | -x \in B\}$ is the symmetric of B.

By composition, the opening is defined as: $A \circ B = (A \ominus B) \oplus B$. The closing is defined as: $A \bullet B = (A \oplus B) \ominus B$.

14.2 Elementary operators

>>>?

Test the functions of dilation, erosion, opening and closing on the image I_2 by varying:

1. the shape of the structuring element,
2. the size of the structuring element.



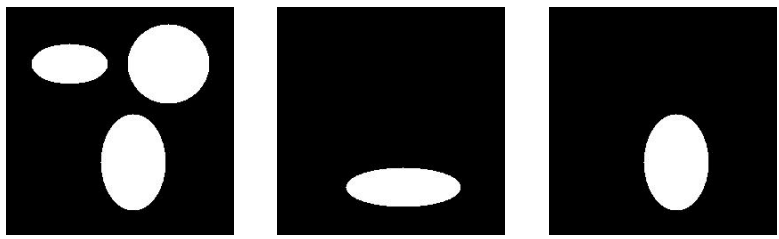
The python functions come from the python module `scipy.ndimage.morphology`. Useful functions are `binary_dilation`, `binary_erosion`, `binary_opening` and `binary_closing`. The function `ndimage.generate_binary_structure` creates a structuring element.

14.3 Morphological reconstruction

The operator of morphological reconstruction ρ is very powerful and largely used for practical applications. The principle is very simple. We consider two binary images: I_1 (the studied binary image) and M (the marker image). The objective is to reconstruct the elements of I_1 marked by M as illustrated in the Fig. 14.2.

To do this, we iteratively dilate the marker M while being included in I_1 (see Eq.14.3). In order to guarantee this inclusion in A, we keep from each dilated set its intersection with I_1. The algorithm is stopped when the process dilation-intersection is equal to the identity transformation (convergence).

Figure 14.2 Illustration of morphological reconstruction of I_1 by M.



Let $\delta_I^c(M) = \delta_{B_1}(M) \cap I$ be the dilation of the marker set M constrained to the set I. Then, the morphological reconstruction is defined as:

$$\rho_I(M) = \lim_{n \to \infty} \underbrace{\delta_I \circ \ldots \circ \delta_I(M)}_{n \text{ times}} \tag{14.3}$$

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Algorithm 5: The algorithm of this morphological reconstruction

Data: image I and marker M
Result: reconstructed image $rec(I, M)$
$r = area(M)$;
$s = 0$;
while $r \neq s$ **do**
  $s = r$;
  $M = I \cap (M \oplus B_1)$;
  $r = area(M)$;
end
$rec(I, M) = M$;

>>>?

1. Implement the algorithm.
2. Test this operator with the images I_1 and M.



Evaluate the area of a set may be done by counting the number of its pixels.

14.4 Operators by reconstruction

>>>?

Using the reconstruction operator, implement the 3 following transformations:

1. removing the border objects,
2. removing the small objects,
3. closing the object holes.

Test these operators on the image I_2.



The morphological reconstruction function to use is `binary_propagation` in the module `ndimage.morphology`.

14.5 Cleaning of the image of cells

>>>?

1. Threshold the image of cells (Fig. 14.1d).
2. Process the resulting binary image with the 3 cleaning processes of the previous question.

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14.6. Python correction

```python
from scipy import ndimage , misc
import numpy as np

import matplotlib.pyplot as plt
```

14.6.1 Elementary operators

First of all, one have to create a structuring element. The following function can be used to create a circular structuring element. A square can also be used.

```python
def disk(radius):
    # defines a circular structuring element with radius given by 'radius'
    x = np.arange(-radius, radius+1, 1);
    xx, yy = np.meshgrid(x, x);
    d = np.sqrt(xx**2 + yy**2);
    return d<=radius;
```

The following code presents basic mathematical morphology operations. First of all, declare the structuring element.

```python
# read binary image (and ensure binarization)
B = imageio.imread("B.jpg");
B = B>100;
# Structuring element
square = np.ones((5,5));
```

Erosion and dilation are the two elementary function of mathematical morphology.

```python
# Erosion
Bsquare_erode = ndimage.morphology.binary_erosion(B, structure=square);
plt.subplot(231);
plt.imshow(Bsquare_erode); plt.title("erosion")
imageio.imwrite('erosion.png', Bsquare_erode);
# Dilation
Bsquare_dilate = ndimage.morphology.binary_dilation(B, structure=square);
plt.subplot(232);
plt.imshow(Bsquare_dilate);plt.title("dilation")
imageio.imwrite('dilation.png', Bsquare_dilate);
```

Opening and closing are a combination of the two previous functions.

```python
# Opening
Bsquare_open = ndimage.morphology.binary_opening(B, structure=square);
plt.subplot(233);
plt.imshow(Bsquare_open);plt.title("opening")
imageio.imwrite('open.png', Bsquare_open);
```

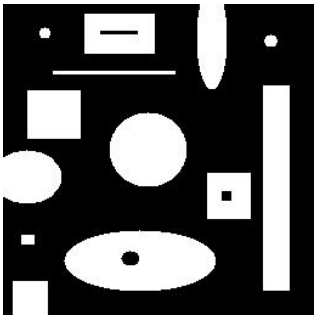
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```
# Closing
Bsquare_close = ndimage.morphology.binary_closing(B, structure=square);
plt.subplot(234);
plt.imshow(Bsquare_close);plt.title("closing")
imageio.imwrite('close.png', Bsquare_close);
```

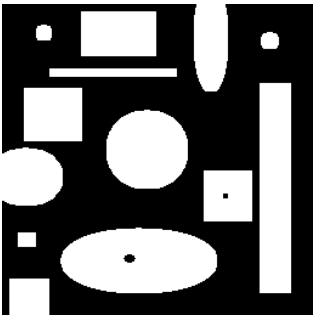
The results are presented in Fig. 14.3.

Figure 14.3 Basic mathematical morphology operations.

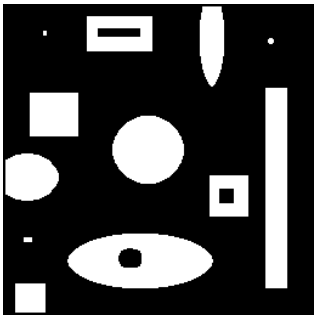
(a) Original image.



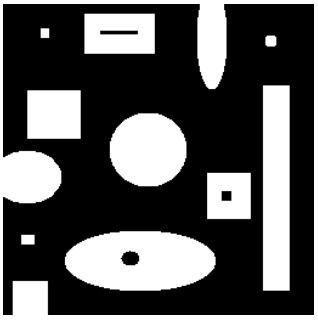
(b) Dilation.



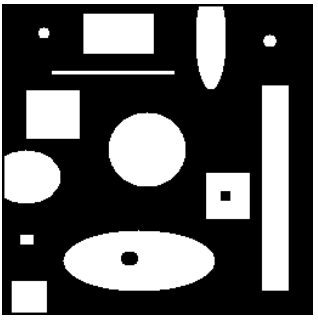
(c) Erosion.



(d) Opening.



(e) Closing.



14.6.2 Morphological reconstruction

The algorithm of morphological reconstruction is coded like this in python:

```
def reconstruct(image, mask):
    # should be binary images
    M = np.minimum(mask, image);

    area = ndimage.measurements.sum(M);
    s=0

    se = np.array([[0, 1, 0], [1, 1, 1], [0, 1, 0]]);
    while (area != s):
        s = area;
        M = np.minimum(image, ndimage.morphology.binary_dilation(M, structure=se));
        area = ndimage.measurements.sum(M);

    return M
```

The Fig. 14.4 illustrates the morphological recontruction.

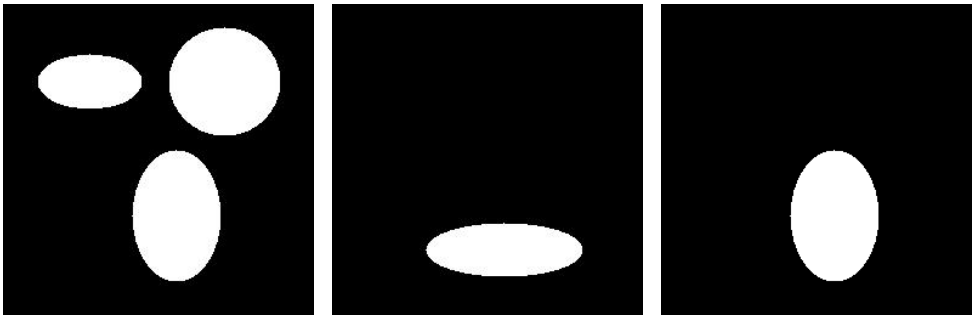
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```
A=imageio.imread('A.jpg');
A = A > 100;
M=imageio.imread('M.jpg');
M = M > 100;
# reconstruction de A par M
AM=reconstruct(A, M);

# display results
plt.subplot(1, 3, 1);
plt.imshow(A);
plt.subplot(1, 3, 2);
plt.imshow(M);
plt.subplot(1, 3, 3);
plt.imshow(AM);
plt.show();
```

Figure 14.4 Morphological reconstruction.

(a) Image A. **(b)** Image M. **(c)** `AM=reconstruct(A, M);`.



14.6.3 Operators by reconstruction

Remove objects touching the borders

The Fig. 14.5 illustrates the suppression of objects touching the borders of the image. If $\mathcal{B}$ represents the border of the image (create an array of the same size as the image, with zeros everywhere and ones at the sides), then this operation is defined by:

$$\text{killBorders}(I) = I \setminus \rho_I(\mathcal{B})$$

```
def killBorders(A):
    # remove cells touching the borders of the image
    m, n = A.shape
    M = np.zeros((m,n));
    M[0,:] = 1;
    M[m-1,:] = 1;
    M[:,0] = 1;
    M[:,n-1] = 1;
    M = reconstruct(A, M);
    return A-M
```

Remove small objects

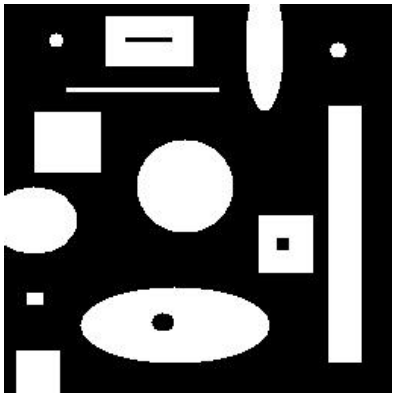
This is illustrated in Fig. 14.6. It consists in an erosion followed by a reconstruction. The structuring element used in the erosion defines the objects considered as “small”.

$$\text{killSmall}(I) = \rho_I(\varepsilon(I))$$

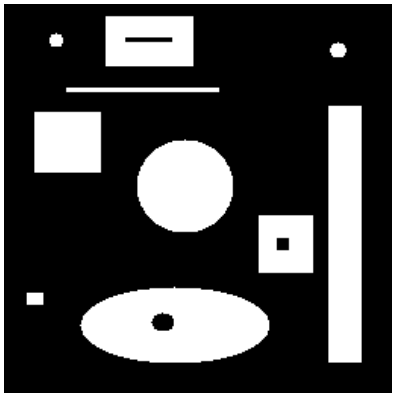
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Figure 14.5 Suppress border objects.

(a) Original image.



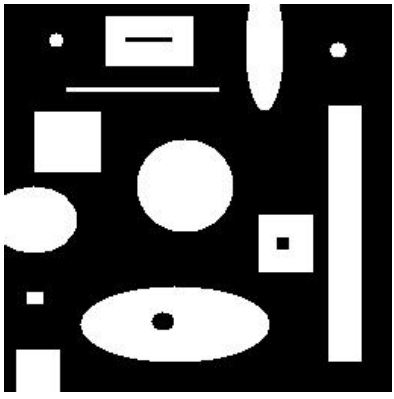
(b) Objects removed.



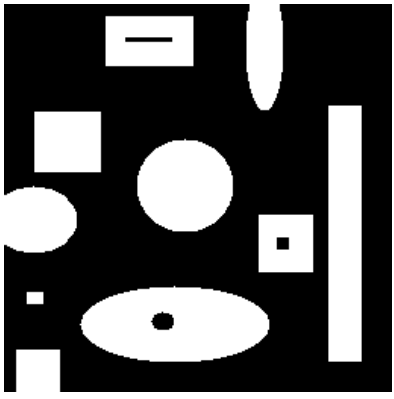
```python
def killSmall(A, n):
    # destroy small objects (size smaller than n)
    se = np.ones((n, n));
    M = ndimage.morphology.binary_erosion(A, structure=se);
    return reconstruct(A, M);
```

Figure 14.6 Small objects removal.

(a) Original image.



(b) Small objects are removed.



Close holes in objects

This is illustrated in Fig. 14.7. The operation is given by the following equation, with $\mathcal{B}$ the border of image I, and X^C denoting the complementary of set X:

$$\text{removeHoles(I)} = \{\rho_{I^C}(\mathcal{B})\}^C$$

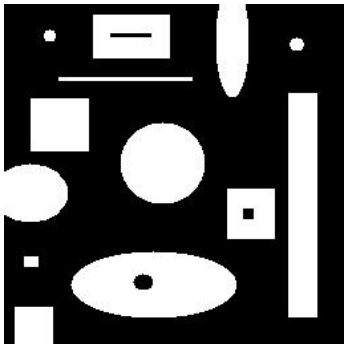
```python
def closeHoles(A):
    # close holes in objects
    Ac = ~A;
    m,n = A.shape;
    M = np.zeros((m,n));
    M[0,:] = 1;
```

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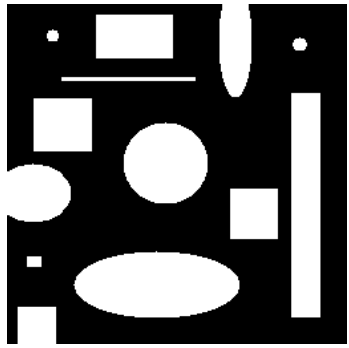
```
    M[m-1,:] = 1;
    M[:,0] = 1;
    M[:,n-1] = 1;
    M = reconstruct(Ac, M);
    return ~M
```

Figure 14.7 Hole filling.

(a) Original image.



(b) Holes in objects are closed.



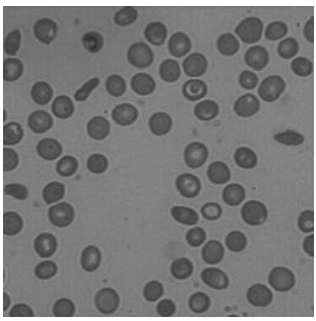
14.6.4 Application

The application shown in Fig. 14.8 presents the segmentation of blood cells after removing small cells, closing holes and removing the cells touching the borders of the image.

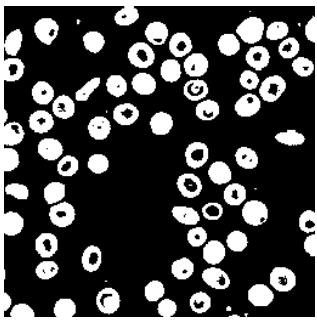
```
cells = imageio.imread('cells.jpg')<98;
imageio.imwrite('cellsbw.png', cells);
B = closeHoles(cells);
B = killBorders(B);
B = killSmall(B, 5);
plt.subplot(1,2,1);
plt.imshow(cells);
plt.subplot(1,2,2);
plt.imshow(B);
plt.title('clean image')
plt.show()
imageio.imwrite('clean.png', B);
```

Figure 14.8 Segmentation of the cells.

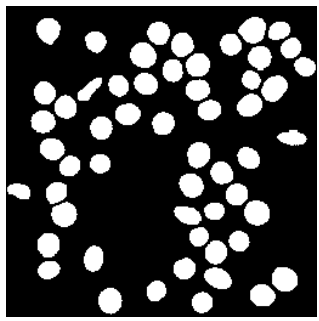
(a) Original image.



(b) Binarization.



(c) Final segmentation of the cells.



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★★★ 15 Morphological Geodesic Filtering

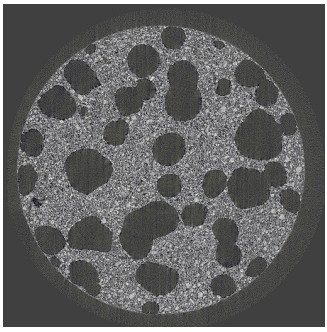
This tutorial aims to test different morphological filters and particularly the geodesic ones (using reconstruction) for gray-level images.

The different processes will be applied on the following images:

(a) Lena



(b) 2-D section of a cement paste (X-ray tomography)



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15.1 Morphological centre

The morphological centre is an auto-dual filter using a family of operators $\{\psi_i\}_i$:

$$C(f) = (f \vee (\wedge\{\psi_i(f)\})) \wedge (\vee\{\psi_i(f)\}) \tag{15.1}$$

>>>?

- Implement this transformation with the family $\{\gamma\phi\gamma, \phi\gamma\phi\}$ where γ denotes the morphological opening and ϕ the morphological closing.
- Test this operator by varying the size of the structuring element.
- Add a 'salt and pepper' noise to the 'Lena' image and compare the morphological center with the median filtering.
- Try to reduce the noisy image 'cement paste'.

15.2 Alternate sequential filters (ASF)

ASF can be defined from a family of openings and closings:

$$N_i(f) = \gamma_i\phi_i \circ \gamma_{i-1}\phi_{i-1} \ldots \gamma_2\phi_2 \circ \gamma_1\phi_1(f) \tag{15.2}$$

$$M_i(f) = \phi_i\gamma_i \circ \phi_{i-1}\gamma_{i-1} \ldots \phi_2\gamma_2 \circ \phi_1\gamma_1(f) \tag{15.3}$$

where γ_k (resp. ϕ_k) denotes the opening (resp. closing) with a structuring element of size k.

>>>?

- Implement these two operators.
- Test these transformations on the noisy image by varying the parameter i of the filter.

15.3 Reconstruction filters

The geodesic dilation of size 1 and n are respectively defined as:

$$\delta_f(g) = \wedge(\delta_{B_1}(g), f) \quad (15.4)$$
$$\delta_f^n(g) = \delta_f(\delta_f \dots (\delta_f(g))) \quad (15.5)$$

where δ_{B_1} denotes the morphological dilation with a disk of radius 1 as structuring element. The opening ($\gamma_k^{rec}(f)$) and closing ($\phi_k^{rec}(f)$) by reconstruction are then defined as:

$$\gamma_k^{rec}(f) = \vee\{\delta_f^n(\epsilon_{B_k}(f)), n > 0\} \quad (15.6)$$
$$\phi_k^{rec}(f) = M - \gamma_k^{rec}(M - f) \quad (15.7)$$

where ϵ_{B_k} denotes the morphological erosion with a disk B of radius k as structuring element.

>>>?

- Implement these two operators $\gamma_k^{rec}(f)$ and $\phi_k^{rec}(f)$.
- Test these transformations by varying the parameter k of the filter.
- Implement and test (on the noisy image) the filters of morphological center and ASF using the geodesic operators. Compare with the classical ones.

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15.4. Python correction

```python
from skimage.util import random_noise
from scipy import misc
import matplotlib.pyplot as plt
from skimage import morphology as m
from skimage import filters
import numpy as np
```

15.4.1 Morphological center

The noisy image is obtained with the function `random_noise` from `skimage.util`.

```python
L = imageio.imread('lena512.bmp');
A = random_noise(L, mode='s&p', amount=.04);
```

Following the definition, the morphological center is obtained with the following code, and illustrated in Fig.15.1:

```python
def morphoCenter(I, c, o, selem=m.disk(1)):
    """
    """
    coc = c(o(c(I, selem=selem), selem=selem), selem=selem);
    oco = o(c(o(I, selem=selem), selem=selem), selem=selem);
    cMin = np.minimum(oco, coc);
    cMax = np.maximum(oco, coc);
    F = np.minimum( np.maximum(A, cMin), cMax);
    return F;

B = morphoCenter(A, m.closing, m.opening);
Bmed= filters.median(A, selem=np.ones((3,3)));
```

Figure 15.1 Morphological center compared to the classical median filter.

(a) Noisy image.



(b) Median filter of size 5×5.



(c) Morphological center.



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15.4.2 Alternate sequential filters

The order of these filters are often chosen empirically. The results are illustrated in Fig.15.2.

```
def asf_n(I, order=3):
    F = I.copy();
    for r in np.arange(1, order+1):
        se = m.disk(r);
        F = m.opening( m.closing(F, selem=se), selem=se);
    return F;
```

```
def asf_m(I, order=3):
    F = I.copy();
    for r in np.arange(1, order+1):
        se = m.disk(r);
        F = m.closing( m.opening(F, selem=se), selem=se);
    return F;
```

Figure 15.2 Alternate Sequential Filters compared to original image.

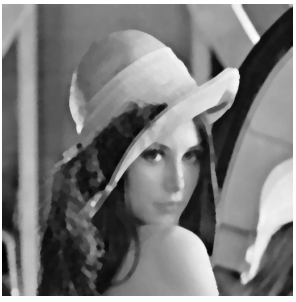
(a) Original image.



(b) ASF of order 3, starting with a closing operation (denoted N).



(c) ASF of order 3, starting with an opening operation (denoted M).



15.4.3 Geodesic reconstruction filters

These two functions are simply implemented using erosion and reconstruction operators. Notice the duality property, that is used to code `closerec`. In this example, 8 bits images (unsigned) are considered, and the results are illustrated in Fig.15.3.

```
def openrec(I, selem=m.disk(1)):
    B = m.erosion(I, selem=selem);
    F = m.reconstruction(B, I);
    return F;
```

```
def closerec(I, selem=m.disk(1)):
    F = 255-openrec(255-I, selem=selem);
    return F;
```

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Figure 15.3 Opening and closing by reconstruction.

(a) Original image.



(b) Opening by reconstruction.



(c) Closing by reconstruction.



15.4.4 ASF by reconstruction

This is an example of a 3rd order alternate sequential filter, illustrated in Fig.15.4.

```
def asfrec(I, order=3):
    A = I.copy();
    for r in np.arange(1, order+1):
        se = m.disk(r);
        A = closerec(openrec(A, selem=se), selem=se);
    return A;
```

Figure 15.4 Alternate Sequential Filtering by reconstruction.

(a) Original image.



(b) ASF of order 3 by reconstruction.



(c) Noisy image.



15.4.5 Morphological center by reconstruction

Morphological center by reconstruction replaces the opening and closing operations by their equivalent by reconstruction (see Fig.15.5).

```
def centerrec(I, selem=m.disk(1)):
    """
    """
    B = morphoCenter(I, closerec, openrec, selem=selem);
    return B;
```

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Figure 15.5 Morphological center by reconstruction.

(a) Original image.



(b) Center by reconstruction.



(c) Noisy image.



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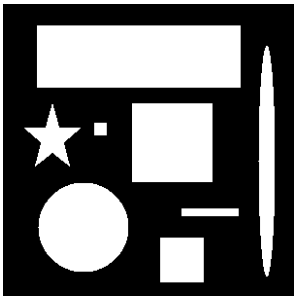
16 Morphological Attribute Filtering

This tutorial aims to test the attribute morphological filters for gray-level images. The objective of such filters is to remove the connected components of the level sets which do not satisfy a specific criterion (area, elongation, convexity...).

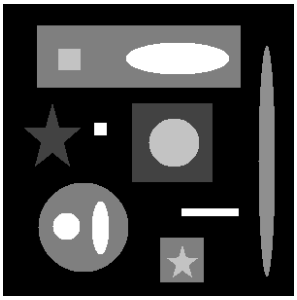
Fig.16.1 are presented some results of attribute filtering applied on the grayscale image.

Figure 16.1 Attribute filtering examples.

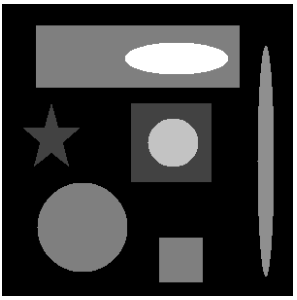
(a) Binary image.



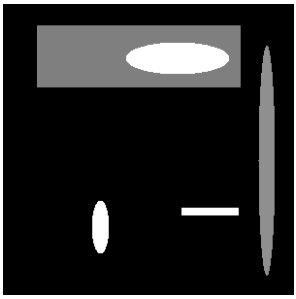
(b) Grayscale image.



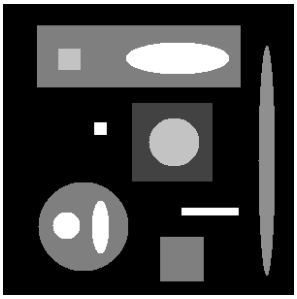
(c) Filtering by area.



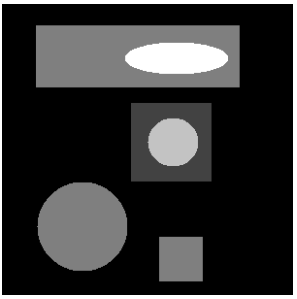
(d) Filtering by elongation.



(e) Filtering by convexity.



(f) Filtering objects larger than a square.



A *binary connected opening* Γ_x transforms a binary image f given a pixel x, by keeping the connected component that contains x and removing all the others.
Binary trivial opening Γ_T operates on a given connected component X according to an increasing criterion T applied to the connected component. If the criterion is satisfied, the connected component is preserved, otherwise it is removed according to:

$$\Gamma_T(X) = \begin{cases} X & \text{if } T(X) = \text{true} \\ \emptyset & \text{if } T(X) = \text{false} \end{cases} \tag{16.1}$$

In general, one or more features of the connected component, on which the filter is applied, are compared to a given threshold defined by the rule.
Binary attribute opening Γ^T, given an increasing criterion T, is defined as a binary trivial opening applied on all the connected components of F. This can be formally represented as:

$$\Gamma^T(F) = \bigcup_{x \in F} \Gamma_T(\Gamma_x(F)) \tag{16.2}$$

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If the criterion T evaluated in the transformation is not increasing, e.g., when the computed attribute is not dependent itself on the scale of the regions (e.g. shape factor, orientation, etc.), the transformation also becomes not increasing. Even if the increasingness property is not fulfilled, the filter remains idempotent and anti-extensive. For this reason, the transformation based on a non-increasing criterion is not an opening, but a thinning. In this case, one speak about a *binary attribute thinning*.

Attribute openings and thinnings introduced for the binary case can be extended to grayscale images employing the threshold decomposition principle. A grayscale image can be represented by thresholding the original image at each of its graylevels. Then, the binary attribute opening can be applied to each binary image and the *grayscale attribute opening* is given by the maximum of the results of the filtering for each pixel and can be mathematically represented as:

$$\gamma^T(f)(x) = \max\{k; x \in \Gamma^T(Th_k(f))\} \tag{16.3}$$

where $Th_k(f)$ is the binary image obtained by thresholding f at graylevel k.

The extension to grayscale of the binary attribute thinning is not straightforward and not unique. For example, a possible definition of a *grayscale attribute thinning* can be analogously defined as Equation (3). However, other definitions are possible, according to the filtering rule considered in the analysis (max, min, subtractive, direct...). Again, if the criterion T is increasing (i.e. the transformation is an opening), all the strategies lead to the same result.

Attribute openings are a family of operators that also includes openings by reconstruction. If we consider a binary image with a connected component X and the increasing criterion "the size of the largest square enclosed by X must be greater than λ", the result of the attribute opening is the same as applying an opening by reconstruction with a squared structuring element of size λ.

16.1 Binary attribute opening/thinning

We are going to implement and test some binary attribute filters according to different criteria (area, elongation, convexity).

>>>?

- Regarding the area criterion, implement the associated binary attribute opening. Test on the binary image.
- Regarding the elongation criterion, implement the associated binary attribute thinning (non-increasing criterion). Test on the binary image.



Code your own function `bwFilter` based on `regionprops` from `skimage.measure`.

16.2 Grayscale attribute opening/thinning

We are going to extend the binary filters to grayscale images.

>>>?

- Implement the decomposition operator into binary sections.
- Conversely, implement the reconstruction operator from binary sections.
- Implement and test the grayscale attribute filters according to the following criteria: area, elongation, convexity.

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16.3. Python correction

```python
from skimage import morphology as m
from scipy import misc
import matplotlib.pyplot as plt
from skimage.measure import regionprops
from skimage.measure import label
import numpy as np
```

16.3.1 Binary attribute filtering

If `bw` is a binary image, the different attribute are evaluated with `regionprops` and filtered according to the given upper and lower thresholds.

```python
def bwFilter(bw, attribute, thresholds):
    """
    binary filtering according to attribute
    bw: binary image
    attribute: string representing attribute, defined by regionprops
    thresholds: threshold values, inside which objects are removed
    returns binary image
    """
    F = bw.copy();
    L = label(bw);
    for region in regionprops(L):
        a = getattr(region, attribute);
        if a < thresholds[1] and a>= thresholds[0]:
            F[L==region.label] = False;
    return F;
```

16.3.2 Grayscale filtering

The grayscale filtering is the previous binary filtering process applied to all level-sets of the original image.

```python
def grayFilter(I, attribute, thresholds):
    """
    grayscale image filtering by attribute
    for 8 bits unsigned images
    I: original grayscale image (N, M) ndarray
    attribute: string representing attribute, defined by regionprops
    thresholds: threshold values, inside which objects are removed
    returns grayscale filtered image
    """
    N, M = I.shape
    F = np.zeros((N, M, 256));
    for s in range(256):
        F[:,:,s] = s * bwFilter(I>=s, attribute=attribute, thresholds=thresholds);

    # reconstruction
    R = np.amax(F, axis=2);
    return R;
```

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Then, for each level, the binary set is filtered by some attribute, and the resulting image is reconstructed by taking the maximum value on all levels.

The shape filtering process do not take the results from the `regionprops` function. The shape is filtered by using the morphological function of reconstruction.

```
def shapeFilter(I, selem=m.square(25)):
    """
    image filtering when attribute is a shape of a given size, defined by selem
    I: grayscale image
    selem: structuring element
    returns: grayscale filtered image
    """
    N, M = I.shape
    F = np.zeros((N, M, 256));
    for s in range(256):
        F[:,:,s] = s * m.reconstruction(m.opening(I>=s, selem=selem), I>=s);

    # reconstruction
    R = np.amax(F, axis=2);
    return R;
```

The examples are generated via the following code:

```
F = bwFilter(I>50, 'area', (0,5000));

F = grayFilter(I, 'area', (0,1000));

F = grayFilter(I, 'eccentricity', (0, 0.75));

F = grayFilter(I, 'solidity', (0, 0.75));

F = shapeFilter(I);
```

Results are illustrated in Fig.16.1.

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★★ 17 Morphological skeletonization

This tutorial aims to skeletonize objects with specific tools from mathematical morphology (thinning, maximum ball…).

The different processes will be applied on the following image:



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17.1 Hit-or-miss transform

The hit-or-miss transformation enables specific pixel configurations to be detected. Based on a pair of disjoint structuring elements $T = (T^1, T^2)$, this transformation is defined as:

$$\eta_T(X) = \{x, T^1_x \subseteq X, T^2_x \subseteq X^c\} \quad (17.1)$$

$$= \epsilon_{T^1}(X) \cap \epsilon_{T^2}(X^c) \quad (17.2)$$

where $\epsilon_B(X)$ denotes the erosion of X using the structuring element B.

>>>?

1. Implement the hit-or-miss transform.
2. Test this operator with the following pair of disjoint structuring elements:

$$\begin{array}{|c|c|c|}\hline +1 & +1 & +1 \\ \hline 0 & +1 & 0 \\ \hline -1 & -1 & -1 \\ \hline\end{array} \quad \left(T^1 = \begin{array}{|c|c|c|}\hline 1 & 1 & 1 \\ \hline 0 & 1 & 0 \\ \hline 0 & 0 & 0 \\ \hline\end{array}, \quad T^2 = \begin{array}{|c|c|c|}\hline 0 & 0 & 0 \\ \hline 0 & 0 & 0 \\ \hline 1 & 1 & 1 \\ \hline\end{array} \right)$$

where the points with $+1$ (resp. -1) belong to T^1 (resp. T^2).

17.2 Thinning and thickening

Using the hit-or-miss transform, it is possible to make a thinning or thickening of a binary object in the following way:

$$\theta_T(X) = X \backslash \eta_T(X) \quad (17.3)$$

$$\chi_T(X) = X \cup \eta_T(X^c) \quad (17.4)$$

These two operators are dual in the sense that $\theta_T(X) = (\chi_T(X^c))^c$.

>>>?

1. Implement these two transformations.
2. Test these operators with the previous pair of structuring elements.

17.3 Topological skeleton

By using the two following pairs of structuring elements with their rotations (90°) in an iterative way (8 configurations are thus defined), the thinning process converges to a resulting object which is homothetic (topologically equivalent) to the initial object.

+1	+1	+1
0	+1	0
−1	−1	−1

0	+1	0
+1	+1	−1
0	−1	−1

>>>?

1. Implement this transformation (the convergence has to be satisfied).
2. Test this operator and comment.

17.4 Morphological skeleton

A ball $B_n(x)$ with center x and radius n is maximum with respect to the set X if there exists neither indice k nor centre y such that:

$$B_n(x) \subseteq B_k(y) \subseteq X$$

In this way, the morphological skeleton of a set X is constituted by all the centers of maximum balls. Mathematically, it is defined as:

$$S(X) = \bigcup_r \epsilon_{B_r(0)}(X) \backslash \gamma_{B_1(0)}(\epsilon_{B_r(0)}(X)) \tag{17.5}$$

>>>?

1. Implement this transformation.
2. Test this operator and compare it with the topological skeleton.

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17.5. Python correction

```python
from scipy import ndimage
import numpy as np

import imageio
import matplotlib.pyplot as plt
```

17.5.1 Hit or miss transform

The hit-or-miss transform is illustrated in Fig.17.1.

```python
def hitormiss(X, T):
    """
    hit or miss transform
    X: binary image
    T: structuring element (values -1, 0 and 1)

    return: result of hit or miss transform (binary image)
    """
    T1 = (T==1);
    T2 = (T==-1);
    E1 = ndimage.morphology.binary_erosion(X, T1);
    E2 = ndimage.morphology.binary_erosion(np.logical_not(X), T2);
    B = np.minimum(E1, E2);
    return B;
```

Figure 17.1 Elementary functions

(a) Hit or miss (intensities are inverted).



(b) Thinning.



(c) Thickening.



17.5.2 Thinning and thickening

The code is split into 2 elementary operations of thinning and thickening, so that the thinning consists in iterating this operation. The thickening operation is obtained by thinning the complementary set.

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```python
def elementary_thinning(X, T):
    """
    thinning function
    X: binary image
    T: structuring element (values -1, 0 and 1)

    return: result of thinning
    """
    B = np.minimum(X, np.logical_not(hitormiss(X, T)));
    return B;
```

```python
def elementary_thickening(X, T):
    """
    thickening function
    X: binary image
    T: structuring element (values -1, 0 and 1)

    return: result of thickening
    """
    B = not(elementary_thinning(not(X), T));
    return B;
```

```python
def thinning(X, TT):
    """
    morphological thinning
    TT is a configuration of 8 pairs of structuring elements
    """
    for T in TT:
       X = elementary_thinning(X, T);

    return X;
```

17.5.3 Skeletons

The topological skeleton is the iteration of the operation of thinning, for structuring elements defined like:

```python
TT = [];
TT.append(np.array([[-1,-1,-1],[0,1,0],[1,1,1]]));
TT.append(np.array([[0,-1,-1],[1,1,-1],[0,1,0]]));
TT.append(np.array([[1,0,-1],[1,1,-1],[1,0,-1]]));
TT.append(np.array([[0,1,0],[1,1,-1],[0,-1,-1]]));
TT.append(np.array([[1,1,1],[0,1,0],[-1,-1,-1]]));
TT.append(np.array([[0,1,0],[-1,1,1],[-1,-1,0]]));
TT.append(np.array([[-1,0,1],[-1,1,1],[-1,0,1]]));
TT.append(np.array([[-1,-1,0],[-1,1,1],[0,1,0]]));
```

```python
def topological_skeleton(X, TT):
    """
    Topological skeleton: preserves topology
    X: binary image to be transformed
```

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```
    TT: set of pairs of structuring elements
    return skeleton
    """
    B = np.logical_not(np.copy(X));
    while not(np.all(X == B)):
        B = X;
        X = thinning(X, TT);
    return B;
```

The topological skeleton is the iteration of the thinning with structuring elements in all 8 directions. It has the property of preserving the topology of the discrete structures, contrary to the morphological skeleton (see Fig.17.2). The morphological skeleton does not preserve the connexity of the branches, but it can be used to reconstruct the original image. Pay attention to the construction of structuring elements, which should be homothetic ($B_r = \underbrace{B_1 \oplus \cdots \oplus B_1}_{r \text{ times}}$).

```
def morphological_skeleton(X):
    """
    morphological skeleton
    X: binary image
    using disk structuring elements

    in order to perform the reconstruction from the skeleton, one has to store
    the value of S for each size of structuring element

    return: S, morphological skeleton, grayscale image
    """
    strel_size = -1;
    pred = True;
    S = np.zeros(X.shape);
    se = ndimage.generate_binary_structure(2, 1);
    E = np.copy(X);
    while pred:
        strel_size+=1;
        E = ndimage.morphology.binary_erosion(X, se);
        if np.all(E==0):
            pred = False;
        D = ndimage.morphology.binary_dilation(E, se);
        S = np.maximum(S, (strel_size+1)*np.minimum(X, np.logical_not(D)));
        X = E;
    return S;
```

```
def reconstruction_skeleton(S):
    """
    Reconstruction of the original image from the morphological skeleton
    S: Skeleton, as constructed by morphological_skeleton

    return: original image I
    """
    X = np.zeros(S.shape).astype("bool");
    n = np.max(S);
    se = ndimage.generate_binary_structure(2, 1);

    for strel_size in range(int(n)):
        Sn = S == strel_size+1;

```

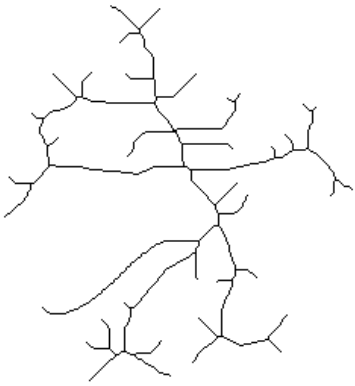
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```
    # this is for preserving homothetic structuring elements
    for k in range(strel_size):
        Sn = ndimage.morphology.binary_dilation(Sn, se);

    X = np.maximum(X, Sn);
  return X;
```

Figure 17.2 Skeletons. The topology is not preserved in the morphological skeleton, but it can be used to reconstruct the original image. The intensities are inverted in order to facilitate the display.

(a) Topological skeleton.



(b) Morphological skeleton.



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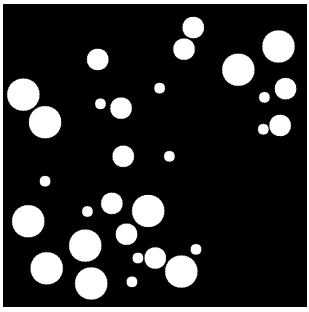
18 Granulometry

This tutorial aims to compute specific image measurements on digital images. It consists in determining the size distribution of the 'particles' included in the image to be analyzed.

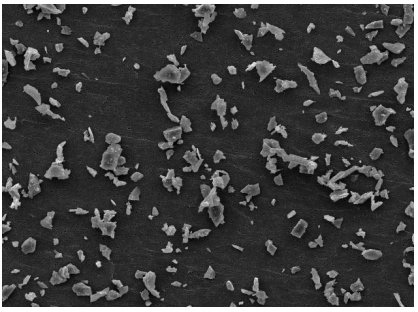
The image measurements will be realized on a simulated image of disks and an image of silicon carbide powder acquired by Scanning Electron Microscopy (SEM, Fig. 18.1).

Figure 18.1 These images are used for computing a granulometry of objects by mathematical morphology.

(a) Simulated image.



(b) Real image of powder, by SEM.



18.1 Morphological granulometry

18.1.1 Introduction to mathematical morphology

The tutorial 14 introduces the basic operations of the mathematical morphology, as well as the morphological reconstruction. More informations can be found in [40].

With Python, the useful functions are `binary_opening` of the module `scipy.ndimage` for the morphological opening, `binary_propagation` for the geodesic reconstruction. For counting the number of objects, one can use `measurements.label` for a labelling and counting algorithm.

18.1.2 Granulometry

>>>?

- Load and visualize the image 'simulation' Fig.18.1.
- Generate n images by applying morphological openings (with reconstruction) to the binary image with the use of homothetic structuring elements of increasing size: $1 < \cdots < n$.

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- Compute the morphological granulometry expressed in terms of surface area density. It consists in calculating the specific surface area of the grains in relation with the size n of the structuring element.
- Compute the morphological granulometry expressed in terms of number density. It consists in calculating the specific number of grains in relation with the size n of the structuring element.
- Compare and discuss.



Use `generate_binary_structure` and `iterate_structure` from python module `scipy.ndimage` to define homothetic structuring elements.

18.2 Real application

>>>?

- Load and visualize the image 'powder' of Fig. 18.1b.
- Realize the image segmentation step. I can simply consist in a binarization by a global threshold, followed by hole filling. Noise can also be removed my mathematical morphology opening.
- Compute the morphological granulometry (surface area, number).
- What can you conclude?

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18.3. Python correction



18.3.1 Simulation

The construction of an homothetic structuring element is necessary for computing a granulometry (through the function `iterate_structure`.



```python
def granulometry(BW, T=35):
    # total original area
    A = ndimage.measurements.sum(BW);

    # number of objects
    label, N = ndimage.measurements.label(BW);

    area=np.zeros((T,), dtype=np.float);
    number=np.zeros((T,), dtype=np.float);

    """
    Warning: the structuring elements must verify B(n) = B(n-1) o B(1).
    """
    se = ndimage.generate_binary_structure(2, 1);
    for i in np.arange(T):
        SE = ndimage.iterate_structure(se, i-1);
        m = ndimage.morphology.binary_erosion(BW, structure=SE);
        G = ndimage.morphology.binary_propagation(m, mask=BW);
        area[i]=100*ndimage.measurements.sum(G)/A
        label, n = ndimage.measurements.label(G);
        number[i] = 100*n/N; # beware of integer division

    plt.figure()
    plt.plot(area, label='Area')
    plt.plot(number, label='Number')
    plt.legend()
    #plt.savefig("granulo_poudre1.pdf");
    plt.show()

    plt.figure();
    plt.plot(-np.diff(area), label='Area derivative');
    plt.plot(-np.diff(number), label='Number derivative');
    plt.legend()
    #plt.savefig("granulo_poudre2.pdf");
    plt.show()
```

The results are shown in Fig. 18.2, generated by the following code:



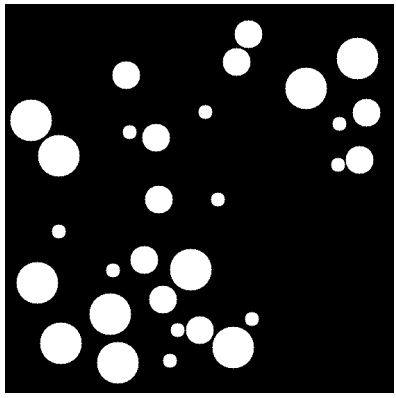
```python
## Granulometry of synthetic image
# read binary simulated image, normalize it
I = imageio.imread("simulation.png")/255;
I = I[:,:,2]>.5;
plt.figure();
plt.imshow(I);
plt.show();

granulometry(I, 35);
```

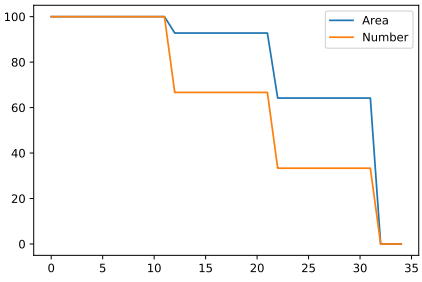
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Figure 18.2 Granulometry on simulated image.

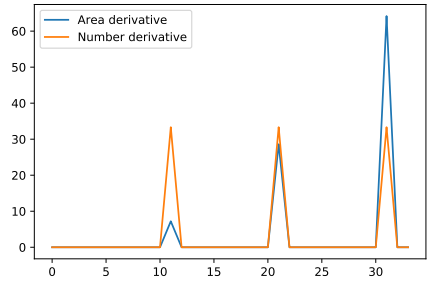
(a) Simulated image of disks.



(b) Granulometry in number and area.



(c) Derivatives.



18.3.2 Powder image and segmentation

First of all, the image must be binarized, i.e. segmented. The following code is a proposition of segmentation, leading to the result presented in Fig. 18.3c.

```
## Granulometry of real image
I = imageio.imread("poudre.bmp");

# segmentation
BW = I>74;
BW = ndimage.morphology.binary_fill_holes(BW);

# suppress small objects
se = ndimage.generate_binary_structure(2, 1);
m = ndimage.morphology.binary_opening(BW);
# opening by reconstruction
BW=ndimage.morphology.binary_propagation(m, mask=BW);

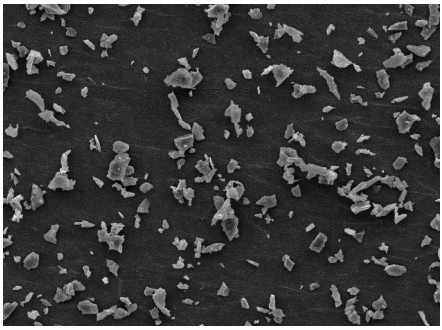
imageio.imwrite("segmentation.png", BW);
plt.imshow(BW)
plt.show()

granulometry(BW, 20);
```

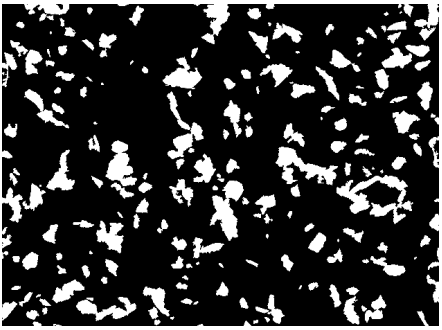
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Figure 18.3 Results of granulometry analysis of original image from (a).

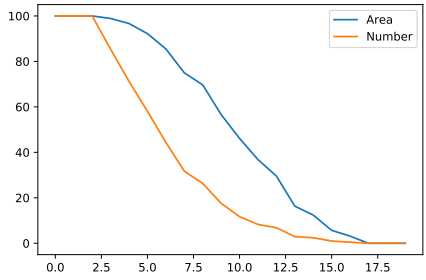
(a) Original image of powder.



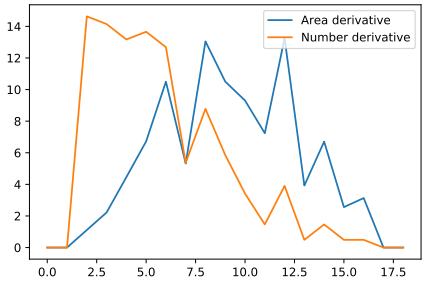
(b) Segmentation of image of (a).



(c) Granulometry.



(d) Derivative.



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Third part

Registration and Segmentation

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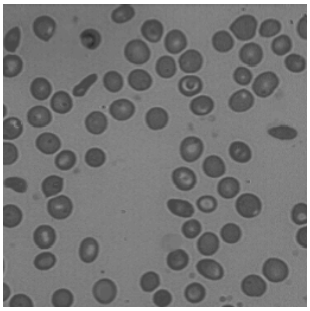
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⋆ 19 Histogram-based image segmentation

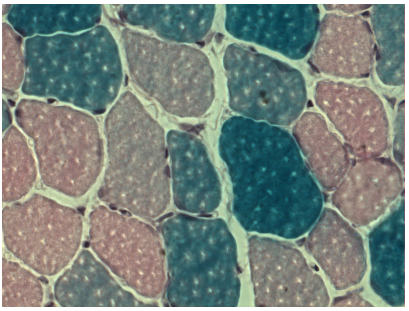
This tutorial aims to implement some image segmentation methods based on histograms (thresholding and "k-means" clustering).

The different processes will be applied on the following images:

(a) Cells.



(b) Muscle cells, author: Damien Freyssenet, University Jean Monnet, Saint-Etienne, France.



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19.1 Manual thresholding

The most simple segmentation method is thresholding.

>>>?

- Visualize the histogram of the grayscale image 'cells'.
- Make the segmentation with a threshold value determined from the image histogram.

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19.2 k-means clustering

Let $X = \{x_i\}_{i\in[1;n],n\in\mathbb{N}}$ be a set of observations (the points) in $\mathbb{R}^d$. The k-means clustering consists in partitioning X in k $(k < n)$ disjoint subsets $\tilde{S}$ such that:

$$\tilde{S} = \arg\min_{S=\{S_i\}_{i\leq k}} \sum_{i=1}^{k} \sum_{x_j\in S_i} \|x_j - \mu_i\|^2 \tag{19.1}$$

where μ_i is the mean value of the elements in S_i. The k-means algorithm is iterative. From a set of k initial elements $\{m_i^{(1)}\}_{i\in[1;k]}$ (randomly selected), the algorithm iterates the following (t) steps:

- Each element of X is associated to an element m_i according to a distance criterion (computation of a Voronoi partition):

$$S_i^{(t)} = \left\{\mathbf{x}_j : \left\|\mathbf{x}_j - \mathbf{m}_i^{(t)}\right\| \leq \left\|\mathbf{x}_j - \mathbf{m}_{i^*}^{(t)}\right\|, \forall i^* \in [1;k]\right\} \tag{19.2}$$

- Computation of the new mean values for each class:

$$\mathbf{m}_i^{(t+1)} = \frac{1}{|S_i^{(t)}|} \sum_{\mathbf{x}_j \in S_i^{(t)}} \mathbf{x}_j \tag{19.3}$$

where $|S_i^{(t)}|$ is the number of elements of $S_i^{(t)}$.

19.3 Grayscale image, $k = 2$ in one dimension

The objective is to binarize image image 'cells', which is a grayscale image. The set X is defined by $X = \{I(p)\}$, for p being the pixels of the image I.

>>>?

- Implement the algorithm proposed below (Alg. 6).
- Test this operator on the image 'cells'.
- Test another method of automatic thresholding (defined by Otsu in [26]).
- Compare the values of the thresholds (manual and automatic).

Algorithm 6: K-means algorithm for automatic threshold computation of grayscale images.

Data: Original image A
Data: Stop condition ε
Result: thresholded image
Initialize T_0, for example at $\frac{1}{2}(\max(A) + \min(A))$;
$done \leftarrow False$;
while *NOT done* **do**
  Segment the image A with the threshold value T;
  it generates two classes G_1 (intensities $\geq T$) and G_2 (intensities $< T$);
  Compute the mean values, denoted μ_1, μ_2, of the two classes G_1, G_2, respectively;
  Compute the new threshold value $T_i = \frac{1}{2}(\mu_1 + \mu_2)$;
  if $|T_i - T_{i-1}| < \varepsilon$ **then**
    $done \leftarrow True$
  end
end
Segment the image with the estimated threshold value.



For use with python, use the module `skimage.filter` and the function `threshold_otsu`.

19.4 Simulation example, $k = 3$ in two dimensions

The objective is to generate a set of 2-D random points (within $k = 3$ distinct classes) and to apply the k-means clustering for separating the points and evaluating the method (the classes are known!).

>>>?

Write a function for generating a set of n random points around a point with coordinates (x, y).



We will use the python function `randn` from the module `numpy.random`.

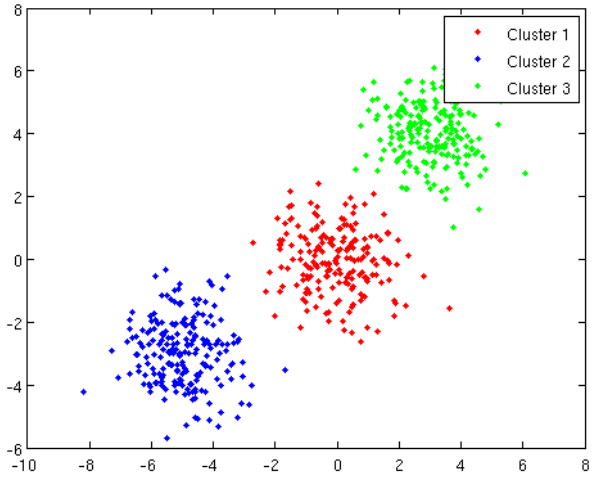
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>>>?

- Use this function to generate 3 set of points (in a unique matrix) around the points $(0, 0)$, $(3, 4)$ and $(-5, -3)$.
- Use the python function `sklearn.cluster.KMeans` for separating the points. The result is presented in Fig.19.1.

Verify the utility of the option `n_init=10`.

Figure 19.1 Resulting clustering of random points.



19.5 Color image segmentation using K-means: $k = 3$ in 3D

The k-means clustering is now used for segmenting the color image representing the muscle cells 'Tv16.png'.

>>>?

Which points have to be separated? Transform the original image into a vector of size $N \times 3$ (where N is the number of pixels) which represent the 3 components R, G and B of each image pixel.

The python function `numpy.reshape` does the same transformation.

>>>?

- Visualize the 3-D map (histogram) of all these color intensities.
- Make the clustering of this 3-D map by using the K-means method.
- Visualize the corresponding segmented image.

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19.6. Python correction

19.6.1 Manual thresholding

Visual analysis of histogram

When manually choosing a threshold value, one has to analysis the histogram (Fig. 19.2).

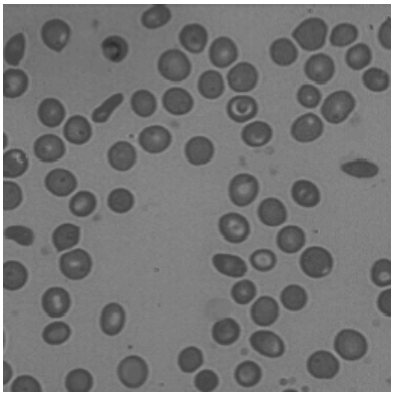
```python
import numpy as np
import imageio
import matplotlib.pyplot as plt # plots
from skimage import filter # otsu thresholding

# read image
cells=imageio.imread('cells.png');

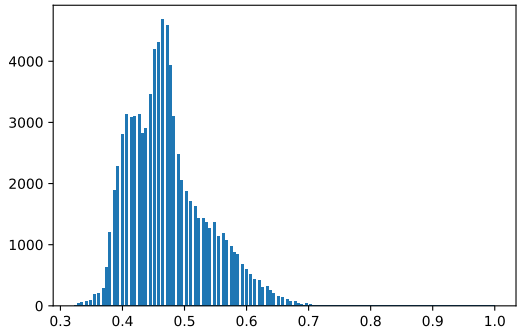
# display histogram
fig=plt.figure();
plt.hist(cells.flatten(), 256)
fig.show();
fig.savefig("histo.pdf");
```

Figure 19.2 Original image and its histogram.

(a) Original image.



(b) Histogram.



Segmentation

```python
fig=plt.figure();
plt.subplot(1,2,1)
plt.imshow(cells, plt.cm.gray); plt.title('Original image');
plt.subplot(1,2,2)
plt.imshow(cells>80, plt.cm.gray); plt.title('Manual segmentation');
fig.savefig("manual.pdf");
```

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19.6.2 Automatic thresholding

```python
def autothresh(image):
    """ Automatic threshold method
    @param image: image to segment
    @return : threshold value
    """
    s = 0.5*(np.amin(image) + np.amax(image));
    done = False;
    while ~done:
        B = image>=s;
        sNext = .5*(np.mean(image[B]) + np.mean(image[~B]));
        done = abs(s-sNext)<.5;
        s = sNext;
    return s
```

The results are displayed using the following code (Fig. 19.3):

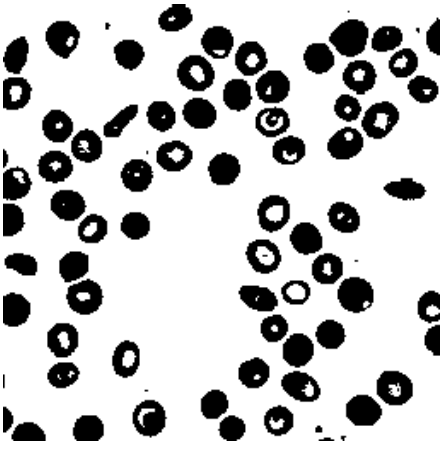
```python
# Automatic threshold
s_auto= autothresh(cells);

# Otsu thresholding
s_otsu =filter.threshold_otsu(cells);

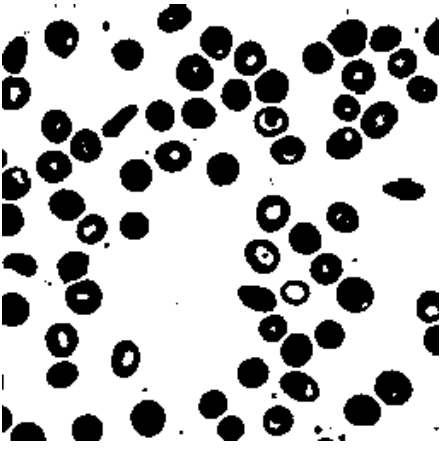
plt.figure();
plt.subplot(1,2,1)
plt.imshow(cells>s_auto, plt.cm.gray); plt.title('Automatic thresholding')
plt.subplot(1,2,2);
plt.imshow(cells>s_otsu, plt.cm.gray); plt.title('Otsu thresholding');
```

Figure 19.3 Automatic thresholding and thresholding by Otsu. Results are almost identical because threshold values are 105.3 and 105, respectively.

(a) Automatic threshold.



(b) Otsu threshold.



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19.6.3 k-means clustering

Different techniques can be found in the scikit documentation. A point cloud will first be generated, from 3 clustered cloud points. The objective is then to segment all the points into their original cluster.

Imports

```python
import numpy as np
import matplotlib.pyplot as plt
import time

from sklearn.cluster import KMeans
```

Generation of point clouds

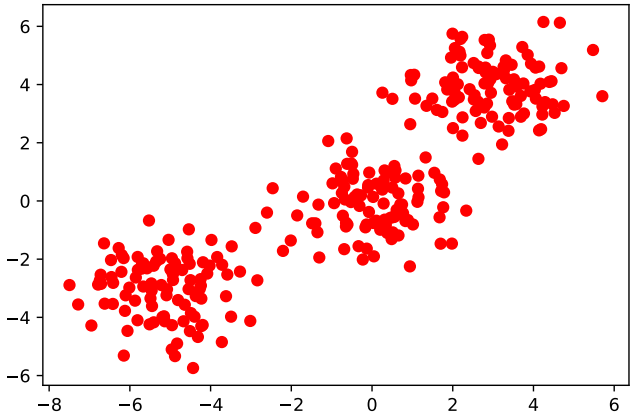
```python
def generation(n, x, y):
    Y = np.random.randn(n, 2) + np.array([[x, y]]);
    return Y

points1=generation(100, 0, 0);
points2=generation(100, 3,4);
points3=generation(100, -5, -3);

pts=np.concatenate((points1, points2, points3));
plt.plot(pts[:,0], pts[:,1], 'ro');

plt.show();
```

Figure 19.4 Point cloud.



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k-means clustering

```python
n=3; # number of clusters

# k-means initialization
k_means = KMeans(init='k-means++', n_clusters=n, n_init=10)
t0 = time.time(); # computation time
k_means.fit(pts); # kmeans segmentation

t_batch = time.time() -t0;

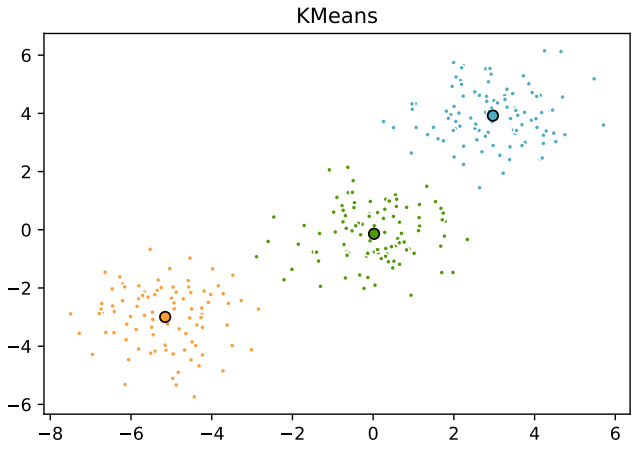
# retrieve results
k_means_labels = k_means.labels_;
k_means_cluster_centers = k_means.cluster_centers_;

# plot
fig = plt.figure()
colors = ['#4EACC5', '#FF9C34', '#4E9A06']

# k-means
# zip agregates values two by two
for k, col in zip(range(n), colors):
   my_members = k_means_labels == k
   cluster_center = k_means_cluster_centers[k]

   # display points
   plt.plot(pts[my_members, 0], pts[my_members, 1], 'w',
         markerfacecolor=col, marker='.')

   # display centroid
   plt.plot(cluster_center[0], cluster_center[1], 'o',
          markerfacecolor=col, markeredgecolor='k',
          markersize=6)
plt.title('KMeans')
plt.show()
fig.savefig("kmeans.pdf");
```



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19.6.4 Color image segmentation

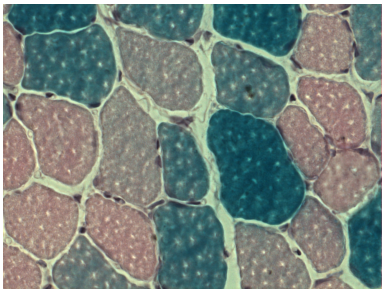
Three different colors can be observed in the image. The objective is to separate the 3 colors with the help of the K-means algorithm. Thus, the segmentation is performed in the RGB color space, and each pixel is represented by a point in this 3D space. Initialization steps are identical to previous code. The data is converted from a color image (of size $(n, m, 3)$) to a vector (of size $(n \times m, 3)$), done by the `reshape` function of numpy.

```
# load color image
cells=imageio.imread('Tv16.png');
[nLines,nCols,channels] = cells.shape
# reshape data
data = np.reshape(cells, (nLines*nCols, channels));
k_means.fit(data);
# convert result to an image
# as we got labels, we expand the dynamic (multiply by 70)
segmentation = 70*np.reshape(k_means.labels_, (nLines, nCols));

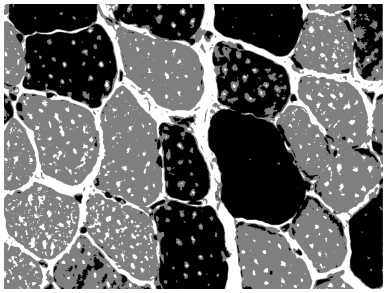
fig=plt.figure();
plt.imshow(segmentation, cmap=plt.cm.gray);
imageio.imwrite("segmentation_kmeans.png", segmentation);
```

Figure 19.5 Segmentation result.

(a) Original image.



(b) Segmented.



3D scatter plot

This is a method to display colors in the RGB cube. This method is really slow, depending on your GPU.

```
from mpl_toolkits.mplot3d import Axes3D # 3D scatter plot
# plot
colors = ['#4EACC5', '#FF9C34', '#4E9A06']

fig = plt.figure()
ax = fig.add_subplot(111, projection='3d')

# Plot scatter points
for k, col in zip(range(n), colors):
   my_members = k_means_labels == k
   cluster_center = k_means_cluster_centers[k]
   ax.scatter(data[my_members, 0], data[my_members, 1],
            data[my_members, 2], c=col)
   ax.scatter(cluster_center[0], cluster_center[1],
            cluster_center[2], s=30, c=col)
```

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20 Segmentation by region growing

This tutorial proposes to program the region growing algorithm.

20.1 Introduction

The region growing segmentation method starts from a seed. The initial region first contains this seed and then grows according to

- a growth mechanism (in this tutorial, the N_8 will be considered)
- an homogeneity rule (predicate function)

The algorithm is simple and barely only needs a predicate function:

Algorithm 7:

Data: I: image
Data: seed: starting point
Data: queue: queue of points to considere
Result: visited: boolean matrix, same size as I
begin
  queue.enqueue(seed);
  while *queue is not empty* **do**
    p = queue.dequeue();
    foreach *neighbor of* p **do**
      if *not visited(p)* ***and*** *neighbor verifies predicate* **then**
        queue.enqueue(neighbor);
        visited(neighbor) = true;
      end
    end
  end
  return visited
end

To get the coordinate of the mouse click, use the matplotlib connect utilities. Define a function `def onpick`.

```
# start by displaying a figure,
# ask for mouse input (click)
fig = plt.figure ();
ax = fig.add_subplot (211);
ax.set_title ('Click on a point')
# load image
img = misc.ascent ();
ax.imshow (img, picker = True, cmap = plt.gray ());
# connect click on image to onpick function
fig.canvas.mpl_connect ('button_press_event', onpick);
plt.show ();
def onpick(event):
    """ connector """
```

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20.2 Region growing implementation

>>>?

The seed pixel is denoted s.

- Code the predicate function: for an image f and a pixel p, p is in the same segment as s implies $|f(s) - f(p)| \leq T$.
- Code a function that performs region growing, from a starting pixel (seed).
- Try others predicate functions like:
  - pixel p intensity is close to the region mean value, i.e.:

$$|I(p) - m_s| \leq T$$

  - Threshold value T_i varies depending on the region R_i and the intensity of the pixel $I(p)$.It can be chosen this way:

$$T_i = (1 - \frac{\sigma_i}{m_i}) \cdot T$$

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20.3. Python correction

20.3.1 imports

```python
import queue
from scipy import misc
import matplotlib.pyplot as plt
import numpy as np
```

20.3.2 Predicate

This function defines the agregation condition.

```python
def predicate(image, i, j, seed) :
  f=image[i,j];
  g=image[seed[0], seed[1]];
  return abs(f-g)<20
```

The following code is used to start the region growing from a pixel manually clicked on an image.

```python
# start of code
fig = plt.figure();
ax = fig.add_subplot(211);
ax.set_title('Click on a point')

# load image
img = misc.ascent();
ax.imshow(img, picker=True,cmap=plt.gray());

fig.canvas.mpl_connect('button_press_event', onpick)
plt.show();
```

And here comes the main function for region growing. The result is illustrated in Fig.20.1.

```python
def onpick (event):
    """
    this functions gets the event 'click', and starts the region growing
        ↪ algorithm
    Notice that img is a global variable
    """
    print("x, y: ", event.xdata, event.ydata);
    # original pixel
    seed = np.array ([int (event.ydata), int (event.xdata)]);
    q = queue.Queue ();

    myfunctions = [predicate, predicate2, predicate3];

    for index,f in enumerate(myfunctions):
```

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```
14
15      # initializes the queue
16      q.put (seed);
17
18      #Visited matrix : result of segmentation
19      #this matrix will contain 1 if in the region, -1 if visited but not in the
            ↪ region, 0 if not visited
20      visited = np.zeros (img.shape)
21      #---------------
22      #Start of algorithm
23      visited[seed[0], seed[1]] = 1;
24
25      while not q.empty ():
26         p = q.get ();
27
28         for i in range (max (0, p[0] -1), min (img.shape[0], p[0] + 2)):
29            for j in range (max (0, p[1] -1), min (img.shape[1], p[1] + 2)):
30               if not visited[i, j]:
31                  if f(img, i, j, seed, visited):
32                     visited[i, j] = 1;
33                     q.put (np.array ([i, j]));
34                  else:
35                     visited[i, j] = -1;
36
37      #visited matrix contains the segmentation result
38      #display results
39      ax = fig.add_subplot (142+index);
40      ax.imshow (visited == 1);
41
42      imageio.imsave(f.__name__ +'_seg.python.png', (visited==1).astype('int'))
43
44   fig.canvas.draw ();
45   plt.show();
46   return;
```

Notice that values -1 of the `visited` matrix avoid testing multiple times the same pixel. In the predicate function, the `visited` matrix is used in case of adapting the predicate to the current region. In the next case, the candidate pixel's graylevel is compared to the mean gray value of the region. The results are illustrated Fig.20.1.

```
1 def predicate2(image, i, j, seed, visited):
2    f = int(image[i, j]);
3    m = np.mean(image[visited==1]);
4    return abs (f -m) < 20
```

Another predicate function would be:

```
1 def predicate3(image, i, j, seed, visited):
2    f = int(image[i, j]);
3    m = np.mean(image[visited==1]);
4    s = np.std(image[visited==1]);
5    return abs (f -m) < 20 * (1-s/m)
```

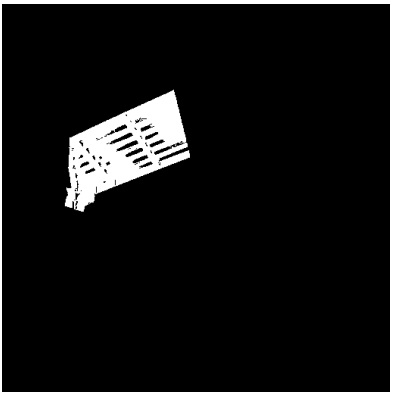
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Figure 20.1 Region growing illustration for pixel (189,136). The segmentation result highly depend on the order used to populate the queue, on the predicate function and on the seed pixel.

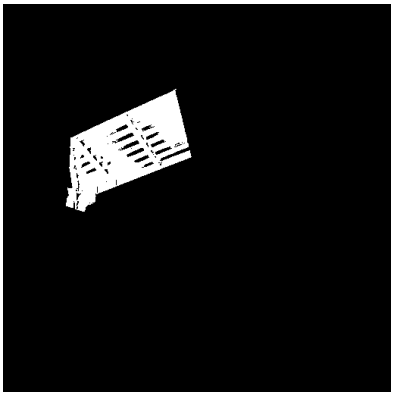
(a) Original image.



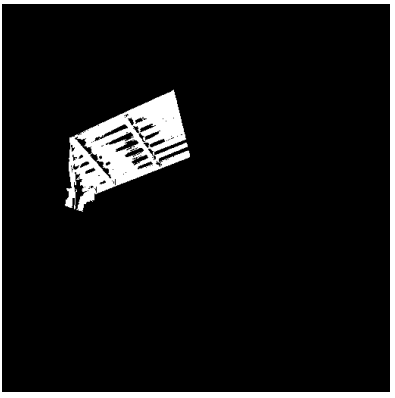
(b) Segmented region.



(c) Segmented region.



(d) Segmented region.



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21 Hough transform and line detection

This tutorial introduces the Hough transform. Line detection operators are implemented.

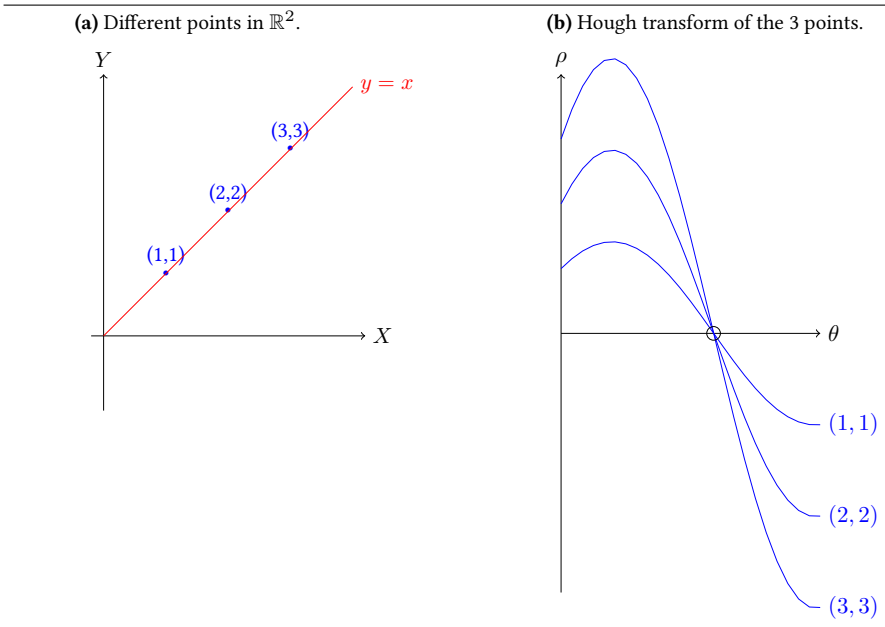
21.1 Introduction

This tutorial deals with line detection in an image. For a given point of coordinates (x, y) in $\mathbb{R}^2$, there exists an infinite number of lines going by this point, with different angles θ. These lines are represented by the following equation:

$$\rho = x \cdot \cos(\theta) + y \cdot \sin(\theta).$$

Thus, for each point (x, y) (Fig. 21.1a) corresponds a curve parametered by $[\theta, \rho]$, where $\theta \in [0;2\pi]$ (Fig. 21.1b). The intersection of these curves represents a line (in this case, $y = x$).

Figure 21.1 Representation of the Hough transform.



21.2 Algorithm

The (general and simple) method for line detection is then:

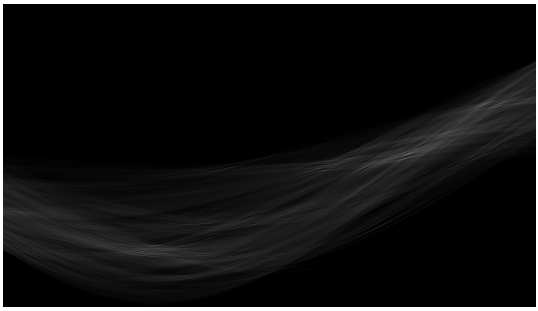
1. Compute contours detections (get a binary image BW).
2. Apply the Hough transform on the contours BW.
3. Detect the maxima of the Hough transform.
4. Get back in the Euclidean space and draw the lines on the image.

Results should look like in Fig. 21.2.

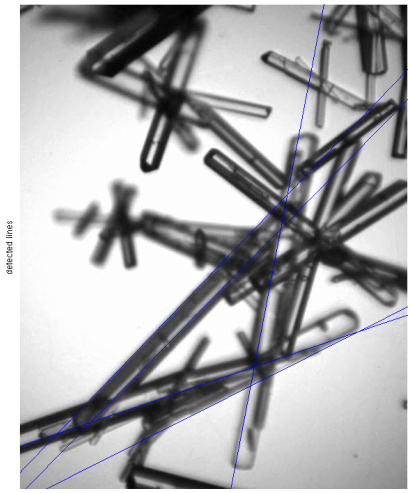
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Figure 21.2 Lines detection via Hough transform.

(a) Hough transform and maxima detection. Angles θ are represented in abscissa, pixels ρ are represented in ordinates. The detection of the absolute maxima of this images will lead to the lines.



(b) Line detection.



21.3 Hough transform

>>>?

Code a function that will transform each point of a binary image into a curve in the Hough space. For each curve, increment each pixel by one in the Hough space.

21.4 Maxima detection

>>>?

Use or code a function to detect maxima (regional maxima). For each maximum, keep only one point.

21.5 Display lines

>>>?

For each maximum, display the corresponding line above the original image.

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21.6. Python correction



This correction makes use of the python modules numpy, opencv, skimage and matplotlib.



```
import numpy as np
import cv2
import matplotlib.pyplot as plt
from skimage.feature import peak_local_max
```

21.6.1 Contours detection



```
img = cv2.imread('TestPR46.png');
plt.figure()
plt.imshow(img)

# perform contours detection
edges = cv2.Canny(img,100,200);
plt.figure()
plt.imshow(edges)
```

21.6.2 Hough transform

Notice that opencv contains Hough fonctions: `HoughLines` and `HoughLinesP`.



```
## Hough transform
# size of image
X = img.shape[0];
Y = img.shape[1];

angular_sampling = 0.01; # angles in radians

# initialization of matrix H
rho_max = np.hypot(X,Y);
rho = np.arange(-rho_max, rho_max, 1);
theta = np.arange(0, np.pi, angular_sampling);
cosTheta = np.cos(theta);
sinTheta = np.sin(theta);
H = np.zeros([rho.size, theta.size]);

# Hough transform
# loop on all contour pixels
for i in range(X):
   for j in range(Y):
      if (edges[i,j] != 0):
         R = i*cosTheta + j*sinTheta;
         R = np.round(R + rho.size/2).astype(int);
         H[R,range(theta.size)] += 1;

plt.imshow(H);
```

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21.6.3 Maxima detection

The function `peak_local_max` from `skimage` is used to detect local maxima in the Hough transform. Matrix H is first smoothed with a Gaussian filter.

```
# Maxima detection
G = cv2.GaussianBlur(H, (5,5), 5);
maxima = peak_local_max(H, 5, threshold_abs=150, num_peaks=5);
plt.figure();
plt.imshow(G);

# display maxima on Hough transform image G
plt.scatter(maxima[:,1], maxima[:,0], c='r');
plt.show();
```

21.6.4 Resulting lines

The result is shown in Fig.21.3.

```
# display the results as lines in image
for i_rho, i_theta in maxima:
   print rho[i_rho], theta[i_theta]
   a = np.cos(theta[i_theta])
   b = np.sin(theta[i_theta])
   y0 = a*rho[i_rho]
   x0 = b*rho[i_rho]
   y1 = int(y0 + 1000*(-b))
   x1 = int(x0 + 1000*(a))
   y2 = int(y0 -1000*(-b))
   x2 = int(x0 -1000*(a))

   cv2.line(img,(x1,y1),(x2,y2),(0,0,255),2)

# display in window
cv2.imshow('hough transform', img);
# write resulting image
cv2.imwrite('cv_hough.png', img);
```

21.6.5 OpenCV builtin function

```
import cv2
import numpy as np

# read image and convert it to gray
img = cv2.imread('TestPR46.png')
gray = cv2.cvtColor(img,cv2.COLOR_BGR2GRAY)
edges = cv2.Canny(gray, 100, 200, apertureSize = 3)

# threshold value for lines selection:
# lower value means more lines
threshold = 150;

# perform lines detection
lines = cv2.HoughLines(edges, 1, np.pi/180, threshold)

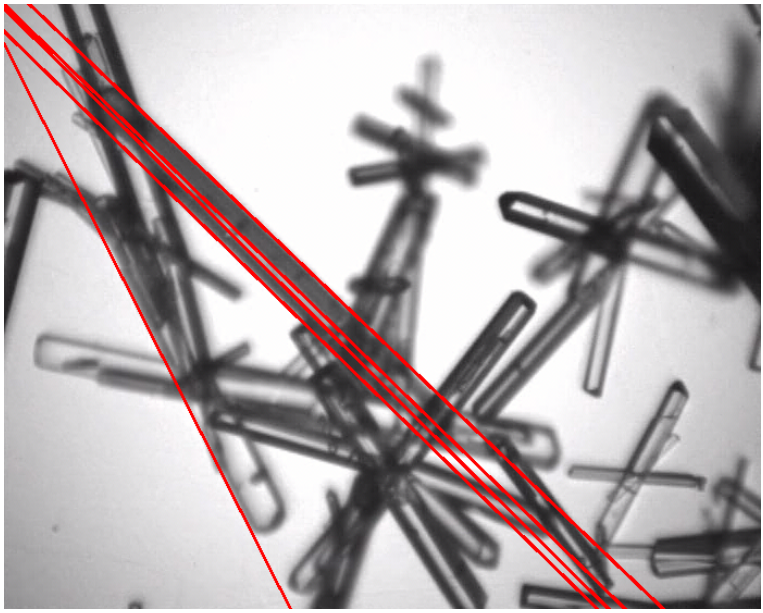
```

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```
# display lines
for rho,theta in lines[0]:
    print rho, theta
    a = np.cos(theta)
    b = np.sin(theta)
    x0 = a*rho
    y0 = b*rho
    x1 = int(x0 + 1000*(-b))
    y1 = int(y0 + 1000*(a))
    x2 = int(x0 -1000*(-b))
    y2 = int(y0 -1000*(a))
    print x1, y1, x2, y2
    cv2.line(img,(x1,y1),(x2,y2),(0,0,255),2)

cv2.imshow('hough transform', img);
cv2.imwrite('cv_hough.png', img);
```

Figure 21.3 Lines detected with the Hough transform.



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22 Active contours

This tutorials aims at introducing the active contours (a.k.a. snakes) method as originally presented in [18]. It is a segmentation method based on the optimization of a contour that will converge to a specific object.

22.1 Definition

A snake is a parametric curve $v(s)$ with $s \in [0;1[$. The energy functional is represented by:

$$E_{snake} = \int_0^1 E_{\text{int}}(v(s))\mathrm{d}s + \int_0^1 E_{\text{ext}}(v(s))\mathrm{d}s.$$

The internal energy is detailed in Eq.22.1. The first order derivation constrains the length of the curve, the second order derivation constrains the curvature. The parameters α and β a priori depend on s, but for simplicity, constant values will be taken.

$$E_{\text{int}}(v(s)) = \frac{1}{2}\left(\underbrace{\alpha(s)|v'(s)|^2}_{length} + \underbrace{\beta(s)|v''(s)|^2}_{curvature}\right) \tag{22.1}$$

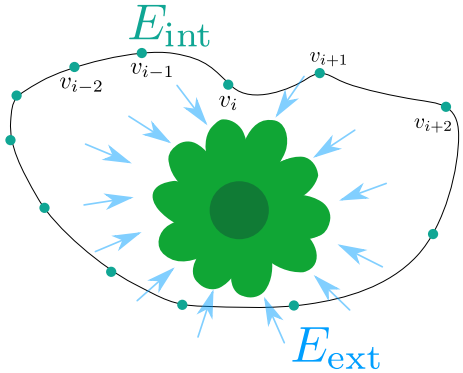
The snake will be attracted by some edges points from the external energy (the image to be segmented). The, the energy functional will be in a local minimum: it is shown that the Euler-Lagrange equation is satisfied:

$$-\alpha v^{(2)} + \beta v^{(4)} + \nabla E_{\text{ext}} = 0$$

with $v^{(2)}$ and $v^{(4)}$ denoting the 2nd and 4th order derivatives. To solve this equation, the gradient descent method is employed: the snake is now transformed into a function of the position s and the time t, with $F_{\text{ext}} = -\nabla E_{\text{ext}}$

$$\frac{\partial s}{\partial t} = \alpha v^{(2)} - \beta v^{(4)} + F_{\text{ext}}$$

Figure 22.1 Illustration of the active contours segmentation method. Two energies are at stake: internal energies depend only on the snake shape and control points, external energies are related to the image properties.



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22.2 Numerical resolution

The spatial derivatives are approximated with the finite difference method, and the snake is now composed of n points, $i \in [1; n]$:

$$\begin{aligned} x^{(2)} &= x_{i-1} - 2x_i + x_{i+1} \\ x^{(4)} &= x_{i-2} - 4x_{i-1} + 6x_i - 4x_{i+1} + x_{i+2} \end{aligned}$$

The gradient descent method can be written as, with γ being the time step and controls the convergence speed:

$$\begin{aligned} \frac{x_t - x_{t-1}}{\gamma} &= A \cdot x_t + f_x(x_{t-1}, y_{t-1}) \\ \frac{y_t - y_{t-1}}{\gamma} &= A \cdot y_t + f_y(x_{t-1}, y_{t-1}) \end{aligned}$$

with

$$A = \begin{bmatrix} -2\alpha{-}6\beta & \alpha{+}4\beta & -\beta & 0 & \cdots & 0 & -\beta & \alpha{+}4\beta \\ \alpha{+}4\beta & -2\alpha{-}6\beta & \alpha{+}4\beta & -\beta & 0 & \cdots & 0 & -\beta \\ -\beta & \alpha{+}4\beta & -2\alpha{-}6\beta & \alpha{+}4\beta & -\beta & 0 & \cdots & 0 \\ 0 & -\beta & \alpha{+}4\beta & -2\alpha{-}6\beta & \alpha{+}4\beta & -\beta & 0 & \cdots \\ \vdots & & \ddots & \ddots & \ddots & \ddots & & \vdots \\ 0 & \cdots & -\beta & \alpha{+}4\beta & -2\alpha{-}6\beta & \alpha{+}4\beta & -\beta & 0 \\ 0 & \cdots & 0 & -\beta & \alpha{+}4\beta & -2\alpha{-}6\beta & \alpha{+}4\beta & -\beta \\ -\beta & 0 & \cdots & 0 & -\beta & \alpha{+}4\beta & -2\alpha{-}6\beta & \alpha{+}4\beta \\ \alpha{+}4\beta & -\beta & 0 & \cdots & 0 & -\beta & \alpha{+}4\beta & -2\alpha{-}6\beta \end{bmatrix}$$

The forces f_x and f_y are the components of F_{ext}. For example for an image I, if $*$ denotes the convolution and G_σ a gaussian kernel of standard deviation σ:

$$F_{\text{ext}} = -\nabla(\|\nabla(G_\sigma * I)\|)$$

>>>?

- Generate a binary image (of size $n \times n$ pixels, with values 0 and 1) containing a disk (of a radius R).
- Generate the initial contour as an ellipse, with the same center as the disk.
- Generate the pentadiagonal matrix A. The different parameters can be $\alpha = 10^{-5}$ and $\beta = 0.05$.
- Program the iterations and visualize the results. For example, $\gamma = 200$ and 1000 iterations may give an idea of the parameters to use.

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22.3. Python correction



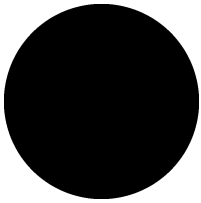
```python
import numpy as np
import matplotlib.pyplot as plt
import scipy
import scipy.ndimage.filters
from scipy import interpolate
import progressbar
```

22.3.1 Binary image generation

A disk (Fig.22.2) is generated via the `meshgrid` function.

```python
# disk: number of points
n = 1024;
# disk: radius
R = 300;
# construct a binary image of a disk
X, Y = np.meshgrid(np.arange(-n/2,n/2,1), np.arange(-n/2,n/2,1));
I = X**2+Y**2<=R**2;
I = I.astype('float')
```

Figure 22.2 Circle.



22.3.2 Initial contour

The choice of the initial contour (Fig.22.3) is crucial in this method. The parameters used in this example ensure the convergence of the snake.

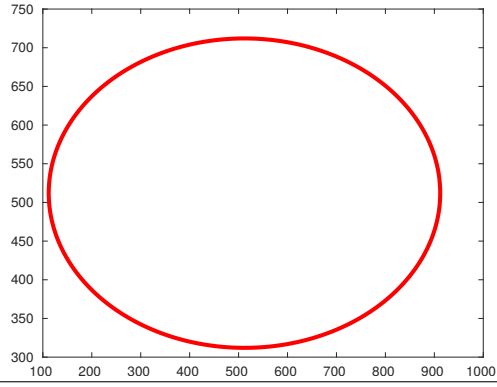
```python
step=.01;
x = n/2 + 400 * np.cos(np.arange(0,2*np.pi+step,step));
y = n/2 + 200 * np.sin(np.arange(0,2*np.pi+step,step));
```

The different parameters are defined by:

```python
k=.1;
alpha = .0001;
beta = 10;
gamma= 100;
iterations = 1000;
```

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Figure 22.3 Circle.



22.3.3 Matrix construction

This is maybe the hardest part of this code, with the use of the `scipy.sparse.diags` function.

```
N = x.size;
X = np.array([-beta, alpha+4*beta, -2*alpha-6*beta, alpha+4*beta, -beta, -beta,
    ↪ alpha+4*beta, -beta, alpha+4*beta])
A = scipy.sparse.diags(X, np.array([-2, -1, 0, 1, 2, N-2, N-1, -N+2, -N+1]),
    ↪ shape=(N,N)).toarray();
AA = np.identity(N)-gamma*A;
invAA = np.linalg.inv(AA);
```

22.3.4 External forces

The external forces are computed with the following code. Notice that axis 0 correspond to the vertical axis (y) and and the axis 1 corresponds to the horizontal axis (x).

```
# external forces computation
G = scipy.ndimage.filters.gaussian_gradient_magnitude(I, 30);
# Notice that horizontal axis x is 1, and vertical axis is 0
Fy = scipy.ndimage.prewitt(G, axis=0);
Fx = scipy.ndimage.prewitt(G, axis=1);
```

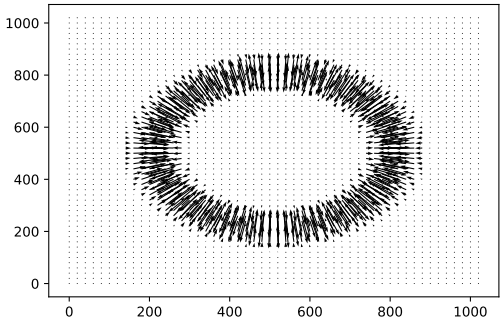
22.3.5 Display results

To enhance the role of the external forces, the arrows showing the force are displayed (`quiver` function, see Fig.22.4).

```
imshow(I,[])
hold on
plot([x;x(1)], [y; y(1)], 'g', 'linewidth', 3);
# display arrows for external forces
step=20;
subx = 1:step:size(I,1);
suby = 1:step:size(I,2);
[Xa, Ya] = meshgrid(subx, suby);
quiver(Xa, Ya, Fx(subx, suby), Fy(subx,suby));
```

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Figure 22.4 External forces that will be applied to the snake.

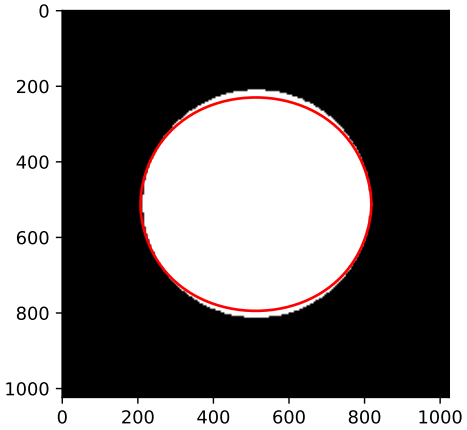


22.3.6 Convergence algorithm

```python
# interpolation methods to get values of the external forces at the
# coordinates of the snake
sx, sy = I.shape;
ix = interpolate.interp2d(np.arange(n), np.arange(n), Fx);
iy = interpolate.interp2d(np.arange(n), np.arange(n), Fy);
# loop for convergence of the snake
bar = progressbar.ProgressBar();
for index in bar(range(iterations)):
    fex = np.array([float(ix(XX,YY)) for XX,YY in zip(x,y)]);
    fey = np.array([float(iy(XX,YY)) for XX,YY in zip(x,y)]);
    #print(np.max(fex), np.min(fex))
    x = np.matmul(invAA, x+gamma*fex);
    y = np.matmul(invAA, y+gamma*fey);
```

The results are displayed in Fig.22.5.

Figure 22.5 Result of the snake converging toward the disk, after 1000 iterations with the proposed parameters.



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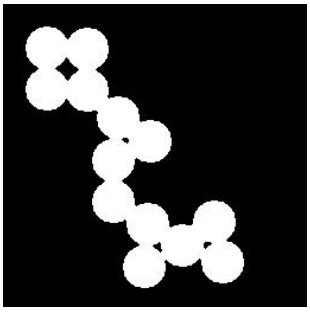
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★★★ 23 Watershed

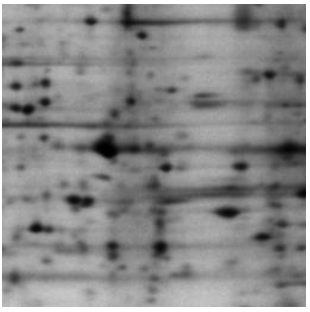
This tutorial aims to study the watershed transform for image segmentation. In image processing, an image can be considered as a topographic surface. If we flood this surface from its minima and if we prevent the merging of the water coming from different sources, we partition the image into two different sets: the catchment basins separated by the watershed lines.

The different processes will be applied on the following images:

(a) circles



(b) gel



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23.1 Watershed and distance maps

The objective is to individualize the disks by disconnecting them with the distance map.

>>>?

- Calculate the distance map of the image 'circles'.
- Take the complementary of this distance map and visualize its minima.
- Calculate the watershed transform of the inverted distance map.
- Subtract the watershed lines to the original image.

Look at the documentation of `scipy.ndimage.morphology` for Euclidean or Chamfer distance transform. Reconstruction operator can be found in `skimage.morphology`.

23.2 Watershed and image gradients

>>>?

- Calculate the Sobel gradient of the image 'gel'.
- Visualize the minima of the image gradient.
- Apply the watershed transform on the gradient image.

The watershed transform, applied in a direct way, leads to an over-segmentation. To overcome this limitation, the watershed operator can be applied on a filtered image.

>>>?

- Smooth the original image with a low pass filter. To stay in the mathematical morphology field, you can use an alternate morphological filter (opening followed by closing). A Gaussian filter is also a good solution.
- Calculate the gradient operator on the filtered image.
- Calculate the corresponding watershed.

23.3 Constrained watershed by markers

In order to indivudualize the image spots, we have to determine the internal and external markers for the constrained watershed.

>>>?

- Calculate the gradient (Sobel) of the filtered image.
- Calculate the internal markers (minima of the filtered image) and external (watershed of the filtered image) as minima of the gradient image.
- Calculate the corresponding watershed.
- Superimpose the watershed lines of the resulting segmentation to the original image.

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23.4. Python correction

```python
import numpy as np
from scipy import misc
import matplotlib.pyplot as plt
from scipy import ndimage as ndi
from scipy.ndimage.morphology import distance_transform_edt
from scipy.ndimage.morphology import distance_transform_cdt
from skimage import morphology
```

23.4.1 Watershed and distance map

Regional maxima

The following code is an implementation of the regional maxima (from mathematical morphology definition). It deals with the case of float images as input.

```python
def rmax(I):
    """
    Own version of regional maximum
    This avoids plateaus problems of peak_local_max
    I: original image, int values
    returns: binary array, with True for the maxima
    """
    I = I.astype('float');
    I = I / np.max(I) * 2**31;
    I = I.astype('int32');
    h = 1;
    rec = morphology.reconstruction(I, I+h);
    maxima = I + h -rec;
    return maxima>0
```

Distance map followed by a watershed

This method is a classical way of performing the separation of some objects by proximity or influence zones. It is illustrated in Fig.23.1.

```python
A = imageio.imread('circles.tif');
# chamfer distance gives integer distances
dm = distance_transform_edt(A);
# regional maxima
local_maxi = rmax(dm);
```

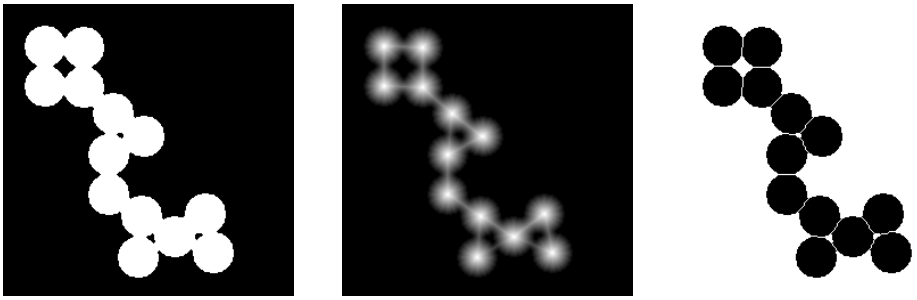
The local maxima will be used as a marker for the watershed operation, in order to perform the separation of the grains, see Fig.23.1.

```python
# watershed segmentation for separating the circles
markers = ndi.label(local_maxi, np.ones((3, 3)))[0]
W = morphology.watershed(-dm, markers, watershed_line=True)
# separation of the grains
B = A & W==0;
separation = ndi.label(B, np.ones((3,3)))[0];
```

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Figure 23.1 Steps of the separation of the grains.

(a) Original image. **(b)** Distance map. **(c)** Separation of the grains.



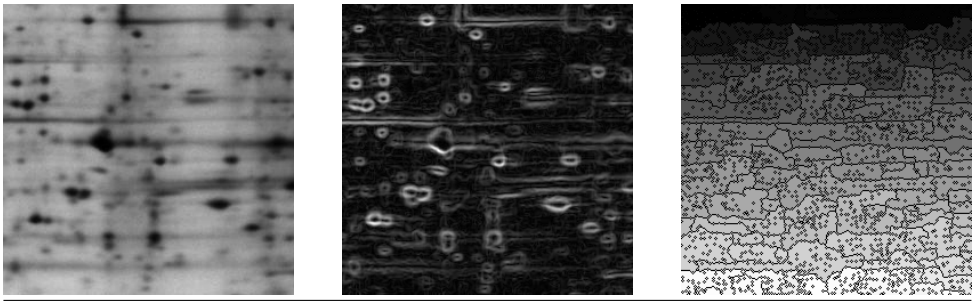
23.4.2 Watershed and image gradients

The gradient image amplifies the noise. Thus, the watershed operator directly applied to the gradient of the image produces an over-segmented image (see Fig.23.2).

```python
def sobel_mag(im):
    """
    Returns Sobel gradient magnitude
    im: image array of type float
    returns: magnitude of gradient (L2 norm)
    """
    dx = ndi.sobel(im, axis=1) # horizontal derivative
    dy = ndi.sobel(im, axis=0) # vertical derivative
    mag = np.hypot(dx, dy) # magnitude
    return mag;
```

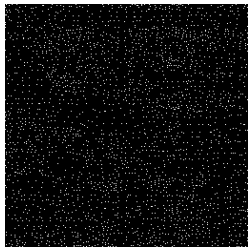
Figure 23.2 Performing the watershed on the gradient image is usually not a good idea.

(a) Original image. **(b)** Amplitude of the gradient (Sobel). **(c)** Watershed segmentation.



In fact, this method produces as many segments as there are minima in the gradient image Fig.23.3.

Figure 23.3 Local minima of the gradient image.



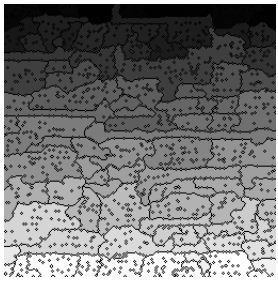
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Solution: filtering the image

Before evaluating the gradient, the image is filtered. The number of minima is lower and this leads to a less over-segmented image (Fig.23.4).

```
SE = morphology.disk(2);
O = morphology.opening(gel, selem=SE);
F = morphology.closing(O, selem=SE).astype('float');
g = sobel_mag(F).astype('float');
```

Figure 23.4 Even if the gradient is performed on the filtered image, there is still a high over-segmentation.



23.4.3 Watershed constrained by markers

The watershed can be constrained by markers: the markers can provide the correct number of regions. This method imposes both the background (external markers) and the objects (internal markers). The results are illustrated in Fig.23.5. The ultimate erosion of the internal markers is used to deconnect these markers from the external markers.

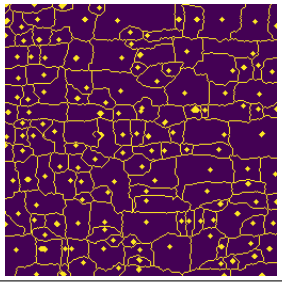
```
local_maxi = rmax(255-F);
markers = ndi.label(local_maxi, np.ones((3, 3)))[0]
W = morphology.watershed(F, markers, watershed_line=True)

markers2 = local_maxi | (W==0);
M = ndi.label(markers2, np.ones((3, 3)))[0]
segmentation = morphology.watershed(g, M, watershed_line=True);

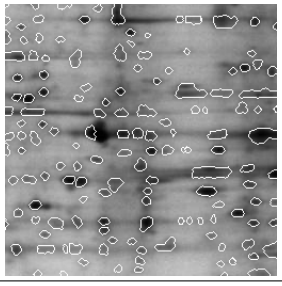
gel[segmentation==0] = 255;
plt.imshow(gel);
plt.show();
imageio.imwrite("segmentation.python.png", gel);
```

Figure 23.5 Watershed segmentation by markers.

(a) Markers of the background and of the objects.



(b) Final segmentation.



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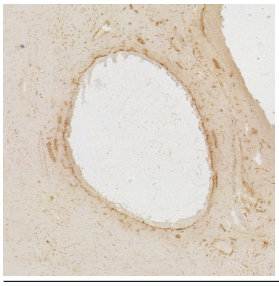
24 Segmentation of follicles

This practical work aims to investigate image segmentation with a direct application to ovarian follicles. The overall objective is to extract and quantify the granulosa cells and the vascularization of each follicle included in an ewe's ovary.

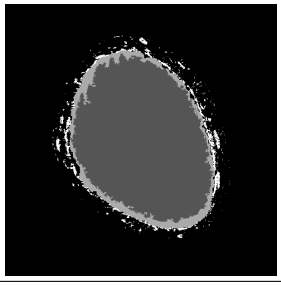
The image to be processed is a 2D histological image of an ewe's ovary acquired by optical microscopy in Fig.24.1. The presented image contains one entire follicle (the white region and its neighborhood) and a part of a second one (right-upper corner). The follicle is composed of different parts shown in: antrum, granulosa cells and vascularization. The theca is the ring region around the antrum where the follicle is vascularized.

Figure 24.1 Different parts of the follicles, to be segmented.

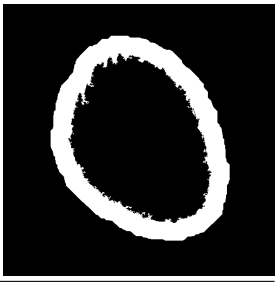
(a) Original image with one entire follicle (white region and its neigborhood).



(b) Antrum (dark gray), granulosa cells (light gray) and vascularization (white) of the follicle.



(c) Theca.



24.1 Vascularization

>>>?

- Load and visualize the image.
- Extract the antrum of the follicle.
- Extract the vascularization (inside a ring around the antrum).

24.2 Granulosa cells

>>>?

Which kind of processing could be suitable for extracting the granulosa cells?

24.3 Quantification

>>>?

Provide some geometrical measurements of the different entities of the follicle (antrum, vascularization, granulosa cells).

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24.4. Python correction

```python
import numpy as np
import matplotlib.pyplot as plt
from scipy import misc,ndimage
from skimage import morphology
```

24.4.1 Vascularization

Antrum segmentation

The first step consists in the segmentation of the antrum by thresholding the blue component. Some post-processes are used to remove artifacts such as holes. This is illustrated in Fig. 24.2.

```python
A = imageio.imread('follicle.png');
plt.imshow(A);
plt.show();
## Antrum
# segmentation by mathematical morphology
# manual selection of the antrum
B = A[:,:,2];
antrum = B > 220;
L = morphology.label(antrum, connectivity=2);
antrum = L == L[300,300];
antrum = ndimage.morphology.binary_fill_holes(antrum);
plt.imshow(antrum);
plt.title('Antrum')
plt.show();
```

Theca segmentation

The second step provides the segmentation of the theca which is extracted as a spatial region (corona) adjacent to and outside the antrum. The width of the corona is selected by the user (expert).

```python
se40 = morphology.disk(40);
theca = morphology.binary_dilation(antrum, selem = se40);
theca = theca -antrum;
plt.imshow(theca); plt.title('Theca')
plt.show()
```

Vascularization segmentation

The final step extracts the vascularization of the considered follicle. Pixels belonging to the vascularization are considered to have a low blue component and they should also be included in the antrum of the follicle.

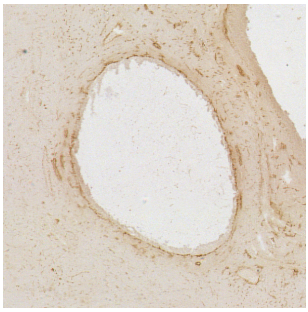
```python
vascularization = B < 140;
vascularization = vascularization * theca;
plt.imshow(vascularization);
plt.title('vascularization')
plt.show();
```

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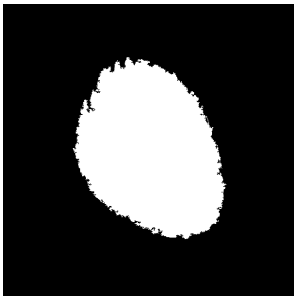
Results

Figure 24.2 Extraction of the different components of the follicle.

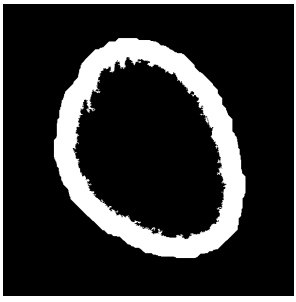
(a) Original image.



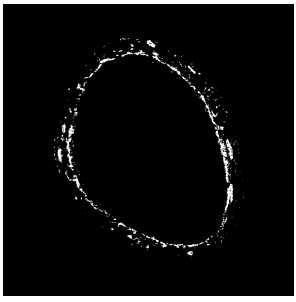
(b) Antrum.



(c) Theca.



(d) Vascularization.



24.4.2 Granulosa cells

First solution

The granulosa cells have a low contrast, so it is difficlut to use thresholding techniques. But we know they are localized between the antrum and the vascularization. Nevertheless the vascularization is not a closed region outside the antrum. Therefore, the proposed solution consits in firt trying to close the vascularization region and taking the corona between this region and the antrum. The result is shown in Fig. 24.3.

```
se10 = morphology.disk(10);
dil = 1-morphology.binary_closing(vascularization, se10);
L = morphology.label(dil, connectivity=1);
dil = L == L[300,300];
granulosa = dil -antrum;
plt.imshow(granulosa);
plt.title('granulosa')
plt.show()
```

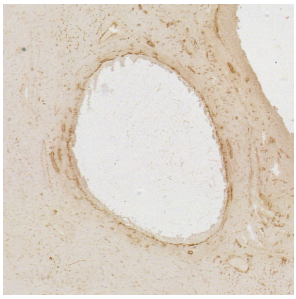
Second solution

This first solution is not really robust. The closing of the vascularization region is not really accurate. A more robust solution consists in using deformable models to get the corona between the vascularization and the antrum. But this kind of method is out of the scope of this tutorial.

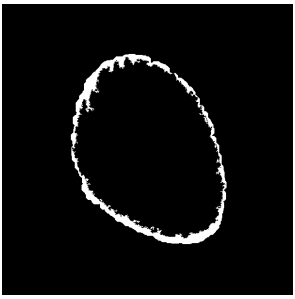
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Figure 24.3 Extraction of the granulosa cells of the follicle.

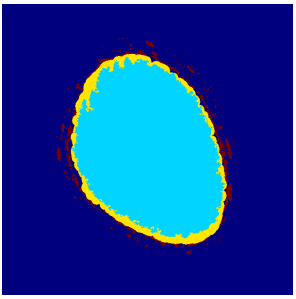
(a) Original image.



(b) Granulosa cells.



(c) Segmentation of the different parts.



24.4.3 Quantification

The quantification is easy to process. In addition, we can represent the different extracted components of the follicle in false colors.

```
result = antrum + 2*granulosa + 3*vascularization;
plt.imshow(result, cmap='jet');
plt.show();
plt.imsave("result.png", result, cmap='jet');

follicle = antrum + theca;
q_vascularization = np.sum(vascularization) / np.sum(follicle);
print('vascularization: ', q_vascularization)
q_granulosa = np.sum(granulosa)/np.sum(follicle);
print('Granulosa: ', q_granulosa);
```

This quantification gives:

```
vascularization: 0.0428495233516
Granulosa: 0.0913707490403
```

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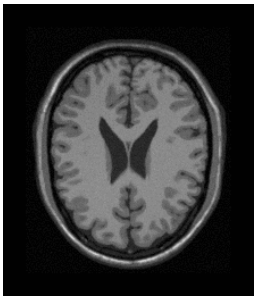
★★★ 25 Image Registration

This tutorial aims to implement the Iterative Closest Point (ICP) method for image registration. More specifically, we are going to estimate a rigid transformation (translation + rotation without scaling) between two images.

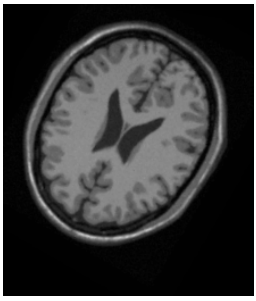
The different processes will be applied on T1-MR images of the brain in Fig.25.1.

Figure 25.1 Original images.

(a) brain1



(b) brain2



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25.1 Transformation estimation

A classical method in image registration first consists in identifying and matching some characteristic points by pairs. Thereafter, the transformation is estimated from this list of pairs (displacement vectors).

25.1.1 Preliminaries

Pairs of points are first manually selected.

>>>?

- Read and visualize the two MR images 'brain1' and 'brain2' (moving and source images).
- Manually select a list of corresponding points.

There is no built-in function for manual selection of pairs of points. You can use the following points or code your own function, see tutorial 20

```
# define control points
A_points = np.array([[136, 100], [127, 153], [96, 156], [87, 99]]);
B_points = np.array([[144, 99] , [109, 140], [79, 128], [100, 74]]);
```

25.1.2 Rigid transformation

With this list of pairs $(p_i, q_i)_i$, this tutorial proposes to estimate a rigid transformation between these points. It is composed of a rotation and a translation (and not scaling). For doing that, we make a Least Squares (LS) optimization, which is defined as follows. The parameters of the rotation R and the translation t minimize the following criterion:

$$C(R,t) = \sum_i ||q_i - R.p_i - t||^2$$

Calculation of the translation :
The optimal translation is characterized by a null derivative of the criterion:

$$\frac{\partial C}{\partial t} = -2\sum_i (q_i - R.p_i - t)^{\mathrm{T}} = 0 \Leftrightarrow \sum_i q_i - R.\left(\sum_i p_i\right) = N.t$$

where N denotes the number of matching pairs. By denoting $\bar{p} = \frac{1}{N}\sum_i p_i$ and $\bar{q} = \frac{1}{N}\sum_i q_i$ the barycenters of the point sets and by changing the geometrical referential: $p'_i = p_i - \bar{p}$ et $q'_i = q_i - \bar{q}$, the criterion can be written as:

$$C'(R) = \sum_i ||q'_i - R.p'_i||^2$$

The estimated rotation $\hat{R}$ will provide the expected translation:

$$\hat{t} = \bar{q} - \hat{R}.\bar{p} \tag{25.1}$$

calculation of the rotation by the SVD method:
We will use the following theorem: Let $U.D.V^{\mathrm{T}} = K$ a singular decomposition of the correlation matrix $K = q'^{\mathrm{T}}.p'$, for which the singular values are sorted in the increasing order. The minimum of the criterion: $C(R) = \sum_i ||q'_i - R.p'_i||^2$ is reached by the matrix :

$$\hat{R} = U.S.V^{\mathrm{T}} \tag{25.2}$$

with $S = DIAG(1, \ldots, 1, \det(U).\det(V))$.

>>>?

- Code a function that takes as parameters the pairs of points, and returns the rigid transformation elements of rotation $\hat{R}$ and translation $\hat{t}$ as defined in Eqs.25.1 and 25.2.
- Apply the transformation to the moving image.
- Visualize the resulting registered image.



- See `svd` function from `scipy.linalg` or `numpy.linalg`.
- See `cv2.warpAffine` and `cv2.transform` for transformation application

25.2 ICP-based registration

When the points are not correctly paired, it is first necessary to reorder them before estimating the transformation. In this way, the ICP (iterative Closest Points) consists in an iterative process of three steps: finding the correspondence between points, estimating the transformation and applying it. The process should converge to the well registered image.

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>>>?

To simulate the mixing of the points, randomly shuffle them selected on the first image and perform the registration with the previous method.



See `np.random.permutation`.

>>>?

1. From the list of the characteristic points p of the image 'brain1', find the nearest neighbors q in the image 'brain2'. Be careful to the order of the input arguments.
2. Estimate the transformation T by using the LS minimization coded previously.
3. Apply this transformation to the points p, find again the correspondence between these resulting points $T(p)$ and q and estimate a new transformation. Repeat the process until convergence.
4. Visualize the resulting registered image.



Look at `scipy.spatial.cKDTree` for nearest neighbor search.

25.3 Automatic control points detection

The manual selection of points may be fastidious. Two simple automatic methods for detecting control points are the so-called Harris corners detection or Shi-Tomasi corner detector.



The function `goodFeaturesToTrack` returns the corners from the Shi-Tomasi method.

>>>?

Replace the manual selection in the two previous parts of this tutorial.

Notice that the automatic points detection does not ensure to give the same order in the points of the two images. More generally, other salient points detectors do not give the same number of points, and thus the algorithms have to remove outliers (non matching points). This case is not taken into account in this tutorial.

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25.4. Python correction

```python
from scipy import misc
import matplotlib.pyplot as plt
import numpy as np
import cv2
from scipy.spatial import cKDTree
```

25.4.1 Transformation estimation based on corresponding points

Image visualization

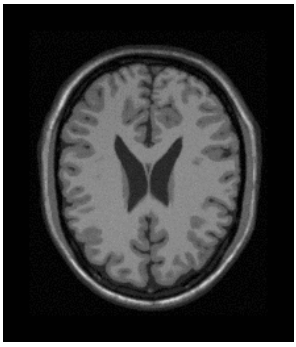
The following code is used to display the images (see Fig.25.2).

```python
# Read images and display
A=imageio.imread("brain1.bmp")
B=imageio.imread("brain2.bmp")
plt.imshow(A,cmap='gray');
plt.show();
plt.imshow(B,cmap='gray');
plt.show();

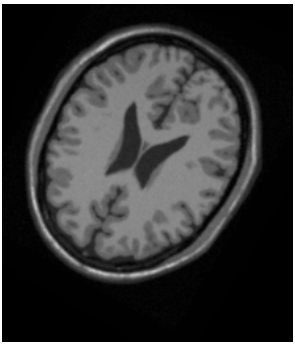
# define control points
A_points = np.array([[136, 100], [127, 153], [96, 156], [87, 99]]);
B_points = np.array([[144, 99], [109, 140], [79, 128], [100, 74]]);
```

Figure 25.2 Initial images.

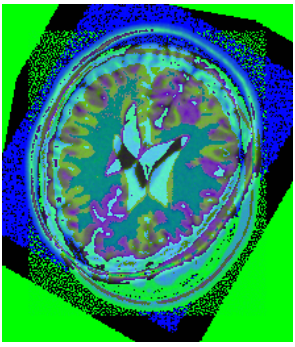
(a) Moving image.



(b) Source image.



(c) Superimposition.



If you want to display and save the fusion of both images, you can use this function:

```python
def superimpose(G1, G2, filename=None):
    """
    superimpose 2 images, supposing they are grayscale images and of same shape
    """
    r,c=G1.shape;
    S = np.zeros((r,c,3));
```

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```
    S[:,:,0] = np.maximum(G1-G2, 0)+G1;
    S[:,:,1] = np.maximum(G2-G1, 0)+G2;
    S[:,:,2] = (G1+G2) / 2;
    S = 255 * S / np.max(S);
    S = S.astype('uint8');
    plt.imshow(S);
    plt.show()
    if filename!=None:
       cv2.imwrite(filename, S);
    return S
```

Manual selection of corresponding points

With openCV, there is not built-in function to make a manual selection of pairs of control points. The following code uses a global variable I in order to manage the display of the points, which are finally stored into the pts variable. First, the callback function `on_mouse` is defined to handle mouse event.

```
pts = [];
def on_mouse(event, x, y, flags, param):
    """
    callback method for detecting click on image
    It draws a circle on the global variable image I
    """
    global pts, I;
    if event == cv2.EVENT_LBUTTONUP:
       pts.append((x, y));
       cv2.circle(I,(x,y), 2, (0,0,255), -1)
```

The function `cpselect` allows the selection of multiple points.

```
def cpselect():
    """
    method for manually selecting the control points
    It waits until 'q' key is pressed.
    """
    cv2.namedWindow("image")
    cv2.setMouseCallback("image", on_mouse)
    print("press 'q' when finished")
    # keep looping until the 'q' key is pressed
    while True:
      # display the image and wait for a keypress
      cv2.imshow("image", I)
      key = cv2.waitKey(1) & 0xFF

      # if the 'c' key is pressed, break from the loop
      if key == ord("q"):
        break

    # close all open windows
    cv2.destroyAllWindows()
    return pts;
```

Transformation estimation

The rigid transformation is estimated from the corresponding points by the following function:

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```python
def rigid_registration(data1, data2):
    """
    Rigid transformation estimation between n pairs of points
    This function returns a rotation R and a translation t
    data1 : array of size nx2
    data2 : array of size nx2
    returns transformation matrix T of size 2x3
    """
    data1 = np.array(data1);
    data2 = np.array(data2);

    # computes barycenters, and recenters the points
    m1 = np.mean(data1,0);
    m2 = np.mean(data2,0);
    data1_inv_shifted = data1-m1;
    data2_inv_shifted = data2-m2;

    # Evaluates SVD
    K = np.matmul(np.transpose(data2_inv_shifted), data1_inv_shifted);
    U,S,V = np.linalg.svd(K);

    # Computes Rotation
    S = np.eye(2);
    S[1,1] = np.linalg.det(U)*np.linalg.det(V);
    R = np.matmul(U,S);
    R = np.matmul(R, np.transpose(V));

    # Computes Translation
    t = m2-np.matmul(R, m1);

    T = np.zeros((2,3));
    T[0:2,0:2] = R;
    T[0:2,2] = t;
    return T;
```

Then, you can apply this function to the manually selected points.

```python
# 1st case, rigid registration, with pairs of points in the correct order
T = rigid_registration(A_points, B_points);

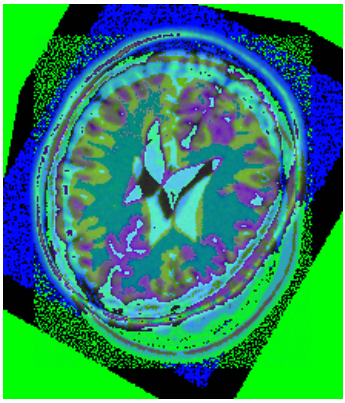
# Apply transformation on control points and display the results
data_dest = applyTransform(A_points, T);
I = B.copy();
for pb,pa in zip(data_dest, B_points):
    cv2.circle(I,totuple(pa), 1, (255,0,0), -1)
    cv2.circle(I,totuple(pb), 1, (0,0,255), -1)
plt.imshow(I);
plt.show();
# Apply transformation on image
rows, cols= B.shape;
dst = cv2.warpAffine(A,T, (cols, rows));
plt.imshow(dst);
superimpose(dst, B, "rigid_manual.png");
```

The result is good, because the manual selection of the points is good (the points are given in the correct order for both images).

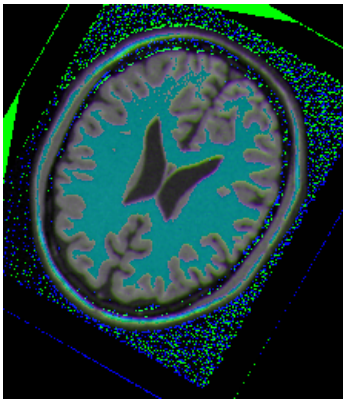
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Figure 25.3 Result of the registration for the manually selected control points.

(a) Without registration.



(b) With registration.



25.4.2 ICP registration

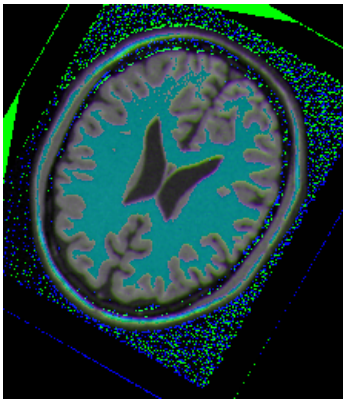
Random permutation of points

The following code randomly shuffles the points of the first vector. The result is of course a wrongly registered image, see Fig.25.4.

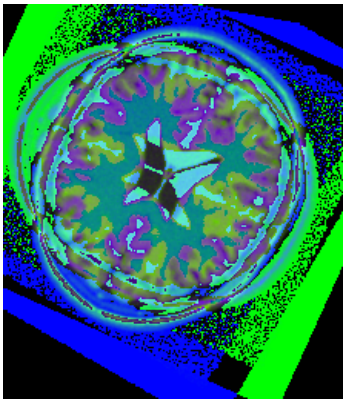
```
# random permutation of the points
p = np.random.permutation(np.arange(4));
A_points = A_points[p];
T = rigid_registration(A_points, B_points);
```

Figure 25.4 Result of the registration for when the control points are not found in the same order.

(a) Matching pairs of points.



(b) Permulation of the points.



ICP

The previous operations simulates a general non-manual selection of the control points: there is not reason to finding the points by matching pairs. Thus, a reordering is necessary.

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This propositions implies that the number of points is exactly the same in order to perform the registration process, and that these are matching points (every point has a matching point in the other image). The ICP method (see code for `icp_transform`) reorders the points via a nearest neighbor rule.

```python
def icp_transform(dataA, dataB):
    """
    Find a transform between A and B points
    with an ICP (Iterative Closest Point) method.
    dataA and dataB are of size nx2, with the same number of points n
    returns the transformation matrix of shape 2x3
    """
    data2A = dataA.copy();
    data2B = np.zeros(data2A.shape);
    T = np.zeros((2,3));
    T[0:2,0:2] = np.eye(2);
    T[0:2,2] = 0;

    nb_loops=5;
    tree = cKDTree( dataB );

    for loop in range(nb_loops):
        # search for closest points and reorganise array of points accordingly
        d, inds = tree.query( data2A);

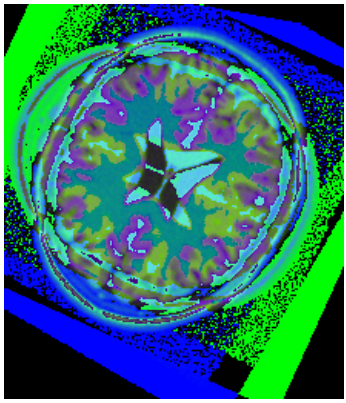
        data2B = dataB[inds,:];
        # find rigid registration with reordered points
        t_loop = rigid_registration(data2A, data2B);

        T = composeTransform(t_loop, T);
        # evaluates transform on control points, to make the iteration
        data2A = applyTransform(dataA, T);

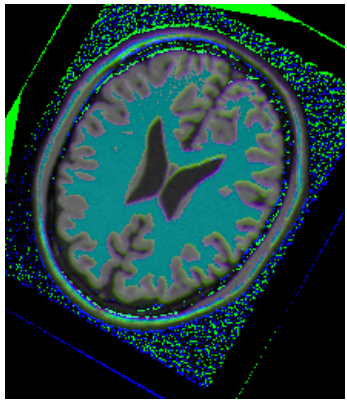
    return T;
```

Figure 25.5 Result of the registration for when the control points are not found in the same order. The ICP algorithm reorders the points and gives a good result.

(a) Random shuffle of points and direct rigid transformation estimation.



(b) ICP registration on the same points.



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Automatic extraction of corner points

Generally, the points are automatically detected, and thus, there is no warranty that they are found in the same order, nor that each pair of point correspond to matching points (some points –called outliers– need to be eliminated to compute the correct transformation). In this tutorial, we do not address the problem of outliers. Please notice that with these parameters and images, by chance, the same points are detected in the correct order.

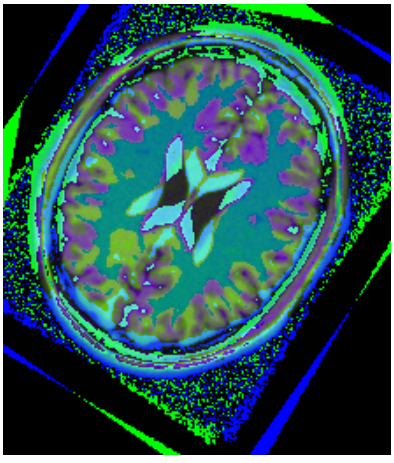
```python
# Automatic extraction of corner points
# Harris corners detection or Shi and Tomasi
# this method do not ensure the correct order in the points (A_points and
# B_points)
nb_points = 4; # number of points to detect
corners = cv2.goodFeaturesToTrack(A,nb_points,0.01,10, blockSize=3,
    ↪ useHarrisDetector=False)
corners = np.int0(corners)
a, b, c = corners.shape;
A_points = np.reshape(corners, (a,c));

corners = cv2.goodFeaturesToTrack(B,nb_points,0.01,10, blockSize=3,
    ↪ useHarrisDetector=False)
corners = np.int0(corners)
a, b, c = corners.shape;
B_points = np.reshape(corners, (a,c));
```

The Fig.25.6 displays the results with the automatic detection of corners (in this case, the method from Shi and Tomasi). Notice that by chance, the points in both images match. In other cases, one would have to remove outliers.

Figure 25.6 Shi and Tomasi corners detection. By chance, the points correspond and the ICP method gives a correct result.

(a)



(b)



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Fourth part

Stochastic Analysis

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26 Stochastic Geometry / Spatial Processes

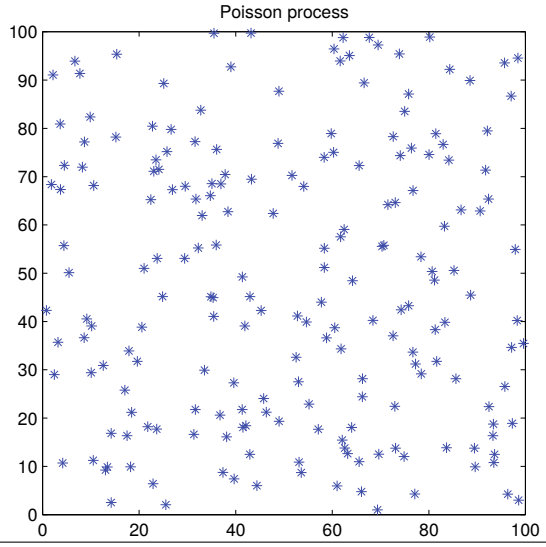
This tutorial aims to simulate different spatial point processes.

26.1 Poisson processes

This process simulates a conditional set of $point_{nb}$ points in a spatial domain D defined by the values $x_{min}, x_{max}, y_{min}, y_{max}$. In order to simulate a non conditional Poisson point process of intensity λ within a domain S, it is necessary to generate a random number of points according to a Poisson law with the parameter λS : $point_{nb} = poisson(\lambda S)$ (i.e. the number of points is a random variable following a Poisson Law).

The coordinates of each point follow a uniform distribution.

Figure 26.1 Conditional Poisson point process, with 200 points.



>>>?

1. Simulate a conditional Poisson point process on a spatial domain D with a fixed number of points (see Fig. 26.1).
2. Simulate a Gaussian distribution of points around a given center.

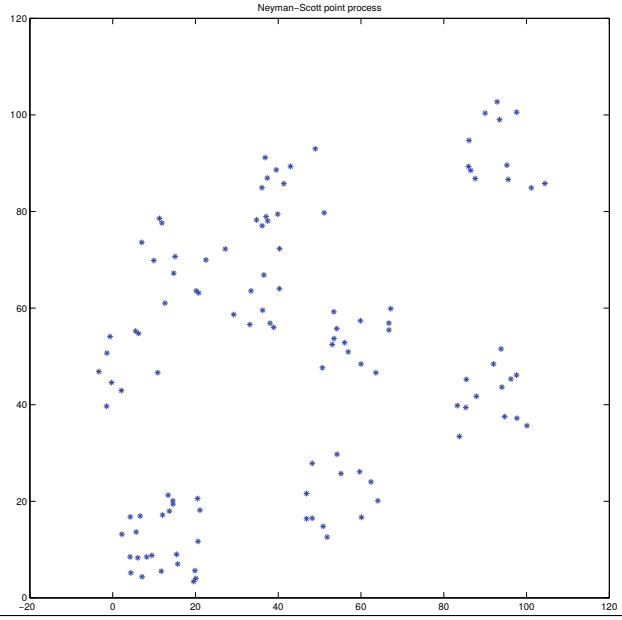
Import `scipy.stats` to use the function `poisson` and `np.random` for more classical stochastic functions.

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26.2 Neyman-Scott processes

This process simulates aggregated sets of points within a spatial domain D defined by the values $x_{min}, x_{max}, y_{min}, y_{max}$. For each aggregate ($n_{par}$), we first generate the random position of the 'parent' point. Then, the 'children' points are simulated in a neighborhood (within a square box of size r^2_{child}) of the 'parent' point. The number of points for each aggregate is either fixed or randomized according to a Poisson law of parameter n_{child} (see Fig. 26.2).

Figure 26.2 Neyman-Scott point process with $h_{child} = 10$ and $n_{par} = 10$



>>>?

1. Simulate a process of 3 aggregates with 10 points.
2. Simulate a process of 10 aggregates with 5 points.

26.3 Gibbs processes

The idea of Gibbs processes is to spatially distribute the points according to some laws of interactions (attraction or repulsion) within a variable range.

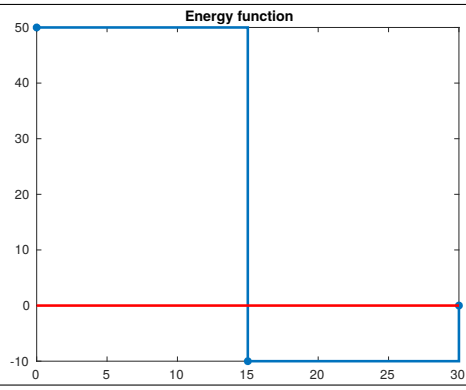
Such a process can be defined by a cost function $f(d)$ that represents the cost associated to the presence of 2 separated points by a distance d (see Fig. 26.3). For a fixed value r, if $f(d)$ is negative, there is a high probability to find 2 points at a distance d (attraction). Conversely, if $f(d)$ is positive, there is a weak probability to find 2 points at a distance d (repulsion).

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- Code such a function, with prototype `function e=f(d)` or `def energy(d):`, where

$$f(d) = \begin{cases} 50 & \text{if } 0 < d \leq 15 \\ -10 & \text{if } 15 < d \leq 30 \\ 0 & otherwise \end{cases}$$

Figure 26.3 Energy function f.



The generation process reorganizes an initial Poisson point process within the spatial domain according to a specific cost piecewise constant function. The reorganization consists in a loop of nb_{iter} iterations. For each iteration, we calculate the total energy:

$$e = \sum_{(i,j),i \neq j} f(dist(x_i, x_j)) \tag{26.1}$$

The objective is to reduce this energy iteratively. At each iteration step, we try to replace a point by four (for example) other random points and we calculate the energy for each new configuration. The initial point is either preserved or replaced (by one of the four points) according to the configuration of minimal energy (see Fig.26.4).

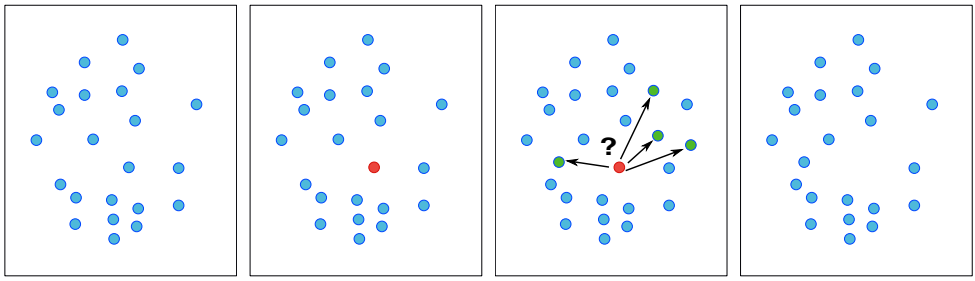
Figure 26.4 Illustration of iterative construction of the Gibbs point process.

(a) Start with an initial distribution of points. The energy is computed for all pairs of points.

(b) A random point is selected.

(c) Four candidate points are randomly generated, the energy of these four new configurations is evaluated.

(d) The configuration with the minimal energy is retained, other points are discarded.



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>>>?

1. Code a function with the following prototype (the function *energyFunction* is previously noticed f). It computes the energy between all the points present in an array of coordinates $[x, y]$ (the points that do not move) and point $[x_k, y_k]$ (the new point). The *energyFunction* converts a distance to an 'energy', reflecting attractivity or repulsivity.

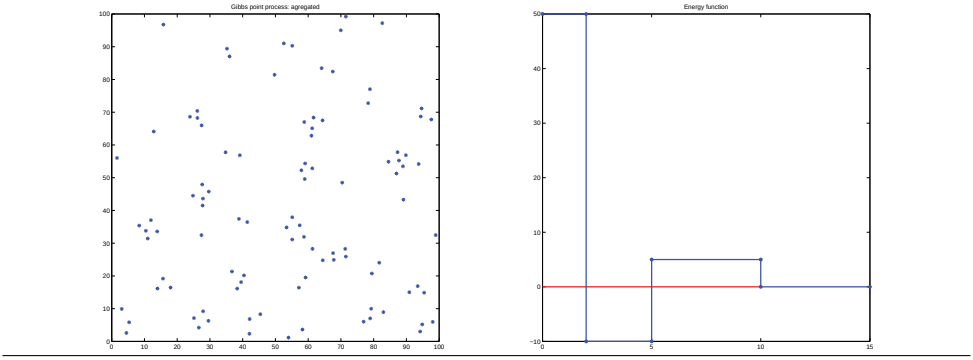
```
def energy(P, eFunction=exampleEnergyFunction):
```

2. Simulate a regular point process by choosing a specific energy function.
3. Change the cost function and simulate a few aggregated point processes (see Fig. 26.5).

Informations

Use the function `pdist` from `scipy.spatial.distance`, which computes pairwise distances of all points.

Figure 26.5 Gibbs agregated point process and its energy function.



26.4 Ripley function

The Ripley function $K(r)$ characterizes the spatial distribution of the points. For a Poisson process of density λ, $\lambda K(r)$ is equal to the mean value of the number of neighbors at a distance lower than r to any point. In the case where the process is not known (λ?), the Ripley function has to be estimated (approximated) with the unique known realization. It is the first estimator of $K(r)$:

$$K(r) = \frac{1}{\lambda}\frac{1}{N}\sum_{i=1}^{N}\sum_{i\neq j} k_{ij} \tag{26.2}$$

where N is the number of points in the studied domain D, $\lambda = N/D$ is the estimator of the density of the process and k_{ij} takes the value 1 if the distance between the point i and the point j is lower than r, and 0 in the other case.

We denote:

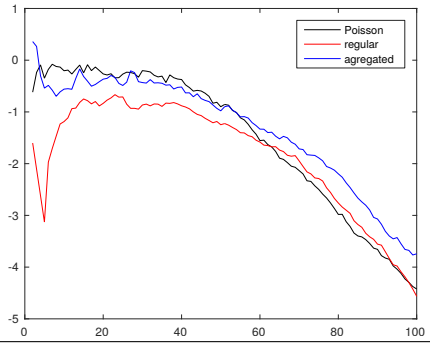
$$L(r) = \sqrt{K(r)/\pi} \tag{26.3}$$

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>>>?

1. Code a function to compute K (`function K=ripley(points, box, r)`), with `points` being the considered points, `box` the simulation domain, and r the distance (or an array of all distances).
2. Calculate the Ripley function for an aggregated point process, a Poisson point process and a regular point process.
3. Display the value $L(r) - r$ as in Fig 26.6.

Figure 26.6 Ripley's function $L(r) - r$.



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26.5 Marked point processes

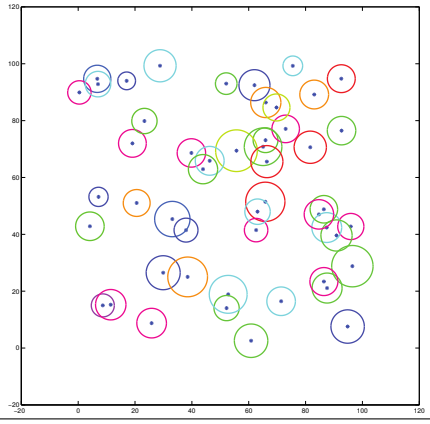
To simulate a complex point process, it can be useful to associate several random variables (marks) for each point.

>>>?

1. Simulate a disk process, where the points (disk centers) are defined according to a Poisson process and the radii are selected with a Gaussian law.
2. Add a second mark for allocating a color to each disk (uniform law).

An example result is shown in Fig. 26.7

Figure 26.7 A Poisson point process is used to generates the center of the circles. The radii are chosen according a Gaussian law, and the color according a uniform law.



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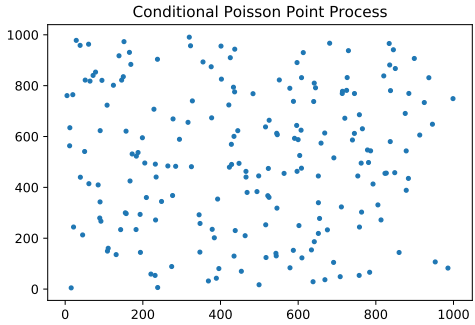
26.6. Python correction

```python
import numpy as np;
import matplotlib.pyplot as plt;
from scipy.spatial.distance import pdist;
from scipy.stats import poisson
```

26.6.1 Conditional Poisson Process

The conditional Poisson Point Process uses a given number of point, contrary to the Poisson Process where the number of points follows a Poisson law. The result is illustrated in Fig.26.8.

Figure 26.8 Conditional Poisson point process, with N=100 points.




```python
def cond_Poisson(nb_points, xmin, xmax, ymin, ymax):
    # Conditional Poisson Point Process
    # uniform distribution
    # nb_points: number of points
    # xmin, xmax, ymin, ymax: defined the domain (window)
    x = xmin + (xmax-xmin)*np.random.rand(nb_points)
    y = ymin + (ymax-ymin)*np.random.rand(nb_points);
    return x,y

def test_ppp():
    # testing function
    x,y = cond_Poisson(100, 0, 100, 0, 100);
    plt.plot(x,y,'+');
```

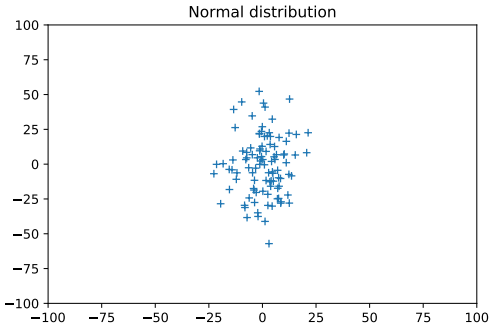
26.6.2 Normal distribution

The normal distribution is illustrated in Fig.26.9. Each marginal distribution (distribution on each axis) follows the normal distribution.

```python
def normal_distribution(nb_points, mu, sigma):
    # Normal distribution centered around the point mu with stdev sigma
    x = mu[0] + sigma[0]*np.random.randn(nb_points);
    y = mu[1] + sigma[1]*np.random.randn(nb_points);
    return x,y;
```

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Figure 26.9 Normal distribution of points around $(0, 0)$, with $\sigma = (10, 20)$.



26.6.3 Neyman-Scott Process

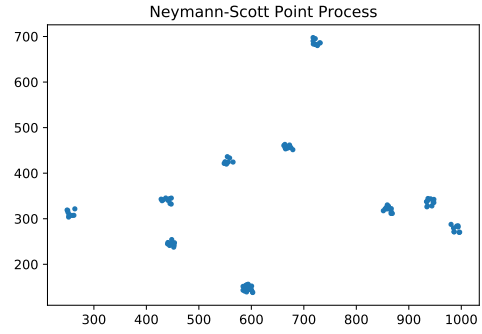
Neymann-Scott point process is an agregated Poisson point process. It is illustrated in Fig.26.10. It consists on a "sub" point processes generated at locations corresponding to a point process.

```python
def neyman_scott(nRoot, xmin, xmax, ymin, ymax, lambdaS, rSon):
    # Neyman-scott process simulation
    # nRoot: number of agregates
    # xmin, xmax, ymin, ymax: domain
    # lambdaS: number of points. lambda is a density, S is the spatial domain
    # rSon: radius around agregate (points are distributed in a square)

    # number of sons
    nSons = poisson.rvs(lambdaS, size=nRoot);
    # results
    x=[];
    y=[];
    # father points coordinates
    xf,yf = cond_Poisson(nRoot, xmin, xmax, ymin, ymax);
    for i in range(nRoot):
        # loop over all agregates
        xs,ys = cond_Poisson(nSons[i], xf[i]-rSon, xf[i]+rSon, yf[i]-rSon, yf[i]+
            ↪ rSon);
        x = np.concatenate((x,xs), axis=0);
        y = np.concatenate((y,ys), axis=0);

    return x,y
```

Figure 26.10 Neyman-Scott point process, with `lambdaS=10` and `rSon=10`.



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26.6.4 Gibbs Point Process

Gibbs point process allows attraction and repulsion at different distances. It is illustrated in Fig.26.11. The attraction/repulsion law is given by the following code for regular or agregated point process.

```python
def exampleEnergyFunction(distance):
    """ This function returns e with the same size as distance
    e takes the value given in the variable energy according to the steps
    """
    e = np.zeros(distance.shape);
    e [distance <10] = 10;
    return e;

def agregatedEnergyFunction(distance):
    """
    Agregated energy function
    """
    e = np.zeros(distance.shape);
    e [distance <2] = 50;
    e [np.logical_and(distance>=2, distance<5)] = -10;
    e [np.logical_and(distance>=5, distance<10)] = 5;

    return e;
```

The evaluation of the energy computes all pairwise distances and sum up the energies associated, or it computes the distances between one single point to a set of points.

```python
def energy(P, eFunction=exampleEnergyFunction):
    """
    This computes the energy in the set of points P, with the energy function
    given as a parameter.
    return a float value
    """
    P = np.transpose(P);
    d = pdist(P);
    e = exampleEnergyFunction(d);
    return np.sum(e);

def energyFromPoint(p, P, eFunction=exampleEnergyFunction):
    """
    Compute energy from point p to all points of P
    """
    dist = np.sqrt((p[0] -P[0,:])**2 + (p[1] -P[1,:])**2);
    ee = eFunction(dist);
    return np.sum(ee);
```

The principle of the algorithm is to iteratively add one point that minimizes the energy after several trials. In order to speed up the process, notice that only one point is moved, and it is thus sufficient to only compute the distances from this point to all others.

```python
def gibbs(nb_points, xmin, xmax, ymin, ymax, nbiter, eFunction=
    ↪ exampleEnergyFunction):
    """
    Gibbs point process
    xmin, xmax, ymin, ymax represents the spatial window
    nb_points: number of generated points
```

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```
    nbiter: number of iterations
    returns (x,y) coordinates of the points
    """

    # start with a Poisson Point Process
    x,y = spat_pp.cond_Poisson(nb_points, xmin, xmax, ymin, ymax);
    nb_moves = 0;
    e_prev = energy(np.vstack((x,y)), eFunction);
    print("initial energy: {0:f}".format(e_prev));

    for i in range(nbiter):
       # choose a random point
       j = np.random.randint(0, nb_points);
       x2 = np.delete(x, j);
       y2 = np.delete(y, j);

       P = np.vstack((x2, y2));
       e1 = energyFromPoint([x[j], y[j]], P, eFunction);

       for m in range(10):
          xm,ym = spat_pp.cond_Poisson(1, xmin, xmax, ymin, ymax);

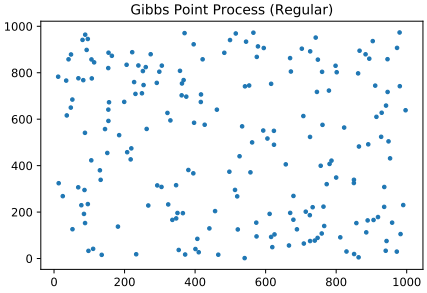
          e2 = energyFromPoint([xm, ym], P, eFunction);
          if e2<e1:
             nb_moves+=1;
             x[j]=xm;
             y[j]=ym;
             e1=e2;

    print( "Number of moves: " + str(nb_moves));
    print("Final energy: " + str(e1));
    return x, y
```

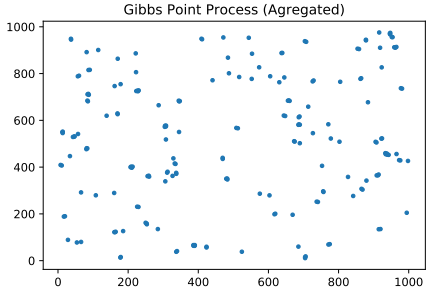
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Figure 26.11 Gibbs point processes (with the same number of points).

(a) Regular Gibbs point process.



(b) Agregated Gibbs point process.



26.6.5 Ripley functions

The Ripley functions are useful to characterize a point process. Agregation and repulsion can be observed with regard to the distance (see Fig.26.12). Notice that this function is biased because points in border of window are counted as points in the center. This could be corrected by the use of `scipy.spatial.distance.cdist`.

```
def ripley(x, y, xmin, xmax, ymin, ymax, edges):
    # Ripley K and L functions, vals is values of radius
```

```
    # this function has border effects!
    # x, y: coordinates of points
    # xmin, xmax, ymin, ymax: window
    # edges: values of bins for histogram evaluation

    # number of points
    nb_points = x.size;

    # compute pairwise distances
    P = np.transpose(np.vstack((x,y)));
    d = pdist(P);

    # compute cumulative histogram
    h,edges = np.histogram(d, edges);
    H = np.cumsum(h);

    # normalization of K
    K = 2*H/nb_points;
    area = (xmax-xmin) * (ymax-ymin);
    density = float(nb_points) / area;
    K = K / density;

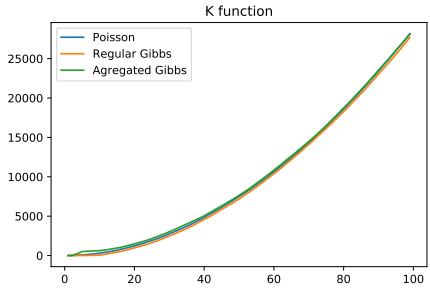
    # L
    L = np.sqrt(K/np.pi);

    # edge values
    vals = edges[:-1] + np.diff(edges);

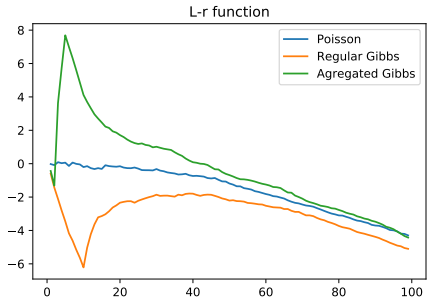
    return K, L, vals
```

Figure 26.12 Ripley functions.

(a) Ripley K function.



(b) Ripley L function.



26.6.6 Marked Point Process

An illustration is presented in Fig.26.13. The algorithm simply consists in adding two new random variables in order to generate the radius and the color of each point.

```
def marked(nb_points, xmin, xmax, ymin, ymax):
    """
    marked point process
    """

    # points
    x,y = spat_pp.cond_Poisson(nb_points, xmin, xmax, ymin, ymax);

```

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```
    # first mark: radii
    sigma = 5;
    mu = 10;
    r = sigma * np.random.randn(nb_points) + mu;
    r[r<0.1] = 0.1;

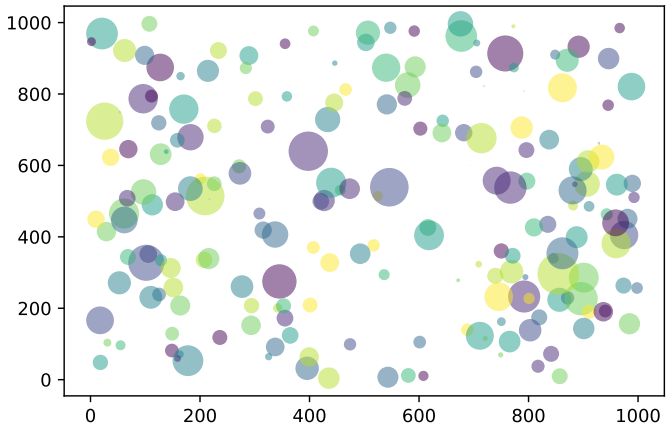
    # second mark: colors
    nb_colors = 10;
    c = np.random.randint(nb_colors,size = nb_points);

    # plot
    plt.scatter(x, y, r**2, c, alpha=.5);

    # save pdf figure
    plt.savefig("marked.pdf");

nb_points = 100;
N=100;
marked(nb_points, 0, N, 0, N);
```

Figure 26.13 Marked point process.



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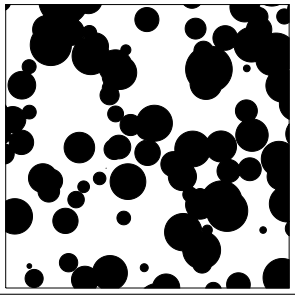
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27 Boolean Models

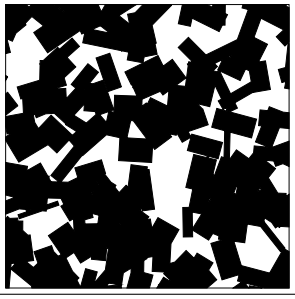
This tutorial aims to study a classical model coming from stochastic geometry: the Boolean model. The first objective is to simulate some realizations of a Boolean model of 2-D disks representing a population of overlapped particles. Thereafter, the geometrical characteristics of the individual disks (from a statistical point of view) will be analyzed.

Figure 27.1 Illustration of 2-D Boolean models observed in a squared window W.

(a) Boolean model of disks



(b) Boolean model of rectangles



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27.1 Simulation of a 2-D Boolean model

Let $\{x_i; i \in \mathbb{N}\}$ be a random collection of points in $\mathbb{R}^2$ forming a stationary Poisson point process with intensity $\gamma > 0$. Let $Z_0, Z_1, Z_2, \dots$ be independent, identically distributed random 2-D convex bodies (nonempty, compact, convex sets) with distribution $\mathbb{Q}$, which are independent of the point process $\{x_i; i \in \mathbb{N}\}$. The random points $x_1, x_2, \dots$ are the germs and the random sets $Z_1, Z_2, \dots$ are the grains of the Boolean model. The random set Z_0 is called the typical grain. The union of the translated grains:

$$Z = \bigcup_{i=1}^{\infty} (Z_i + x_i) \tag{27.1}$$

is a random closed set, which is called the stationary Boolean model with intensity λ and grain distribution $\mathbb{Q}$. The random collection $X = \{Z_1 + x_1, Z_2 + x_2, \dots\}$ of the shifted grains is the particle process underlying the Boolean model.

Figure 27.1 shows a realization of two different Boolean models Z observed in a compact and convex observation window W.

We are going to simulate some realizations of a Boolean model of 2-D disks in a squared observation window. The final simulated model will be represented as a discrete binary image.

>>>?

- Generate a 2-D discrete observation window W of size 500×500.
- Generate the random germs that follows a Poisson law with intensity $\lambda = 100/(500 * 500)$. Take care of the edge effects (a grain with a germ outside the observation window could intersect it!)
- Generate the random grains (as disks). The disk radius will follow a uniform distribution $\mathcal{U}(10, 50)$.
- Vizualize the realization.



Look at the `numpy` functions `random.poisson` and `random.randint`.
Use `skimage.draw.circle` to generate the disks in an array.

27.2 Geometrical characterization of a 2-D Boolean model

Assume we observe Z in a compact, convex observation window W with positive volume (as shown in Figure 27.1). Our aim is to extract distributional information from the geometric properties of the sample $Z \cap W$. Thus, we assume we can measure geometric functionals like the perimeter of the sample $Z \cap W$ which is a finite union of convex bodies (a polyconvex set). By a geometric functional ϕ we mean a real-valued functional defined on the space of polyconvex sets with specific additional properties. Important examples of geometric functionals are the Minkowski functionals W_ν that are related in the 2-D space to the measures of area (A), perimeter (P) and Euler number (χ):

$$W_0 = A \tag{27.2}$$
$$W_1 = P/2 \tag{27.3}$$
$$W_2 = \pi\chi \tag{27.4}$$

The boundary of the observation window W has a disturbing effect. It is therefore of advantage to assume a sufficiently large observation window and to consider only limits as the window tends to infinity. This motivates the introduction of the density (or specific value) of the Boolean model for a geometric functional ϕ. The density of ϕ is the combined spatial and probabilistic mean value:

$$\overline{\phi}(Z) = \lim_{r\to\infty} \frac{\mathbb{E}[\phi(Z \cap rW)]}{W_0(rW)} \tag{27.5}$$

The crucial problem when studying a Boolean model is, that the particles overlap and can therefore not be observed individually.

For this purpose, the Miles formula gives relationships between the global Minkowski densities and the Minkowski densities of the particle. For isotropic Boolean models and by using the densities of the particle process X:

$$\overline{\phi}(X) = \gamma\mathbb{E}[\phi(Z_0)] \tag{27.6}$$

Miles formulas express the observable Minkowski densities $\overline{W}_\nu(Z)$ in terms of the Minkowski densities $\overline{W}_\nu(X)$ and can be inverted.
For example in 2-D:

$$\overline{W}_0(Z) = 1 - e^{-\overline{W}_0(X)} \tag{27.7}$$
$$\overline{W}_1(Z) = e^{-\overline{W}_0(X)}\overline{W}_1(X) \tag{27.8}$$
$$\overline{W}_2(Z) = e^{-\overline{W}_0(X)}\left(\overline{W}_2(X) - \overline{W}_1(X)^2\right) \tag{27.9}$$

>>>?

- Generate different realizations of the previous Boolean model and compute the Minkowski densities of Z (by using the functions done in the tutorial "Integral Geometry").
- Compute the theoretical Minkowski densities of Z by using the Miles formulas.
- Compare the computed and theoretical values.

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27.3. Python correction

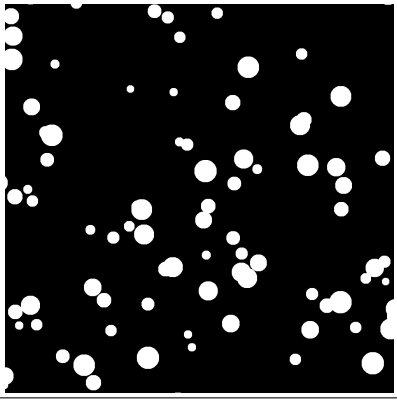
```python
import numpy as np
from skimage import draw
from scipy import misc,signal
import matplotlib.pyplot as plt
import progressbar
```

27.3.1 Simulation of a 2-D Boolean model

The process for simulating the proposed Boolean model of 2-D disks consists in four steps:

1. Generate the random number of points (by using the intensity parameter of the Poisson distribution).
   In order to avoid edge effects, one consider a larger window than the observation window to generate the disks. Indeed, a germ outside the observation window can generate a disk that intersects the observation window.
2. Generate the random locations of the germs (random coordinates from a uniform distribution).
3. Generate the random size of the disks (random radius from a probability distribution).
4. Generate the union of disks.

Figure 27.2 Boolean model of disks, with $Wsize = [1000, 1000]$ and $RadiusParam = [10, 30]$.



When executing this simulation with the following parameters, we get a realization of the Boolean model as a binary image in Fig.27.2.

```python
Wsize=[1000, 1000];
gamma = 100 / (Wsize[0] * Wsize[1]);
radius = [10, 30];
Z = booleanModel(Wsize, gamma, radius);
plt.imshow(Z);
plt.show();
```

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Here is the global function for generating such a Boolean model as a binary image:

```python
def booleanModel(Wsize, gamma, radius):
    """
    Generation of a 2D boolean model of disks, in a window of size Wsize
    Wsize: 2x1 array
    gamma: numerical value to control the Poisson process
    radius: min and max values of radii, 2x1 array
    returns: boolean array of size Wsize
    """
    edgeEffect =2 * np.max(radius) + 100;
    WsizeExtended = Wsize + 2*edgeEffect;
    # nb of points
    areaW = WsizeExtended[0] * WsizeExtended[1];
    nbPoints = np.random.poisson(lam = gamma * areaW);
    # positions of the germs
    x = np.random.randint(0, WsizeExtended[0], nbPoints);
    y = np.random.randint(0, WsizeExtended[1], nbPoints);
    # grains
    rGrains = np.random.randint(radius[0], radius[1], nbPoints);
    # union of grains
    Z = np.zeros((WsizeExtended[0], WsizeExtended[1]));
    for r, xx, yy in zip(rGrains, x, y):
       rr, cc = draw.circle(xx, yy, radius=r, shape=Z.shape)
       Z[rr, cc] = 1;
    # restrain window for side effects
    Z = Z[edgeEffect:edgeEffect+Wsize[0], edgeEffect:edgeEffect+Wsize[1]];
    return Z;
```

27.3.2 Geometrical characterization of a 2-D Boolean model

We can use the following function to compute the Minkowski functionals of the Boolean model (see the tutorial on Integral Geometry). The `regionprops` function from `skimage.measure` is not used because it computes the properties of each object.

```python
def minkowskiFunctionals(X):
    """
    Evaluation of the Minkowski functionals
    X: boolean 2D array
    returns area, perimeter, euler number N8, euler number n4

    """
    F = np.array([[0, 0, 0], [0, 1, 4], [0, 2, 8]]);
    XF = signal.convolve2d(X,F,mode='same');
    edges = np.arange(0, 17 ,1);
    h,edges = np.histogram(XF[:],bins=edges);
    f_intra = [0,1,0,1,0,1,0,1,0,1,0,1,0,1,0,1];
    e_intra = [0,2,1,2,1,2,2,2,0,2,1,2,1,2,2,2];
    v_intra = [0,1,1,1,1,1,1,1,1,1,1,1,1,1,1,1];
    EulerNb8 = np.sum(h*v_intra -h*e_intra + h*f_intra)
    f_inter = [0,0,0,0,0,0,0,0,0,0,0,0,0,0,0,1];
    e_inter = [0,0,0,1,0,1,0,2,0,0,0,1,0,1,0,2];
    v_inter = [0,1,0,1,0,1,0,1,0,1,0,1,0,1,0,1];
    EulerNb4 = np.sum(h*v_inter -h*e_inter + h*f_inter)
    Area = sum(h*f_intra)
    Perimeter = sum(-4*h*f_intra + 2*h*e_intra);

    return Area, Perimeter, EulerNb8, EulerNb4;
```

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So we can estimate the Minkowski densites on different realizations of the Boolean model:

```python
def realizations(Wsize, gamma, radius, n=100):
    """
    This function iterates the different realizations
    Wsize: window size
    gamma: value of gamma, see booleanModel
    radius: min and max values of the radii of the generated disks
    """
    W = np.zeros((n, 3));
    areaWsize = Wsize[0] * Wsize[1];
    bar = progressbar.ProgressBar();
    for i in bar(range(n)):
        Z = booleanModel(Wsize, gamma, radius);
        a, p, chi8, chi4 = minkowskiFunctionals(Z);
        W[i,:] = np.array([a, p/2, chi8*np.pi]) / areaWsize;

    return W;
```

Therefater, we can compare the estimated Minkowski mean densities of the Boolean model with the theoretical ones (by using the known parameters of the different probability distributions of this Boolean model):

```python
W = realizations(Wsize, gamma, radius, 1000);
W = np.mean(W, axis=0);
# comparison with analytical values
rMean = np.mean(radius);
areaMean = np.pi*rMean**2;
perMean = 2*np.pi*rMean;

W_X = gamma * np.array([areaMean, perMean/2, np.pi]);
W_0 = 1-np.exp(-W_X[0]);
W_1 = np.exp(-W_X[0]) * W_X[1];
W_2 = np.exp(-W_X[0]) * (W_X[2] -W_X[1]**2);

error_0 = np.abs(W_0-W[0]) / W_0;
error_1 = np.abs(W_1-W[1]) / W_1;
error_2 = np.abs(W_2-W[2]) / W_2;
```

Here are the results for 100 specific realizations:

```
errorW0: 0.0190201754056
errorW1: 0.200478931771
errorW2: 0.0342984925035
```

The errors can be large due to the biais estimation of the Minkowski densities within an observation window (specifically for the perimeter and the Euler number). But you can use unbiased estimators which can be found in the literature.
Note that the Miles formulas can be inverted to estimate the Minkowski functionals of the typocal grain from the Minkowski mean densities of the Boolean model.

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28 Geometry of Gaussian Random Fields

This tutorial aims at simulating Gaussian random fields and analyzing their geometry.

28.1 Introduction

Let ϕ be a real-valued stationary Gaussian Random Field (GRF) on $\mathbb{R}^2$. $\forall p \in \mathbb{R}^2$, $\phi(p)$ defines a random variable. The family $(\phi(p), p \in \mathbb{R}^2)$ consists of identically distributed random variables on a probability space $\Omega, \mathcal{F}, P$ that satisfies for any subset of $\{p_1, ..., p_n \in \mathbb{R}^2\}$ and $\alpha_k \in \mathbb{R}$ that the random variable $\sum_{k=1}^{n} \alpha_k \phi(p_k)$ is normally distributed. The reader could find more informations in [43, 2, 3].

Thus, ϕ is completely characterized by its mean and its covariance:

$$m = \mathbb{E}(\phi(p)) = \mathbb{E}(\phi(0)) \quad , p \in \mathbb{R}^2 \tag{28.1}$$

$$C(p) = \mathbb{E}(\phi(0)\phi(p)) - m^2 = \mathbb{E}(\phi(q)\phi(p+q)) - m^2, p, q \in \mathbb{R}^2 \tag{28.2}$$

In this tutorial, we will assume $m = 0$. The goal is to construct ϕ for a given covariance C.

28.2 Simulation

For more details on algorithms simulating GRFs in $\mathbb{R}^d$, see [22].

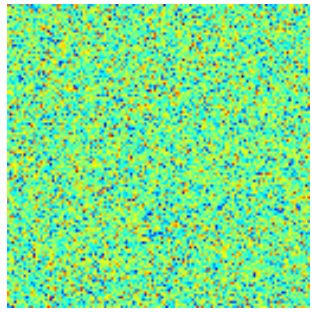
28.2.1 Gaussian white noise random field

>>>?

- Generate a white noise on $\mathbb{R}^2$. Choose an $n \times n$ size. Display it on the screen (see for example Fig. 28.1).
- Modify the variance and observe the results.

Use `randn` from `numpy.random`. Use `imshow` from `matplotlib.pyplot`.

Figure 28.1 Gaussian White Noise, with $m = 128$ and $\sigma = 30$ for display purposes.



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28.2.2 Gaussian Random Field

Let W be an independent centered white noise random fields. $\mathcal{F}$ is the Fourier Transform. The gaussian random field ϕ is defined by:

$$p \in \mathbb{R}^2, \phi(p) = \mathcal{F}^{-1}(\hat{\phi})(p)$$

and

$$\hat{\phi}(k) = \sqrt{\mathcal{F}(C)(k)\mathcal{F}(W)}$$

>>>?

- Generate a 2D Gaussian covariance function , see Fig. 28.2a (we recall the definition, $u^2 = x^2 + y^2$):

$$C(u) = e^{-\frac{u^2}{2\sigma^2}}$$

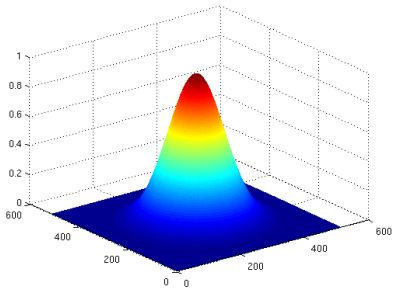
- Generate the Gaussian random field (see Fig. 28.2b). Test with different values of σ.



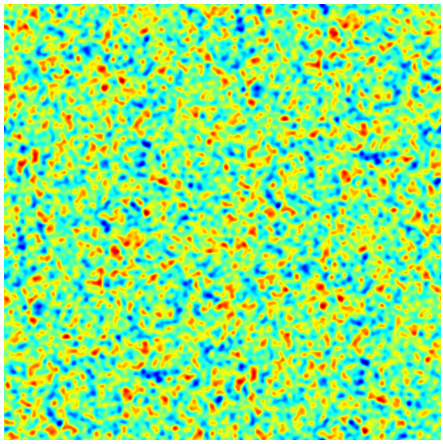
Use `meshgrid` from `numpy`.

Figure 28.2 Covariance and Gaussian random field examples.

(a) Generation of a 2D Gaussian function.



(b) Generation of a 2D Gaussian random field with Gaussian covariance.



28.3 Geometry

28.3.1 Excursion set

Let $Y(x)$, $x \in \mathbb{R}^2$, be a stationary real-valued random field. An excursion set, denoted by $E_h(Y, S)$, of Y inside a compact subset $D \subset \mathbb{R}^2$ above a level h, is defined as:

$$E_h(Y, D) = \{p \in D : Y(p) \geq h\}$$

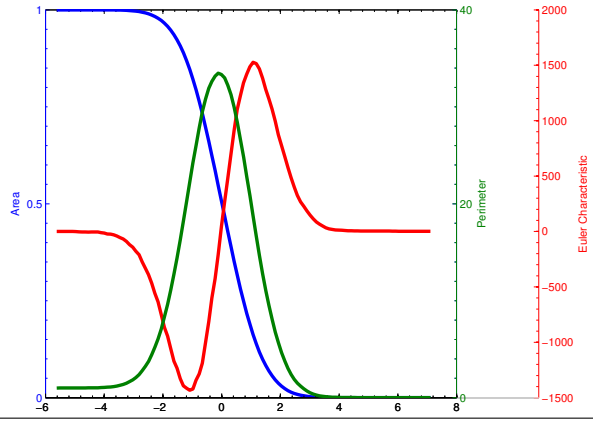
In $D \subset \mathbb{R}^2$, an excursion set is a binary image.

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>>>?

Represent, for each level h, the area A, the perimeter P and the Euler number χ of $E_h(Y, D)$ (see Fig. 28.3). You can have a look at the tutorial about integral geometry for perimeter, area and Euler number computation.

Figure 28.3 Example of computation of Area, Perimeter and Euler number of level sets E_h.



28.3.2 Analytical values

We define three values, area A, perimeter C (Contour length) and Euler number χ, as functions of the level h, with:

$$A(h) = \mathcal{L}_2(D)\rho_0(h) \tag{28.3}$$

$$C(h) = 2\left(\mathcal{L}_1(D)\rho_0(h) + \frac{\pi}{2}\mathcal{L}_2(D)\rho_1(h)\right) \tag{28.4}$$

$$\chi(h) = \mathcal{L}_0(D)\rho_0(h) + \mathcal{L}_1(D)\rho_1(h) + \mathcal{L}_2(D)\rho_2(h) \tag{28.5}$$

with $\mathcal{L}_0(D) = \chi(D) = 1$, $\mathcal{L}_1(D)$ is half the boundary length of the rectangle D and $\mathcal{L}_2(D)$ is its area.

>>>?

- First, compute the following values:

$$\rho_0(h) = \int_h^\infty \frac{1}{\sqrt{2\pi}} e^{-u^2/2} du \tag{28.6}$$

$$\rho_1(h) = \frac{\sqrt{\lambda}}{2\pi} e^{-h^2/2} \tag{28.7}$$

$$\rho_2(h) = \frac{\lambda}{(2\pi)^{\frac{2}{3}}} e^{-h^2/2} h \tag{28.8}$$

$$\lambda = \frac{1}{\sigma^2} \tag{28.9}$$

- Then, compute the analytical values of A, C and χ.
- Compare the analytical values to the empirical ones.



Use `erfc` from `scipy.special`.

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28.4. Python correction



28.4.1 White noise

The white noise is generated with the following code.



```
%% white noise simulation
W = np.random.randn (N, N) ;
```

28.4.2 Gaussian Random Field

The Gaussian function that will serve as a covariance function is generated via the given code. Pay attention to the discretization grid: the FFT implies that functions are periodic, and in order to do that, the discretization must be set between $[-N/2 : N/2[$.

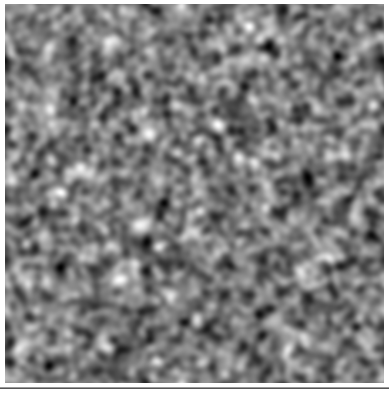
The Gaussian Random Field can be generated via the formula already presented (see Fig.28.4).



```
def grf2D(N, sigma):
    # Discrete space
    x = np.arange(-N/2 , N/2) ;
    [ X , Y ] = np.meshgrid( x , x ) ;
    # Covariance function
    C = np.exp(-1/2 * ( (X/ sigma /np.sqrt(2))**2+(Y/sigma/np.sqrt(2) )** 2 ) ) ;
    Cmat = np.fft.fftshift (C) ;
    # real positive part, then square root
    Cf = np.real(np.fft.fft2( Cmat ) ) ;
    Cf = np.sqrt ( np.maximum ( np.zeros ( Cf.shape ) , Cf ) ) ;
    # Complex white noise
    W = np.random.randn (N, N) ;

    A = Cf * np.fft.fft2(W);
    G = np.real ( np.fft.ifft2 (A) ) ;
    return G;
```

Figure 28.4 Gaussian Random Field, with $\sigma = 10$ (pixels) and $N = 2^{10} = 1024$ pixels.



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28.4.3 Minkowski functionals

The Minkowski functionals are illustrated in Fig.28.5. The code follows.
The measures can be performed with the code from the tutorial 32.

```python
def bwminko(X):
    # zero padding of input
    X = np.pad(X, ((1,1), (1,1)), mode='constant');
    # Neighborhood configuration
    F = np.array([[0, 0, 0], [0, 1, 4], [0, 2, 8]]);
    XF = signal.convolve2d(X,F,mode='same');
    edges = np.arange(0, 17 ,1);
    h,edges = np.histogram(XF[:],bins=edges);

    f_intra = [0,1,0,1,0,1,0,1,0,1,0,1,0,1,0,1];
    e_intra = [0,2,1,2,1,2,2,2,0,2,1,2,1,2,2,2];
    v_intra = [0,1,1,1,1,1,1,1,1,1,1,1,1,1,1,1];
    f_inter = [0,0,0,0,0,0,0,0,0,0,0,0,0,0,0,1];
    e_inter = [0,0,0,1,0,1,0,2,0,0,0,1,0,1,0,2];
    v_inter = [0,1,0,1,0,1,0,1,0,1,0,1,0,1,0,1];
    EulerNb4 = np.sum(h*v_inter -h*e_inter + h*f_inter)
    Area = np.sum(h*f_intra)
    Perimeter = np.sum(-4*h*f_intra + 2*h*e_intra)
    return Area, Perimeter, EulerNb4;
```

Then, the measurements consists in taking all the level-sets and evaluating the properties from these binary sets. Notice that the perimeter is allways a difficult task and is not really precise.

```python
def minkoMeasured(G, sigma, hmin, hmax):
    H = np.arange(hmin, hmax, .1);
    A = [];
    P = [];
    E = [];
    bar = progressbar.ProgressBar();
    for h in bar(H):
        levelset = G >= h;
        a, p, e = bwminko(levelset);
        A.append(a);
        P.append(p);
        E.append(e);
    return A, P, E;
```

The analytical values are simply evaluated with the formulas.

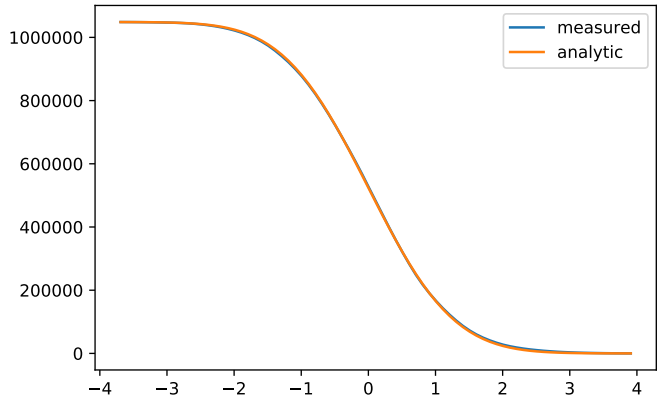
```python
def minkoAnalytical(N, sigma, hmin, hmax):
    l = 1/(2*sigma**2);
    # analytical values
    H = np.arange(hmin, hmax, .1);
    rho_0 = 1/2 * erfc(H / np.sqrt(2));
    rho_1 = np.sqrt(l) * np.exp(- H**2 / 2) /(2*np.pi);
    rho_2 = l / (2*np.pi)**(3/2) * np.exp(- H**2 / 2) * H;

    Aa = N**2 * rho_0;
    Pa = 4*N*rho_0 + np.pi*N**2*rho_1;
    Ea = rho_0 + 2*N*rho_1 + N**2*rho_2;
    return Aa, Pa, Ea;
```

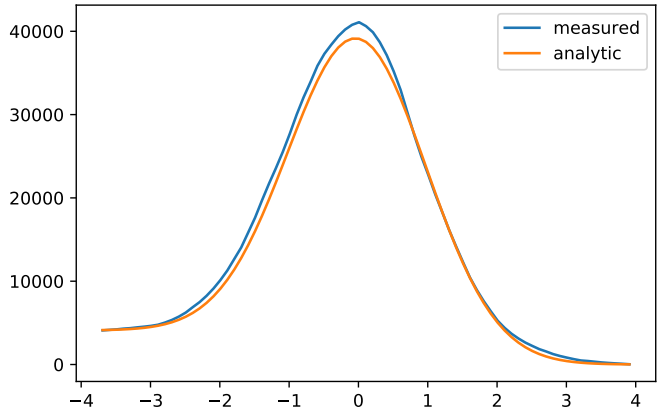
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Figure 28.5 Illustration of the simulated and analytical values of the Minkowski functionals of the level sets of the Gaussian Random Field, for $\sigma = 10$ and $N = 1024$.

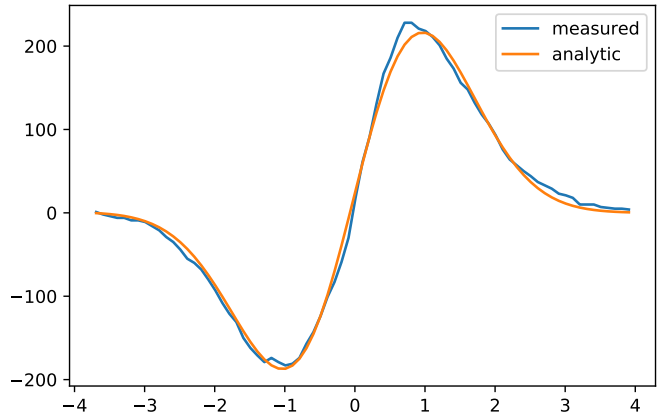
(a) Area.



(b) Perimeter.



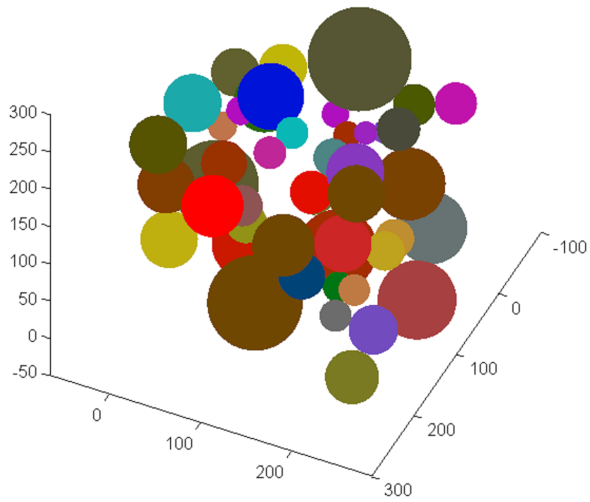
(c) Euler number in 4 connectivity.



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★★★ 29 Stereology and Bertrand's paradox

This tutorial introduces the problems of stereological measurements, based on simple probes (points, lines...). In a second part, the Bertrand's paradox is explored in the case of the analysis of the distribution of chord lengths of disks and spheres. This tutorial uses the notation that can be found in [35] (among others).



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29.1 Classical measurements of stereology

Let start by some definitions. The stereology is based on some measures, that can be seen as samples, called probes. A probe can be a point, a line, a curve, a plane, a surface... These probes allow us to estimate global geometrical properties through partial measures. Very simple and practical probes are now presented and used. The notation $\langle \cdot \rangle$ denotes an expected count for some normalized value.

Probe name	Notation	Definition
Point count	$\langle P_P \rangle$	Fraction of points in phase
Line intercept count	$\langle P_L \rangle$	Number of intersections per length
Area fraction	$\langle A_A \rangle$	Fraction of area in intersection

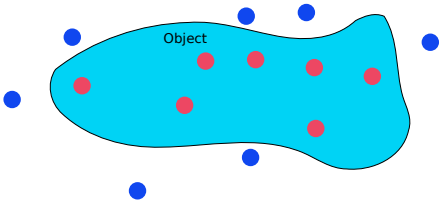
29.1.1 Probes

The measures are performed with the following definitions:

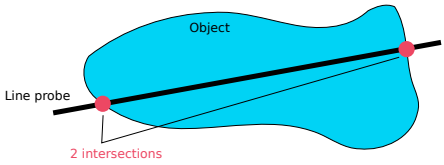
- $\langle P_P \rangle$: the count of the points that lie in the phase, normalized by the total number of points.
- $\langle P_L \rangle$: the count of the number of intersection of lines and the surface of the phase, normalized by the total length of the lines (in m^{-1}, see Fig.29.1). L_A is the ratio between the perimeter of the phase and the total area.
- $\langle A_A \rangle$: in a 3D object, the probes are planes and $\langle A_A \rangle$ is the area of the intersections of the planes and the phase, normalized by the total area of the planes.

Figure 29.1 Probes examples: points and lines.

(a) Evaluation of P_P: count the number of points that lie in the objects, normalized by the total number of points.



(b) Evaluation of P_L: count the number of intersection of some lines with the surface of the phase (object). Then, perform a ratio with the total length of the lines.



>>>?

- Generate a 2-D binary image containing a population of disks.
- Estimate its area fraction by using points as probe population ($< P_P >= A_A$).
- Estimate its length per area by using lines as probe population ($< P_L >= \frac{2}{\pi} L_A$).
- Load the 3-D image and verify the following relation: $< A_A >= V_V$ with V_V being the volume fraction.

29.2 Random chords of a disk, and Bertrand's paradox

The goal of this exercise is to simulate the distribution of random chord lengths on a disk. In the field of process engineering, optical particle sizers provide chord length distributions of objects that are considered as spheres. These developments are not only theoretical, they have a practical use in laboratories or in industrial reactors.

29.2.1 Bertrand's paradox

From Wikipedia[1], the Bertrand paradox goes as follows: Consider an equilateral triangle inscribed in a circle. Suppose a chord of the circle is chosen at random. What is the probability that the chord is longer than a side of the triangle?

Bertrand provided three different methods in order to evaluate this probability. These gave three different values.

The objective is to evaluate the distribution of the chord lengths for two of these methods. The bertrand's paradox lays on the fact that the question is ill-posed, and the choice "at random" must be clarified. The reader will find more details in the different citations.

29.2.2 Random radius

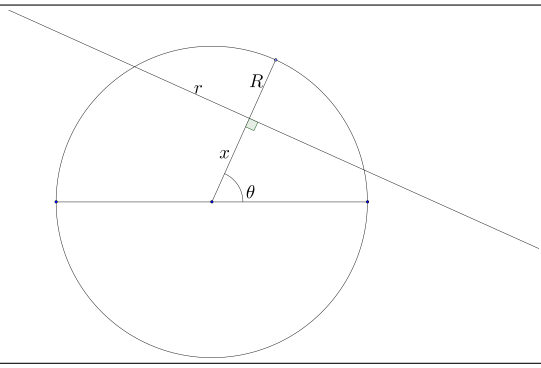
The intersection of a random line with a disk of radius R is a segment whose half length r is linked to the distance x between the segment and the center of the disk (Eq. 29.1 and Fig. 29.2).

$$r = \sqrt{R^2 - x^2} \tag{29.1}$$

[1] https://en.wikipedia.org/wiki/Bertrand_paradox_(probability)

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Figure 29.2 Relation between the radius of the chord and the distance to the center of the disk.



As presented in Fig. 29.2, θ is randomly chosen in $[0; 2\pi[$ (uniform law), and x is randomly chosen in $[0; R]$ (uniform law).

>>>?

Repeat the simulation of r by the so-called random radius method a large number of times ($N = 1e7$), and compute the probability density function of the distribution.

This method is in agreement with the analytical results.

29.2.3 Random endpoints

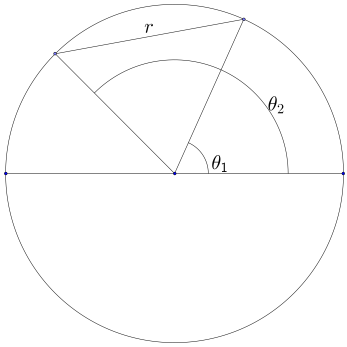
In this second case, two random angles θ_1 and θ_2 are randomly chosen (uniform law in $[0; 2\pi]$). This defines two points and thus a chord (see Fig 29.3).

>>>?

Make the simulation for the "random endpoints" and compare it to the analytical values and to the first simulation. Notice that this simulation gives different values (search for the Bertrand paradox for more details).

This method is NOT in agreement with the analytical results.

Figure 29.3 Second method for simulating a random chord of the disk.



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29.2.4 Analytical values

The probability to obtain a chord of half length x between a and b is given by Eq. 29.2:

$$\mathbb{P}(x \in [a;b]) = \int_a^b \frac{\rho}{R\sqrt{R^2-\rho^2}} \mathrm{d}\rho \tag{29.2}$$

>>>?

By discretizing the interval $[0;R]$, compute the analytical value of the probability density function of the distribution of the radii with the Eq. 29.2.

29.3 Random sections of a sphere and a plane

The two previous strategies can be applied on the sphere. What we are looking for are radii of the intersection of the sphere with a random plane.

29.3.1 First simulation: random radius

To find and random plane $\mathcal{P}$ intersecting a sphere $\mathcal{S}$ of radius R, one have to choose a direction $\vec{u}$ (i.e. a point on the sphere), find a point P between the latter and the center O of the sphere, and considere the plane $\mathcal{P}$ that is orthogonal to the direction $\vec{u}$ and passing at this point P (Fig. 29.4).

>>>?

Code the following method:

- A random point on the sphere is chosen with the following method (see [24]): let x, y and z be 3 Gaussian random variables, the point on the sphere is defined by the normed vector $\vec{u}$, such that:

$$\vec{u} = \frac{1}{\sqrt{x^2+y^2+z^2}} \begin{pmatrix} x \\ y \\ z \end{pmatrix} \tag{29.3}$$

- The point P is chosen as $\vec{OP} = \alpha\vec{u}$, with O being the center of the sphere, and α being a uniform random variable in $[0;R]$. The plane $\mathcal{P}$ is orthogonal to $\vec{u}$, passing at P (see Fig. 29.4).

Notice that this simulation is equivalent to the first presented case (random radius) of the random chords of a disk, and that the choice of the random point on the sphere is useless.

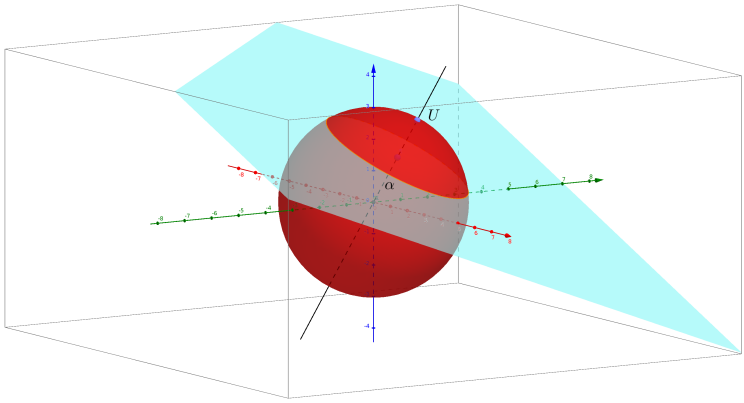
The method that consists to choose a point by two angles does not provide a uniform distribution of the points on the sphere.

29.3.2 Second simulation: 3 random endpoints

The random plane $\mathcal{P}$ is defined by 3 random points laying on the sphere (see Eq. 29.3).

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Figure 29.4 First simulation method of a random intersection of a sphere and a plane.



>>>?

- Analytically, find the distance between the center of the sphere O and the plane $\mathcal{P}$.
- Simulate a high number of intersections and find numerically the distribution of the radii of these intersection disks.

29.3.3 Third simulation: 2 random endpoints

Choose 2 random points laying on the sphere (see Eq. 29.3) and evaluate their half distance.

>>>?

Simulate a high number of couple of points and evaluate the distribution of their half distances.

The distribution of the length of the chords on a sphere is linear, and is different from the distribution of the radii resulting from the intersection of a random plane and the sphere.

29.3.4 Comparison

>>>?

Compare the 3 results and comment.

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29.4. Python correction

```python
import numpy as np
import matplotlib.pyplot as plt
import skimage.measure
import scipy
```

29.4.1 Classical measurements of stereology

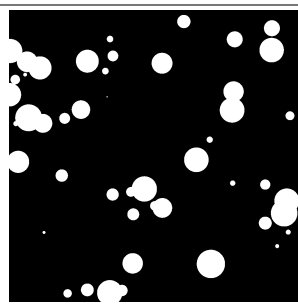
To generate a binary image with overlapping random disks (see Fig.29.5), the following function is used:

```python
def popDisks(nb_disks, S, Rmax):
    """ Generates an image with random disks, with uniform distribution of the
        ↪ centers, and of the radii.
    @param nb_disks: number of disks
    @type S: int
    @param S: Size of spatial support
    @param rmax: maximum radius of disks
    @return: binary image of disks
    """
    centers = np.random.randint(S, size=(nb_disks,2));
    radii = Rmax * np.random.rand(nb_disks);

    N=1000;
    x = np.linspace(0, S, 1000);
    y = np.linspace(0, S, 1000);
    X, Y = np.meshgrid(x, y);
    I = np.zeros((N,N));
    for i in range(nb_disks):
        I2 = (X-centers[i,0])**2 + (Y-centers[i,1])** 2 <= radii[i]**2;
        I = np.logical_or(I, I2);

    return I;
```

Figure 29.5 Random population of disks.



Area fraction

The area fraction counts the number of probes that lay inside the objects. In order to verify this probe, the next function evaluates the real area covered by the disks.

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```python
def areaFraction(nb_probes, I):
    """
    Evaluates area fraction via point probes
    @param nb_probes: number of probes
    @param I: binary image, square
    """
    P = np.random.randint(I.shape[0], size = (nb_probes,2));

    # count the number of probes in phase
    count = np.sum(I[P[:,0], P[:,1]]);
    return float(count) / nb_probes;
```

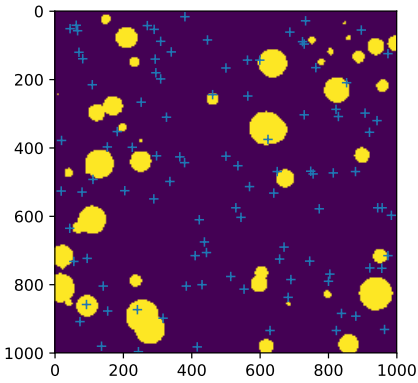
```python
def verifyAreaFraction():
    """
    Verify area fraction
    """
    I = popDisks(50, 1000, 20);
    plt.imshow(I);
    AA = float(np.sum(I)) / np.size(I);
    PP = areaFraction(3000, I);

    print("AA (true number of pixels): {:.2%}".format(AA));
    print("PP (evaluated fraction) : {:.2%}".format(PP));
```

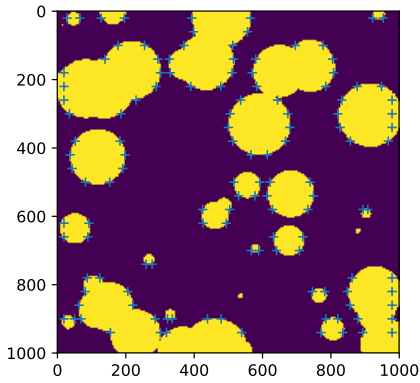
There is a good agreement between AA and PP. The method is illustrated in Fig.29.6a.

Figure 29.6 Illustration of the positions of the different probes.

(a) Area fraction evaluation.



(b) Length per area evaluation.




```
AA (true number of pixels): 2.05%
PP (evaluated fraction) : 1.87%
```

Length per area

A certain number of segments are used in order to perform the probing. The number of times a segment goes through the surface of the object is evaluated. This is illustrated in Fig.29.6b.

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```python
def lengthPerArea(I):
    """
    Evaluates the length per area
    """
    perim= skimage.measure.perimeter(I.astype(int), 8);
    LA = perim / np.sum(I);
    print("LA (true count): {:.2%}".format(LA));

    # lines probes, every 10 pixels
    probe = np.zeros(I.shape);
    probe[20:-20:10, 20:-20] = 1;
    lines = I.astype(int) * probe;

    # count number of intercepts
    h = np.array([[1, -1, 0]]);
    points = scipy.signal.convolve2d(lines, h, mode='same');

    nb_lines = np.sum(lines);
    nb_points= np.sum(np.abs(points));
    PL = float(nb_points) / nb_lines;
    print("pi/2*PL (true count): {:.2%}".format(np.pi/2*PL));
```

```python
def verifyLengthPerArea():
    I = popDisks(50, 1000, 20);
    plt.imshow(I);
    plt.show();
    lengthPerArea(I);
```

The perimeter evaluation may vary a lot according to the implementations or to the connectivity chosen.

```
LA (true count): 18.02%
pi/2*PL (evaluated fraction): 15.20%
```

Volume fraction

This example loads a MATLAB® matrix.

```python
def volumeFraction(volume):
    """
    """
    VV = float(np.sum(volume)) / np.size(volume);
    probe= np.zeros(volume.shape);
    probe[10:-10:50, 10:, 10:] = 1;

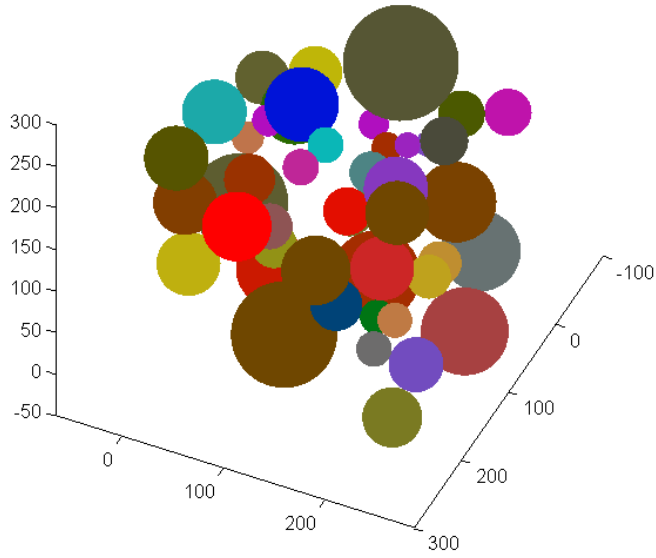
    s = np.sum(probe);
    probe = probe * volume;
    AA = float(np.sum(probe)) / s;

    print("VV (true count): {:.2%}".format(VV));
    print("AA (true count): {:.2%}".format(AA));

def verifyVolumeFraction():
    sphere = scipy.io.loadmat("spheres.mat");
    volumeFraction(sphere['A']);
```

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Figure 29.7 Random population of 3D overlapping spheres. This function uses povray and the vapory python API.



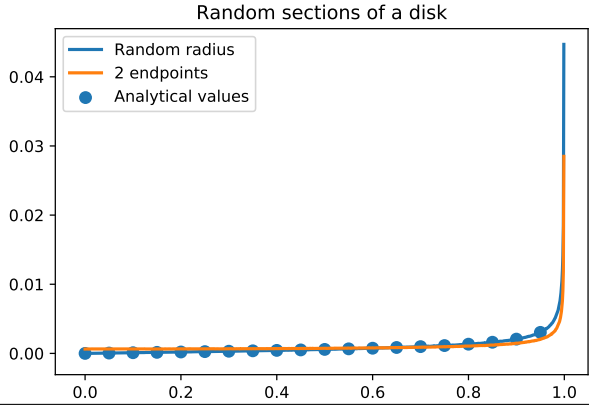
As for the area fraction, the volume fraction is precise. The results on this example are:

```
VV (true count): 5.02%
AA (evaluated fraction): 5.28%
```

29.4.2 Random sections of a disk

The value N is the number of simulations performed. To find the probability, N values x are randomly chosen between 0 and R. The formula $r = \sqrt{R^2 - x^2}$ yields to the half length r of the chord. After discretizing the interval $[0; R]$ in $nBins$, the number of values x in each bin is counted (with python `np.histogram` function). The results are presented in Fig. 29.8.

Figure 29.8 Simulations of random chords of a disk.



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```python
import numpy as np
import matplotlib.pyplot as plt
N = 10000000;
nBins = 1000;
R = 1.;
# first simulation method: random radius
d = R * np.random.rand(N);
radii = np.sqrt(R**2 -d**2);
probaSimu = np.histogram(radii, bins=nBins);
plt.plot(probaSimu[1][:-1], probaSimu[0]/N, linewidth=2);
```

The second method consists in choosing 2 random points on the circle, given by two random angles.

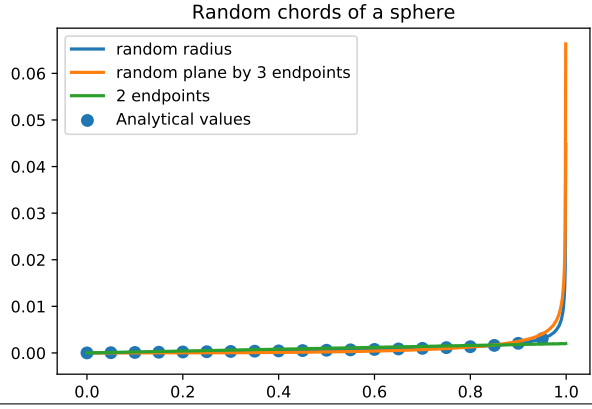
```python
#2nd method: random points on the circle
# from 2 random angles
theta = np.pi*2*np.random.rand(int(N),2);
dX = np.diff(R * np.cos(theta))
dY = np.diff(R * np.sin(theta));
radii = 1./2 * np.sqrt(dX**2 + dY**2);
probaSimu2 = np.histogram(radii, bins=nBins);
plt.plot(probaSimu2[1][:-1], probaSimu2[0]/N, linewidth=2);
```

Finally, the analytical results are computed for comparison.

```python
# analytical values
step = .05;
r2 = np.arange(0, R, step);
probaReal = 1./R * r2 / np.sqrt(R**2-r2**2);
probaReal = probaReal * R / nBins; # approximation of the integral
plt.scatter(r2, probaReal, 50);
# display results
plt.legend(["Unique random points", "2 random points", "Analytical values"])
plt.show()
plt.savefig('sections_disk.pdf')
```

29.4.3 Random planar sections of a sphere

Figure 29.9 Simulations of random chords of a sphere.



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```python
import numpy as np
import matplotlib.pyplot as plt

def generatePointsOnSphere(nb_points, R):
    """
    Generate points on a sphere
    @param nb_points: number of points
    @return n: array of size nb_points x 3
    """
    n = np.random.randn(nb_points, 3);
    mynorm = np.linalg.norm(n, axis=1);
    n = R * n / np.transpose(np.matlib.repmat(mynorm, 3, 1));

    return n

def dot(A, B, ax=1):
    """ dot product for arrays
    """
    return np.sum(A.conj()*B, axis=ax );
```

First simulation: random radius

This method is equivalent to the first case of the disk chord. The 3D property of the sphere is not used and thus the code is strictly equivalent to the 2D case.

```python
# initial values
N = 1e7;   # number of samples, float number
R = 1;     # radius of the sphere
nBins = 1000; # number of bins for histogram computation
# first simulation method: random radius
d = R * np.random.rand(int(N));
radii = np.sqrt(R**2 -d**2);
probaSimu = np.histogram(radii, bins=nBins);
plt.plot(probaSimu[1][:-1], probaSimu[0]/N, linewidth=2);
```

Second simulation: 3 endpoints

Define a random plane from 3 points randomly chosen on the sphere. Let n_1, n_2 and n_3 be 3 points on the sphere. These points define the plane $\mathcal{P}$. The distance between the center of the sphere O and the plane $\mathcal{P}$ is given by the relation:

$$d(0,\mathcal{P}) = \frac{|\vec{n}\cdot\vec{u}|}{||\vec{n}||}$$

with $\vec{u} = \vec{n_2} - \vec{n_1}$, $\vec{v} = \vec{n_3} - \vec{n_1}$, and $\vec{n} = \vec{u} \wedge \vec{v}$ the normal vector to the plane. The results are presented in Fig. 29.9.

This is a case of Bertrand's paradox: the definition of randomness is not good in the present case.

```python
# second simulation
# choose 3 points to define a plane,
# then, compute the distance from the origin to this plane
n1 = generatePointsOnSphere(N, R);
n2 = generatePointsOnSphere(N, R);
n3 = generatePointsOnSphere(N, R);
# u and v belong to the plane
u=n2-n1;
v=n3-n1;
```

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```
# n: normal vector to the plane
n=np.cross(u,v);
x = dot(n, n1) / np.linalg.norm(n, axis=1);
# distance from the origin to the plane:
r = np.sqrt(R**2 -x**2);
probaSimu = np.histogram(r, bins=nBins);
plt.plot(probaSimu[1][:-1], probaSimu[0]/N, linewidth=2);
```

3rd simulation: 2 endpoints

This situation presents the random choice of two points on the sphere, and the computation of their distance. This produces a linear probability (see Fig.29.9).

```
# 3rd case:
# 2 points on the sphere and distance between them
n1 = generatePointsOnSphere(N);
n2 = generatePointsOnSphere(N);
r = 1./2 * np.linalg.norm(n1-n2, axis=1);
probaSimu = np.histogram(r, bins=nBins);
plt.plot(probaSimu[1][:-1], probaSimu[0]/N, linewidth=2);
```

Analytical values

This code evaluates analytical values.

```
# analytical values
step = .05;
r2 = np.arange(0, R, step);
probaReal = 1./R * r2 / np.sqrt(R**2-r2**2);
probaReal = probaReal * R / nBins; # approximation of the integral
plt.scatter(r2, probaReal, 50);

# display
plt.legend(["random plane by 3 points on the sphere", "2 points on the sphere",
    ↪ "Analytical values"])
plt.show();
plt.savefig("section_sphere.pdf") # save as pdf file
```

The results are displayed in Fig. 29.9.

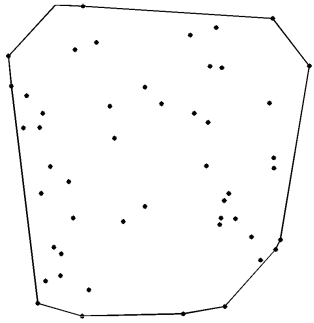
The Bertrand's paradox is illustrated by the fact that "at random" can provide several different interpretations. The objective here is to focus on the computational choices that can be made in order to provide random chords or random points on a sphere.

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30 Convex Hull

This tutorial aims to determine the convex hull of a set of 2D points with a simple and classical algorithm. This tool is largely used in computational geometry and image modeling. This tutorial is widely inspired of the Wikipedia page https://en.wikipedia.org/wiki/Graham_scan.

Figure 30.1 Convex Hull example.



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30.1 Graham scan

The Graham scan is a method of computing the convex hull of a finite set of points in the plane with time complexity $O(n \log n)$, n is the number of points. It is an evolution of the Gift wrapping algorithm ($O(nh)$, h is the number of points in the hull) in the sense that it avoids evaluating all pairs of angles by first sorting the points.

30.1.1 Lowest y-coordinate point

The first step, as in the gift wrapping algorithm, is to find the point with the lowest y-coordinate. If two points exist in the set, choose the one with the lowest x-coordinate: it is denoted P. This step obviously takes $O(n)$.



Use the `numpy.lexsort` function.

30.1.2 Sort by angle

Next, the set of points must be sorted in increasing order of the angle they and the point P make with the x-axis.



Use the `numpy.argsort` function.

This is the limiting step, it takes $O(n \log n)$. Notice that the cosine of the angle is a decreasing function between 0 and 180 degrees, and will thus avoid to evaluate the angle itself. The sorted set of points is denoted $\mathcal{S}$ (it does not contain P).

30.1.3 Check angles: left or right turn?

From the star-like shape issued from the sorting algorithm, construct a list $\mathcal{L}$ of points as: $\mathcal{L} = \{P, \mathcal{S}, P\}$.

Then, for each triplet of consecutive points (P_i, P_{i+1}, P_{i+2}) of $\mathcal{L}$, check if the angle $P_i\widehat{P_{i+1}P_{i+2}}$ is a right turn or a left turn. In case of a right turn, remove P_{i+1} from the list $\mathcal{L}$. Process the entire list this way.

30.1.4 Left or right turn?

Again, determining whether three points constitute a "left turn" or a "right turn" does not require computing the actual angle between the two line segments, and can actually be achieved with simple arithmetic only. Consider the cross product of the vectors $\overrightarrow{P_iP_{i+1}}$ and $\overrightarrow{P_iP_{i+2}}$.

Procedure `ccw`(p_1, p_2, p_3)
  return $(p_2.x - p_1.x) * (p_3.y - p_1.y) - (p_2.y - p_1.y) * (p_3.x - p_1.x)$;

Three points are a counter-clockwise turn if $ccw > 0$, clockwise if $ccw < 0$, and collinear if $ccw = 0$ because ccw is a determinant that gives the signed area of the triangle formed by p_1, p_2 and p_3.

30.1.5 Convex hull algorithm

This pseudo-code shows a different version of the algorithm, where points in the hull are pushed into a new list instead of removed from $\mathcal{L}$.

Data: n: number of points
Data: $\mathcal{L}$: sorted list of $n + 1$ elements
Data: First and last elements are the starting point P.
Data: All other points are sorted by polar angle with P.
`stack will denote a stack structure, with push and pop functions.`
Data: stack.push($\mathcal{L}(1)$)
Data: stack.push($\mathcal{L}(2)$)
for $i = 3$ *to* $n + 1$ **do**
  while *stack.size*≥ 2 *AND* `ccw(`*stack.secondlast, stack.last,* $\mathcal{L}(i)$`)` < 0 **do**
    stack.pop();
  end
  stack.push($\mathcal{L}(i)$);
end

In this pseudo-code, stack.secondlast is the point just before the last one in the stack. When coding this algorithm, you might encounter problems with floating points operations (collinearity or equality check might be a problem).

>>>?

1. Generate a set of random points.
2. Implement and apply the algorithm, and visualize the result.

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30.2. Python correction



```python
import numpy as np
import matplotlib.pyplot as plt
```

30.2.1 Graham scan algorithm

For convex hull and other computational geometry algorithms, robustness must be handled with special care. Floating points operations may be really tricky and the following code is not ensured to work for all cases.

```python
# very naive precision handling
points = np.round(points, decimals=4);
```

The first step is to get the starting point.

```python
# sort first by y, then x. get first point
ind=np.lexsort(points.transpose());
P = points[ind[0],:];

# all points but first one
pp =points[:-1,:]
```

Then, the points are sorted by the cosinus of the angle. This step has complexity $O(n \log n)$.

```python
# sort all points by angle
hypothenuse=np.sqrt( (pp[:,0]-P[0])**2 + (pp[:,1]-P[1])**2 );
adj_side = pp[:,0] -P[0];
# as cos is decreasing, we use minus
cosinus= -adj_side/hypothenuse;
ind=cosinus.argsort();

# construct ordered list of points
list_points = [];
list_points.append(P.tolist());
list_points= list_points + pp[ind,:].tolist();
list_points.append(P.tolist());
```

Finally, the sorted points allow to construct the convex hull by testing the orientation of the turn of the hull (see Fig.30.2).

```python
first = list_points.pop(0);
second= list_points.pop(0);
hull = []; # convex hull
hull.append(first);
hull.append(second);

```

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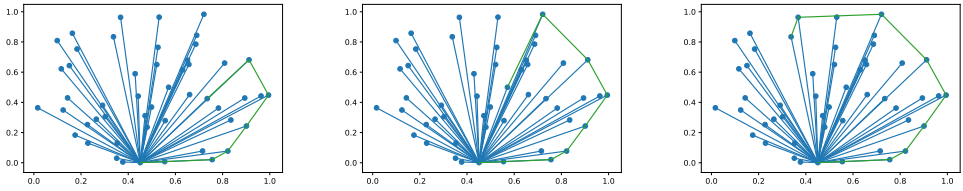
```
for i, p in enumerate(list_points):
   while len(hull)>=2 and crossProduct(hull, p)<0:
      hull.pop();

   hull.append(p);

   # display result every 10 points
   if i%10 == 0:
      displayPointsAndHull(points, P, hull, 'chull_'+str(i)+'.python.pdf');
```

Figure 30.2 Graham scan illustration while constructing the convex hull.

(a) After 10 tested points. **(b)** After 20 tested points. **(c)** After 30 tested points.



30.2.2 Useful functions

The cross-product function first extract the last two points of the hull, and check if there is a left-turn or a right-turn to go to the point p_3.

```
def crossProduct(hull, p3):
   """
   Cross product
   hull : list that should contain at least 2 points
   p3  : point
   """
   p1 = hull[-2];
   p2 = hull[-1];

   c= (p2[0] -p1[0])*(p3[1] -p1[1]) -(p3[0] -p1[0])*(p2[1] -p1[1]);
   return c;
```

In order to display the results, one function is proposed.

```
def displayPointsAndHull(points, P, hull, filename=None):
   """
   Fonction for display points and hull
   optionally save figure into pdf file
   """
   fig = plt.figure();
   if P is not(None):
      for i in np.arange(points.shape[0]):
         plt.plot([P[0],points[i,0]], [P[1],points[i,1]], 'C0');
   plt.scatter(points[:,0], points[:,1]);

   hull = np.array(hull);
   plt.plot(hull[:,0], hull[:,1], 'C2');
   plt.show()
   if filename:
      fig.savefig(filename, bbox_inches='tight');
```

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30.2.3 Simple tests

For 5 points:

```
Points=np.array([[ 1, 2],
      [ 1, -4],
      [ 2, -1],
      [ 3, -4],
      [ 4, 1],
      [ 3, 0]])

H = conv_hull(Points);
displayPointsAndHull(Points, H, 'sample_hull.python.pdf');
```

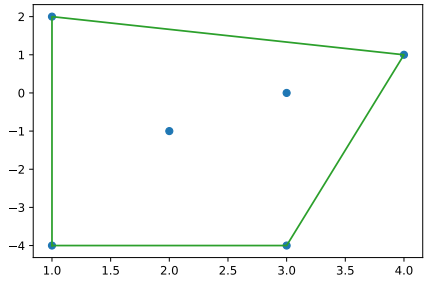
For a few random points:

```
nb=50;
Points = np.random.rand(nb, 2);
H = conv_hull(Points);
displayPointsAndHull(Points, H, 'random_hull.python.pdf');
```

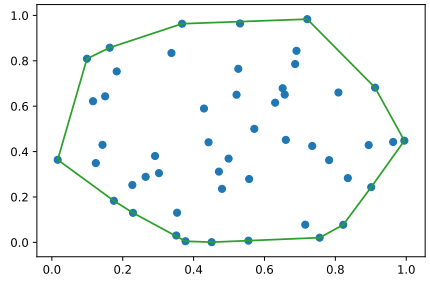
The results are illustrated in Fig.30.3.

Figure 30.3 Illustration of the convex hull computation.

(a) Convex points of 5 points.



(b) Convex hull of 50 random points.



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31 Voronoï Diagrams and Delaunay Triangulation

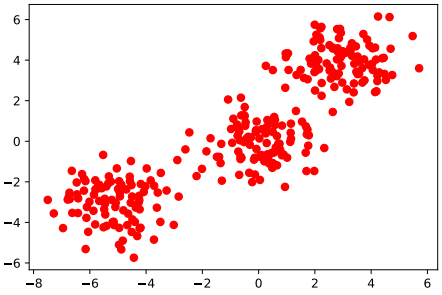
This tutorial aims to spatially characterize a spatial point pattern by using some tools of computational geometry: the Voronoi diagram, the Delaunay triangulation and the Minimum Spanning Tree (MST), illustrated in Fig.31.1.
For biomedical issues, this point pattern analysis can help the biologists to classify different populations of cells.

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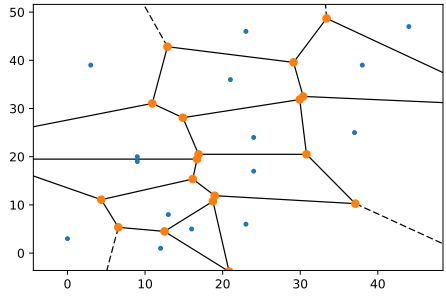
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Figure 31.1 Random point pattern and some geometrical structures used to characterize it.

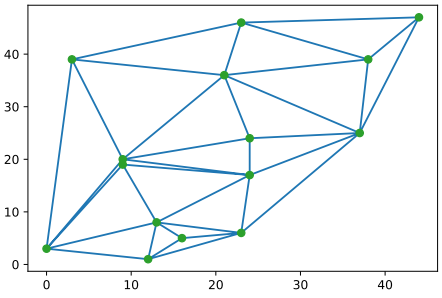
(a) Initial points



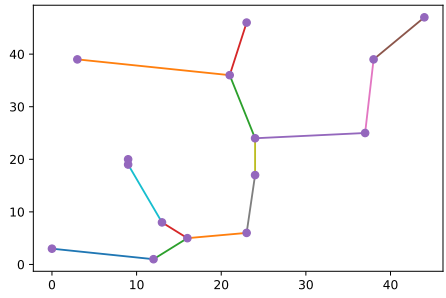
(b) Voronoi diagram



(c) Delaunay triangulation



(d) Minimum spanning tree of the Delaunay triangulation



31.1 Voronoi and Delaunay

A voronoi diagram, in 2D, is defined as a partition of the plane into cells R_k according to a distance function d and a set of seeds (germs) P_k.

$$R_k = \{x \in X \mid d(x, P_k) \leq d(x, P_j) \text{ for all } j \neq k\}$$

The Delaunay graph is the dual graph that links the germs of the neighborhing Voronoi cells.

31.1.1 Random tesselation

Follow these instructions to generate a random tesselation:

>>>?

1. Generate a random point process.
2. Determine the Delaunay triangulation.
3. Determine the Voronoi diagram.



Use the python functions `Delaunay` and `Voronoi` from `scipy.spatial`.

31.1.2 Characterization of the Voronoi diagram

This basic approach characterizes the set of the cells. With the help of the Voronoi diagram, it is possible to make the two following measurements, Area Disorder (AD) and Round Factor Homogeneity (RFH), defined by:

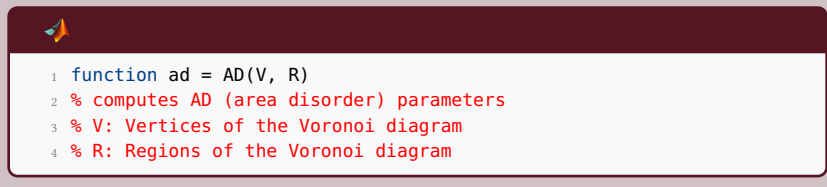
$$AD = 1 - \frac{1}{1 + \frac{\sigma(A)}{\mu(A)}} \tag{31.1}$$

$$RFH = 1 - \frac{\sigma(RF)}{\mu(RF)} \tag{31.2}$$

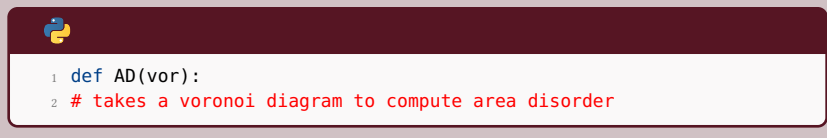
where A and RF are calculated on the regions R_k of the Voronoi diagram. μ and σ are the mean and standard deviation of the areas of the Voronoi cells. The circularity (RF) of a polygon can be defined as the ratio between its area and the area of the disk of an equivalent perimeter.

>>>?

- Code these measurements with the following prototypes:



```
function ad = AD(V, R)
% computes AD (area disorder) parameters
% V: Vertices of the Voronoi diagram
% R: Regions of the Voronoi diagram
```



```
def AD(vor):
# takes a voronoi diagram to compute area disorder
```

  In order to evaluate the area of each Voronoi cell, transform each cell to a polygon.
- Represent the couple (ad, rfh) in a graph, which gives a characterization of the Voronoi diagram.



See `shapely.geometry.Polygon` for evaluating the area of a polygon.

31.1.3 Characterization of the Delaunay graph

If L denotes the set of the edge lengths of the Delaunay triangulation, the mean and the standard deviation of L can also give informations on the graph.

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>>>?

- Compute and display in a graph the point of coordinates $(\mu(L), \sigma(L))$, with μ representing the mean and σ the standard deviation.

31.2 Minimum spanning tree

Definition from Wikipedia: a minimum spanning tree (MST) or minimum weight spanning tree is a subset of the edges of a connected, edge-weighted undirected graph that connects all the vertices together, without any cycles and with the minimum possible total edge weight. That is, it is a spanning tree whose sum of edge weights is as small as possible.

One of the methods to compute the MST is the Kruskal algorithm.

>>>?

- Compute the MST.
- Compute $(\mu(L^*), \sigma(L^*))$ where L^* denotes the set of the edge lengths of the MST.

31.3 Characterization of various point patterns

>>>?

1. Generate n condition Poisson point processes of 100 points each. For each realization, calculate the parameters (AD, RFH), $(\mu(L), \sigma(L))$ and $(\mu(L^*), \sigma(L^*))$. Display these n points in a 2D diagram in order to analyze the robustness of the quantification.
2. Generate 3 different point processes with regular, uniform and Gaussian dispersion. Display the different diagrams. Which one is the most discriminant?

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31.4. Python correction

```python
from scipy.spatial import Voronoi, voronoi_plot_2d, Delaunay, distance
import numpy as np

import matplotlib.pyplot as plt
from shapely import geometry # for polygons, area and perimeter
from scipy.sparse import csgraph # minimum spanning tree
```

31.4.1 Random tessellations

Random tessellations are generated following normal standard and uniform distribution. A regular pattern is also employed. They are illustrated in Fig.31.2.

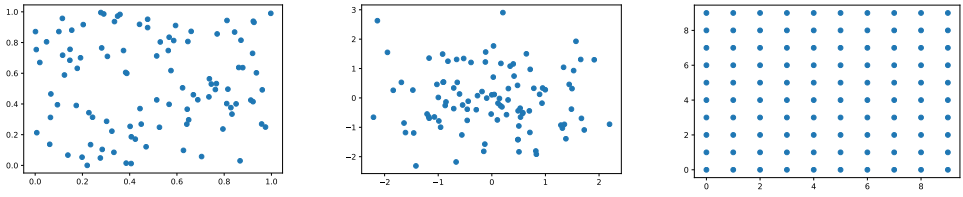
```python
def dist_poisson(N=100):
    points = np.random.rand(N, 2)
    return points

def dist_gaussienne(N=100):
    points = np.random.randn(N, 2)
    return points

def dist_regular(N=100):
    c = np.floor(np.sqrt(N));
    x2, y2 = np.meshgrid(range(int(c)), range(int(c)));
    points = np.vstack([x2.ravel(), y2.ravel()])
    return points.transpose();
```

Figure 31.2 Different point patterns.

(a) Uniform distribution. **(b)** Gaussian distribution. **(c)** Regular distribution.



31.4.2 Voronoi diagram and analysis

The Voronoi diagram is simply generated via the following command, with `points` being generated with the previous functions:

```python
vor = Voronoi(points);
```

The two characterization functions RFH and AD are defined on the Voronoi cells.

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```python
def RFH(vor):
    """
    Evaluates Round Factor Homogeneity from voronoi diagram
    """
    rfs=[];
    for cell in vor.regions:
       if cell and -1 not in cell:
          poly = geometry.Polygon([(vor.vertices[p-1]) for p in cell]);
          rfs.append(4*np.pi*poly.area/(poly.length**2));
    res = 1 -np.std(rfs) / np.mean(rfs);
    return res;
```

```python
def AD(vor):
    """
    Evaluates Area Disorder from voronoi diagram
    """
    areas=[];
    for cell in vor.regions:
       if cell and -1 not in cell:
          poly = geometry.Polygon([(vor.vertices[p-1]) for p in cell]);
          areas.append(poly.area);
    res = 1 -1/(1+np.std(areas) / np.mean(areas));
    return res;
```

31.4.3 Delaunay triangulation and minimum spanning tree

The Delaunay triangulation is computed with

```python
tri = delaunay(points);
```

Then, the characterization of the triangulation is done by measuring the distances of the edges.

```python
def characterization(tri):
    """
    Characterization of the Delaunay triangulation (mean and std dev of edges)
    """
    M = triToMat(tri);
    m = np.mean(M[M>0]);
    s = np.std(M[M>0]);
    return m, s;
def triToMat(tri, value=0.):
    """
    Transforms the triangulation into a matrix representation,
    for simplicity
    """
    M = np.full((tri.npoints, tri.npoints), value);
    d = distance.pdist(tri.points);
    distances = distance.squareform(d);
    for s in tri.simplices:
       M[s[0], s[1]] = distances[s[0], s[1]];
       M[s[1], s[2]] = distances[s[1], s[2]];
       M[s[2], s[0]] = distances[s[2], s[0]];
    return M;
```

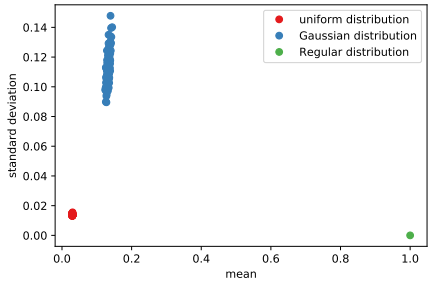
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31.4.4 Characterization of different realizations

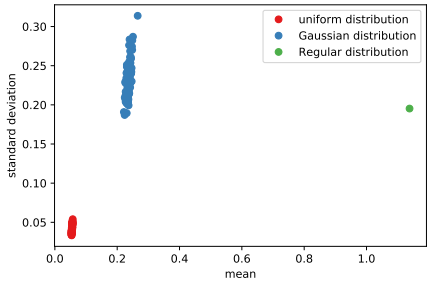
n realizations of the two distributions (uniform and Gaussian) are simulated. Then, the Voronoi diagram and the Delaunay triangulation are computed and characterized. The results are presented in Fig.31.3.

Figure 31.3 Characterization of several point processes. Each color represent a different process, and each point represent one realization. These characterizations can enhance a difference between the spatial distributions of the points.

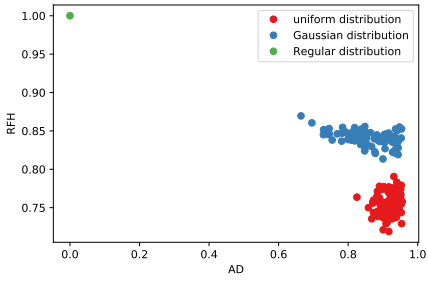
(a) Characterization by the mean and standard deviation of the lengths of the Delaunay triangulation.



(b) Characterization of the minimum spanning tree of the Delaunay triangulation by the mean and standard deviation of the lengths of the MST.



(c) AD and RFH on the Voronoi diagram.



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Fifth part

Image Characterization and Pattern Analysis

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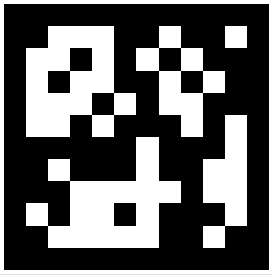
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32 Integral Geometry

This tutorial aims to characterize objects by measurements from integral geometry.

The different processes will be applied on the following synthetic image:

Figure 32.1 X

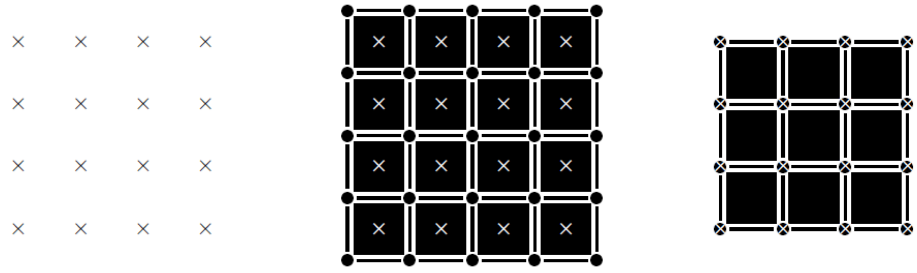


32.1 Cell configuration

The spatial support of an image can be covered by cells associated with pixels. A cell (square of interpixel distance size) is composed of 1 face, 4 edges and 4 vertices. Either a cell is centered in a pixel (intrapixel cell) or a cell is constructed by connecting pixels (interpixel cell). The following figure shows the two possible representations of an image with 16 pixels:

Figure 32.2 Pixels representation.

(a) Image. **(b)** Intrapixel cells. **(c)** Interpixel cells.



We respectively denote f^{intra} (resp. f^{inter}), e^{intra} (resp. e^{inter}) and v^{intra} (resp. v^{inter}) the number of faces, edges and vertices for the intrapixel (resp. interpixel) cell configuration Using these two configurations, the measurements from integral geometry (area A, perimeter P, Euler number χ_8 or χ_4) can be computed as:

$$A = f^{intra} = v^{inter} \quad (32.1)$$

$$P = -4f^{intra} + 2e^{intra} \quad (32.2)$$

$$\chi_8 = v^{intra} - e^{intra} + f^{intra} \quad (32.3)$$

$$\chi_4 = v^{inter} - e^{inter} + f^{inter} \quad (32.4)$$

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>>>?

1. Count manually the number of faces, edges and vertices of the image X for the two configurations (Intra- and Inter-pixel) of Fig. 32.1.
2. Deduce the measurements from integral geometry (Eq. 32.1-32.4).

32.2 Neighborhood configuration

In order to efficiently calculate the number of vertices, edges and faces of the object, the various neighborhood configurations (of size 2x2 pixels) of the original binary image X are firstly determined. Each pixel corresponds to a neighborhood configuration α. Thus, sixteen configurations are possible, presented in Tab. 32.1.

Table 32.1 Neighborhood configurations.

	$\begin{matrix}0&0\\0&0\end{matrix}$	$\begin{matrix}0&0\\0&1\end{matrix}$	$\begin{matrix}0&1\\0&0\end{matrix}$	$\begin{matrix}0&1\\0&1\end{matrix}$	$\begin{matrix}0&0\\1&0\end{matrix}$	$\begin{matrix}0&0\\1&1\end{matrix}$	$\begin{matrix}0&1\\1&0\end{matrix}$	$\begin{matrix}0&1\\1&1\end{matrix}$
α	0	1	2	3	4	5	6	7
	$\begin{matrix}1&0\\0&0\end{matrix}$	$\begin{matrix}1&0\\0&1\end{matrix}$	$\begin{matrix}1&1\\0&0\end{matrix}$	$\begin{matrix}1&1\\0&1\end{matrix}$	$\begin{matrix}1&0\\1&0\end{matrix}$	$\begin{matrix}1&0\\1&1\end{matrix}$	$\begin{matrix}1&1\\1&0\end{matrix}$	$\begin{matrix}1&1\\1&1\end{matrix}$
α	8	9	10	11	12	13	14	15

Thereafter, each configuration contributes to a known number of vertices, edges and faces (Tab. 32.2). To determine the neighborhood configurations of all the pixels, an efficient algorithm effective consists in convolving the image X by a mask F, whose values are powers of two, and whose origin is the top-left pixel:

$$F = \begin{pmatrix} 1 & 4 \\ 2 & 8 \end{pmatrix}$$

The resulting image is $X * F$. Notice that this image X has no pixel touching the borders, your code should ensure this (for example by padding the array with zeros). In this way, the histogram h of $X * F$ gives the distribution of the neighborhood configurations from image X. And each configuration contributes to a known number of vertices, edges and faces:

$$v = \sum_{\alpha=0}^{15} v_\alpha h(\alpha) \tag{32.5}$$

$$e = \sum_{\alpha=0}^{15} e_\alpha h(\alpha) \tag{32.6}$$

$$f = \sum_{\alpha=0}^{15} f_\alpha h(\alpha) \tag{32.7}$$

The following table gives the values of v_α, e_α and f_α for each cell configuration.

>>>?

1. Compute the distribution of the neighborhood configurations from image X.
2. Deduce the number of vertices, edges and faces for each cell representation and compare these values with the previous (manually computed) results.

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Table 32.2 Contributions of the neighborhood configurations to the computation of v, e and f

intrapixel cells																
α	0	1	2	3	4	5	6	7	8	9	10	11	12	13	14	15
f_α	0	1	0	1	0	1	0	1	0	1	0	1	0	1	0	1
e_α	0	2	1	2	1	2	2	2	0	2	1	2	1	2	2	2
v_α	0	1	1	1	1	1	1	1	1	1	1	1	1	1	1	1

interpixel cells																
α	0	1	2	3	4	5	6	7	8	9	10	11	12	13	14	15
f_α	0	0	0	0	0	0	0	0	0	0	0	0	0	0	0	1
e_α	0	0	0	1	0	1	0	2	0	0	0	1	0	1	0	2
v_α	0	1	0	1	0	1	0	1	0	1	0	1	0	1	0	1

32.3 Crofton perimeter

The Crofton perimeter could be computed form the number of intercepts in different random directions. In discrete case, only the directions $0, \pi/4, \pi/2$ and $3\pi/4$ are considered; they are selected according to the desired connexity.

The number of intercepts are denoted $i_0, i_{\pi/4}, i_{\pi/2}$ and $i_{3\pi/4}$ for the orientation angles $0, \pi/4, \pi/2$ and $3\pi/4$ respectively.

In this way, the Crofton perimeter (in 4 and 8 connexity) is defined in discrete case as:

$$P_4 = \frac{\pi}{2}\left(i_0 + i_{\pi/2}\right) \tag{32.8}$$

$$P_8 = \frac{\pi}{4}\left(i_0 + \frac{i_{\pi/4}}{\sqrt{2}} + i_{\pi/2} + \frac{i_{3\pi/4}}{\sqrt{2}}\right) \tag{32.9}$$

These perimeter measurements can be computed from the neighborhood configurations of the original image:

$$P_4 = \sum_{\alpha=0}^{15} P_\alpha^4 h(\alpha) \tag{32.10}$$

$$P_8 = \sum_{\alpha=0}^{15} P_\alpha^8 h(\alpha) \tag{32.11}$$

with the following weights P_α^4 and P_α^8 of these linear combinations (Tab. 32.3):

Table 32.3 Weights for the computation of the Crofton perimeter

α	0	1	2	3	4	5	6	7
P_α^4	0	$\frac{\pi}{2}$	0	0	0	$\frac{\pi}{2}$	0	0
P_α^8	0	$\frac{\pi}{4}\left(1+\frac{1}{\sqrt{2}}\right)$	$\frac{\pi}{4\sqrt{2}}$	$\frac{\pi}{2\sqrt{2}}$	0	$\frac{\pi}{4}\left(1+\frac{1}{\sqrt{2}}\right)$	0	$\frac{\pi}{4\sqrt{2}}$

α	8	9	10	11	12	13	14	15
P_α^4	$\frac{\pi}{2}$	π	0	0	$\frac{\pi}{2}$	π	0	0
P_α^8	$\frac{\pi}{4}$	$\frac{\pi}{2}$	$\frac{\pi}{4\sqrt{2}}$	$\frac{\pi}{4\sqrt{2}}$	$\frac{\pi}{4}$	$\frac{\pi}{2}$	0	0

>>>?

Evaluate the perimeters P_4 and P_8 with the previous formula on Fig.32.1

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32.4. Python correction



32.4.1 Cell configurations

The following values are reported:

$$f^{intra} = 50$$
$$e^{intra} = 158$$
$$v^{intra} = 107$$

$$f^{inter} = 4$$
$$e^{inter} = 42$$
$$v^{inter} = 50$$

Then, it is easy to compute the following values:

$$\begin{aligned} A &= f^{intra} = 50 \\ P &= -4f^{intra} + 2e^{intra} = 116 \\ \chi_8 &= v^{intra} - e^{intra} + f^{intra} = -1 \\ \chi_4 &= v^{inter} - e^{inter} + f^{inter} = 12 \end{aligned}$$

32.4.2 Neighborhood configuration

The configuration is computed using the convolution function `scipy.signal.convolve2d`. The histogram of the different configurations is presented in Fig.32.3.

Be aware that this algorithms works if there is no object pixel touching the borders of the image. The example image is in this case, but you can ensure this property by padding 0 values around the image:



```
X = np.pad(I, ((1,1),), mode='constant');
```

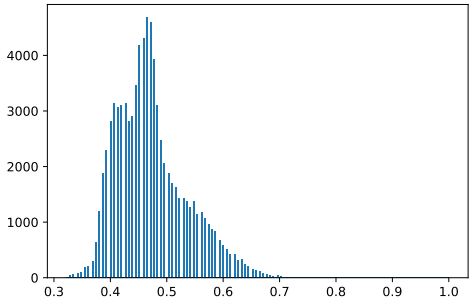


```
# Neighborhood configuration
F = np.array([[0, 0, 0], [0, 1, 4], [0, 2, 8]]);
XF = signal.convolve2d(X,F,mode='same');
edges = np.arange(0, 17 ,1);
h,edges = np.histogram(XF[:],bins=edges);
plt.figure()
plt.bar(edges[0:-1], h);
plt.title("Histogram of the different configurations")
plt.show()
```

The Minkowski functionals are computed using the cells contributions:

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Figure 32.3 Distribution of the different neighborhood configurations.




```
# Computation of the functionals
f_intra = [0,1,0,1,0,1,0,1,0,1,0,1,0,1,0,1];
e_intra = [0,2,1,2,1,2,2,2,0,2,1,2,1,2,2,2];
v_intra = [0,1,1,1,1,1,1,1,1,1,1,1,1,1,1,1];
EulerNb8 = np.sum(h*v_intra -h*e_intra + h*f_intra)
f_inter = [0,0,0,0,0,0,0,0,0,0,0,0,0,0,0,1];
e_inter = [0,0,0,1,0,1,0,2,0,0,0,1,0,1,0,2];
v_inter = [0,1,0,1,0,1,0,1,0,1,0,1,0,1,0,1];
```

Then, the values are easily verified.

```
EulerNb4 = np.sum(h*v_inter -h*e_inter + h*f_inter)
Area = sum(h*f_intra)
Perimeter = sum(-4*h*f_intra + 2*h*e_intra)
print("E_4:{0}, A:{1}, P:{2}".format(EulerNb4, Area, Perimeter));
```

```
E_4:12, A:50, P:116
```

32.4.3 Crofton perimeter

The Crofton perimeter is a good approximation of a perimeter. One should notice that there is no definitive solution to perimeter evaluation. The Crofton perimeter is approximated in 2 or 4 directions, denoted P_4 and P_8 with a reference to the connectivity.

```
# Crofton perimeter
P4 = [0,np.pi/2,0,0,0,np.pi/2,0,0,np.pi/2,np.pi,0,0,np.pi/2,np.pi,0,0];
Perimeter4 = sum(h*P4)
P8 = [0,np.pi/4*(1+1/(np.sqrt(2))),np.pi/(4*np.sqrt(2)),np.pi/(2*np.sqrt(2)),0,
      ↪ np.pi/4*(1+1/(np.sqrt(2))),0,np.pi/(4*np.sqrt(2)),np.pi/4,np.pi/2,np.pi
      ↪ /(4*np.sqrt(2)),np.pi/(4*np.sqrt(2)),np.pi/4,np.pi/2,0,0];
Perimeter8 = sum(h*P8)
```

```
Perimeter4: 91.10618695410399, Perimeter8: 77.76399477870015
```

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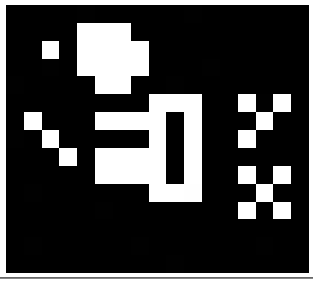
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33 Topological Description

The objective of this tutorial is to classify all foreground points of a binary image according to their topological signification: interior, isolated, border.... The reader can refer to [6]for more details.

The different processes will be realized on the following binary image.

Figure 33.1 Test



Preliminary definitions:

- y is 4-adjacent to x if $|y_1 - x_1| + |y_2 - x_2| \leq 1$.
- y is 8-adjacent to x if $\max(|y_1 - x_1|, |y_2 - x_2|) \leq 1$.
- $V_4(x) = \{y : y \text{ is 4-adjacent to } x\}$; $V_4^*(x) = V_4(x) \backslash \{x\}$.
- $V_8(x) = \{y : y \text{ is 8-adjacent to } x\}$; $V_8^*(x) = V_8(x) \backslash \{x\}$.

Figure 33.2 Different neighborhoods. By convention, pixels in white are of value 1, in black of value 0.

(a) $V_4(x)$ **(b)** $V_8(x)$ **(c)** $V_4^*(x)$ **(d)** $V_8^*(x)$



- a n-path is a point sequence $(x_0, \ldots, x_k)$ with x_j n-adjacent to x_{j-1} for $j = 1, \ldots, k$.
- two points $x, y \in X$ are n-connected in X if there exists a n-path $(x = x_0, \ldots, x_k = y)$ such that $x_j \in X$. It defines an equivalence relation.
- the equivalence classes of the previous binary relation are the n-components of X.

33.1 Connectivity numbers

Let $Comp_n(X)$ be the number of n-components ($n = 4$ or $n = 8$ within the selected topology V_4 or V_8) of the set X of foreground points (object). We define the following set:

$$CAdj_n(x, X) = \{C \in Comp_n(X) : C \text{ is n-adjacent to } x\}$$

We select the 8-connectivity for the set X of foreground points (object) and the 4-connectivity for the complementary $\overline{X}$.

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Warning: the definition of $CAdj_n$ introduces the n-adjacency to the central pixel x. In the case of the following configuration (Fig.33.3), $T_8 = 2$, $\overline{T}_8 = 2$ and $TT_8 = 3$.

Figure 33.3 The pixel in the bottom right corner is not C-adjacent-4 to x.

(a) X **(b)** $V_8^*(x) \cap X$



>>>?

1. Create a function for determining the connectivity number: $T_8(x, X) = \#CAdj_8(x, V_8^*(x) \cap X)$,
2. Create a function for determining the connectivity number: $\overline{T}_8(x, X) = \#CAdj_4(x, V_8^*(x) \cap \overline{X})$,
3. Create a function for determining the number: $TT_8(x, X) = \#(V_8^*(x) \cap X)$.

Test these functions on some foreground points of the image 'test'.

Use `scipy.ndimage.measurements`.

33.2 Topological classification of binary points

From the connectivity numbers $T_8(x, X)$, $\overline{T}_8(x, X)$ and $TT_8(x, X)$, it is possible to classify a foreground point x within the binary image X according to its topological signification:

$T_8(x, X)$	$\overline{T}_8(x, X)$	$TT_8(x, X)$	Type
0	1		isolated point
1	0		interior point
1	1	> 1	border point
1	1	1	end point
2	2		2-junction point
3	3		3-junction point
4	4		4-junction point

The following Fig. 33.4 shows the classification of 4 points.

Figure 33.4 Points configurations.

(a) end **(b)** isolated **(c)** border **(d)** interior



>>>?

With the help of this table, classify the points of the image 'test'.

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33.3. Python correction

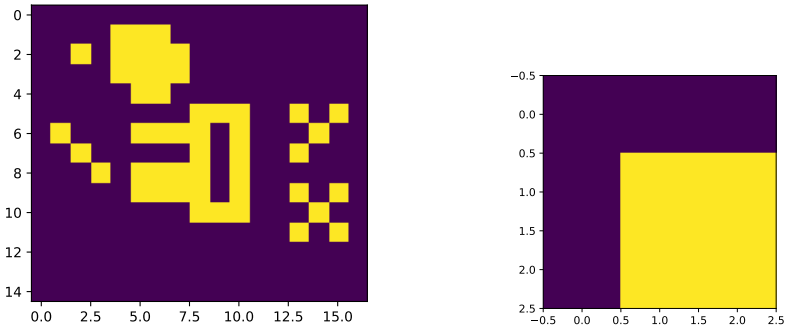
33.3.1 Toplogical description

The operations are not difficult, except that the $CAdj_4$ should be coded carefully.

```python
def nc(A):
    # A : block 3x3, binary
    # complementary set of A
    invA=1-A;
    # neighborhoods
    V8=np.ones((3,3)).astype(int);
    V8_star=np.copy(V8);
    V8_star[1,1] = 0;
    V4=np.array([[0, 1, 0],[1, 1, 1],[0, 1, 0]]).astype(int);
    # intersection is done by the min operation
    X1=np.minimum(V8_star,A);
    TT8=np.sum(X1);
    L, T8 = mes.label(X1, structure=V8);
    # The C-ajd-4 might introduce some problems if a pixel is not 4-connected
    # to the central pixel
    X2=np.minimum(V8,invA);
    Y=np.minimum(X2,V4);
    X=morpho.reconstruction(Y,X2,selem=V4);
    L, T8c = mes.label(X, structure=V4);

    return T8, T8c, TT8
```

Figure 33.5 Extraction of the window centered in $x = (1, 4)$, given as (row,col).



33.3.2 Topological classification

The different types are given by the following code.

```python
def nc_type(X):
    # evaluates the connectivity numbers
    a,b,c=nc(X);
    if (a==0):
        y=1; # isolated point
```

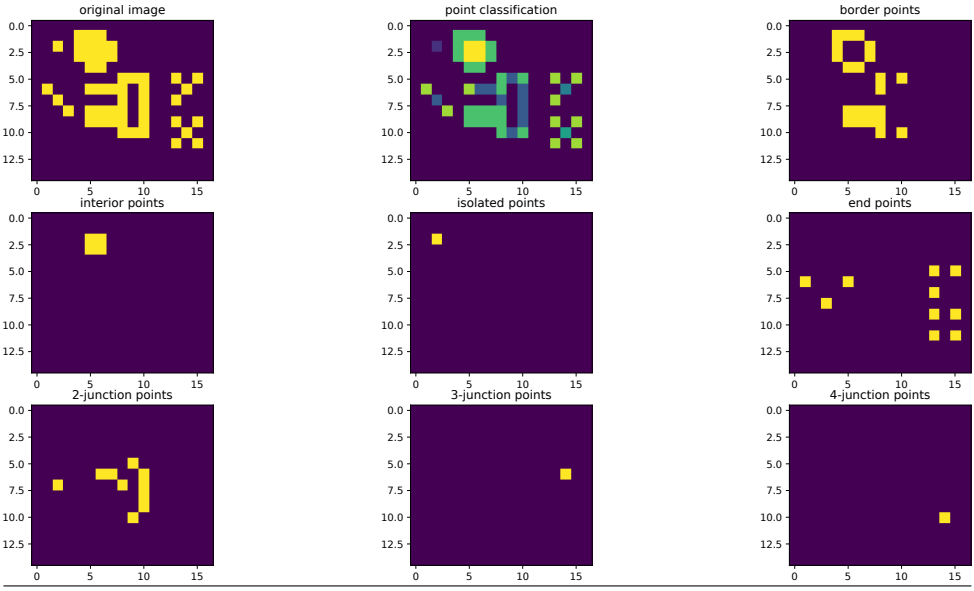
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```
    if ((a==1) and (b==1) and (c>1)):
        y=5; # border point
    if (b==0):
        y=7; # interior point
    if ((a==1) and (b==1) and (c==1)):
        y=6; # end point
    if (a==2):
        y=2; # 2-junction point
    if (a==3):
        y=3; # 3-junction point
    if (a==4):
        y=4; # 4-junction point:
    return y;
```

In order to perform the classification of all pixels of an image, one has to loop over all the pixels, except the ones at the sides. The results are presented in Fig.33.6

```
def classification(A):
     # for the whole image
    m, n = A.shape
    B=np.zeros((m,n));
    for i in range(1, m-1):
        for j in range(1, n-1):
            if A[i,j]> 0:
                X=A[i-1:i+2,j-1:j+2];
                B[i,j]=nc_type(X);
    return B
```

Figure 33.6 Classification of all the pixels of the the original image.



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34 Image Characterization

This tutorial aims to characterize objects by geometrical and morphometrical measurements.

The different processes will be applied on synthetic images as well as images from the Kimia database [1, 39]:

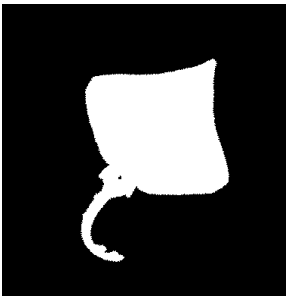
(a) Bat.



(b) Camel.



(c) Ray.



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34.1 Perimeters

We are going to calculate the perimeter using the Crofton formula. This formula consists in integrating the intercept number of the object with lines of various orientation and positions. Its expression in the 2-D planar case is given by:

$$P(X) = \pi \int \chi(X \cap L) dL$$

where the Euler-poincaré characteristic χ is equal to the number of connected components of the intersection of X with a line L.
In the discrete case, the Crofton formula can be estimated by considering the intercept numbers for the horizontal i_0, vertical $i_{\pi/2}$ and diagonal orientations $i_{\pi/4}$ and $i_{3\pi/4}$ as:

$$P(X) = \pi \times \frac{1}{4}\left(i_0 + \frac{1}{\sqrt{2}} i_{\pi/4} + i_{\pi/2} + \frac{1}{\sqrt{2}} i_{3\pi/4}\right)$$

>>>?

1. Calculate the intercept number of a binary object from the Kimia database with lines oriented in the following four directions: $0, \pi/4, \pi/2, 3\pi/4$.
2. Deduce the value of the Crofton perimeter.
3. Compare the result with the classical perimeter functions.

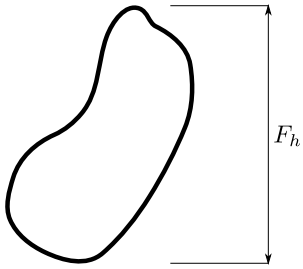


See `perimeter` from `skimage.measure`.

34.2 Feret Diameter

The Feret diameter (a.k.a. the caliper diameter) is the length of the projection of an object in one specified direction Fig.34.1.

Figure 34.1 Feret diameter of the object in horizontal direction.



>>>?

1. Calculate the projections in different directions of a binary object from the Kimia database.
2. Deduce the minimum, maximum and mean value of the Feret diameters.

34.3 Circularity

We want to know if the object X is similar to a disk. For that, we define the following measurement (circularity criterion):

$$circ(X) = \frac{4\pi A(X)}{P(X)^2}$$

where $A(X)$ and $P(X)$ denote the area and perimeter of the object X.

>>>?

1. Show that the circularity of a disc is equal to 1.
2. Generate an array representing an object as a discrete disc.
3. Calculate its circularity and comment the results.

Use `numpy.meshgrid`.

34.4 Convexity

We want to know if the object X is convex. For that, we define the following measurement:

$$conv(X) = \frac{A(X)}{A(CH(X))}$$

where $CH(X)$ denotes the filled convex hull of the object X.

>>>?

1. Compute the convex hull of a pattern from the Kimia database.
2. Evaluate the area of the filled convex hull.
3. Deduce the convexity of the pattern.

See `ConvexHull` from `scipy.spatial`.

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34.5. Python correction

```python
import matplotlib.pyplot as plt
import numpy as np
from scipy import ndimage
from scipy import signal
from scipy import misc
from scipy import spatial
from skimage import measure
```

34.5.1 Perimeters

The convolution is used here as an easy way of getting the borders of the object in one direction, i.e. counting the number of intercepts. This method is efficient because, for one given direction, a high number of lines are considered. Keep in mind that only 4 orientations are used in the proposed code.

```python
def countIntercepts(I, h):
    B = np.abs( signal.convolve2d(I, h, mode='same'));
    n = np.sum(B) / 2;
    return n;

def perimCrofton(I):
    """
    Approximate the Crofton perimeter with 4 directions
    I is the input binary image
    return the perimeter, float value
    """
    # defines an orientation
    h = np.array([[-1, 1]]);
    n1 = countIntercepts(I, h);

    n2 = countIntercepts(I, h.transpose());

    h = np.array([[1, 0], [0, -1]]);
    n3 = countIntercepts(I, h.transpose());

    h = np.array([[0, 1], [-1, 0]]);
    n4 = countIntercepts(I, h.transpose());

    perim_Crofton = np.pi/4 * (n1+n2+ 1/np.sqrt(2)*(n3+n4));
    return perim_Crofton;
```

```
Crofton perimeter: 1305.50015965
Classical perimeter in N4: 1374.19509294
Classical perimeter in N8: 1642.82842712
```

34.5.2 Feret diameter

The code consists in rotating the image and evaluating the projected diameter. The rotation function can interpolate the pixel, the nearest method is thus required. The function `np.max` directly performs the projection in one direction.

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```python
def feretDiameter(I):
    """
    I: input binary image
    Returns min, max and mean Feret diameter, which is the length of the
    projected object in one direction
    """
    diameter = [];
    for angle in range(180):
        I2 = ndimage.interpolation.rotate(I, angle, mode='nearest');
        I3 = I2.max(axis=0);
        diameter.append(np.sum(I3 > 0));

    return np.min(diameter), np.max(diameter), np.mean(diameter);
```

For the camel image [1], the Feret diameters are:

```
min, Max, average Feret diameters: 182 325 266.05
```

34.5.3 Circularity

For a disk, the perimeter is $\pi \cdot D$ and the surface is $\pi \cdot \frac{D^2}{4}$, which shows that the circularity criterion has value 1 for a disk.

In order to generate a binary image containing a disk, one simple way is to use the formula: $(x - x_0)^2 + (y - y_0)^2 \leq R^2$. The efficient way to do this is to use `np.meshgrid`.

```python
def disk(t, r):
    """
    Generates a binary array representing a disk, centered, of radius r
    an array of size [2t,2t] is generated
    """
    x = np.arange(-t, t, 1);
    X,Y = np.meshgrid(x, x);
    I = (X**2 + Y**2)<= r**2;
    return I;
```

The circularity uses the perimeters as evaluated earlier.

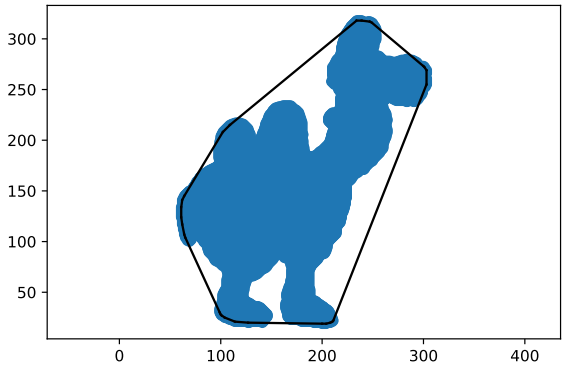
```python
def circularity(I):
    """
    Circularity criterion
    4*pi*A/P**2
    returns crofton and classic
    """
    P = perimCrofton(I);
    print("Perimeter by crofton: ", P)
    A = np.sum(I);
    C = np.pi*4*A/P**2;

    p = measure.perimeter(I, neighbourhood=4);
    print("Usual perimeter: ", p)
    c = np.pi*4*A/p**2;
    return C, c;
```

This gives for the camel image:

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Figure 34.2 Convex hull of the image Camel.




```
Perimeter by crofton: 2514.43300853
Usual perimeter: 2649.36074863
circularity by crofton: 0.999019146137
circularity usual 0.89985338478
```

34.5.4 Convexity

The convex hull is computed with the `scipy.spatial` tools. The following function plots the result. Notice that the coordinates of an image and the coordinates of an array are different, and one has to flip the image array in order to display both data in the same figure.

```python
def convexity(I):
    """
    Evaluates the convexity criterion
    I is a binary image (np array)
    return convexity
    """
    # be careful that coordinates between images and arrays are inversed
    # thus, image is flipped before extracting points coordinates
    points = np.transpose(np.where(np.flip(I,0)));
    hull = spatial.ConvexHull(points);
    A = np.sum(I);
    Ah = hull.volume;

    plt.figure()
    for simplex in hull.simplices:
        plt.plot(points[simplex, 1], points[simplex, 0], 'k-')
    plt.axis('equal')
    plt.show()
    return A/Ah;
```

This criterion is between 0 and 1. This is illustrated in Fig.34.2.

```
convexity of Camel: 0.644014426566
```

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35 Shape Diagrams

The objective is to study some shape diagrams and the possibility to define properties that may be useful in order to distinguish the different objects.

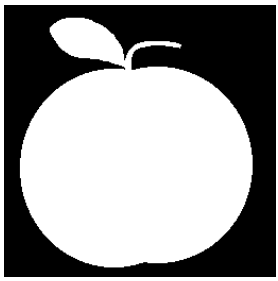
Shape diagrams are representations of single shapes (connected compact sets, see [30, 31, 32]) as points in the 2-D unit square plane. They are based on inequalities between 6 geometrical measurements: area A, perimeter P, radius of the inscribed circle r, radius of the circumscribed circle R, minimum Feret diameter ω and maximum Feret diameter d. In this way, the morphometrical functionals used in the different shape diagrams are normalized ratios of such geometrical functionals. The following table shows the morphometrical functionals for non-convex sets:

Table 35.1 Morphometrical functionals.

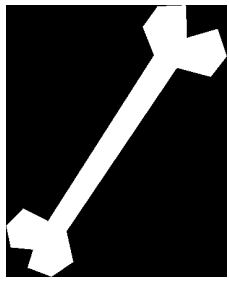
Geometrical functionals	Inequalities	Morphological functionals
r, R	$r \leq R$	r/R
ω, R	$\omega \leq 2R$	$\omega/2R$
A, R	$A \leq \pi R^2$	$A/\pi R^2$
d, R	$d \leq 2R$	$d/2R$
r, d	$2r \leq d$	$2r/d$
ω, d	$\omega \leq d$	ω/d
A, d	$4A \leq \pi d^2$	$4A/\pi d^2$
R, d	$\sqrt{3}R \leq d$	$\sqrt{3}R/d$
r, P	$2\pi r \leq P$	$2\pi r/P$
ω, P	$\pi\omega \leq P$	$\pi\omega/P$
A, P	$4\pi A \leq P^2$	$4\pi A/P^2$
d, P	$2d \leq P$	$2d/P$
R, P	$4R \leq P$	$4R/P$
r, A	$\pi r^2 \leq A$	$\pi r^2/A$
r, ω	$2r \leq \omega$	$2r/\omega$

Figure 35.1 The different processes will be applied on images from the Kimia database [1, 39].

(a) Apple.



(b) Bone.



(c) Camel.



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35.1 Geometrical functionals

>>>?

Code functions in order to evaluate the different parameters:

- the area, Crofton perimeter and Feret diameters have been already presented in tutorial 32;
- the radius of the inscribed circle can be defined from the ultimate erosion of a set.

The function `scipy.ndimage.morphology.distance_transform_cdt` computes the distance map of a binary image (chamfer distance transform).

35.2 Morphometrical functionals

>>>?

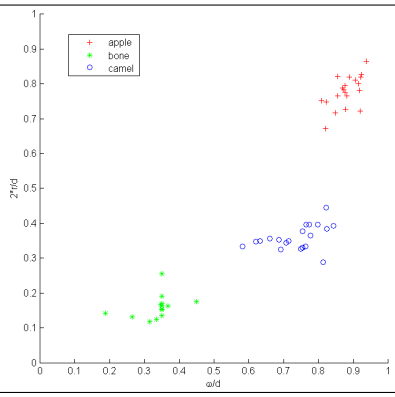
Code and evaluate some of the morphometrical functionals listed in the table 35.1. Note that each of them has a physical meaning, e.g. $\frac{4\pi A}{P^2}$ (circularity), $\frac{4A}{\pi d^2}$ (roundness), $2\omega/P$ (thinness).

35.3 Shape diagrams

>>>?

- Visualize the different shape diagrams for all the images (from the Kimia database) within the three classes 'apple', 'bone' and 'camel'. The Fig.35.2 illustrates the result for the shape diagram $(x = 2r/d, y = P/\pi d)$.
- Which shape diagram is the most appropriate for the discrimination of such objects?

Figure 35.2 Example of a shape diagram.



35.4 Shape classification

>>>?

- Use a K-means clustering method for automatic classification of such shapes.
- Propose a method to quantify the classification accuracy for each shape diagram.

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35.5. Python correction

```python
import numpy as np

import scipy.ndimage
import imageio # imread and imwrite
import matplotlib.pyplot as plt
import skimage.measure # some geometrical descriptors

# for reading files
import glob

from sklearn.cluster import KMeans
```

35.5.1 Geometrical functionals

The Crofton perimeter is defined by multiple projections, as well as the Feret diameter. Be careful while performing the rotation of the object (as it is a binary object, the interpolation method could introduce non integer values).

```python
def crofton_perimeter(I):
    """ Computation of crofton perimeter
    """
    inter = [];
    h = np.array([[1, -1]]);
    for i in range(4):
        II = np.copy(I);
        I2 = scipy.misc.imrotate(II, 45*i,interp='nearest');
        I3 = scipy.ndimage.convolve(I2, h);

        inter.append(np.sum(I3>100));


    crofton = np.pi/4. * (inter[0]+inter[2] + (inter[1]+inter[3])/np.sqrt(2));
    return crofton
```

```python
def feret_diameter(I):
    """
    Computation of the Feret diameter
    minimum: d (meso-diameter)
    maximum: D (exo-diameter)

    Input: I binary image
    """
    d = np.max(I.shape);
    D = 0;

    for a in np.arange(0, 180, 30):
        I2 = scipy.misc.imrotate(I, a, interp='nearest');
        F = np.max(I2, axis=0);
        measure = np.sum(F>100);

```

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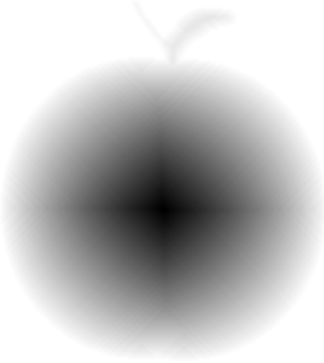
```
        if (measure<d):
            d = measure;
        if (measure>D):
            D = measure;
    return d,D;
```

The inscribed circle is just the maximum of the distance transform inside the object. The distance map for an image apple is shown in Fig.35.3a.

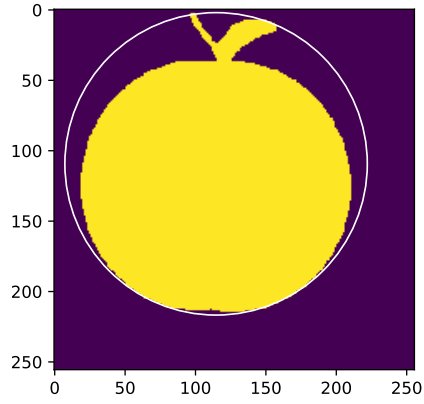
```
def inscribedRadius(I):
    """
    computes the radius of the inscribed circle
    """
    dm = scipy.ndimage.morphology.distance_transform_cdt(I>100);
    radius = np.max(dm);
    return radius;
```

Figure 35.3 Illustration of the computation of two shape parameters.

(a) Distance map of an object apple. The inverse is actually displayed in order to see correctly the progression. The maximum of the distance map is the radius of the inscribed circle.



(b) Circumscribed circle.



The smallest enclosing circle is computed by using the code from the Project Nayuki[1] published under the GNU Lesser General Public License. The result is presented in Fig.35.3b.

```
def circumCircle(I):
    """
    this version uses a function provided by Project Nayuki
    under GNU Lesser General Public License
    """
    points = np.argwhere(I > 100);
    c = smallestenclosingcircle.make_circle(points);
    return c;
```

[1] https://www.nayuki.io/page/smallest-enclosing-circle

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35.5.2 Shape diagrams

The shape diagrams are constructed by reading all the images and computing the shape descriptors.

```python
def diagrams():
    name=['apple-*.bmp', 'Bone-*.bmp', 'camel-*.bmp'];
    elongation=[];
    thinness=[];
    roundness=[];
    z=[];
    for pattern in name:
        namesList = glob.glob(pattern);
        for fichier in namesList:
            I = imageio.imread(fichier);
            radius = inscribedRadius(I);
            d,D = feret_diameter(I);
            crofton = crofton_perimeter(I);

            elongation.append(d/D);
            thinness.append(2*radius / D);
            roundness.append(4*np.sum(I>100)/(np.pi * D**2));
            z.append(crofton / (np.pi * D));
```

The display of the different plots is just a use of the function `plt.plot`.

```python
    plt.plot(elongation[0:20], thinness[0:20], "o", label='Apple')
    plt.plot(elongation[20:40], thinness[20:40], "+", label='Bone')
    plt.plot(elongation[40:60], thinness[40:60], ".", label='Camel')
    plt.legend(name)
    plt.show
    evaluateQuality(elongation, thinness);

    plt.figure();
    plt.plot(z[0:20], roundness[0:20], "o", label='Apple')
    plt.plot(z[20:40], roundness[20:40], "+", label='Bone')
    plt.plot(z[40:60], roundness[40:60], ".", label='Camel')
    plt.legend(name)
    plt.show
    evaluateQuality(z, roundness);

    plt.figure();
    plt.plot(thinness[0:20], z[0:20], "o", label='Apple')
    plt.plot(thinness[20:40], z[20:40], "+", label='Bone')
    plt.plot(thinness[40:60], z[40:60], ".", label='Camel')
    plt.legend(name)
    plt.show
    evaluateQuality(thinness, z);
```

35.5.3 Shape classification

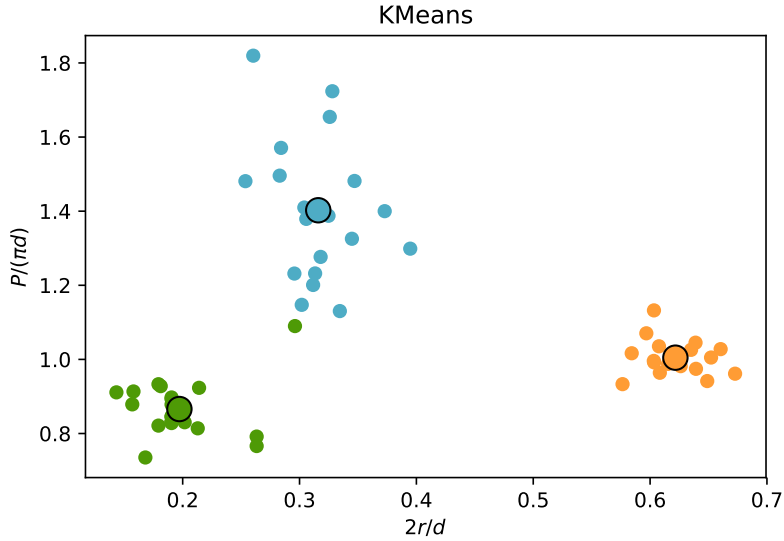
The following code evaluates the quality by comparing the known class of the shape with the segmented (via the kmeans method) class. The result is illustrated in Fig.35.4 with an accurary of 98.3%.

```python
def evaluateQuality(x, y):
    global i
    n = 3;
```

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```
k_means = KMeans(init='k-means++', n_clusters=n)
X = np.asarray(x);
Y = np.asarray(y);
pts = np.stack((X, Y));
pts = pts.T;
#print(pts)
k_means.fit(pts);
k_means_labels = k_means.labels_;
k_means_cluster_centers = k_means.cluster_centers_;
# plot
fig = plt.figure()
colors = ['#4EACC5', '#FF9C34', '#4E9A06']
# KMeans
for k, col in zip(range(n), colors):
   my_members = k_means_labels == k
   cluster_center = k_means_cluster_centers[k]
   plt.plot(pts[my_members, 0], pts[my_members, 1], 'o',
         markerfacecolor=col, markersize=6)
   plt.plot(cluster_center[0], cluster_center[1], 'o', markerfacecolor=col,
         markeredgecolor='k', markersize=12)
plt.title('KMeans')
plt.show()
fig.savefig("kmeans"+str(i)+".pdf");
i += 1;
"""
Evaluation of the quality: count the number of shapes correctly detected
"""
accuracy = np.sum(k_means_labels[0:20] == scipy.stats.mode(k_means_labels
    ↪ [0:20]));
accuracy +=np.sum(k_means_labels[20:40] == scipy.stats.mode(k_means_labels
    ↪ [20:40]));
accuracy +=np.sum(k_means_labels[40:60] == scipy.stats.mode(k_means_labels
    ↪ [40:60]));
accuracy = accuracy / 60 * 100;
print('Accuracy: {0:.2f}%'.format(accuracy));
```

Figure 35.4 Illustration of the accuracy of the classification from a k-means method. The k-means method is not necessarily the adapted to these data. The measured accurary if of 98.3%.



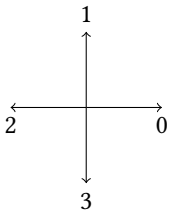
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36 Freeman Chain Code

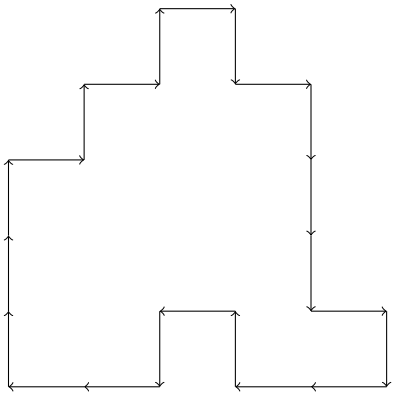
This tutorial is focused on shape representation by the Freeman chain code. This code is an ordered sequence of connected segments (of specific sizes and directions) representing the contour of the shape to be analyzed. The direction of each segment is encoded by a number depending on the selected connectivity (Fig. 36.1). In this example, the contour of the shape and its Freeman code are given in 4-connectivity.

Figure 36.1 Freeman chain code examples.

(a) 4-connected neighborhood.

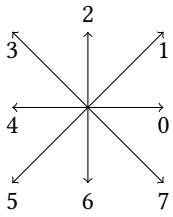


(b) Example Freeman code in a 4-neighborhood.



11101010303330322123 22

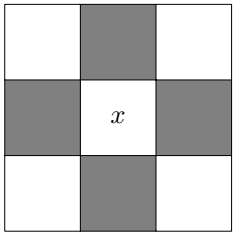
(c) 8-connected neighborhood.



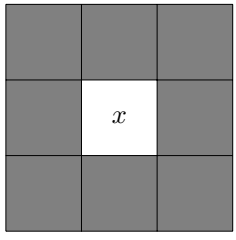
Notations:

- y is 4-adjacent to x if $|y_1 - x_1| + |y_2 - x_2| \leq 1$.
- y is 8-adjacent to x if $\max(|y_1 - x_1|, |y_2 - x_2|) \leq 1$.
- $N_4(x) = \{y : y \text{ is 4-adjacent to } x\}$; $N_4^*(x) = N_4(x) \backslash \{x\}$.
- $N_8(x) = \{y : y \text{ is 8-adjacent to } x\}$; $N_8^*(x) = N_8(x) \backslash \{x\}$.

(a) $V_4(x)$



(b) $V_8(x)$



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36.1 Shape contours

Before determining the Freeman chain code of the shape, it is necessary to extract its contour.

>>>?

1. Generate or load a simple shape as a binary image A.
2. Extract its contour $C_4(A)$ ou $C_8(A)$ according to the 4-connectivity or the 8-connectivity, respectively:

$$\begin{aligned} x \in C_4(A) &\Leftrightarrow \exists y \in N_8(x) \quad y \in {}^cA \\ x \in C_8(A) &\Leftrightarrow \exists y \in N_4(x) \quad y \in {}^cA \end{aligned}$$

Informations

You can erode the object and subtract this erosion to it, with a structuring element that corresponds to N_4 or N_8 if you want to have 8 or 4 connectivity, respectively.

36.2 Freeman chain code

From the shape contours, the Freeman chain code can be calculated.

>>>?

1. From the binary array of pixels, extract the first point belonging to the shape (from left to right, top to bottom).

   Informations

   You can use `np.argwhere` to locate the first point.

2. From this initial point, determine the Freeman chain code c (counterclockwise direction) using the N_4 or N_8 connectivity.

36.3 Normalization

The Freeman chain code is depending on the initial point and is not invariant to shape rotation. It is then necessary to normalize this code.

1. The first step consists in defining a differential code d from the code c :

   $$d_k = c_k - c_{k-1} (\text{mod } 4 \text{ or } 8)$$

   In this example, $d = 30031313313001330311 30$;
2. The second step consists in normalizing the code d. We have to extract the lowest number p from all the cyclic translations of d.
   In this example, $p = 00133031130300313133 13$.
   This Freeman chain code p is then independant from the initial point and invariant by rotations of angles $k * \pi/2$ radians ($k \in \mathbb{Z}$).

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>>>?

- Code above steps 1 and 2. Prototypes of functions are given.
- Validate your code by rotating the shape of $3\pi/2$ radians.

```python
def codediff(fcc, connectivity=8):
# computes differential code
```

Use `numpy.roll` for circularly shifting the freeman code array. Code a small function that tests all elements of array, one by one, in order to get the minimum of two arrays.

36.4 Geometrical characterization

36.4.1 Perimeter

From the Freeman chain code, it is possible to make different geometrical measurement of the shape.

>>>?

Calculate the perimeter of the shape (take care of the diagonals).

36.4.2 Area

The area is evaluated by the following algorithm:

- The area is initialized to 0 and the parameter B is initialized to 0.
- For each iteration on the Freeman chain code c, the area and the parameter value B are incremented with the following rules:

8-code	area	B
0	-B	0
1	-B-0.5	1
2	0	1
3	B+0.5	1
4	B	0
5	B-0.5	-1
6	0	-1
7	-B+0.5	-1

>>>?

Calculate the area of the shape in 8-connectivity. Note that the area does not correspond to the total number of pixels belonging to the shape.

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36.5. Python correction

```python
import matplotlib.pyplot as plt
import numpy as np
from skimage.morphology import binary_erosion,disk,rectangle
from skimage.measure import perimeter
```

36.5.1 Shape contours

To generate a simple object, here is an example:

```python
A = np.zeros((20,20)).astype('bool');
A[4:14, 9:17] = True;
A[1:18,11:16]=True;
```

The contours are computed in 4- or 8-connectivity, see Fig.36.2. This function uses the mathematical morphology in order to get the contour.

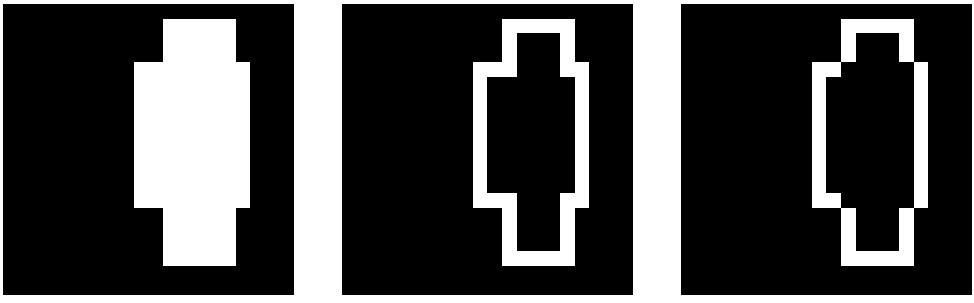
```python
def bwperim(I, connectivity=8):
    """
    Morphological inner contour, in 4 or 8 connectivity
    I: binary image
    return: binary image representing the contour
    """
    if connectivity==8:
        SE = disk(1);
    else:
        SE = rectangle(3,3);

    E = binary_erosion(I, selem=SE);

    return I^E;
# compute the contours
contours8 = bwperim(A, 4);
contours4 = bwperim(A, 8);
```

Figure 36.2 Simple object and its contours in 4- or 8-connectivity.

(a) Sample object. **(b)** Contour in 4-connectivity. **(c)** Contour in 8-connectivity.



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36.5.2 Freeman chain code

First point of the shape

The important thing is to find one point in the contour. The Freeman chain code is sensitive to this choice, but several methods can transform this code so that this first choice does not have any importance.

```python
def firstPoint(C):
    """
    find first point of contour
    returns point (as array)
    """
    p = np.argwhere(C);
    return p[0];
```

```
>>[r0,c0]=firstPoint(A)

r0 =
     5
c0 =
    10
```

Freeman chain code

The principle is to follow the contour, delete each pixel at each step, and find the direction of the next pixel.

```python
def freeman(C, p, connectivity=8):
    def getIndex(contour, point, connectivity):
        """ subfunction for getting the local direction
        """
        if connectivity==8:
            lut= np.array([[1, 2, 3], [8, 0, 4], [7, 6, 5]]);
        else:
            lut= np.array([[0, 2, 0], [8, 0, 4], [0, 6, 0]]);

        window = contour[point[0]-1:point[0]+2, point[1]-1:point[1]+2];
        window = window * lut;
        index = np.max(window);
        return index-1;
    # Be careful that these LUTs consider coordinates from left to rith, top to
        ↪ bottom
    lutx = np.array([-1, -1, -1, 0, 1, 1, 1, 0]);
    luty = np.array([-1, 0, 1, 1, 1, 0, -1, -1]);
    lutcode = np.array([3, 2, 1, 0, 7, 6, 5, 4]);

    nbrpoints = np.sum(C);
    code=[];
    point = p.copy();
    C2 = C.copy();

    for i in np.arange(nbrpoints):
        C2[point[0], point[1]] = 0;

        index = getIndex(C2, point, connectivity);

        if (index==0):
            C2[p[0], p[1]] = 1;
            index = getIndex(C2, point, connectivity);
```

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```
32
33        # new point
34        point[0] = point[0] + lutx[index];
35        point[1] = point[1] + luty[index];
36
37        # add code
38        code.append(lutcode[index]);
39
40    return code;
```

```
code = freeman(C8, p);
```

```
code = array([6, 6, 5, 4, 6, 6, 6, 6, 6, 6, 6, 6, 6, 0, 7, 6, 6, 6, 0, 0, 0, 0,
      ↪ 2, 2, 2, 1, 2, 2, 2, 2, 2, 2, 2, 2, 3, 2, 2, 4, 4, 4, 4])
```

36.5.3 Normalization

Differential code

This is the first step towards independence from the first point.

```
def codediff(fcc, connectivity=8):
    sr = np.roll(fcc, 1);
    d = fcc -sr;
    return d%connectivity;
```

Normalization

The differential code is then normalized, in order to get a rotation invariant code. All the circular shifts are evaluated, and a criterion (the minimum value) is established to be able to always find the same result, for every position of the first point.

```
def minmag(code):
    # high value for min computing
    codemin = np.max(code)* np.ones(code.shape);
    nb = len(code);
    for i in np.arange(len(code)):
        C = np.roll(code, i);

        for j in np.arange(nb):
            if C[j] > codemin[j]:
                break;
            elif C[j] < codemin[j]:
                codemin = C;
                break;
            if j == nb:
                codemin = C;

    return codemin;
```

The differential code is evaluated in `d8`, the normalization gives `shapenumber8`:

```
c = codediff(code, 8);
shapenumber8 = minmag(c);
```

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```
c= array([2, 0, 7, 7, 2, 0, 0, 0, 0, 0, 0, 0, 0, 2, 7, 7, 0, 0, 2, 0, 0, 0, 2, 0,
      ↪  0, 7, 1, 0, 0, 0, 0, 0, 0, 0, 0, 1, 7, 0, 2, 0, 0, 0])

shapenumber8= array([0, 0, 0, 0, 0, 0, 0, 0, 1, 7, 0, 2, 0, 0, 0, 2, 0, 7, 7, 2,
      ↪  0, 0, 0, 0, 0, 0, 0, 0, 2, 7, 7, 0, 0, 2, 0, 0, 0, 2, 0, 0, 7, 1])
```

Validation

This validation shows the effect on a different starting point.

```
p = np.array([4, 9]);
```

Another test is to verify the result after a rotation. To prevent discretization problems, we use 90 degrees and take the transpose of the matrix.

```
# check for rotation by 90 deg
contours8rot=contours8';
```

The same code should be found in both cases.

36.5.4 Geometrical characterization

Perimeter for 8-connectivity

We first need to extract the codes in the diagonal directions and apply a $\sqrt{2}$ factor, then add the number of codes in vertical and horizontal directions.

```
def Perimeter(fcode):
    """
    fcode: Freeman code
    """
    nb_diag = np.sum(np.array(fcode)%2);
    perim = nb_diag*np.sqrt(2) + len(fcode)-nb_diag;
    return perim;
```

The perimeter is evaluated in the same way in `skimage`.

```
Perimeter: 43.65685424949238
skimage.measure.perimeter: 43.65685424949238
```

Area for 8-connectivity

```
def Area(fcode):
    area = 0;
    B = 0;
    lutB = np.array([0, 1, 1, 1, 0, -1, -1, -1]);
    for i in np.arange(len(fcode)):
        lutArea = np.array([-B, -(B+0.5), 0, (B+0.5), B, (B-0.5), 0, -(B-0.5)]);
        area = area + lutArea[fcode[i]];
        B = B + lutB[fcode[i]];
    return area;
```

Notice that the area evaluated by this way is different from the number of pixels.

```
Area: 93.0
Number of pixels (area): 115
```

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37 Machine Learning

The objective of this tutorial is to classify images by using machine learning techniques. Some images, as illustrated in Figure 37.1 of the Kimia database will be used [1, 39].

Figure 37.1 The different processes will be applied on images from the Kimia database. Here are some examples.

(a) bird **(b)** camel **(c)** ray **(d)** turtle



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37.1 Feature extraction

The image database used in this tutorial is composed of 18 classes. Each class contains 12 images. All these 216 images come from the Kimia database. In order to classify these images, we first have to extract some features of each binary image.

>>>?

1. For each image in the database, extract a number of different features, denoted *nbFeatures*.
2. Organize these features in an array of *nbFeatures* lines and 216 columns. In this way, each column i represents the different features of the image i.

You can use the Python function `skimage.measure.regionprops` to extract the same geometrical features.

37.2 Image classification

In order to classify the images, we are going to use neural networks. Pattern recognition networks are feedforward networks that can be trained to classify inputs according to target classes. The inputs are the features of each image. The target data are the labels, indicating the class of each image.

>>>?

1. Build the target data, representing the class of each image. The target data for pattern recognition networks should consist of vectors of all zero values except for a 1 in element i, where i is the class they are to represent. In our example, the target data will be an array of 18 lines and 216 columns.
2. The database will be divided into a training set (75%) and a test set (25%).
3. Run the training task and classify the test images.
4. Show the classification confusion matrix as well as the overall performance.
5. Try to run the same process. What can you conclude?
6. Try to change the parameters of the network to improve the classification performance.



Look at the Python module `sklearn.neural_network.MLPClassifier` to make the classification. Notice that your data may be normalized before performing the classification.

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37.3. Python correction

The following imports may be considered.

```python
# image manipulation and features construction
import glob
from skimage import measure, io
import numpy as np
import matplotlib.pyplot as plt
# preprocessing data and normalization
from sklearn.preprocessing import StandardScaler
from sklearn.preprocessing.data import QuantileTransformer
# learning methods
from sklearn import svm
from sklearn.neural_network import MLPClassifier
from sklearn.model_selection import train_test_split
from sklearn.metrics import classification_report,confusion_matrix
# plot confusion matrix
import seaborn as sn
import pandas as pd
```

37.3.1 Feature extraction

We make a loop on the whole database to extract some features of each image. The 9 features used here are: area, convex area, eccentricity, equivalent diameter, extent, major axis length, minor axis length, perimeter and solidity.

```python
# Definitions of the database, classes and images
rep = 'images_Kimia216/';
classes = ['bird','bone','brick','camel','car','children',
    'classic','elephant','face','fork','fountain',
    'glass','hammer','heart','key','misk','ray','turtle'];
nbClasses = len(classes);
nbImages = 12;
# The features are manually computed
properties = np.zeros((nbClasses*nbImages,9));
target = np.zeros(nbClasses * nbImages);
index=0;
for ind_c, c in enumerate(classes):
    filelist = glob.glob(rep+c+'*');
    for filename in filelist:
        I = io.imread(filename);
        prop = measure.regionprops(I);
        properties[index, 0] = prop[0].area;
        properties[index, 1] = prop[0].convex_area;
        properties[index, 2] = prop[0].eccentricity;
        properties[index, 3] = prop[0].equivalent_diameter;
        properties[index, 4] = prop[0].extent;
        properties[index, 5] = prop[0].major_axis_length;
        properties[index, 6] = prop[0].minor_axis_length;
        properties[index, 7] = prop[0].perimeter;
        properties[index, 8] = prop[0].solidity;
        target[index] = ind_c;

        index = index+1;
```

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Note that in the same time, the target array (required in the following) is built within this loop. It represents the true classes of the objects.

37.3.2 Classification

We used a training set of 75% of the database and 25% for the test set. The scaler is used in order to rescale the data having different ranges and dimensions. Other scalers are proposed in `sklearn.preprocessing`.

```
# percentage of the data used for splitting into train/test
percentTest = .25;
# MLP Classifier (Multi-Layer Perceptron)
# the data are first scaled
propertiesMLP = StandardScaler().fit_transform(properties);
prop_train, prop_test, target_train, target_test = train_test_split(
    ↪ propertiesMLP, target,test_size=percentTest, random_state=0);
```

The network is created with 1 hidden layers of 10 neurons. One could also use SVM instead of MLP (`classifier = svm.SVC(kernel='linear');`).

```
# feedforward neural network
# max_iter should be extended max_iter=100000 for adam or sgd solvers
mlp = MLPClassifier(hidden_layer_sizes=(10,), solver='lbfgs');
target_pred = mlp.fit(prop_train, target_train).predict(prop_test)
print("Training set score: %f" % mlp.score(prop_train, target_train))
```

The training score should be around 1, according to the training dataset and the different parameters employed.

```
Training set score: 1.000000
```

37.3.3 Performance

The confusion matrix gives an idea of the overall performance. The following function uses the modules `seaborn` and `pandas` to generate a `heatmap` that displays the confusion matrix.

```
def plot_cm(cm, classes, normalize=False, cmap=plt.cm.Blues):
    """
    Plot confusion matrix
    cm: confusion matrix, as ouput by sklearn.metrics.confusion_matrix
    classes: labels to be used
    normalize: display number (False by default) or fraction (True)
    cmap: colormap
    returns: figure that can be used for pdf export
    """
    if normalize:
        cm = cm.astype('float') / cm.sum(axis=1)[:, np.newaxis]
    fmt = '.1f' if normalize else 'd'
    df_cm = pd.DataFrame(cm, index = classes, columns = classes);

    fig = plt.figure();
    sn.set(font_scale=.8)
    sn.heatmap(df_cm, annot=True, cmap = cmap, fmt=fmt);
    plt.xlabel('Target label')
    plt.ylabel('True label')

    return fig;
```

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The previous function is then used, and illustrated in Fig.37.2.

```
cnf_matrix = confusion_matrix(target_test, target_pred);
fig=plot_cm(cnf_matrix, classes, normalize=True);
```

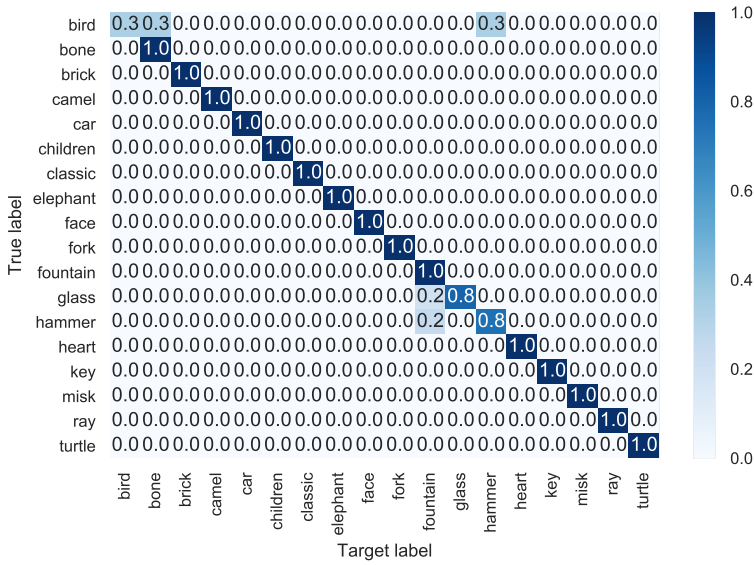
`sklearn.metrics.classification_report` can be used to display the performance.

```
             precision recall f1-score support

       bird     0.75    1.00    0.86      3
       bone     1.00    1.00    1.00      5
      brick     1.00    1.00    1.00      1
      camel     1.00    1.00    1.00      3
        car     1.00    1.00    1.00      1
   children     1.00    1.00    1.00      2
    classic     1.00    1.00    1.00      5
   elephant     1.00    1.00    1.00      3
       face     1.00    1.00    1.00      4
       fork     1.00    1.00    1.00      2
   fountain     1.00    1.00    1.00      3
      glass     1.00    1.00    1.00      5
     hammer     1.00    0.75    0.86      4
      heart     1.00    1.00    1.00      2
        key     1.00    1.00    1.00      3
       misk     1.00    1.00    1.00      3
        ray     1.00    1.00    1.00      4
     turtle     1.00    1.00    1.00      1

avg / total     0.99    0.98    0.98     54
```

Figure 37.2 Normalized confusion matrix of the classification result.



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38 Harris corner detector

The aim of this tutorial is to develop a simple Harris corner detector. This is the first step in pattern matching, generally followed by a feature descriptor construction, and a matching process.

38.1 Corner detector and cornerness measure



Use the `sobel` and `gaussian_filter` from the `scipy.ndimage` module.

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38.1.1 Gradient evaluation

The Harris corner detector is based on the gradients of the image, I_x and I_y in x and y directions, respectively.

>>>?

Apply a Sobel gradient in both directions in order to compute I_x and I_y.

38.1.2 Structure tensor

The structure tensor is defined by the following matrix. The coefficients ω follow a gaussian law, and each summation represents a gaussian filtering process. W is an operating window.

$$M = \begin{bmatrix} \sum\limits_{(u,v)\in W} \omega(u,v) I_x(u,v)^2 & \sum\limits_{(u,v)\in W} \omega(u,v) I_x(u,v) I_y(u,v) \\ \sum\limits_{(u,v)\in W} \omega(u,v) I_x(u,v) I_y(u,v) & \sum\limits_{(u,v)\in W} \omega(u,v) I_y(u,v)^2 \end{bmatrix} = \begin{bmatrix} M_1 & M_2 \\ M_3 & M_4 \end{bmatrix}$$

>>>?

- Evaluate M_1 to M_4 for each pixel of the image.

38.1.3 Cornerness measure

The cornerness measure C, as proposed by Harris and Stephens, is defined as follows for every pixel of coordinates (x, y):

$$C(x,y) = \det(M) - K\,\mathrm{trace}(M)^2$$

with K between 0.04 and 0.15.

>>>?

Compute C for all pixels and display it for several scales σ.

38.2 Corners detection

A so-called Harris corner is the result of keeping only local maxima above a certain threshold value. You can use the checkerboard image for testing, or load the sweden road sign image Fig.38.1.

Use the following function to generate a checkerboard pattern.

```python
def checkerboard(nb_x=2, nb_y=2, s=10):
"""
checkerboard generation
a grid of size 2*nb_x by 2*nb_y is generated
each square has s pixels.
"""
C = 255*np.kron([[1, 0] * nb_x, [0, 1] * nb_x] * nb_y, np.ones((s, s)))
return C
```

Figure 38.1 Sweden road sign to be used for corner detection.



>>>?

- Evaluate the extended maxima of the image.
- Only the strongest values of the cornerness measure should be kept. Two strategies can be employed in conjonction:
  - Use a threshold value t on C: the choice of this value is not trivial, and it strongly depends on the considered image. An adaptive method would be preferred.
  - Keep only the n strongest values.
- The previous operations are affected by the borders of the image. Thus, eliminate the corner points near the borders.
- The detected corners may contain several pixels. Keep only the centroid of each cluster.

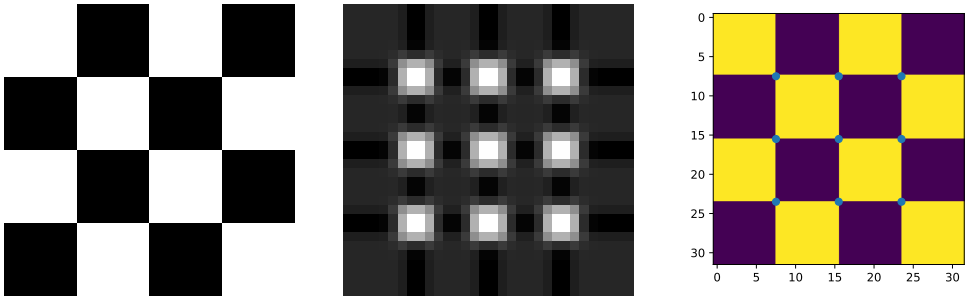
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38.3. Python correction

38.3.1 Cornerness measure

Figure 38.2 Cornerness measure for the checkerboard image. The next step is to locate the corners by thresholding the measure, extracting the local maxima, eliminating points near the edges...

(a) Checkerboard. **(b)** Cornerness measure. **(c)** Harris corner points.



The first step is to compute the gradient in both x and y directions.

```
Ix = scipy.ndimage.sobel(I, axis=0);
Iy = scipy.ndimage.sobel(I, axis=1);
```

Then, the coefficients of the matrix are computed.

```
M1 = np.multiply(Ix, Ix);
M2 = np.multiply(Iy, Ix);
M4 = np.multiply(Iy, Iy);
```

In case of using a scale parameter, these coefficients should be filtered (for example via a gaussian filter).

```
M1 = scipy.ndimage.gaussian_filter(M1, sigma);
M2 = scipy.ndimage.gaussian_filter(M2, sigma);
M4 = scipy.ndimage.gaussian_filter(M4, sigma);
```

Finally, the cornerness measure is evaluated.

```
C = (np.multiply(M1, M4) -np.multiply(M2, M2)) -K * np.multiply(M1+M4, M1+M4);
```

The cornerness measure is displayed in Fig.38.2.

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38.3.2 Corners detection

In order to keep only the strongest corner points, a threshold value t is applied on C. This value is really depending on the considered image, thus such a global threshold is not generally a good idea. One would probably prefer a h-maximum or equivalent operator. For the purpose of this tutorial, we will keep this strategy.

```
C[C<t] = 0;
```

The local maxima are then extracted.

```
corners = peak_local_max(C, indices=False, min_distance=2);
```

The result is a binary image, where some clusters of points are the corner points. To keep only one point per cluster, the centroid of each is detected. The final result is presented in Fig.38.2c.

```
L = measure.label(corners);
props = measure.regionprops(L);
centers=[];
for prop in props:
    centers.append(prop.centroid);
```

38.3.3 Road sign image application

In this case, the values $t = 10^7$ and $\sigma = 3$ are used. The result is illustrated in Fig.38.3.

Figure 38.3 Harris corner detection with scale $\sigma = 3$ and threshold value $t = 10^7$.

(a) Cornerness measure.



(b) Corner points.



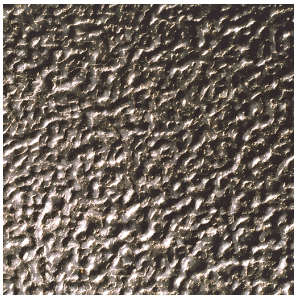
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39 Local Binary Patterns

This tutorial aims to study a texture descriptor named 'Local Binary Patterns'. The first objective is to implement this descriptor. Therefater, digital images of textures will be classified using this descriptor and the k-means algorithm.

The different processes will be applied on this kind of texture images:

(a) metal image



(b) sand image



(c) ground image



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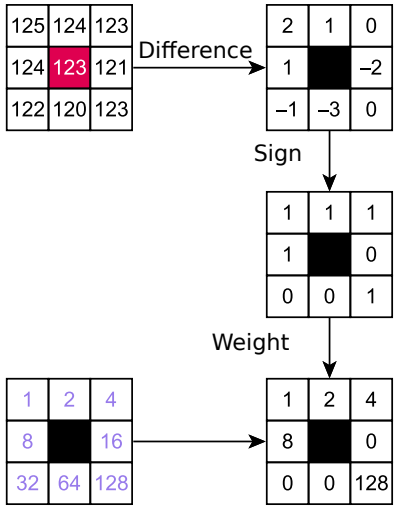
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39.1 Local Binary Patterns

The Local Binary Patterns (LBP) descriptor is a simple yet very efficient texture operator which labels the pixels of an image by thresholding the neighborhood of each pixel and considers the result as a binary number. Due to its discriminative power and computational simplicity, LBP texture operator has become a popular approach in various applications. It can be seen as a unifying approach to the traditionally divergent statistical and structural models of texture analysis. Perhaps the most important property of the LBP operator in real-world applications is its robustness to monotonic gray-scale changes caused, for example, by illumination variations. Another important property is its computational simplicity, which makes it possible to analyze images in challenging real-time settings.
The LBP feature vector, in its simplest form, is created in the following manner:

- For each pixel, compare the pixel to each of its 8 neighbors (on its left-top, left-middle, left-bottom, right-top, etc.). Follow the pixels along a circle, i.e. clockwise or counter-clockwise.
- Where the center pixel's value is greater than the neighbor's value, write "1". Otherwise, write "0". This gives an 8-digit binary number (which is usually converted to decimal for convenience).
- Compute the histogram of the frequency of each "number" occurring (i.e., each combination of which pixels are smaller and which are greater than the center).
- Normalize the histogram.

Figure 39.1 Local binary pattern. From wikipedia, author Xiawi, CC-By-SA.



>>>?

- Code a function for computing the Local Binary Patterns.
- Test this operator on a texture image from the given database.

Consider the function `numpy.histogram` for histogram computation.

39.2 Classification of texture images

The objective is to classify the texture images from the given databse by using the LBP descriptor.

>>>?

1. Calculate the LBP descriptor for each image of the database.
2. Compare the descriptors for each class of images.
3. Compute the distance between each pair of images in order to get a dissimilarity matrix. Comment the result.
4. Use the k-means algorithm to classify the images of the database into three classes ($k = 3$).

See `KMeans` from `sklearn.cluster`.

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39.3. Python correction

The following imports are used.

```
import numpy as np
from scipy import misc
import matplotlib.pyplot as plt
import glob
import seaborn as sn
import pandas as pd
import os
from sklearn.cluster import KMeans
```

39.3.1 LBP computation

Each pixel is given a specific 8 bits value according to a code as follows.

```
def LBP(I):
    B = np.zeros(np.shape(I));
    code = np.array([[1,2,4],[8,0,16],[32,64,128]]);

    # loop over all pixels except border pixels
    for i in np.arange(1,I.shape[0]-2):
        for j in np.arange(1, I.shape[1]-2):
            w = I[i-1:i+2, j-1:j+2];
            w = w >= I[i,j];
            w = w * code;
            B[i,j] = np.sum(w);
```

Then, all values (except for border values) are summarized in the histogram.

```
h,edges = np.histogram(B[1:-1, 1:-1], density=True, bins=256);
```

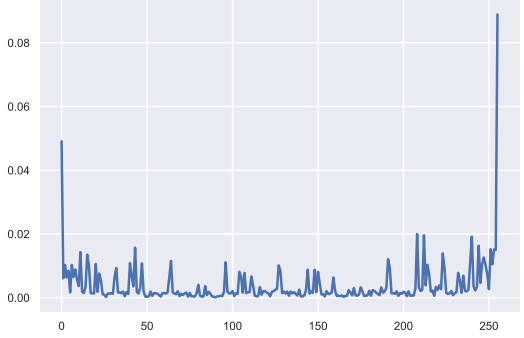
For the first image of sand, the histogram is shown in Fig.39.2.

Figure 39.2 Illustration of the Local Binary Pattern computed on an entire image.

(a) Texture image.



(b) LBP of texture.



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39.3.2 Classification

For all images of the same family, the LBP are computed and represented in the same graph. The histograms really look similar (see Fig.39.3). The following code is used for the "sand" family.

```
classes = ['Terrain', 'Metal', 'Sand'];
names = [];
hh = [];
for c in classes:
   print(c);
   fig=plt.figure();
   for file in sorted(glob.glob('../matlab/images/'+ c + '*.bmp')):
      names.append(os.path.basename(file));
      I = imageio.imread(file);
      I = I[:,:,1];
      h, edges = LBP(I);
      plt.plot(h);
      hh.append(h);
```

Figure 39.3 Illustration of the LBP of 4 images of each family. The histogram are almost equivalent, which shows that this descriptor can be employed to discriminate between the different families.

(a) Metal image example.



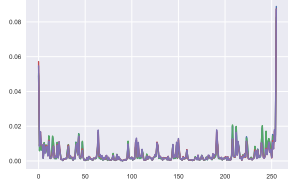
(b) Sand image example.



(c) Terrain image example.



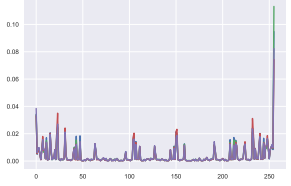
(d) Four metal images.



(e) Four sand images.



(f) Four terrain images.



A distance criterion is used to compare the different histograms: the classical SAD (Sum of Absolute Differences) gives a numerical values. All pairs of distances are concatenated in a matrix, displayed as an image in Fig.39.4.

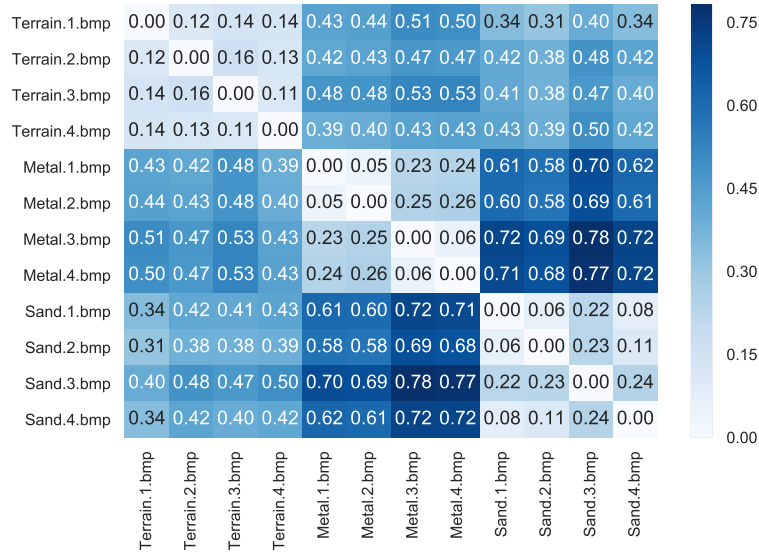
```
# compute distance between LBPs
n = len(hh);
dists = np.zeros((n, n))
for i in np.arange(n):
   for j in np.arange(n):
      dists[i,j] = np.sum(np.abs(hh[i]-hh[j]))
fig=plot_dists(dists, names);
```

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In order to display this matrix, the module seaborn is used.

```python
def plot_dists(dists, classes, cmap=plt.cm.Blues):
    """
    Plot matrix of distances
    dists: all computed distances
    classes: labels to be used
    cmap: colormap
    returns: figure that can be used for pdf export
    """
    df_cm = pd.DataFrame(dists, index = classes, columns = classes);
    fig = plt.figure();
    sn.set(font_scale=.8)
    sn.heatmap(df_cm, annot=True, cmap = cmap, fmt='.2f');
    return fig;
```

Figure 39.4 Sum of Absolute Differences between the different LBP histograms of each image. 3 families of 4 textures are represented here, terrain images are in the first part, metal images in the second and sand images in the last. Black represents 0 distance and white is 1 (highest distance, the values are normalized).



The kmeans algorithm uses such a distance, and we can verify that the clustering process works as expected. The result is presented in the next box.

```python
# kmeans clustering
n=3;
k_means = KMeans(init='k-means++', n_clusters=n, n_init=10)
k_means.fit(hh);
print(k_means.labels_)
```

The result show that the kmeans algorithm perfectly performs the classification.

```
[1 1 1 1 0 0 0 0 2 2 2 2]
```

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Sixth part

Exams

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40 Practical exam 2016

All printed documents allowed. Send your code via the campus website (zip files if several files are to be sent).

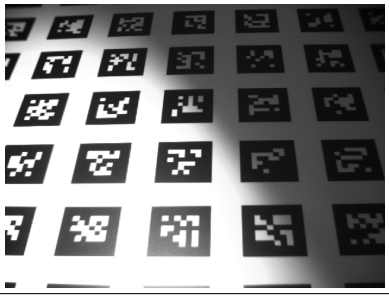
40.1 Segmentation (13 points)

>>>?

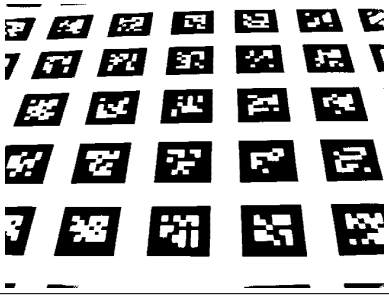
- Segment the image.

Figure 40.1 Test image

(a) Image to be segmented, from [4].



(b) Segmented image



40.2 Integral image (7 points)

If the original image is denoted f, the integral image I is defined by the following equation, for all pixels of coordinates (x, y):

$$I(x,y) = f(x,y) + I(x-1,y) + I(x,y-1) - I(x-1,y-1)$$

>>>?

- Code a function that computes this integral image. The prototype of this function must be `function II=int_image(I)`.
- Code a function that computes the local average of the image f. Notice that:

$$\sum_{x=x_1}^{x_2}\sum_{y=y_1}^{y_2} f(x,y) = I(x_2,y_2) - I(x_2,y_1-1) - I(x_1-1,y_2) + I(x_1-1,y_1-1)$$

- Compare it to a mean filter.

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41 Theoretical exam 2016

41.1 Basic notions

41.1.1 Image characterisation

>>>?

- Cite the names of the major image file formats and their main differences. What is DICOM?
- Define sampling in numerical images. Define the image resolution.

41.1.2 Sensors

>>>?

- What is a Bayer filter?
- Explain the principles of demosaicing.

41.1.3 Image processing

>>>?

- Define the operation of histogram equalization.
- What is the difference with histogram stretching?

>>>?

- From the mathematical definition of the derivative, explain the construction of the gradient operator, and then of the Laplacian.
- Cite some method for contours detection, and list their pros and cons.

41.2 Open question

>>>?

The Fig. 41.1 shows a human retina (eye fundus). Propose a method for segmenting:

- the vessels,
- the optical nerve (bright disk).

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Justify your choices. Indicate all elements that seem important and the way to deal with them. Look carefully at the shapes and intensities of objects you need to segment.
For your record, ophthalmologists need to measure the diameter and the circularity of the optical nerve, as well as the length and the number of vessels (branches, tortuosity...).

Figure 41.1 Human retina.

(a) Color image.



(b) Red channel.



(c) Green channel.



(d) Blue channel.



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42 Theoretical exam 2017

42.1 Warm-up questions

42.1.1 Thresholding methods

>>>?

Cite different methods in order to find a threshold value to binarize a grayscale image. Explain the Otsu's method. What are its limits?

42.1.2 Image filtering

>>>?

- What is the difference between a rank filter and a linear filter?
- Cite the name of a filter of each type.
- In case of a salt and pepper noise present in the image, what type of filter would you require to restore it? Why?
- For the latter, precise its limits and propose a way to improve the result.

42.1.3 Retina images

>>>?

As a project, you coded a method for retina vessels segmentation. Explain the principles of the algorithm.

42.2 Open question: QR code

A QR code is a binary code represented as a 2D matrix. A scanner is in charge of reading it (via a camera) and translating it into the actual code. The structure of a QR code is represented in Fig.42.1.

>>>?

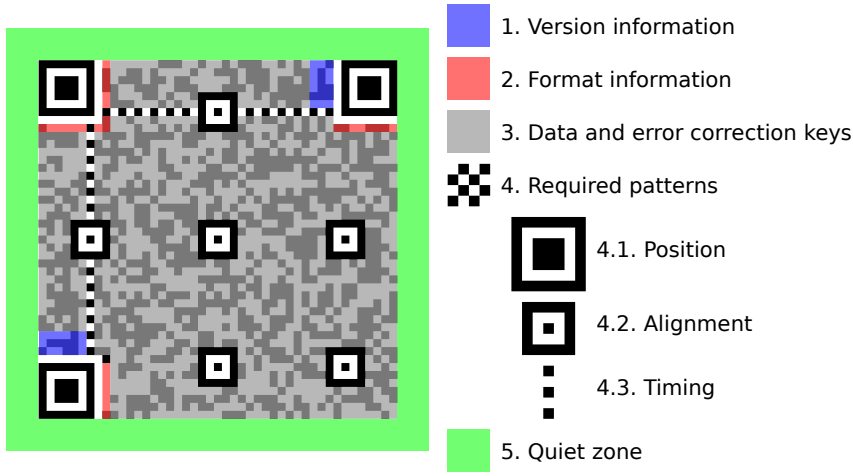
Describe the different steps required to perform the acquisition and geometric transformation of the QRcode into a binary 2D matrix representing the code (1 value for 1 square, see Fig.42.1).

- List different situations that may complicate the image acquisition and analysis.
- Propose some (image processing) solutions in order to deal with these situations. Explain them, give the necessary details describing the methods.

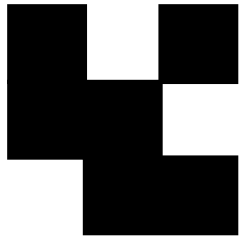
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Figure 42.1 Conversion of a binary pattern into a binary matrix.

(a) Structure of a QR code, Wikipedia, author: Bobmath, CC-By-SA



(b) Code.



(c) Matrix.

1	0	1
1	1	0
0	1	1

Figure 42.2 Different QR codes. The image acquisition and analysis must be tolerant to different observation conditions... Images from Collectif Raspouteam http://raspouteam.org/. Other images from unknown sources.



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Index

A

Aliasing 12, 20

C

Characterization 267, 273, 280, 287
- Circularity 268
- Convexity 268
- Diameter 268
- Perimeter 267

Classification 287, 298

Color
- Chromaticity diagram 87
- Color Matching Functions 86
- Color Spaces 85

Computational Geometry
- Convex Hull 243, 268
- Delaunay Triangulation 249
- Minimum Spanning Tree 249
- Voronoi Diagram 249

F

Features 287
- Detection 197
- Harris Corner Detector 293
- Local Binary Patterns 297

Filtering
- Choquet 94
- Convolution 13
- Degenerate Diffusion 105
- High-pass 13, 22
- Linear Diffusion 103
- Low-pass 13, 20
- Non Linear Diffusion 104
- Partial Differential Equations 103

Fourier Transform 37, 59
- 2D FFT 31
- Application 32
- Filtering 32
- Inverse 32, 60

Frameworks
- Color Logarithmic Image Processing 85
- General Adaptive Neighborhood Image Processing 93
- Logarithmic Image Processing 79

Freeman Chain Code 279

G

Geometry
- Crofton Perimeter 259
- Integral Geometry 257

Gradient
- Prewitt 14, 22
- Sobel 14, 22

H

Heat Equation 103

Histogram 12, 18
- Definition 24
- Equalization 24
- Matching 25

I

Image
- Display 11, 15
- Load 11, 15

L

Laplacian 13, 22

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M

Mapping 19
Mathematical Morphology 127, 191
  Alternate Sequential Filters 135
  Attribute Filters 141
  Dilation 128
  Erosion 128
  General Adaptive Neighborhood . . 95
  Geodesic Filtering 135
  Granulometry 151
  Hit-or-miss Transform 145
  Reconstruction 128, 136
  Skeleton 145
  Topological Skeleton 145
  Watershed 185
Multiscale 111
  Filtering 112
  Kramer & Bruckner 112
  Pyramid 111

N

Noise
  Exponential 49
  Gaussian 49
  Salt & Pepper 49
  Uniform 49

P

Point Spread Function 59

Q

Quantization 11, 17

R

Random Fields 225
Registration 195
Resizing 16
Restoration
  Adaptive median filter 50
  Blind deconvolution 63
  Deconvolution 59
  Lucy-Richardson filter 63
  Median filter 50
  Van Cittert filter 62
  Wiener filter 61

S

Segmentation 191
  Active Contours 179
  Distance Map 185
  Histogram 159
  Hough Transform 173
  K-means 159, 274, 298
  Otsu thresholding 160
  Region Growing 167
  Threshold 159
  Watershed 185
  Watershed by Markers 186
Shape From Focus 71
  SML 72
  Tenengrade 73
  Variance 73
  Variance of Tenengrad 73
Spatial Processes 207
  Boolean Models 219
  Characterization 210, 219
  Gibbs Point Process 208
  Marked Process 211
  Miles Formula 220
  Neyman-Scott Point Process 208
  Poisson Point Process 207
  Ripley Functions 210
Stereology 231
  Random Chords 232
  Random Planes 234

T

Tomography 119
  Backprojection 120
  Filtered Backprojection 120
Topology
  Classification 264
  Neighborhood 257, 263, 279

W

Wavelets
  Definition 37

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Bibliography

[1] http://vision.lems.brown.edu/content/available-software-and-databases. (*cf.* pp. 267, 270, 273, and 287).

[2] R. J. Adler. *The Geometry of Random Fields*. Wiley, Chichester, UK, June 1981. (*cf.* p. 225).

[3] O. S. Ahmad. *Stochastic representation and analysis of rough surface topography by random fields and integral geometry – Application to the UHMWPE cup involved in total hip arthroplasty*. PhD thesis, École Nationale Supérieure des Mines de Saint-Etienne, 2013. (*cf.* p. 225).

[4] D. Bradley and G. Roth. Adaptive thresholding using the integral image. *Journal of graphics tools*, 12(2):13–21, 2007. (*cf.* p. 305).

[5] F. Catté, P.-L. Lions, J.-M. Morel, and T. Coll. Image Selective Smoothing and Edge Detection by Nonlinear Diffusion. *SIAM Journal on Numerical Analysis*, 29(1):182–193, 1992. (*cf.* p. 104).

[6] M. Couprie and G. Bertrand. Discrete topological transformations for image processing. In *Digital Geometry Algorithms*, pages 73–107. Springer, 2012. (*cf.* p. 263).

[7] M. Fernandes, Y. Gavet, and J.-C. Pinoli. Improving focus measurements using logarithmic image processing. *Journal of Microscopy*, 242(3):228–241, 2010. (*cf.* pp. 71 and 73).

[8] M. Fernandes, Y. Gavet, and J.-C. Pinoli. Robust 3-D reconstruction of surfaces from image focus by local cross-sectional multivariate statistical analyses: Application to human *ex vivo* corneal endotheliums. *Medical Image Analysis*, 16(6):1293–1306, 2012. (*cf.* pp. 71 and 73).

[9] Y. Gavet, J. Debayle, and J.-C. Pinoli. The Color Logarithmic Image Processing (CoLIP) Antagonist Space. In *Color Image and Video Enhancement*, pages 155–182. Springer International Publishing, 2015. (*cf.* p. 85).

[10] Y. Gavet, J. Debayle, and J.-C. Pinoli. The Color Logarithmic Image Processing (CoLIP) Antagonist Space and Chromaticity Diagram. In *International Workshop on Computational Color Imaging*, pages 131–138. Springer International Publishing, 2015. (*cf.* p. 85).

[11] R. C. Gonzalez and R. E. Woods. *Digital Image Processing*. Pearson, 2007. (*cf.* pp. 50 and 57).

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[12] H. Gouinaud. *Traitement logarithmique d'images couleur*. PhD thesis, Ecole Nationale Supérieure des Mines de Saint-Etienne, 2013. (*cf.* p. 85).

[13] H. Gouinaud, Y. Gavet, J. Debayle, and J.-C. Pinoli. Color correction in the framework of color logarithmic image processing. In *Image and Signal Processing and Analysis (ISPA), 2011 7th International Symposium on*, pages 129–133. IEEE, 2011. (*cf.* p. 85).

[14] E. Grisan, A. Paviotti, N. Laurenti, and A. Ruggeri. A lattice estimation approach for the automatic evaluation of corneal endothelium density. In *Engineering in Medicine and Biology Society, 2005. IEEE-EMBS 2005. 27th Annual International Conference of the*, pages 1700–1703, 2005. (*cf.* p. 36).

[15] F. C. Groen, I. T. Young, and G. Ligthart. A comparison of different focus functions for use in autofocus algorithms. *Cytometry*, 6(2):81–91, 1985. (*cf.* p. 73).

[16] M. Jourlin and J. C. Pinoli. Logarithmic image processing. *Acta Stereologica*, 6:651–656, 1987. (*cf.* p. 79).

[17] M. Jourlin and J.-C. Pinoli. Image Dynamic Range Enhancement and Stabilization in the Context of the Logarithmic Image Processing Model. *Signal Process.*, 41(2):225–237, Jan. 1995. (*cf.* p. 80).

[18] M. Kass, A. Witkin, and D. Terzopoulos. Snakes: Active contour models. *International journal of computer vision*, 1(4):321–331, 1988. (*cf.* p. 179).

[19] J. Koenderink. The structure of images. *Biological Cybernetics*, 50(5):363–370, 1984. (*cf.* p. 104).

[20] H. P. Kramer and J. B. Bruckner. Iterations of a non-linear transformation for enhancement of digital images. *Pattern Recognition*, 7(1):53 – 58, 1975. (*cf.* p. 112).

[21] E. Krotkov. Focusing. *International Journal of Computer Vision*, 1(3):223–237, 1988. (*cf.* p. 73).

[22] A. Lang and J. Potthoff. Fast simulation of Gaussian random fields. *Monte Carlo Methods and Applications*, 17(3):195–214, 2011. (*cf.* p. 225).

[23] P. Maragos and M. Akmal Butt. Partial differential equations in image analysis: continuous modeling, discrete processing. In *Image Processing, 1996. Proceedings., International Conference on*, volume 3, pages 61–64 vol.3, Sep 1996. (*cf.* p. 105).

[24] G. Marsaglia. Choosing a Point from the Surface of a Sphere. *Ann. Math. Statist.*, 43(2):645–646, 04 1972. (*cf.* p. 234).

[25] S. K. Nayar and Y. Nakagawa. Shape from focus. *Pattern analysis and machine intelligence, IEEE Transactions on*, 16(8):824–831, 1994. (*cf.* p. 72).

[26] N. Otsu. A Threshold Selection Method from Gray-Level Histograms. *Systems, Man and Cybernetics, IEEE Transactions on*, 9(1):62–66, Jan 1979. (*cf.* p. 160).

[27] P. Perona and J. Malik. Scale-space and edge detection using anisotropic diffusion. *Pattern Analysis and Machine Intelligence, IEEE Transactions on*, 12(7):629–639, Jul 1990. (*cf.* p. 104).

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[28] J. C. Pinoli. *Contribution à la modélisation, au traitement et à l'analyse d'image.* PhD thesis, Département de Mathématiques, Université de Saint-Etienne, France, 1987. (*cf.* p. 79).

[29] J. C. Pinoli. The logarithmic image processing model: Connections with human brightness perception and contrast estimators. *Journal of Mathematical Imaging and Vision*, 7(4):341–358, Oct. 1997. (*cf.* p. 79).

[30] S. Rivollier, J. Debayle, and J.-C. Pinoli. Shape diagrams for 2d compact sets-part i: analytic convex sets. australian journal of. *The Australian Journal of Mathematical Analysis and applications*, 7(2), 2010. (*cf.* p. 273).

[31] S. Rivollier, J. Debayle, and J.-C. Pinoli. Shape diagrams for 2d compact sets-part ii: analytic simply connected sets. *The Australian Journal of Mathematical Analysis and applications*, 7(2), 2010. (*cf.* p. 273).

[32] S. Rivollier, J. Debayle, and J.-C. Pinoli. Shape diagrams for 2d compact sets-part iii: convexity discrimination for analytic and discretized simply connected sets. *The Australian Journal of Mathematical Analysis and applications*, 7(2), 2010. (*cf.* p. 273).

[33] A. Ruggeri, E. Grisan, and J. Jaroszewski. A new system for the automatic estimation of endothelial cell density in donor corneas. *Br J Ophthalmol*, 89(3):306–311, 2005. (*cf.* p. 36).

[34] A. Ruggeri, E. Grisan, and J. Schroeter. Evaluation of repeatability for the automatic estimation of endothelial cell density in donor corneas. *Br J Ophthalmol*, 0, 2007. (*cf.* p. 36).

[35] J. C. Russ and R. T. Dehoff. *Practical Stereology.* Kluwer Academic, 2nd edition, 2000. (*cf.* p. 231).

[36] D. Sage, L. Donati, F. Soulez, D. Fortun, G. Schmit, A. Seitz, R. Guiet, C. Vonesch, and M. Unser. Deconvolutionlab2: An open-source software for deconvolution microscopy. *Methods*, 115:28 – 41, 2017. Image Processing for Biologists. (*cf.* p. 59).

[37] B. Selig, K. A. Vermeer, B. Rieger, T. Hillenaar, and C. L. Luengo Hendriks. Fully automatic evaluation of the corneal endothelium from in vivo confocal microscopy. *Biomed central*, 2015. (*cf.* pp. 32 and 36).

[38] J. Serra. *Image Analysis and Mathematical Morphology.* London: academic press, 1982. (*cf.* p. 127).

[39] D. Sharvit, J. Chan, H. Tek, and B. B. Kimia. Symmetry-based indexing of image databases. In *Content-Based Access of Image and Video Libraries, 1998. Proceedings. IEEE Workshop on*, pages 56–62. IEEE, 1998. (*cf.* pp. 267, 273, and 287).

[40] P. Soille. *Morphological Image Analysis: Principles and Applications.* Springer-Verlag New York, Inc., Secaucus, NJ, USA, 2nd edition, 2003. (*cf.* pp. 127 and 151).

[41] S. A. Sugimoto and Y. Ichioka. Digital composition of images with increased depth of focus considering depth information. *Applied optics*, 24(14):2076–2080, 1985. (*cf.* p. 73).

[42] J. M. Tenenbaum. *Accommodation in computer vision.* PhD thesis, STANFORD UNIV CA DEPT OF COMPUTER SCIENCE, 1970. (*cf.* p. 73).

[43] K. Worsley. The geometry of random fields. *Chance*, 9(1):27–40, 1997. (*cf.* p. 225).

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